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(54) **TISSUE THICKNESS COMPENSATOR
COMPRISING STRUCTURE TO PRODUCE A
RESILIENT LOAD**

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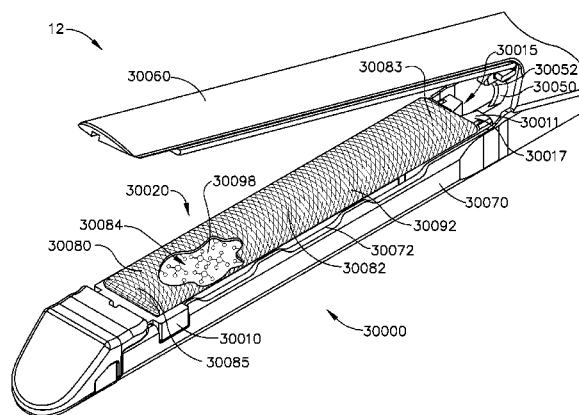
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(57) **ABSTRACT**

A fastener cartridge assembly for an end effector of a surgical
instrument can comprise a cartridge body, a deformable tube,
and a fastener moveable between an initial position and a fired
position. The deformable tube can be longitudinally posi-
tioned along a length of the cartridge body. When the fastener
is moved to the fired position, the fastener can compress a
portion of the deformable tube. The deformable tube can
comprise a resilient material such that deformation of the
deformable tube generates a restoring force. The deformable
tube can comprise a lattice of strands woven together to form
a tube wall. Further, the deformable tube can be bioabsorb-
able and can hold a therapeutic agent. The fastener cartridge
assembly can comprise multiple, substantially parallel
deformable tubes positioned side-by-side and/or within each
other.

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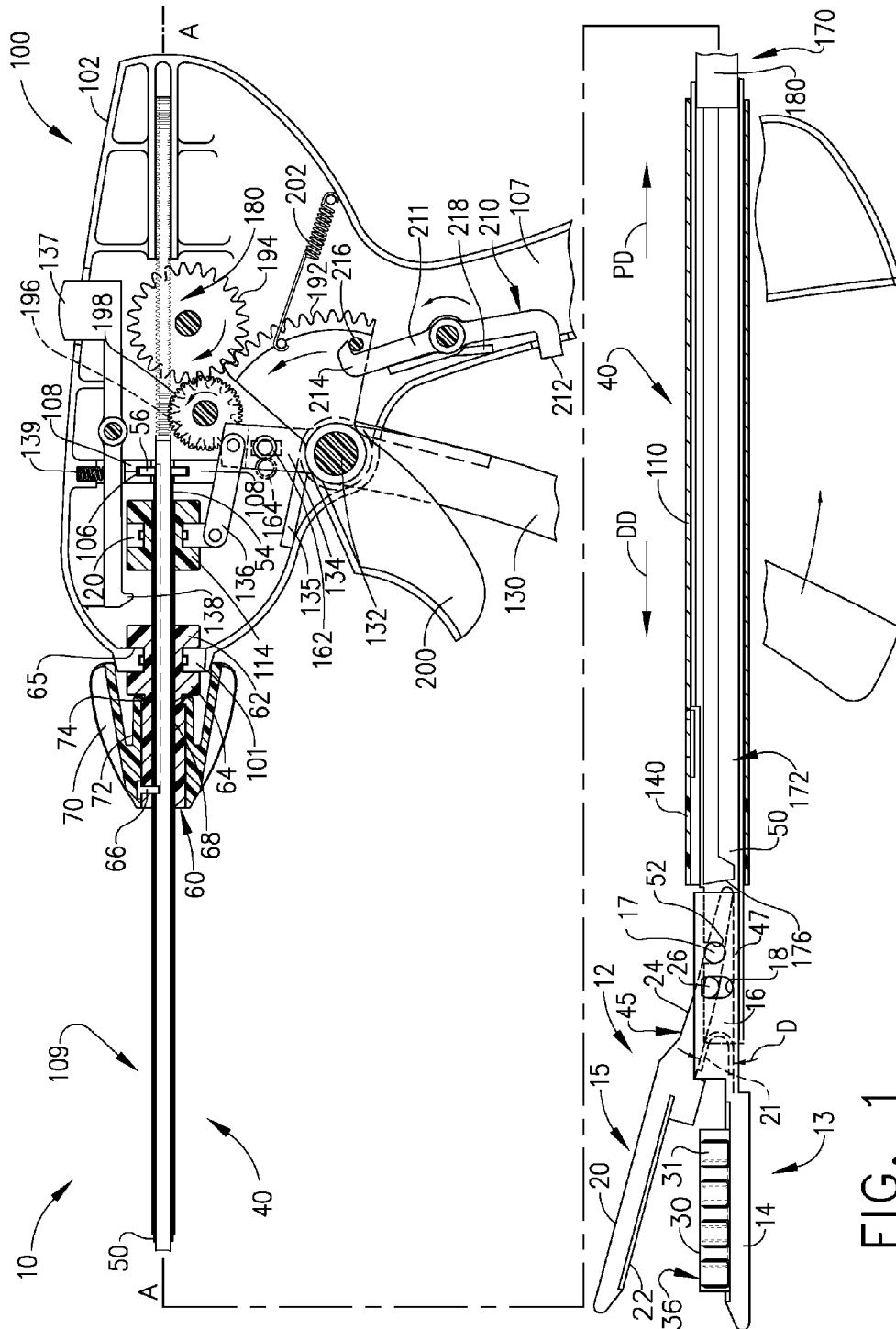
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U.S. Appl. No. 14/226,076, filed Mar. 26, 2014.
U.S. Appl. No. 14/226,111, filed Mar. 26, 2014.
U.S. Appl. No. 14/226,125, filed Mar. 26, 2014.

* cited by examiner



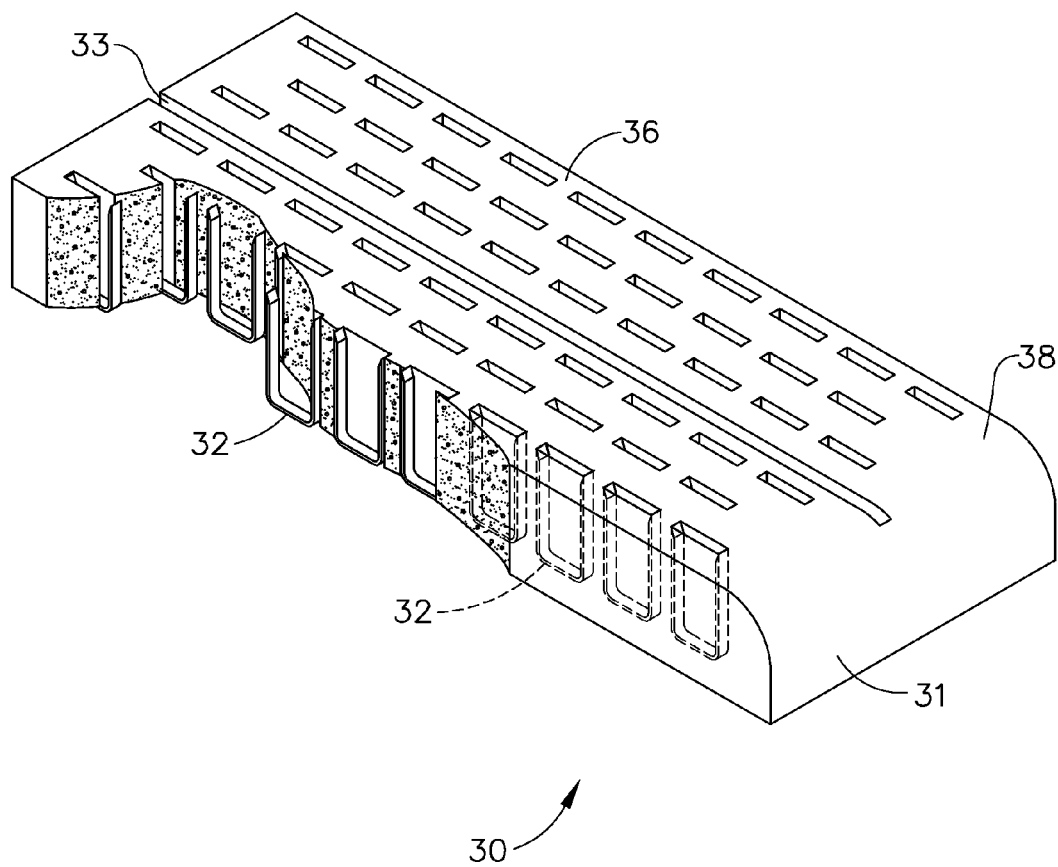


FIG. 1A

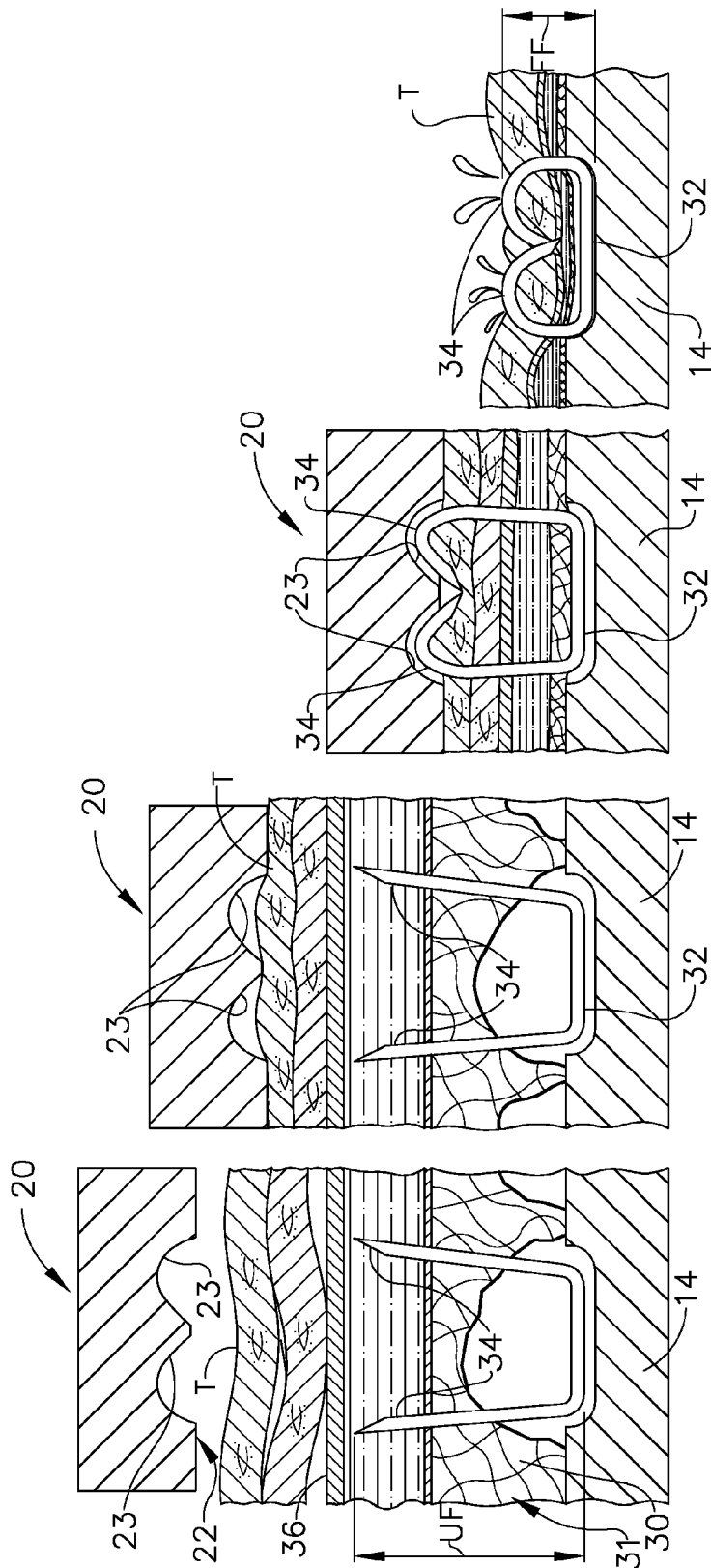


FIG. 1B FIG. 1C FIG. 1D FIG. 1E

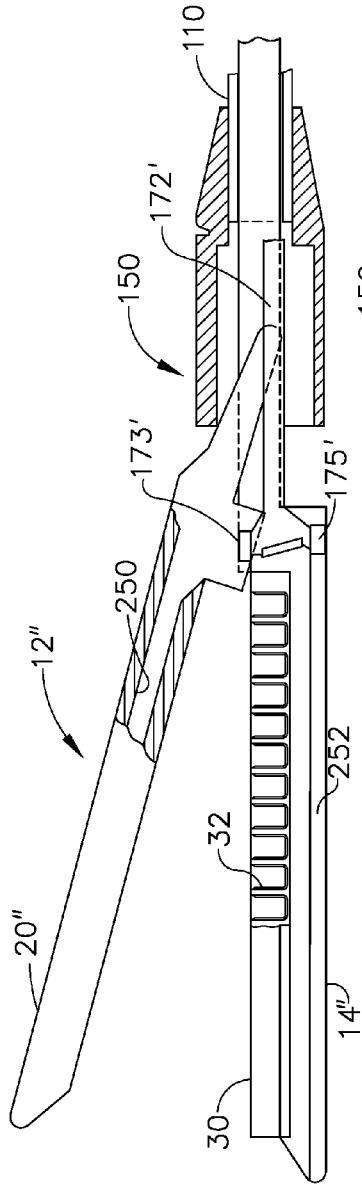


FIG. 2

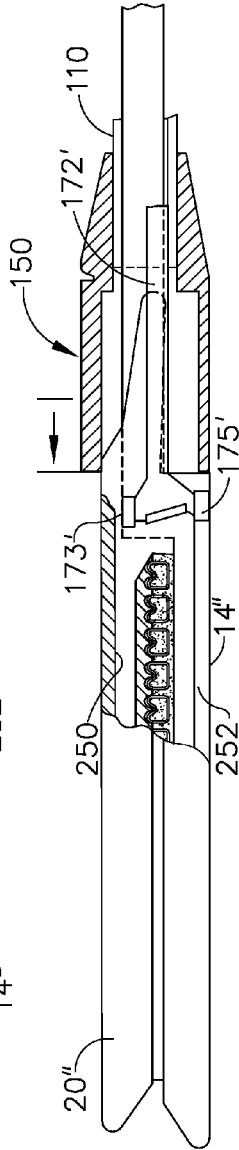


FIG. 3

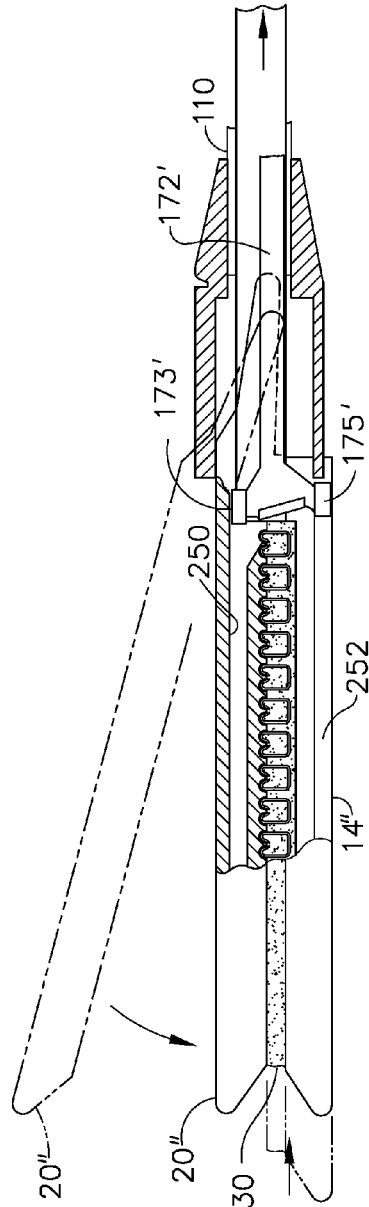


FIG. 4

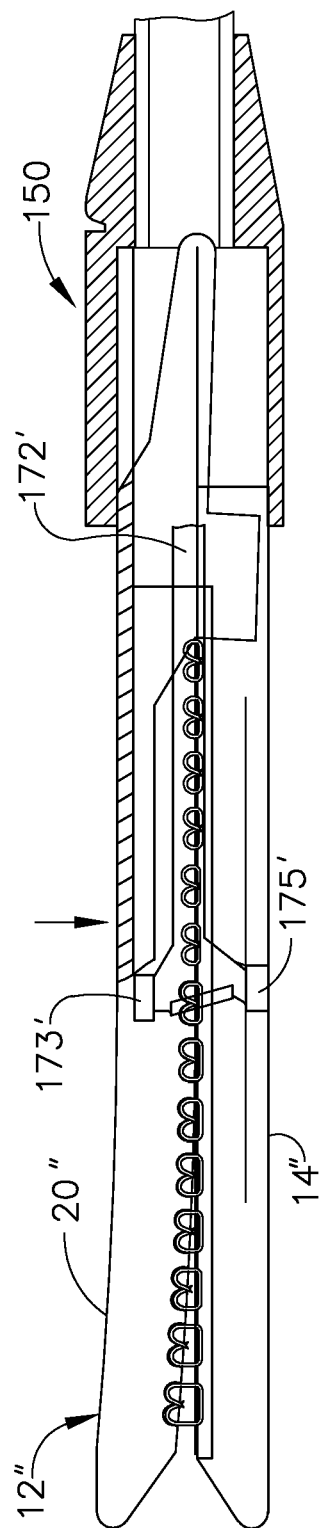
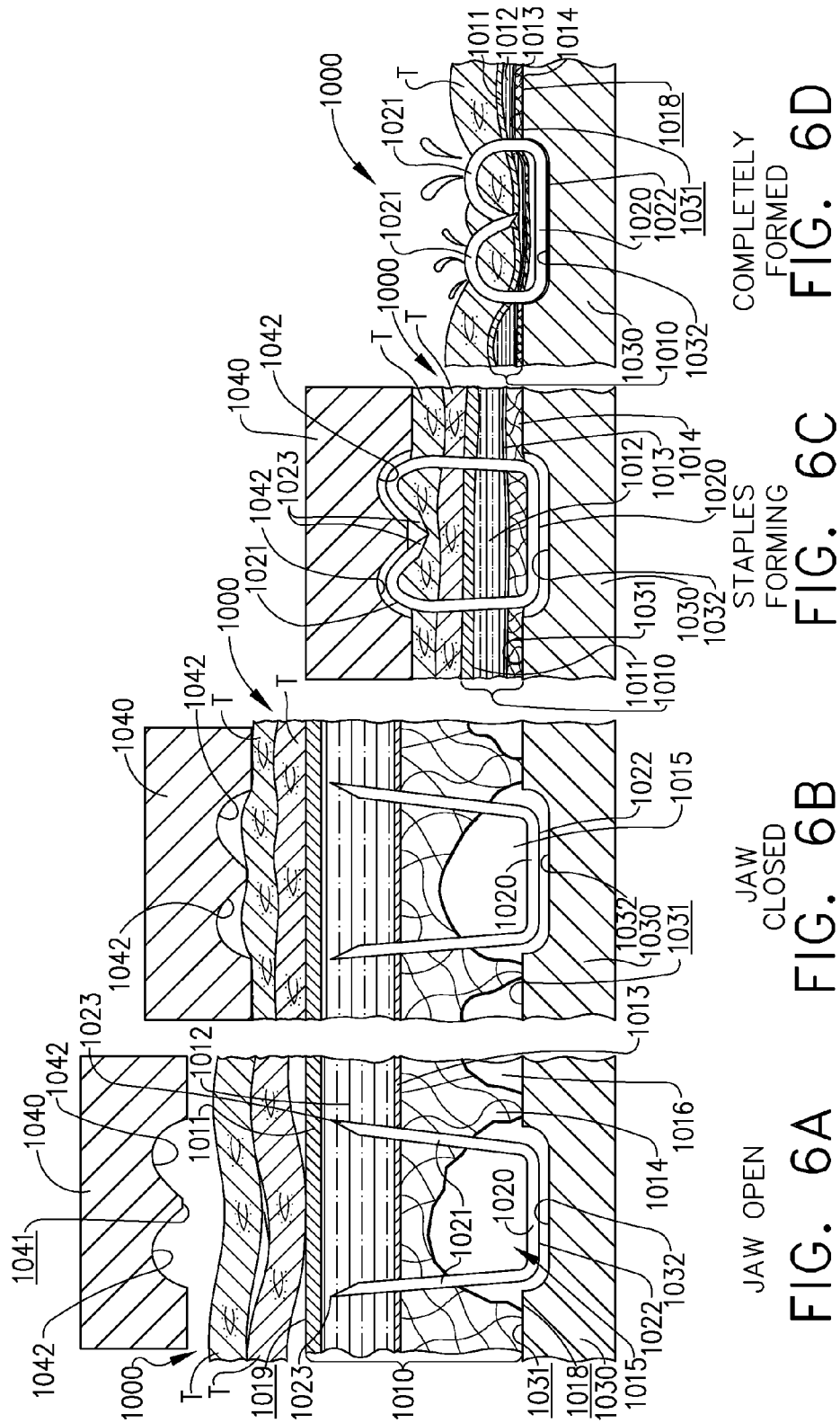


FIG. 5



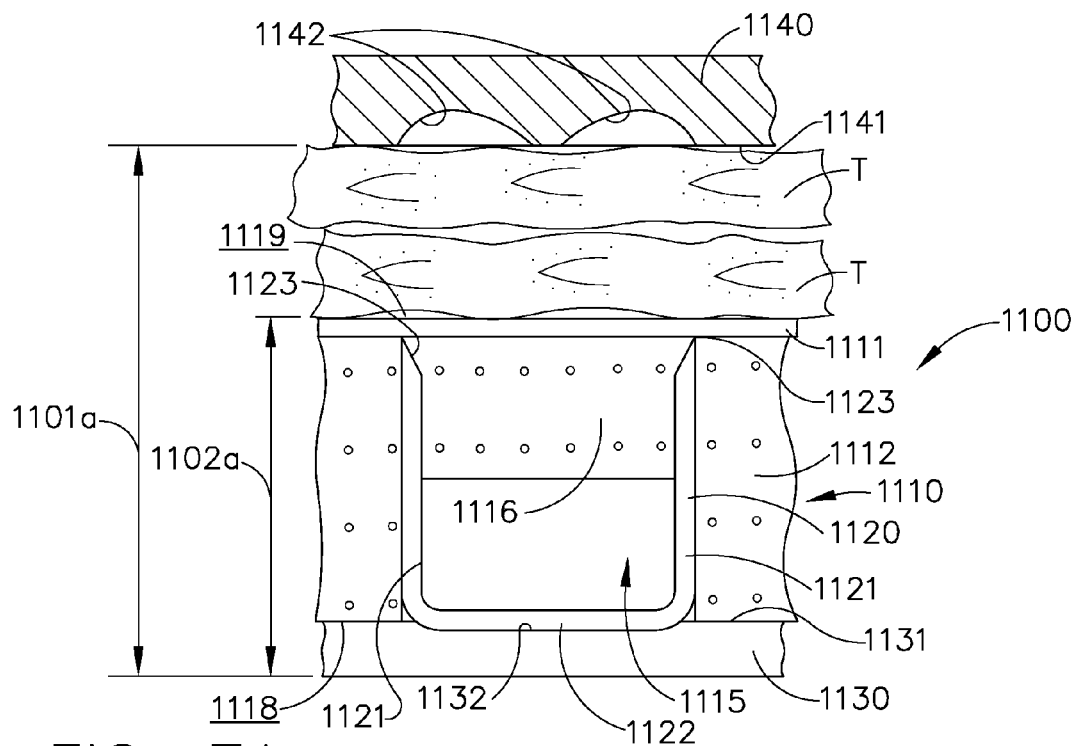


FIG. 7A

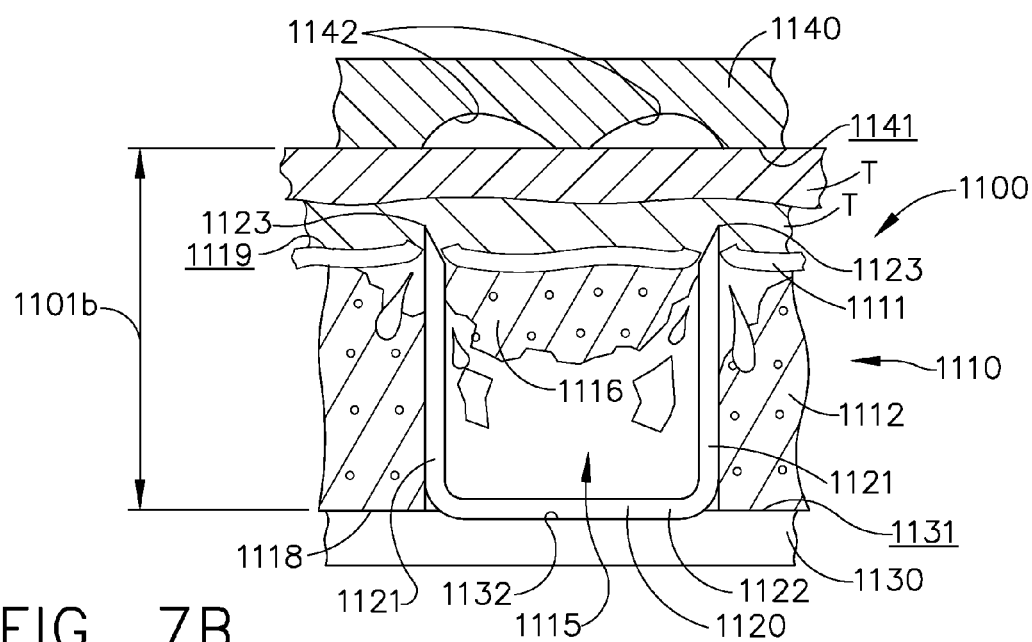


FIG. 7B

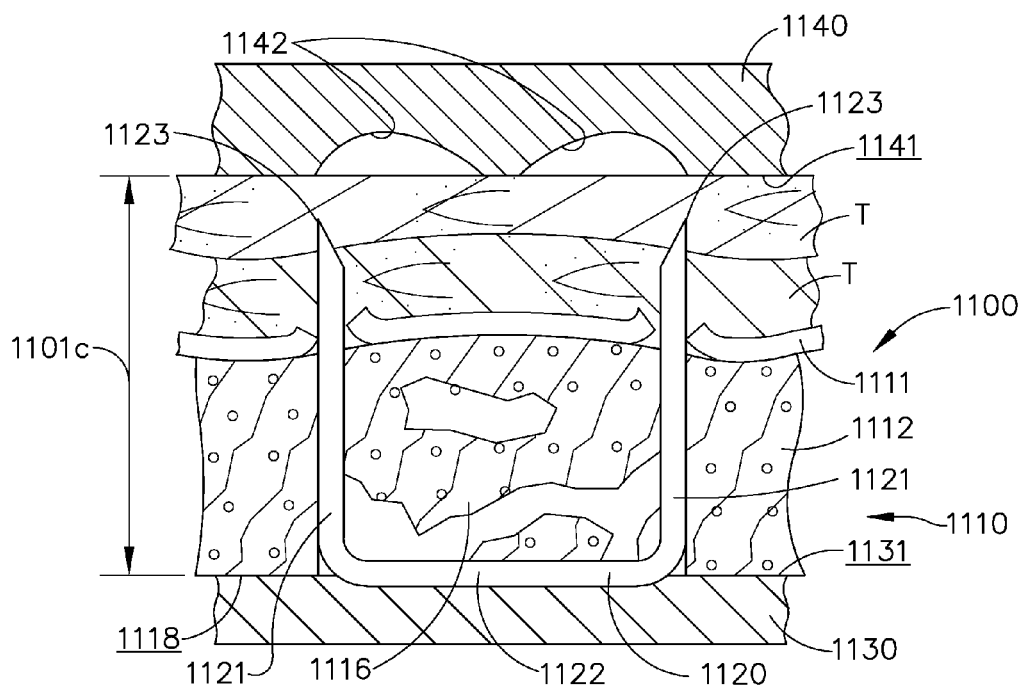


FIG. 7C

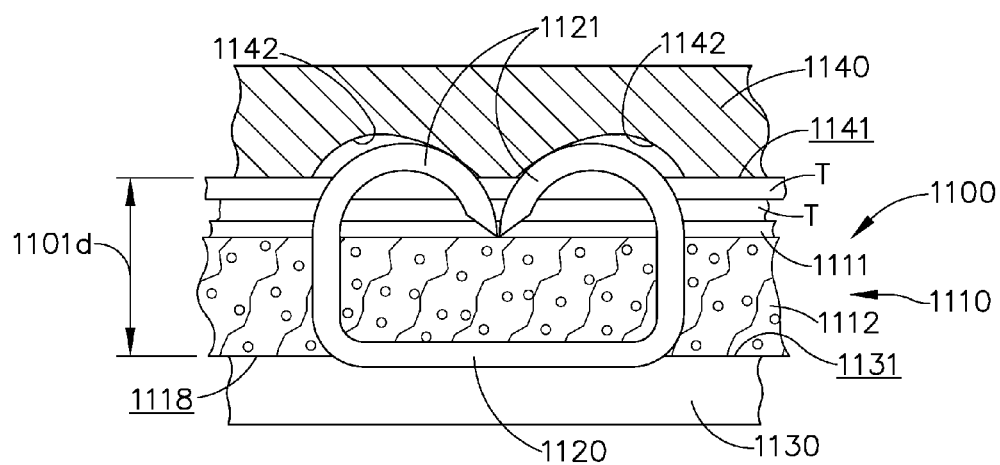


FIG. 7D

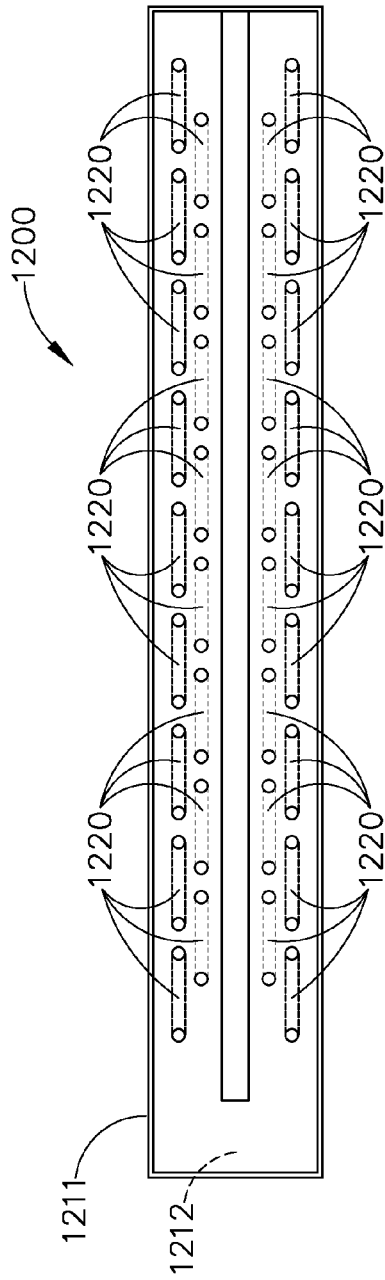


FIG. 8

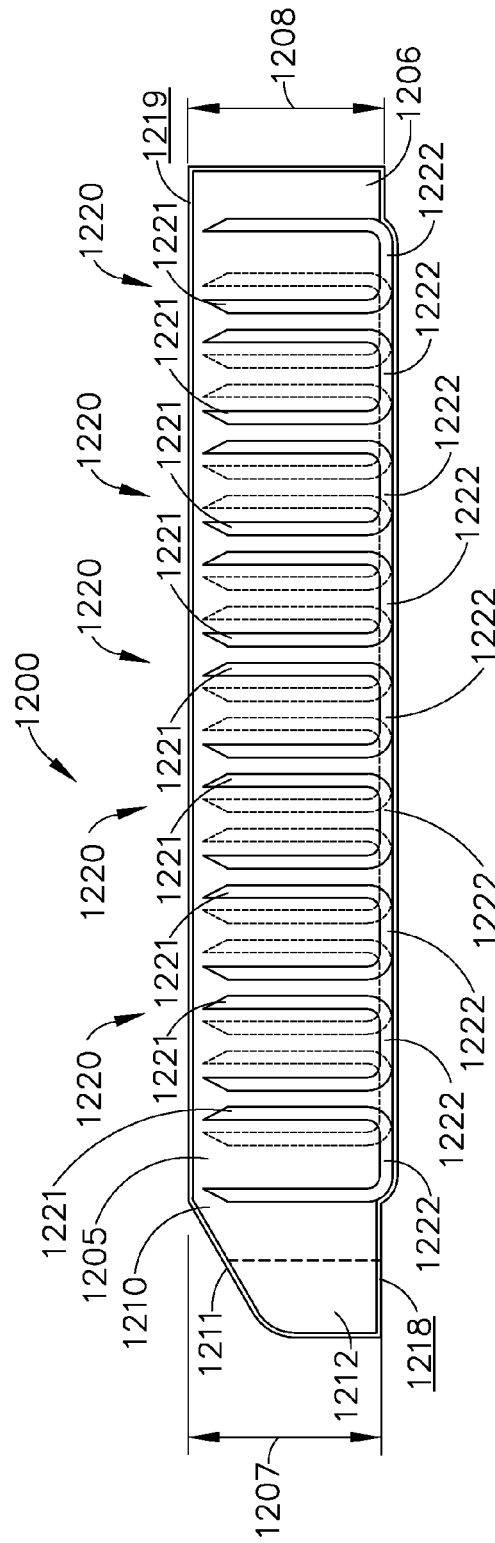


FIG. 9

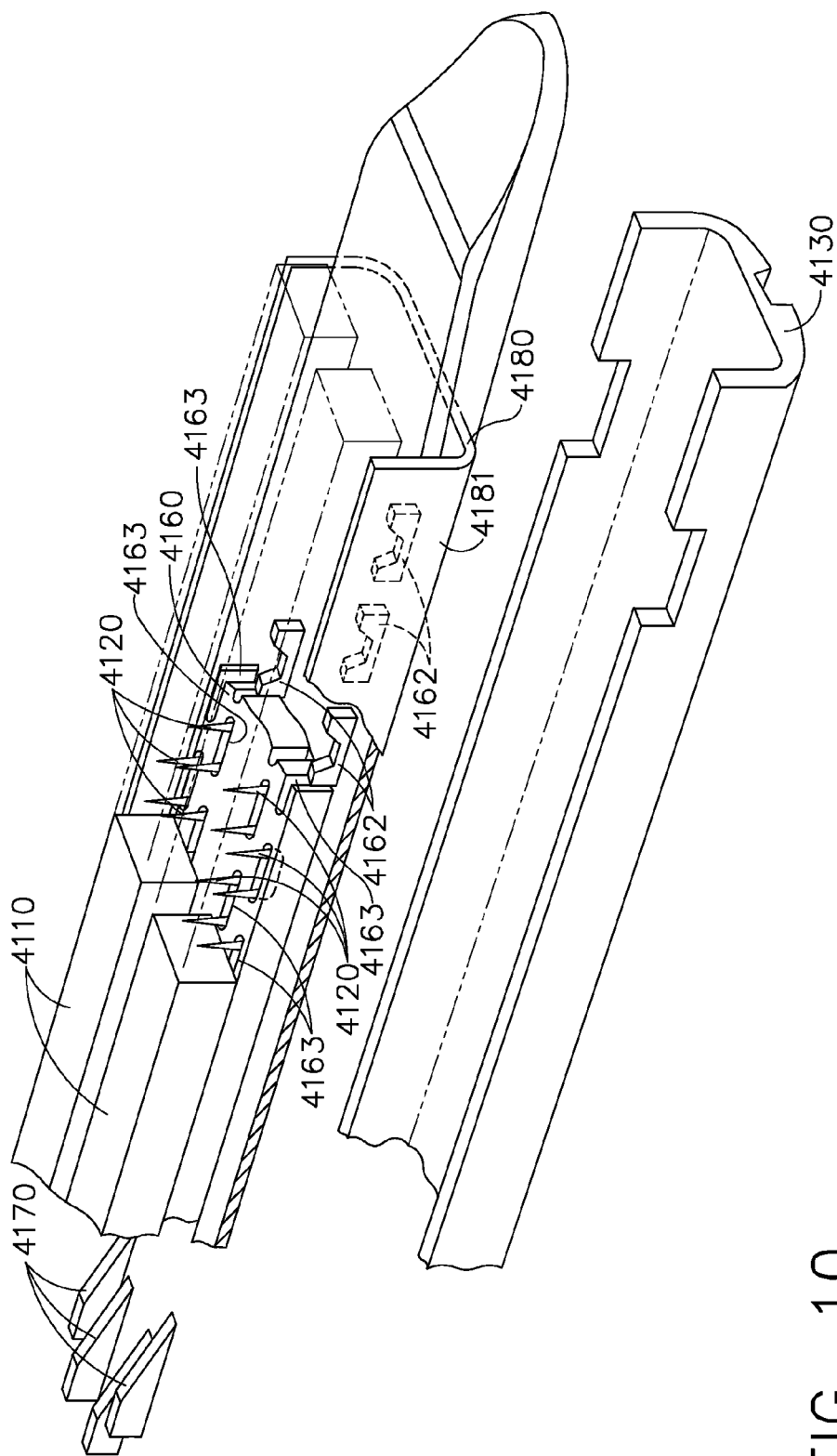


FIG. 10

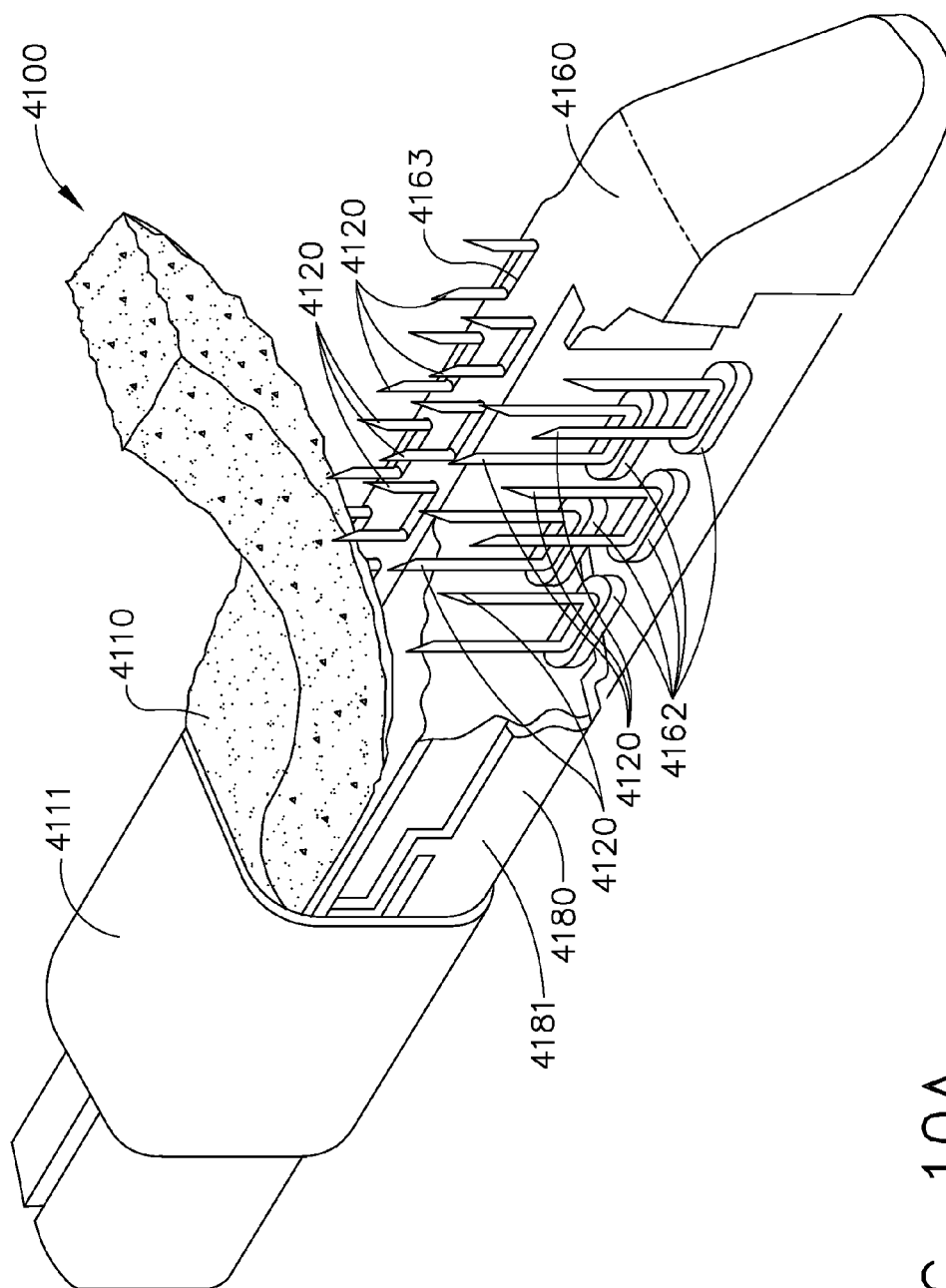


FIG. 10A

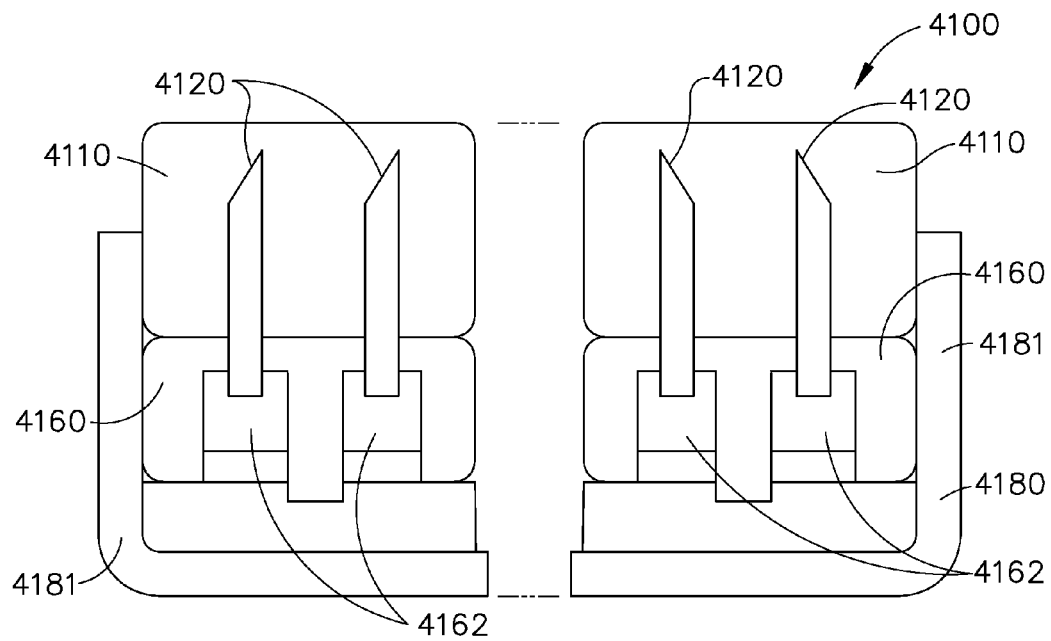


FIG. 11



FIG. 12

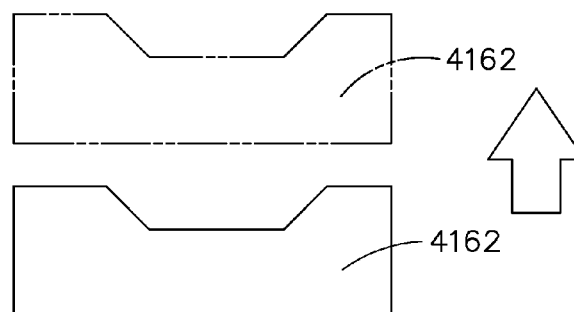


FIG. 13

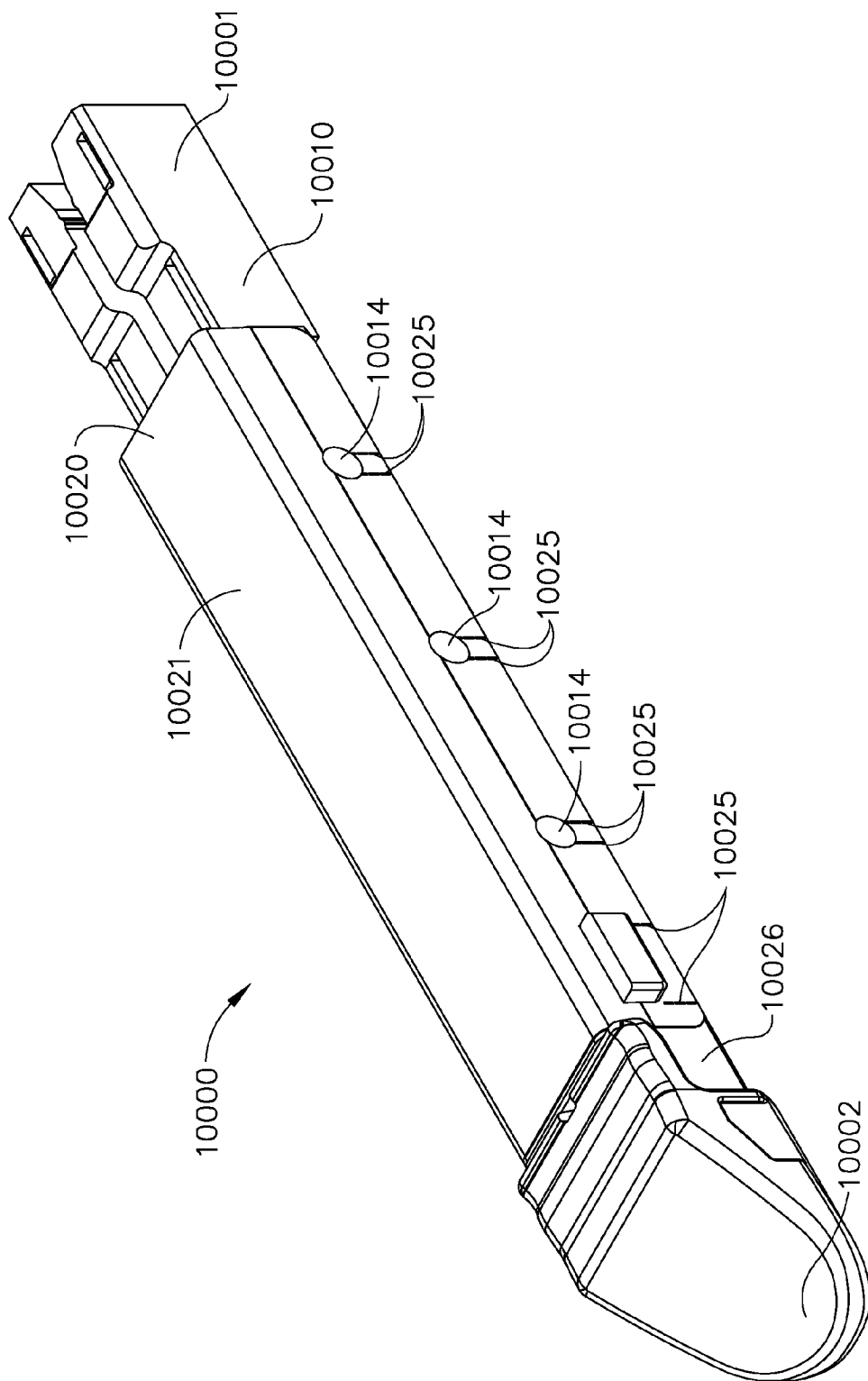
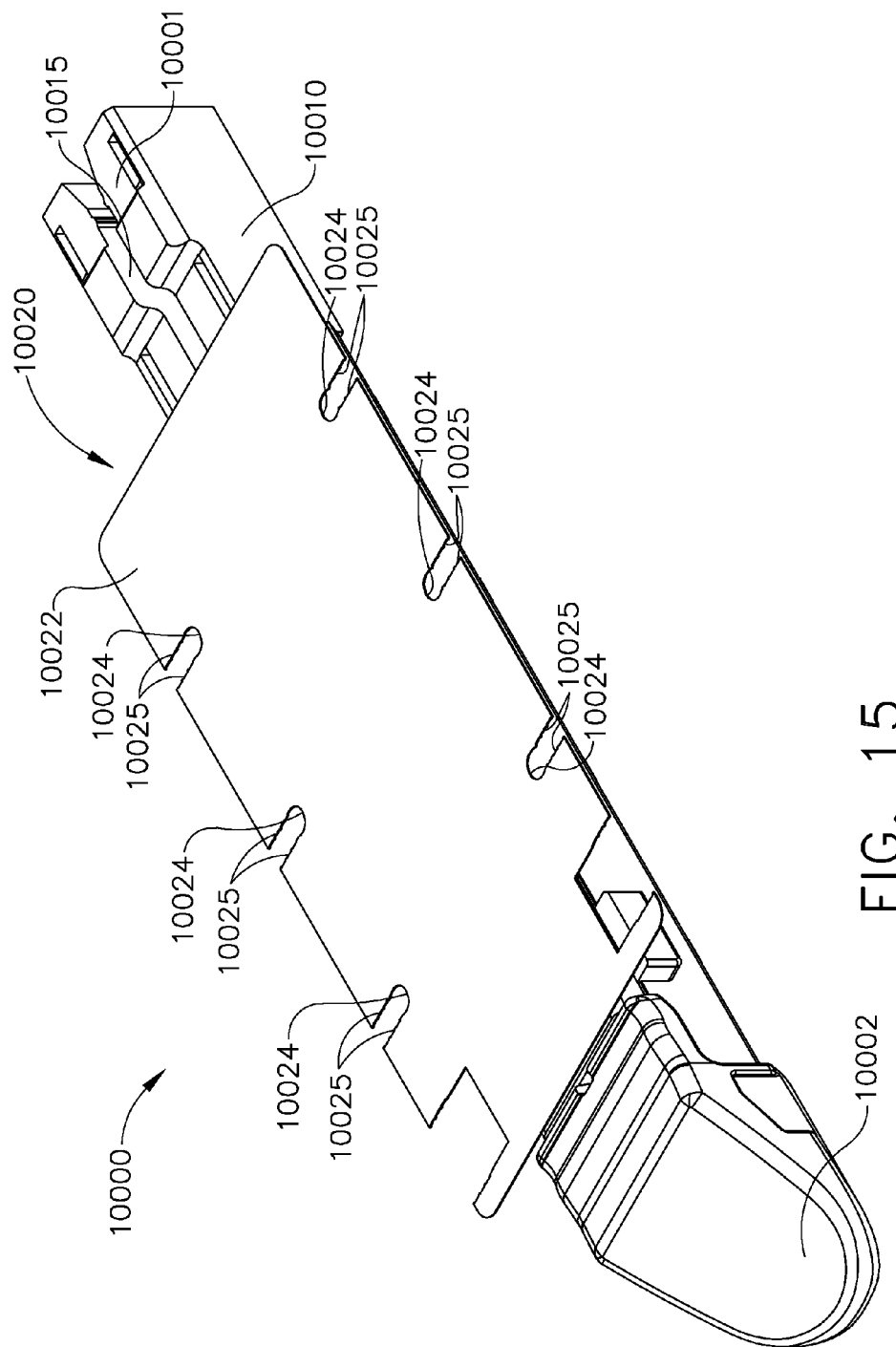


FIG. 14



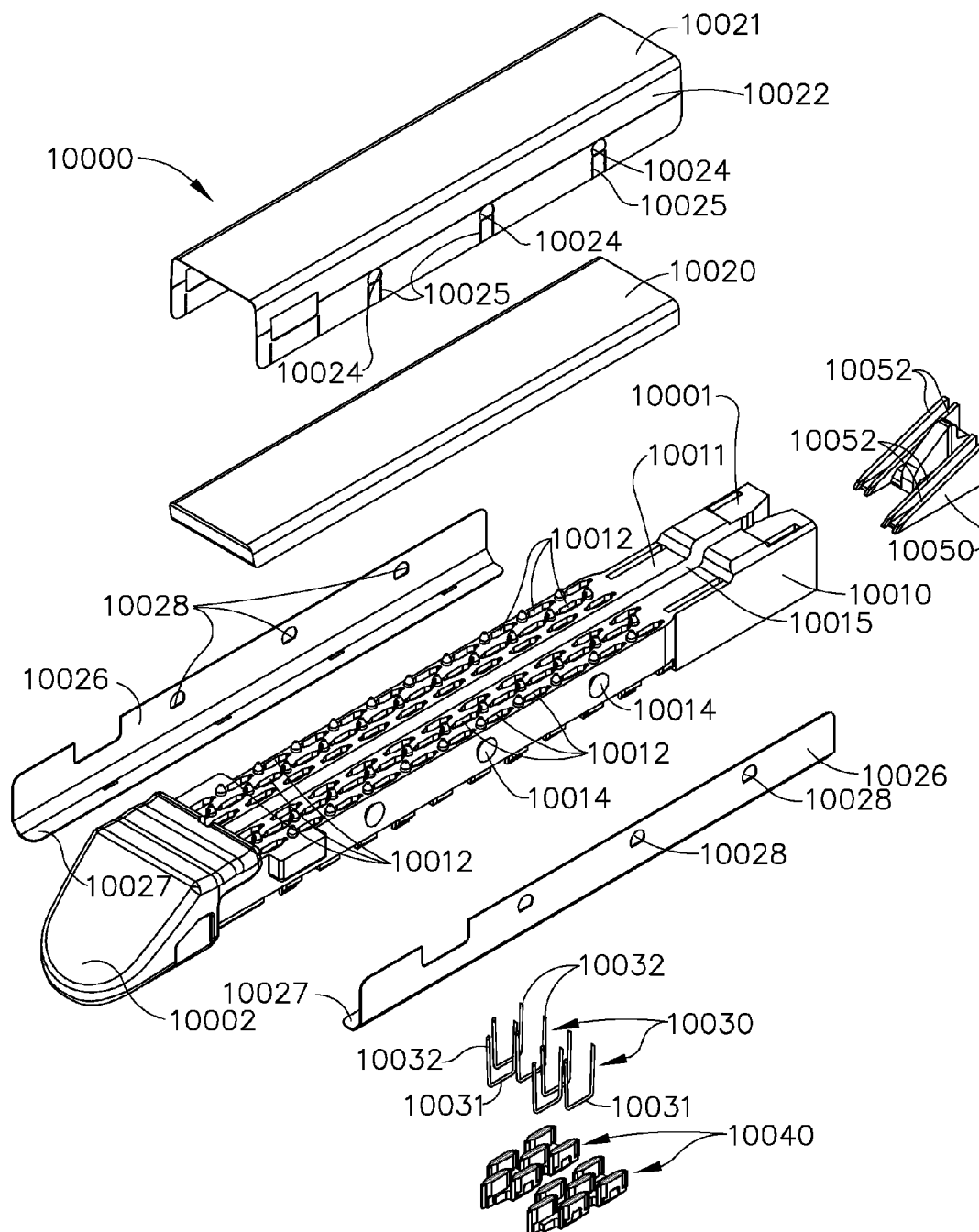


FIG. 16

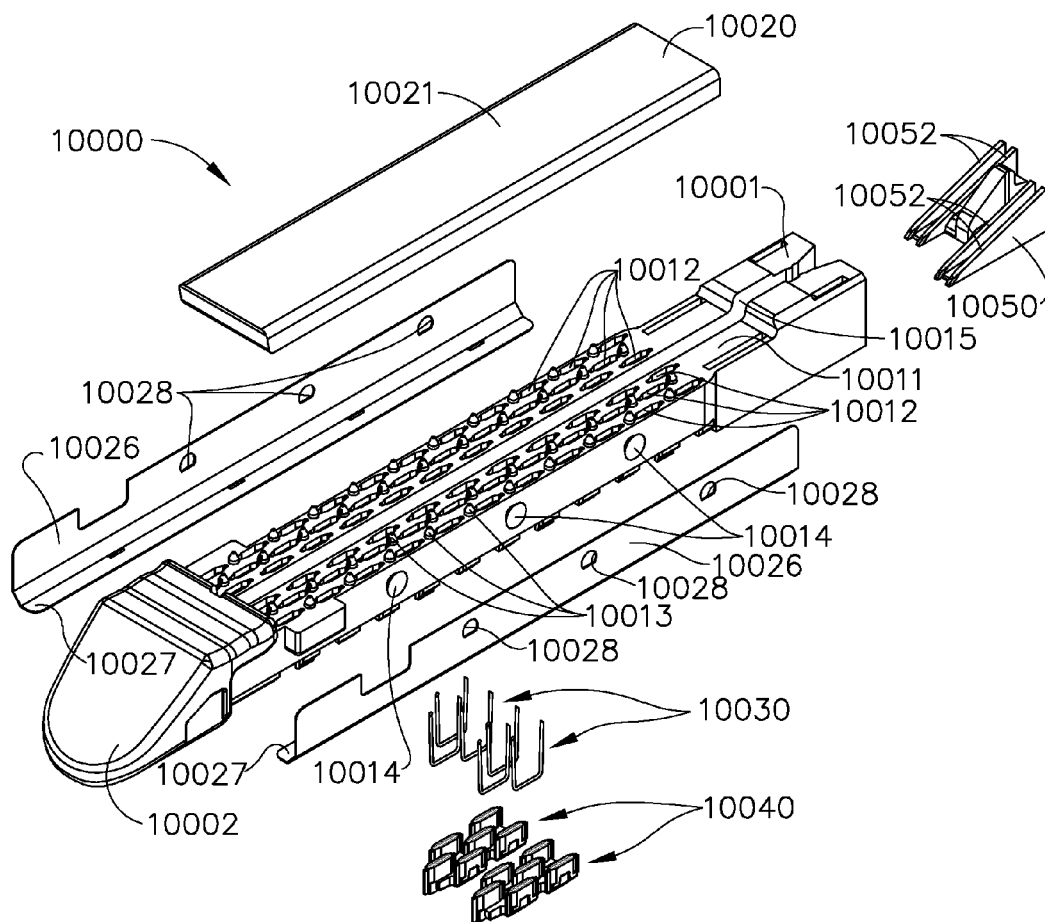


FIG. 17

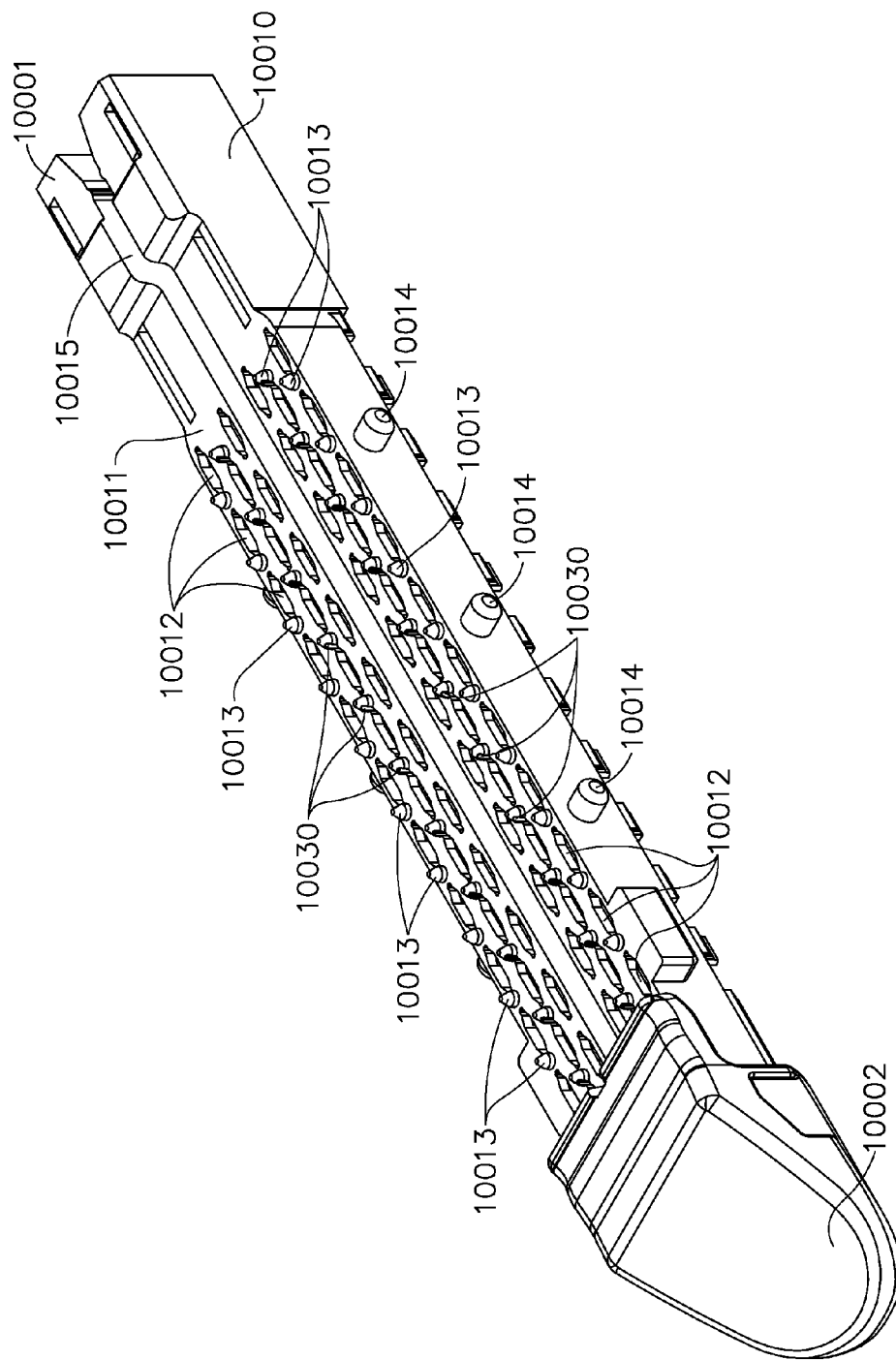


FIG. 18

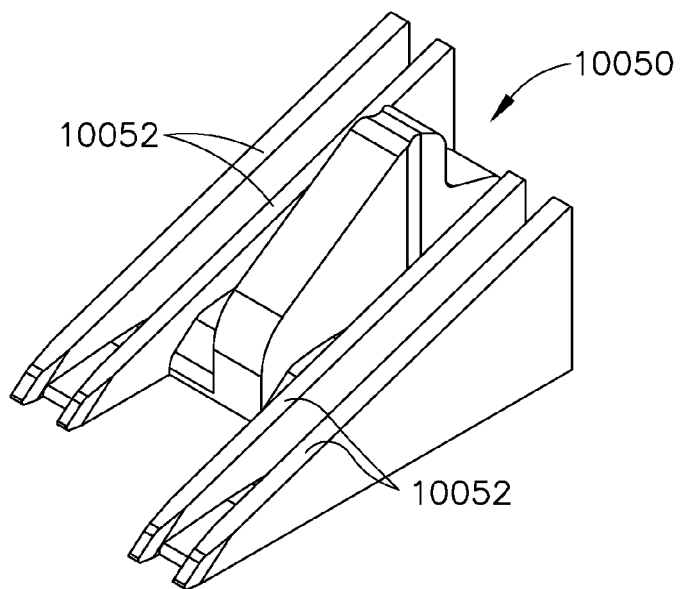


FIG. 19

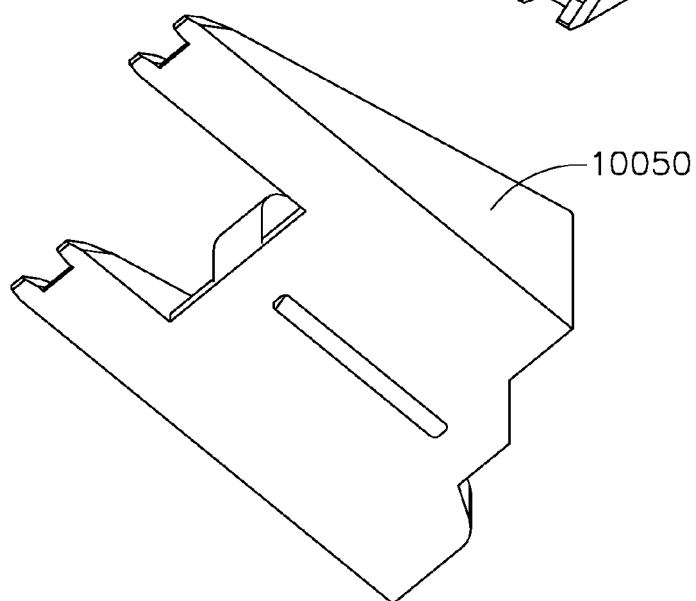


FIG. 20

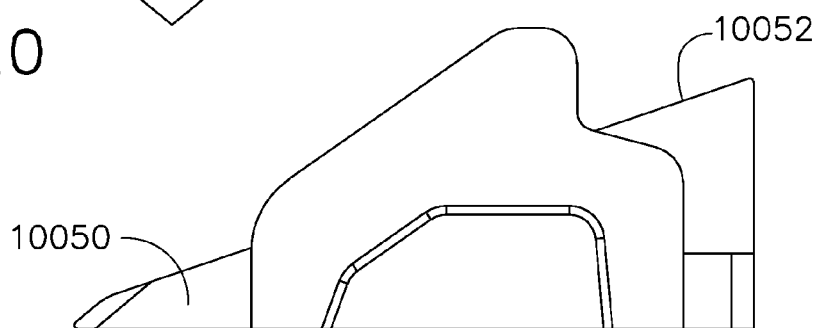


FIG. 21

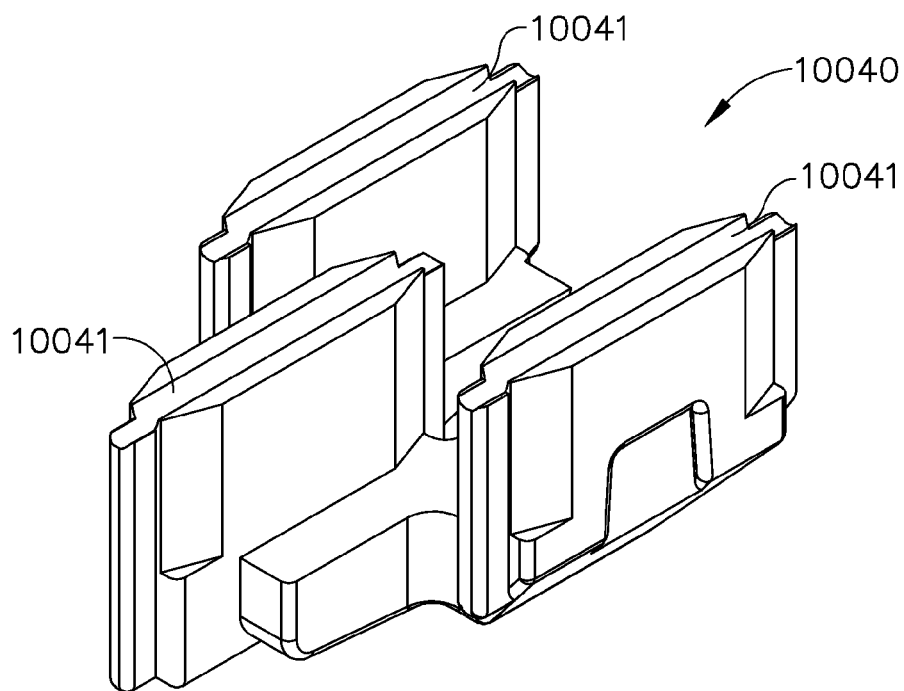


FIG. 22

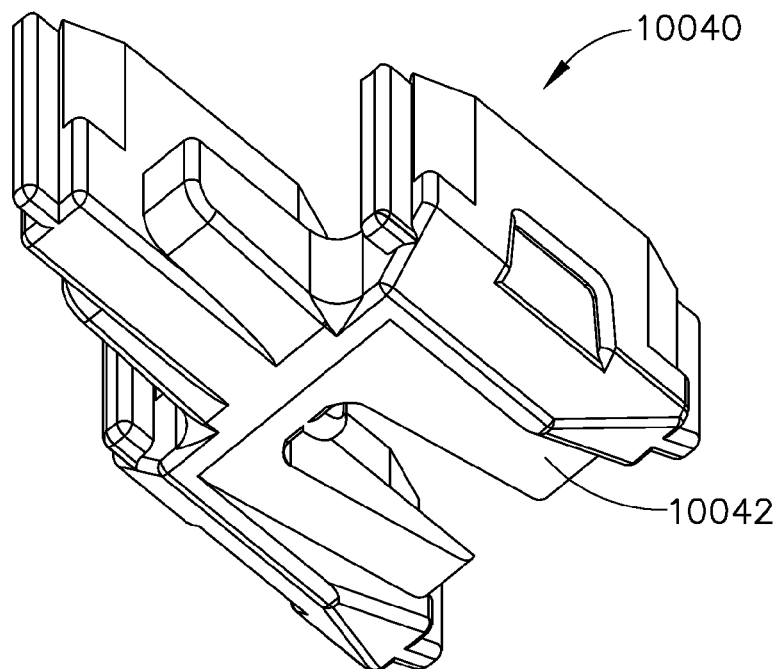


FIG. 23

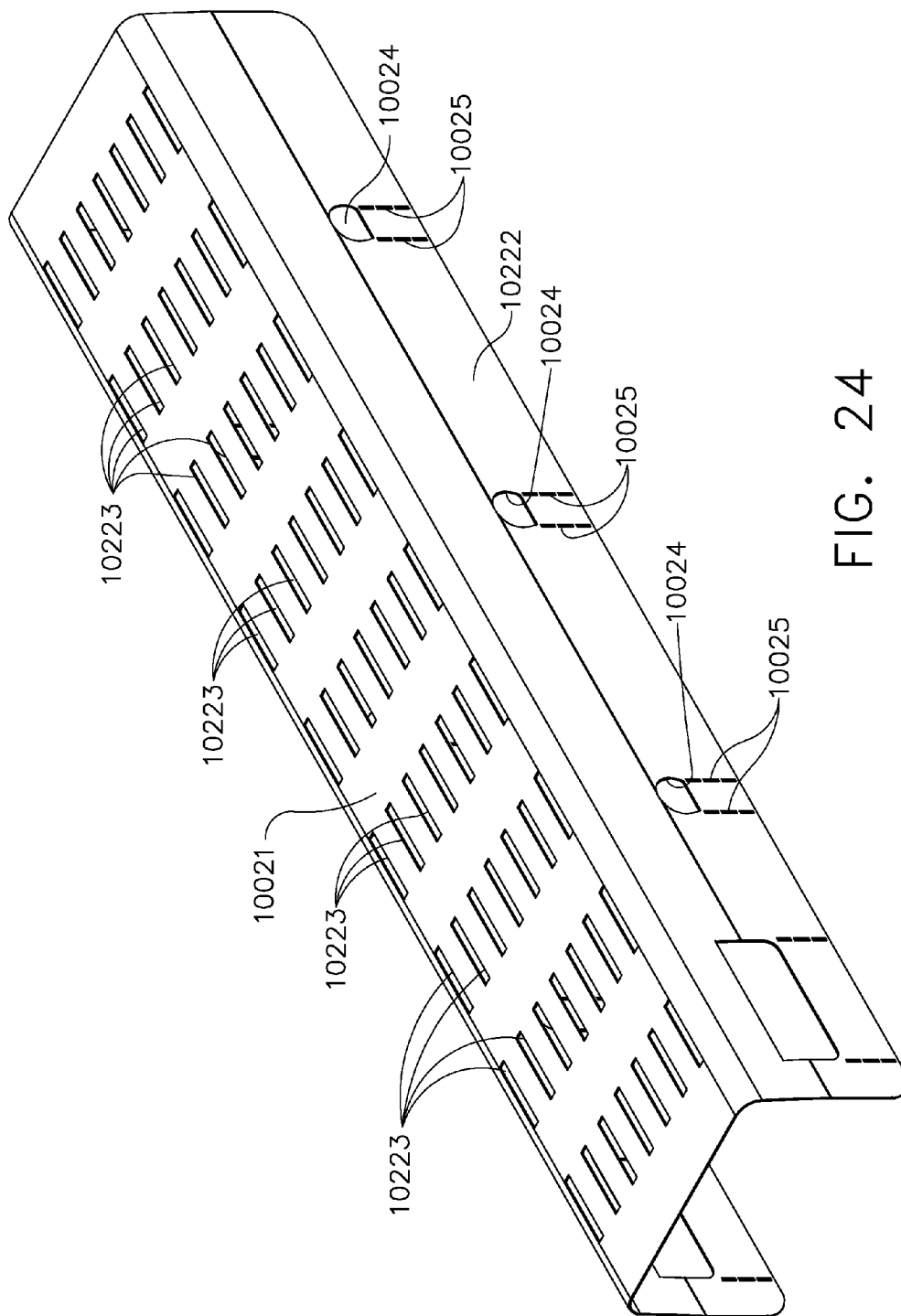


FIG. 24

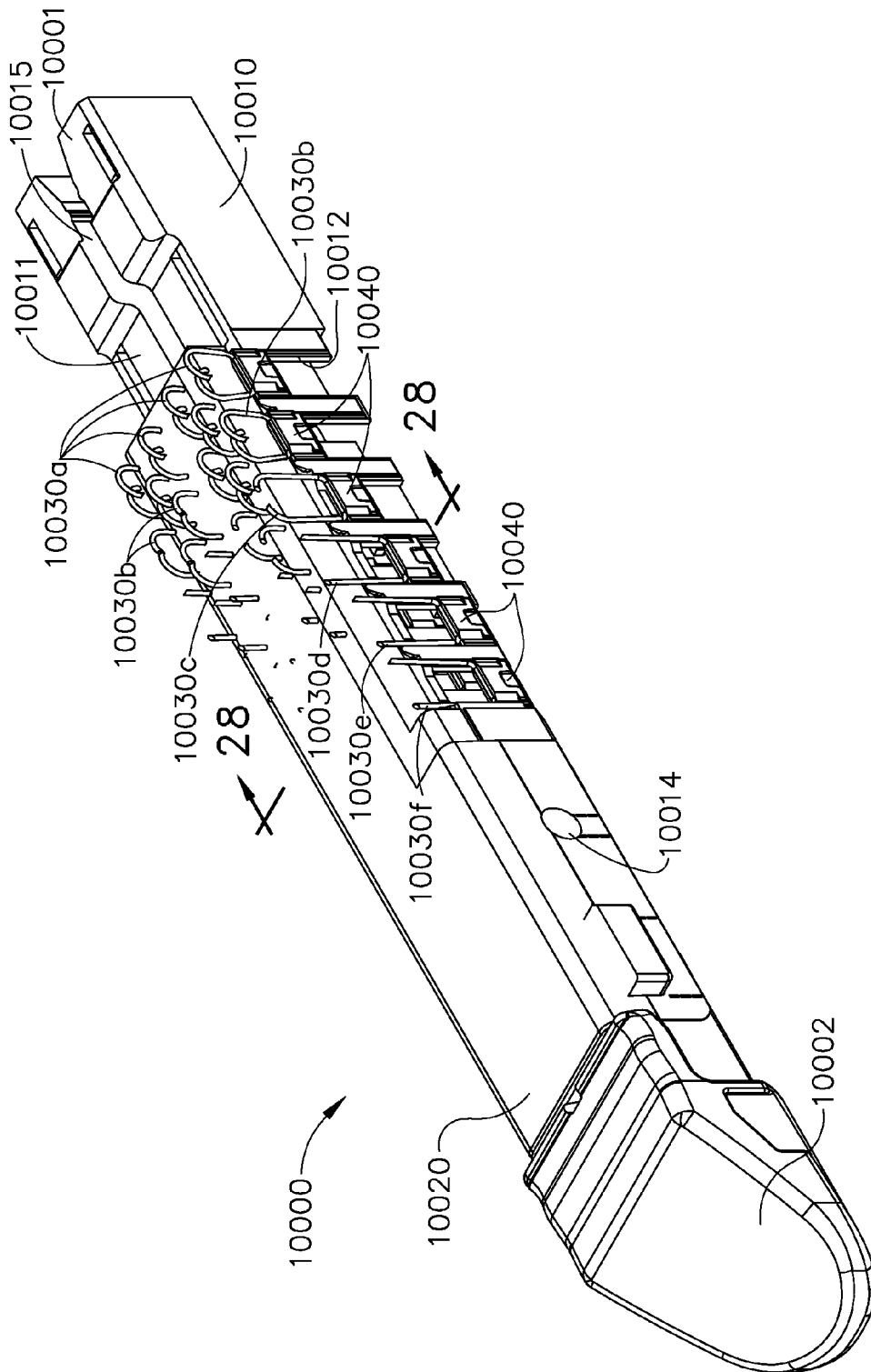


FIG. 25

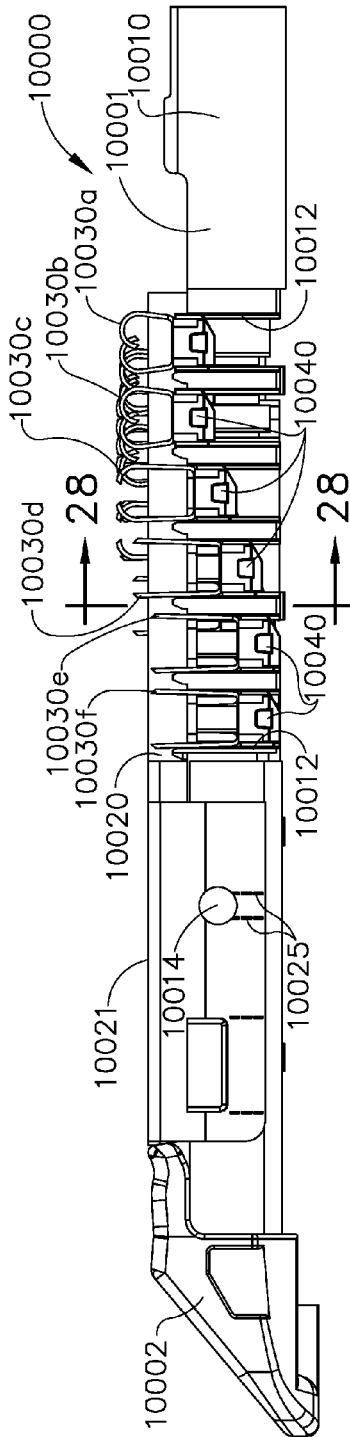


FIG. 26

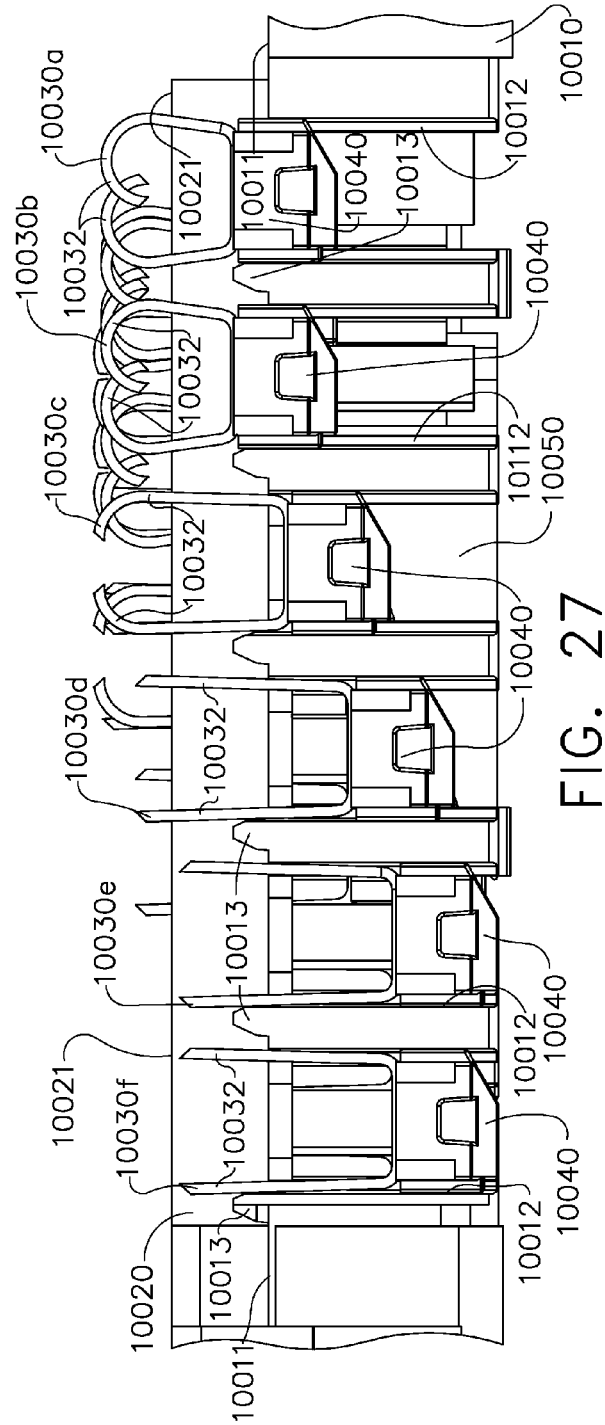
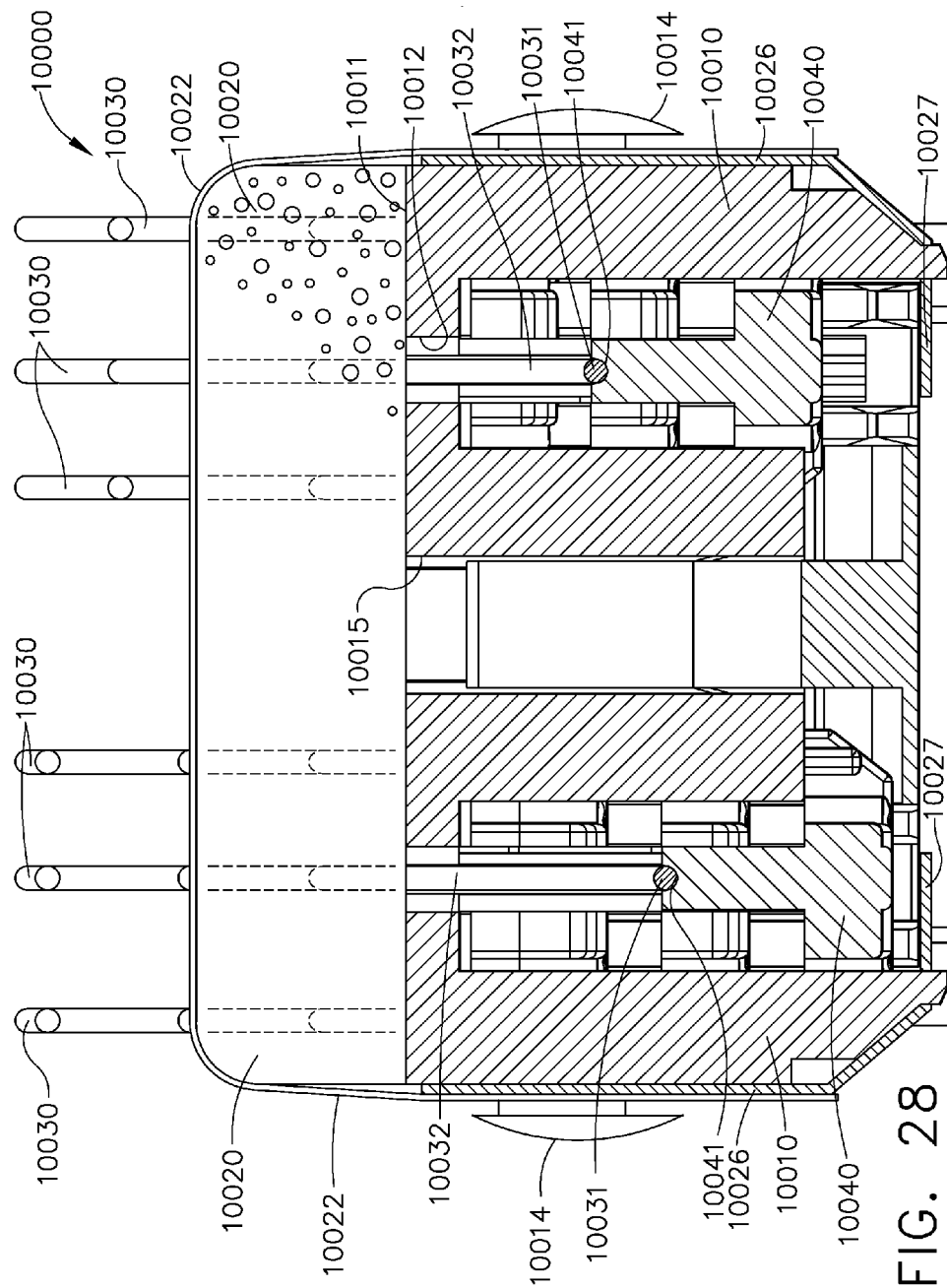


FIG. 27



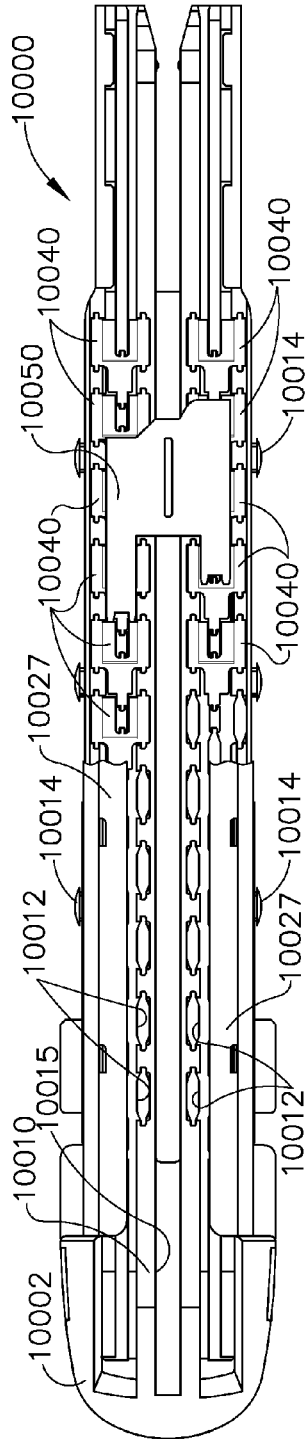


FIG. 29

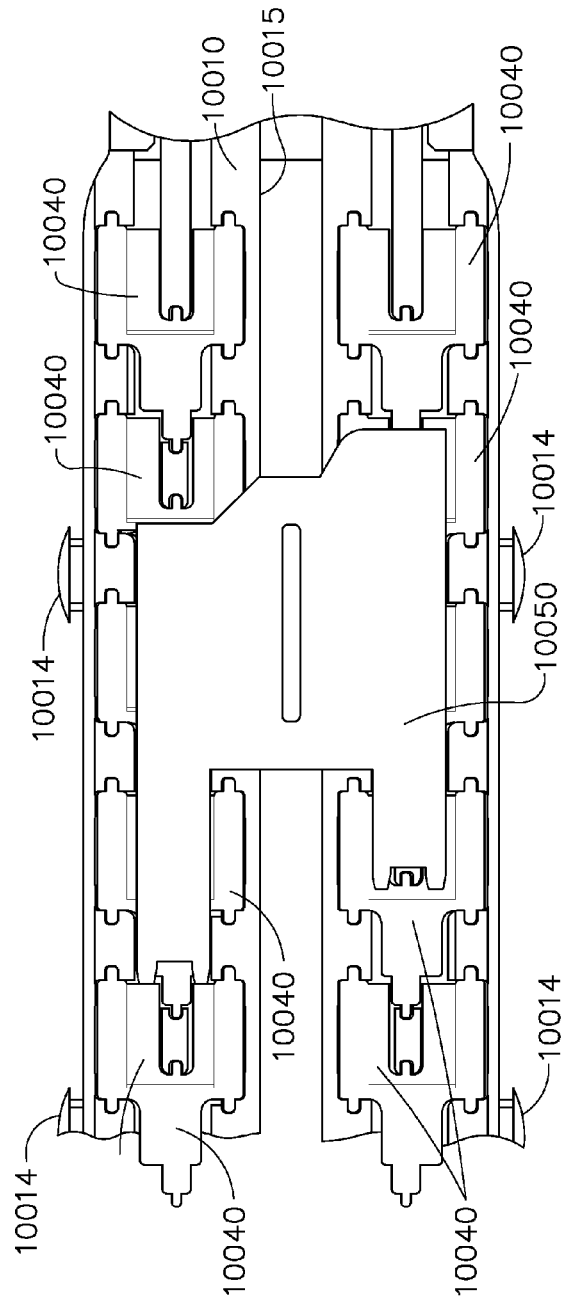
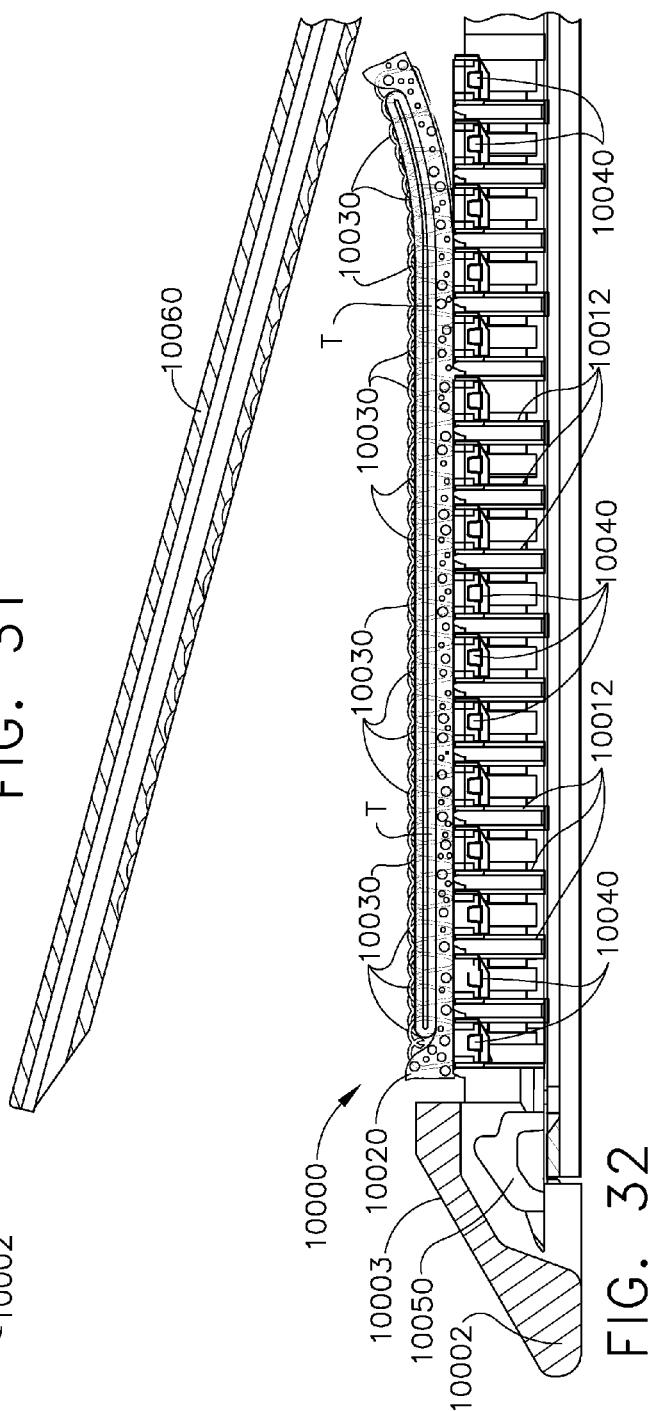
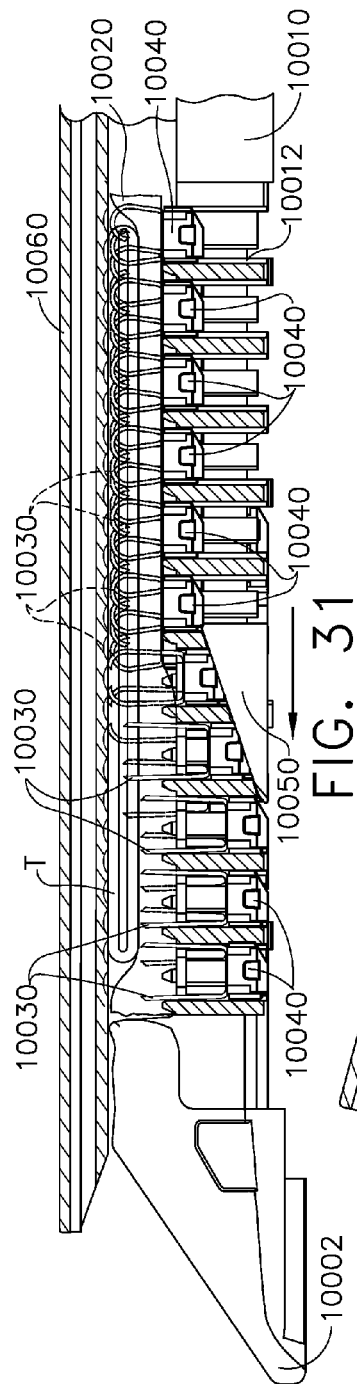


FIG. 30



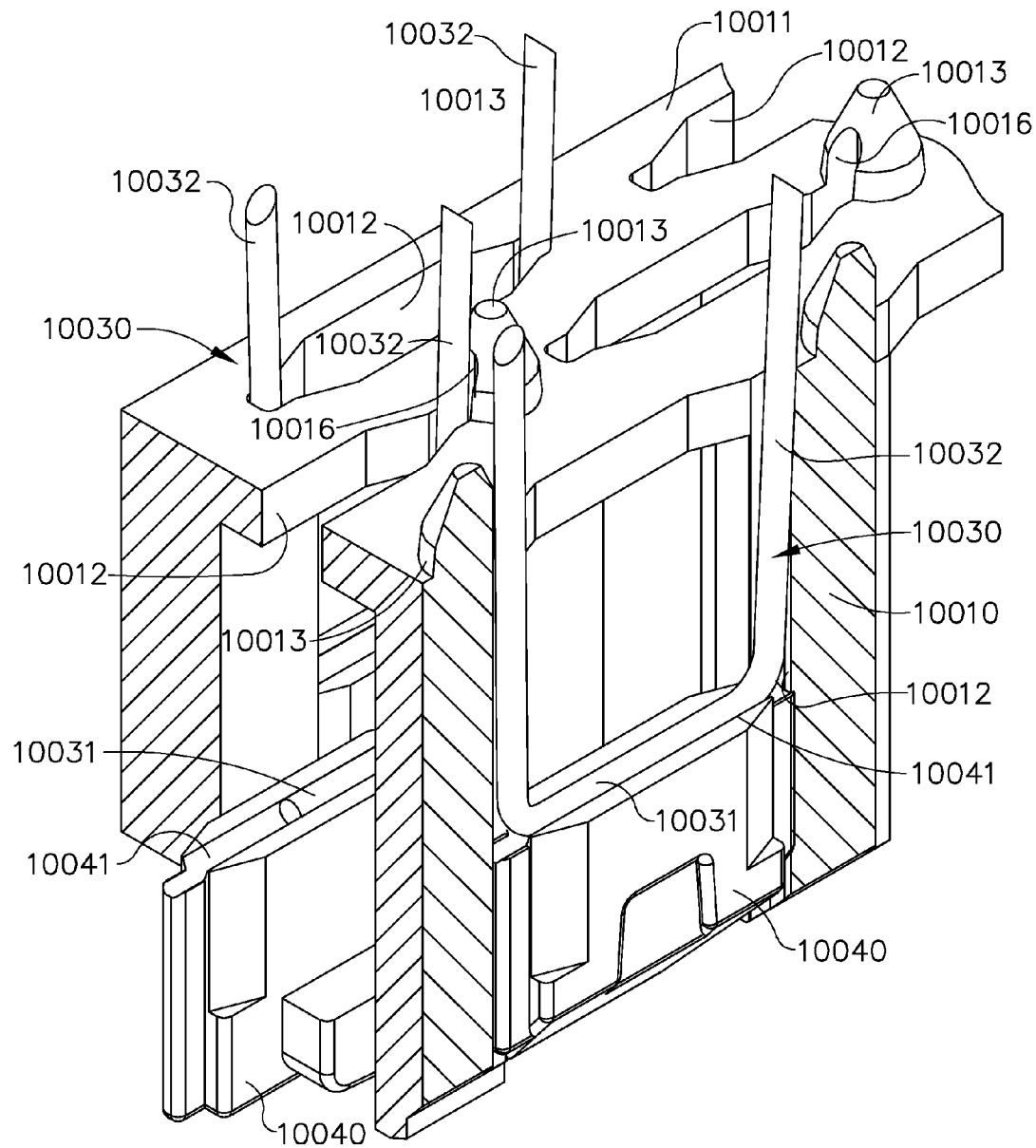


FIG. 33

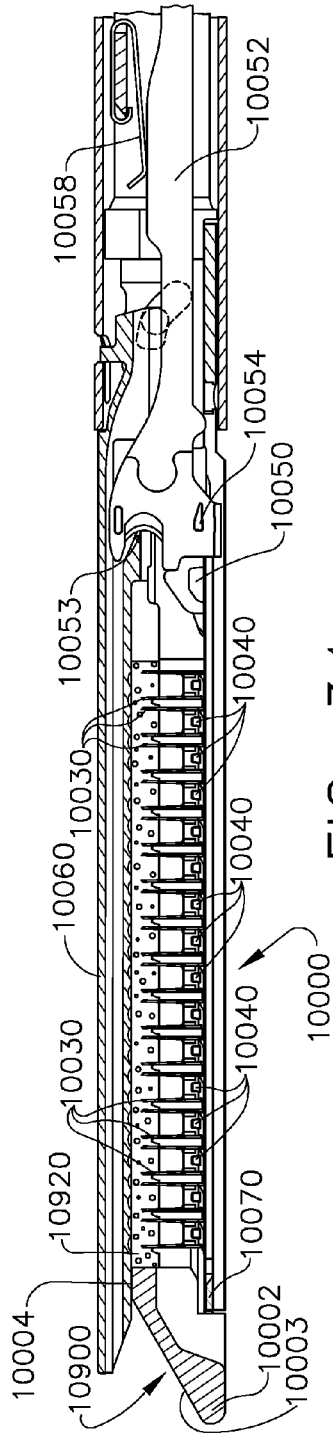


FIG. 34

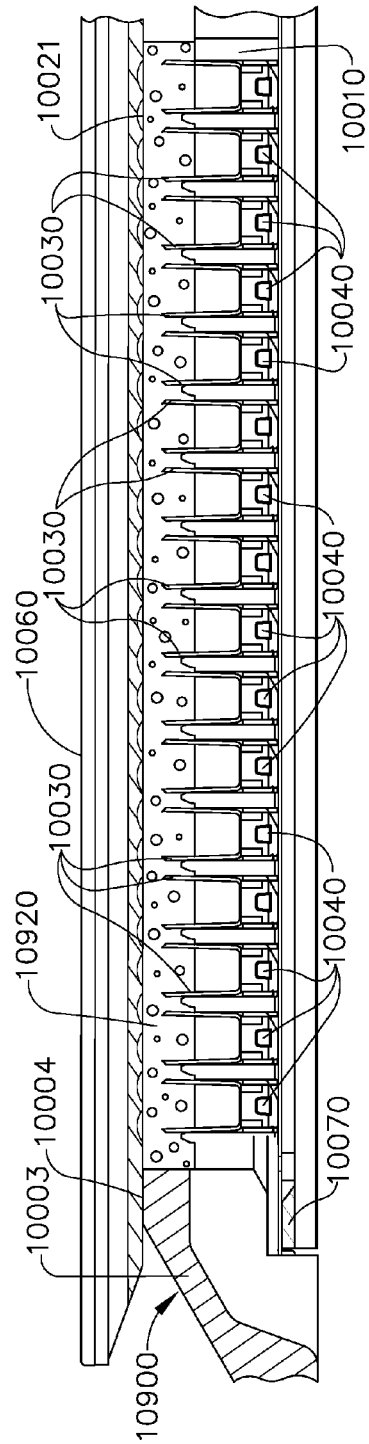


FIG. 35

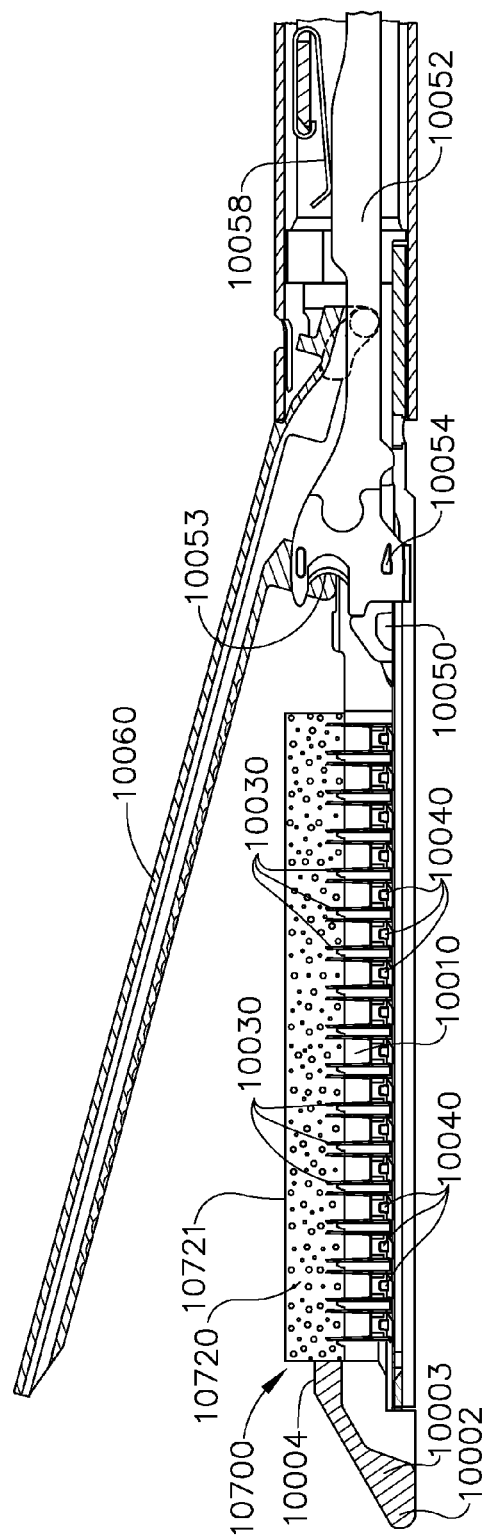


FIG. 36

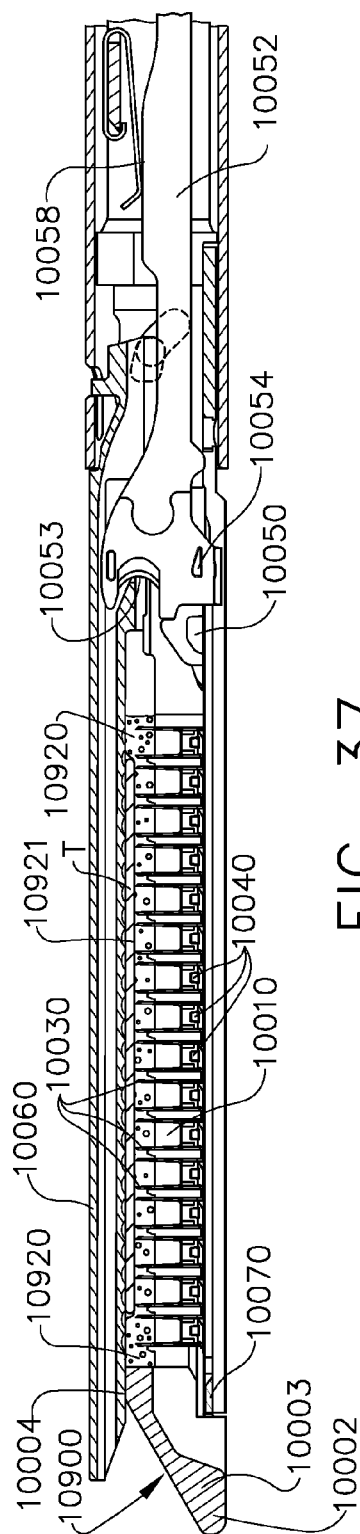


FIG. 37

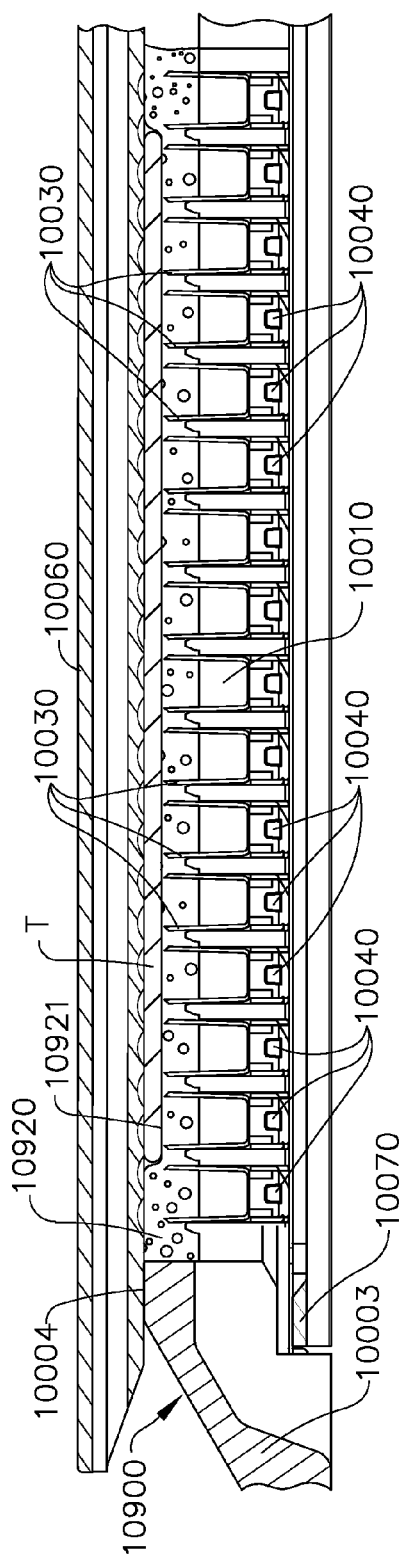


FIG. 38

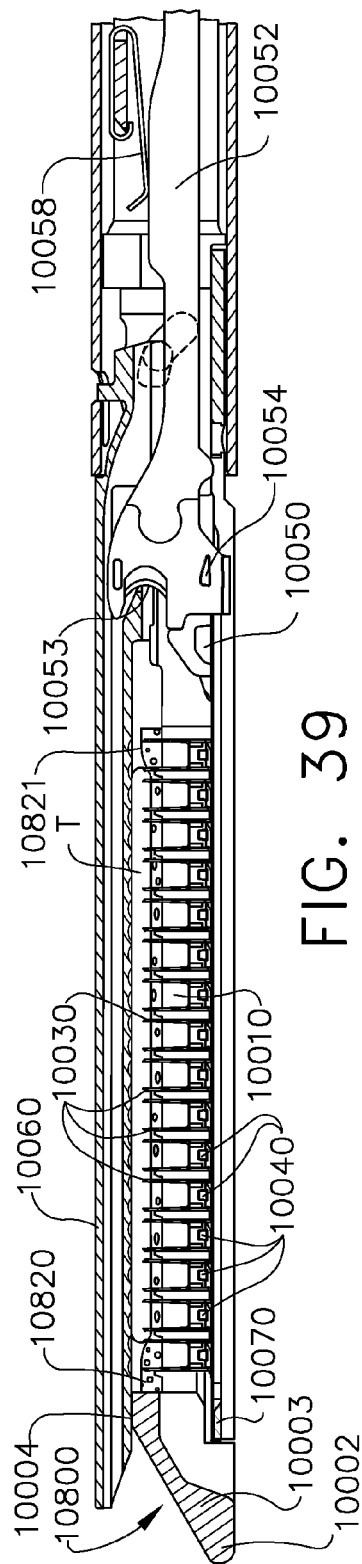


FIG. 39

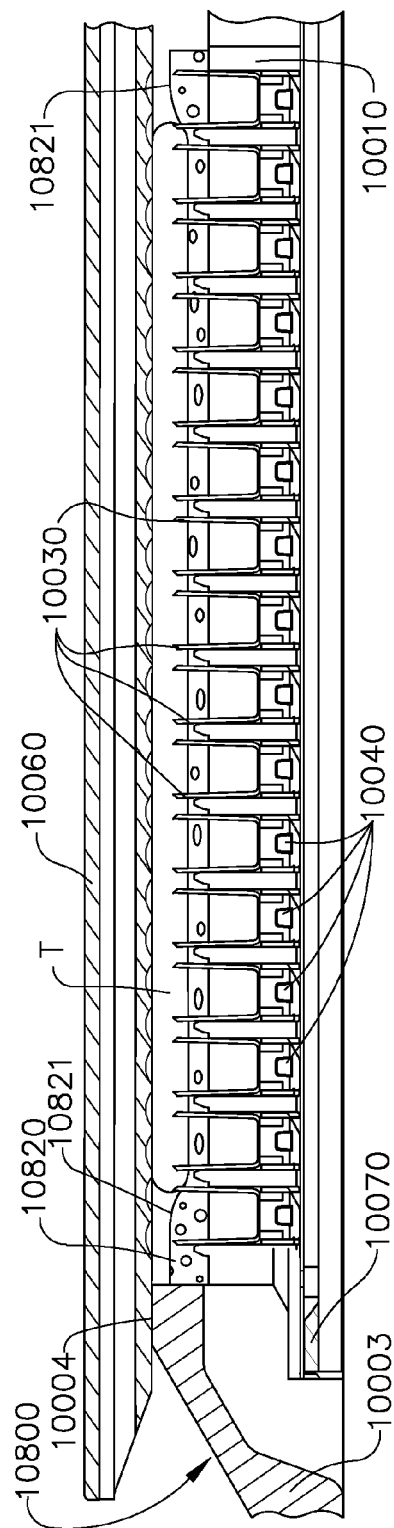


FIG. 40

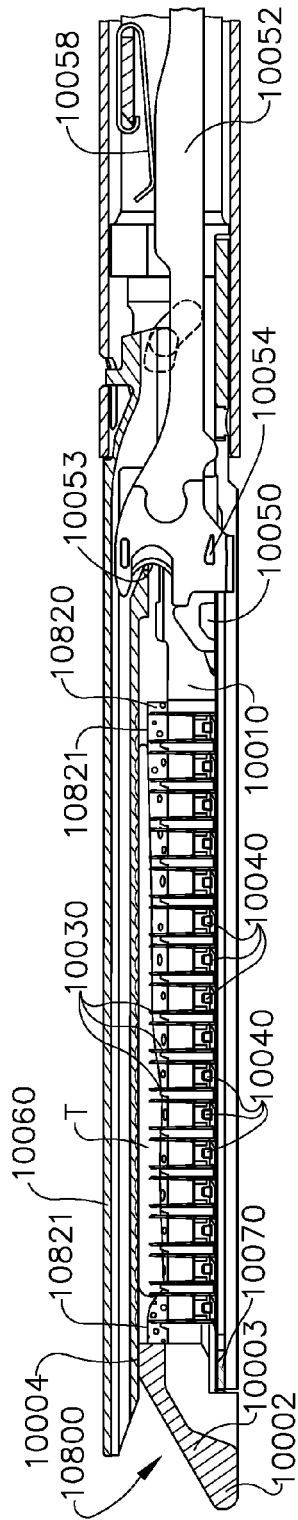


FIG. 41

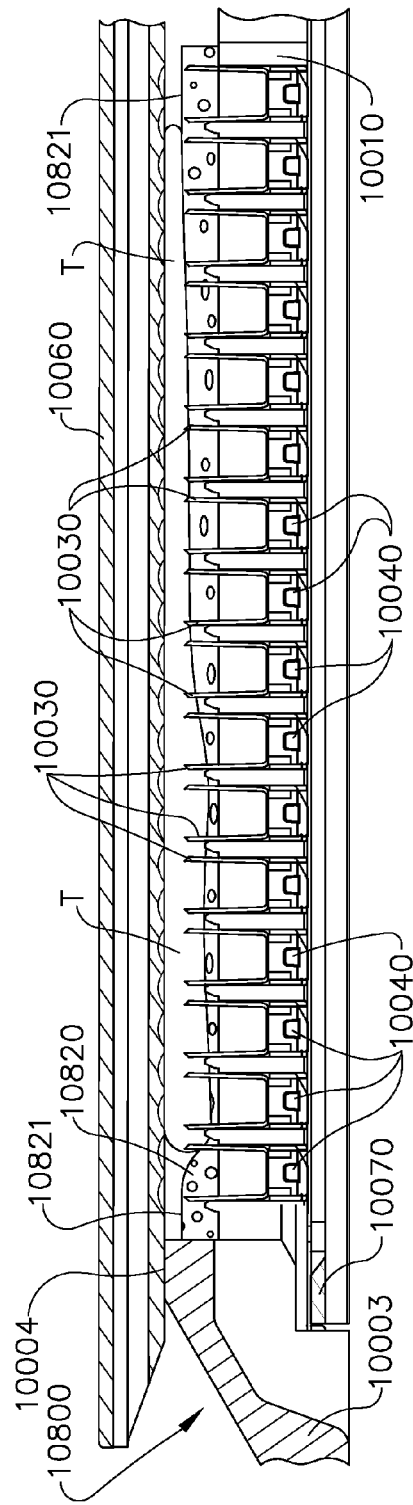


FIG. 42

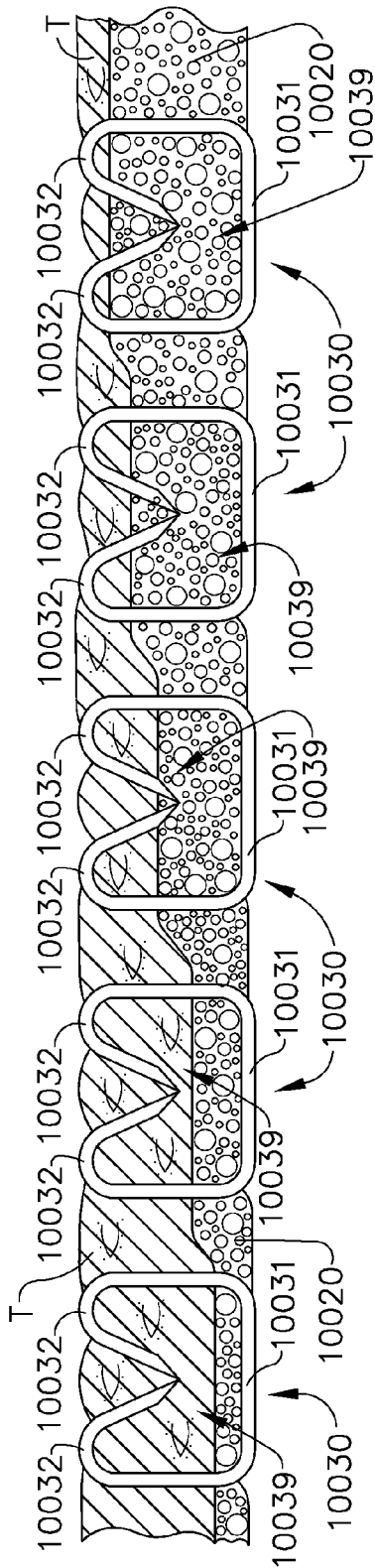


FIG. 43

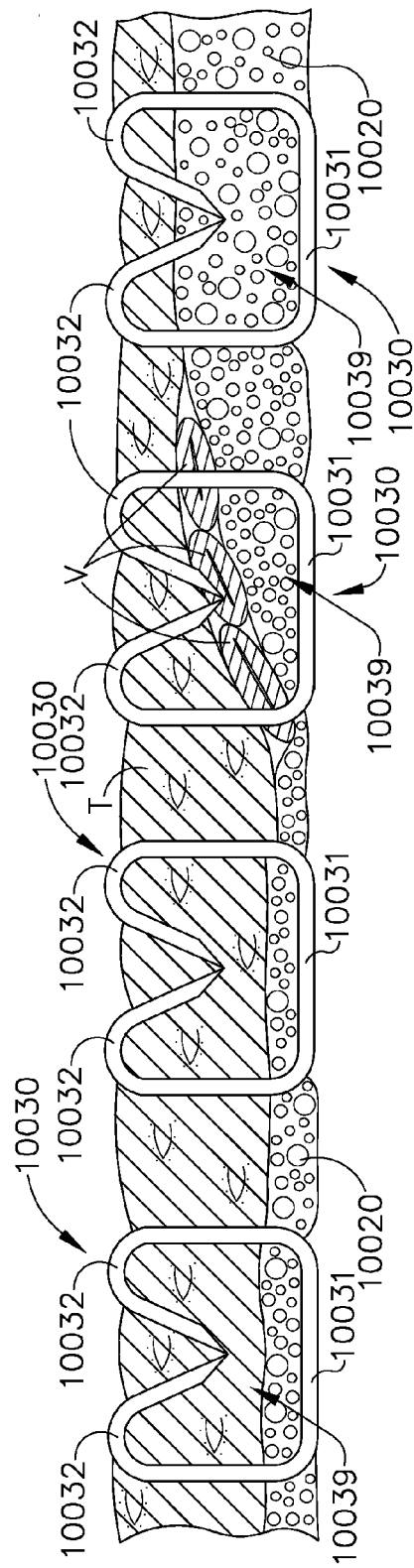


FIG. 44

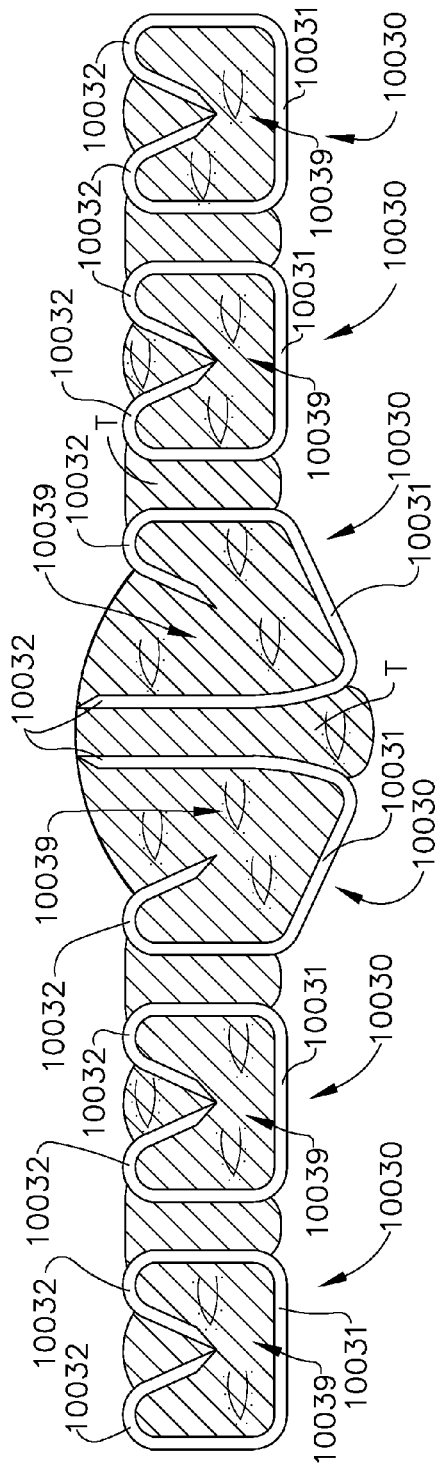


FIG. 45

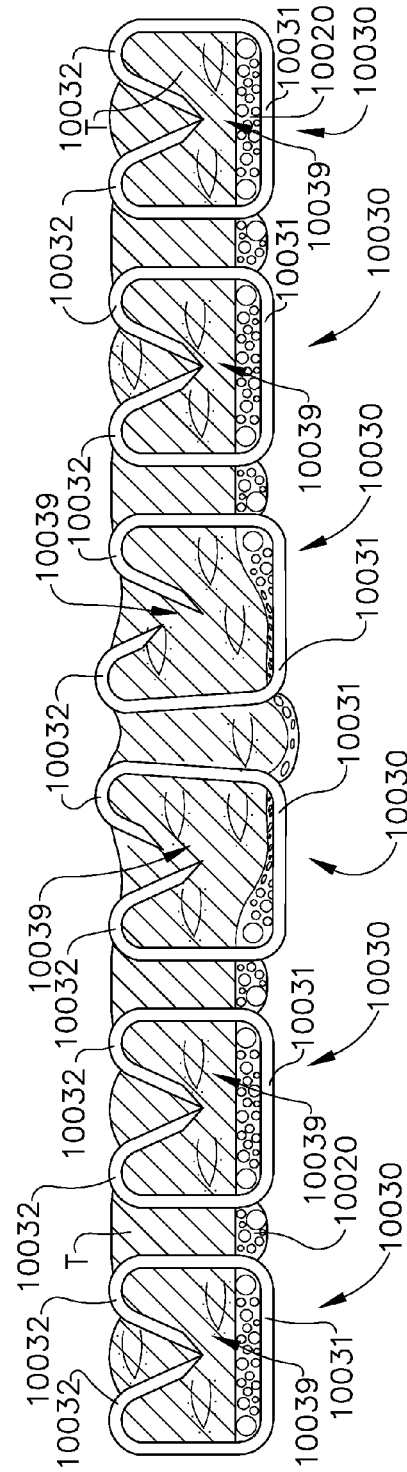


FIG. 46

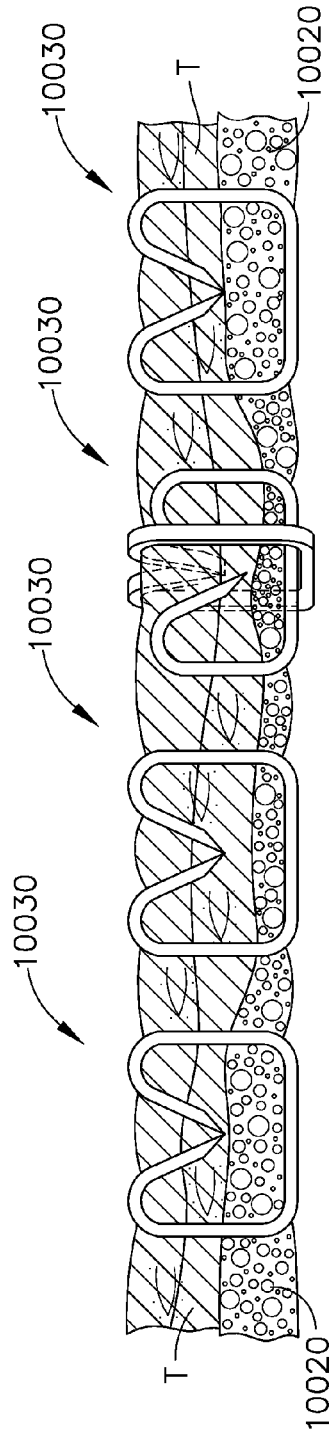


FIG. 47

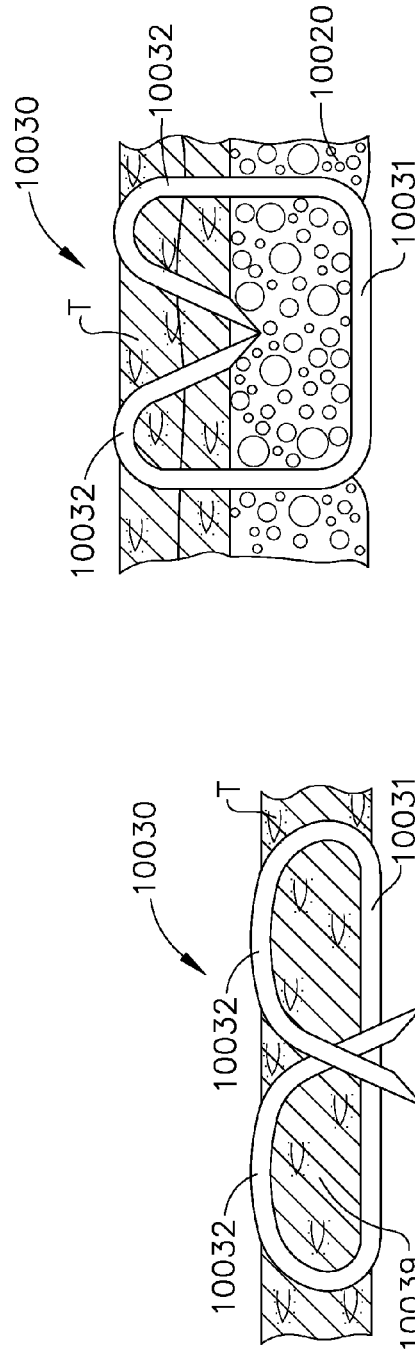


FIG. 48

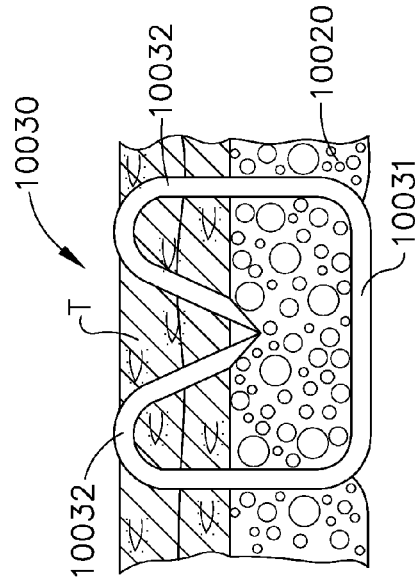


FIG. 49

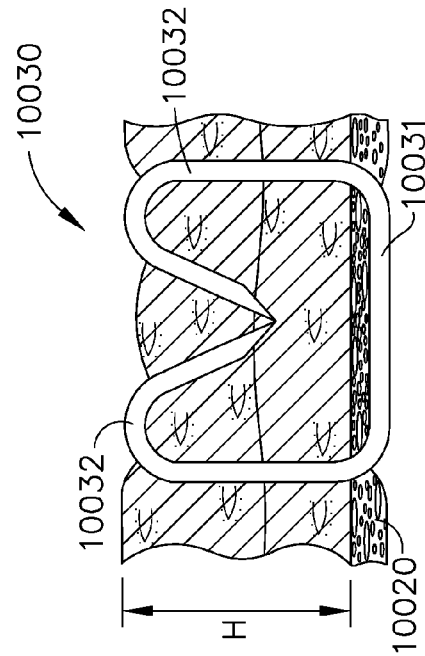


FIG. 50

FIG. 51

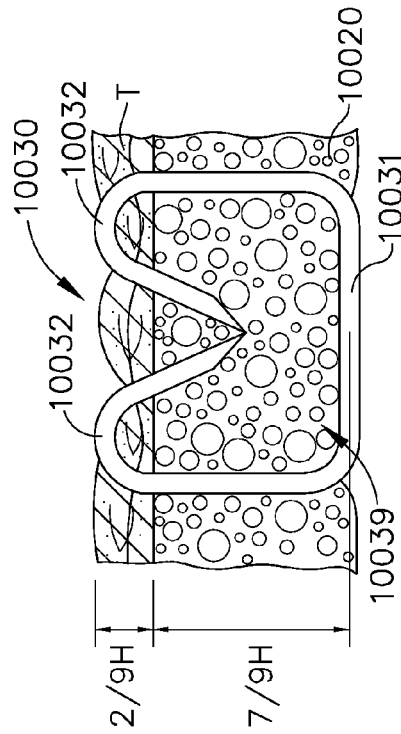


FIG. 52

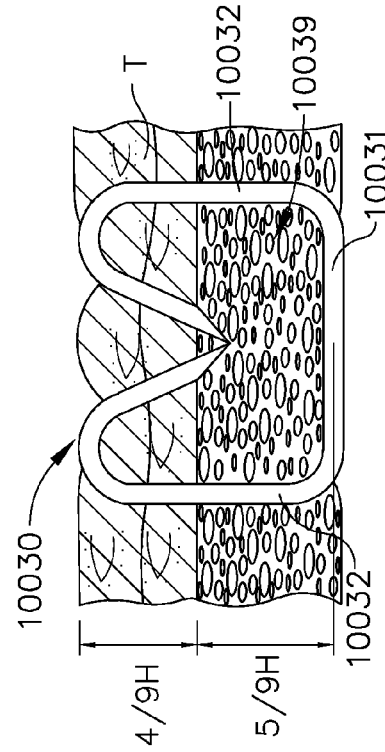


FIG. 53

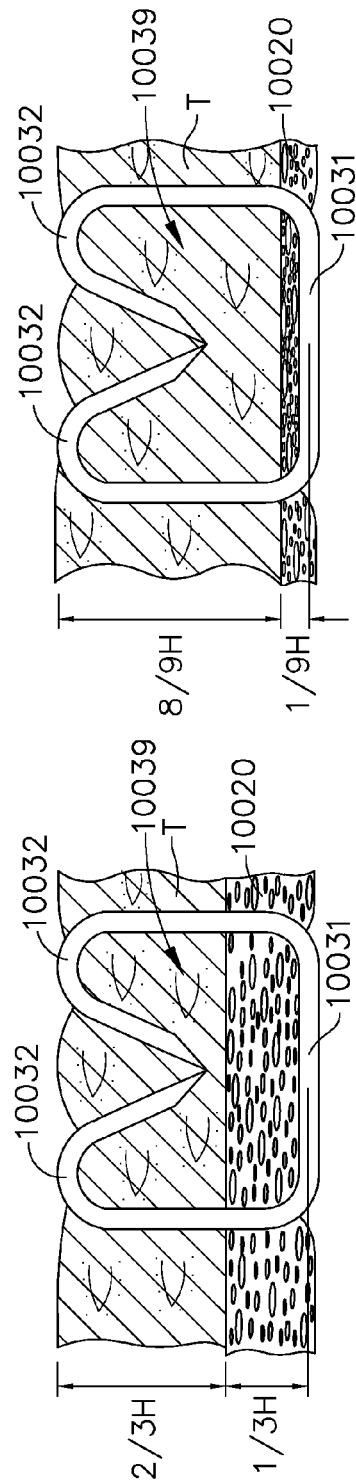


FIG. 54

FIG. 55

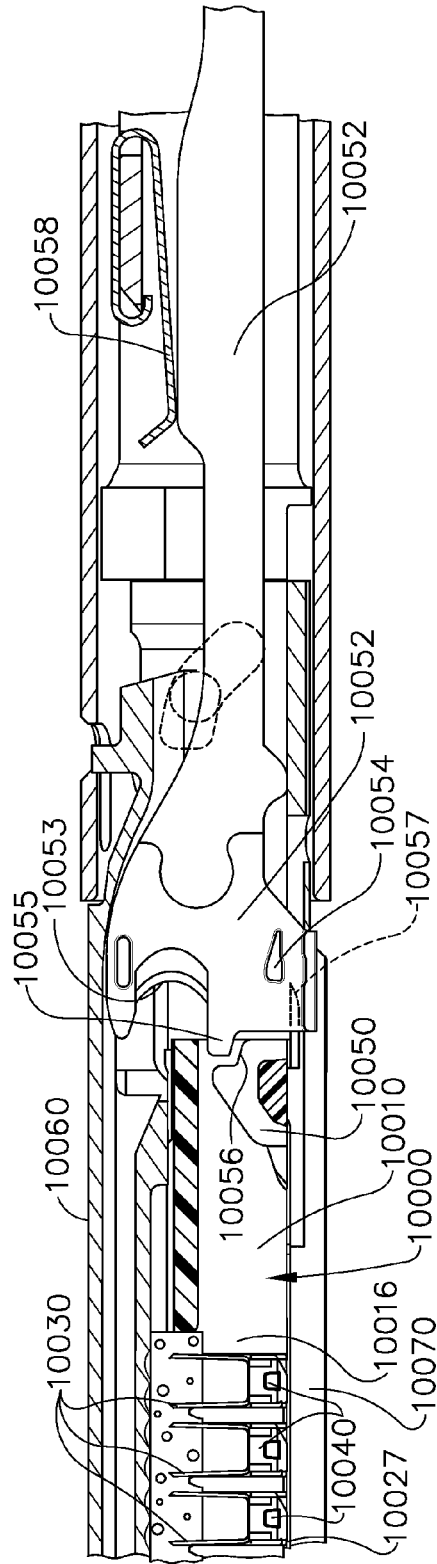


FIG. 56

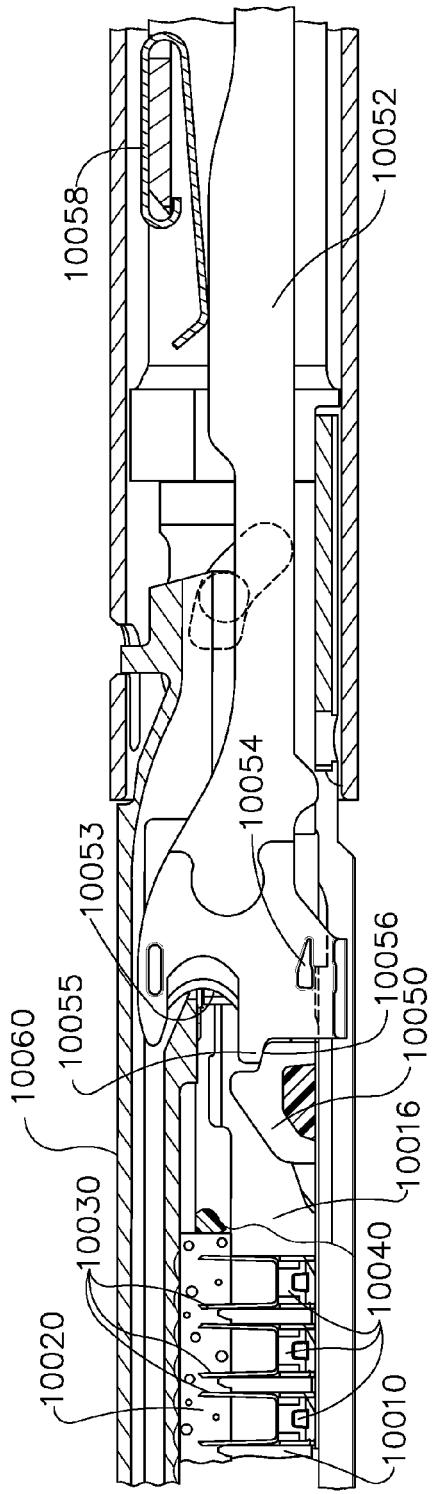


FIG. 57

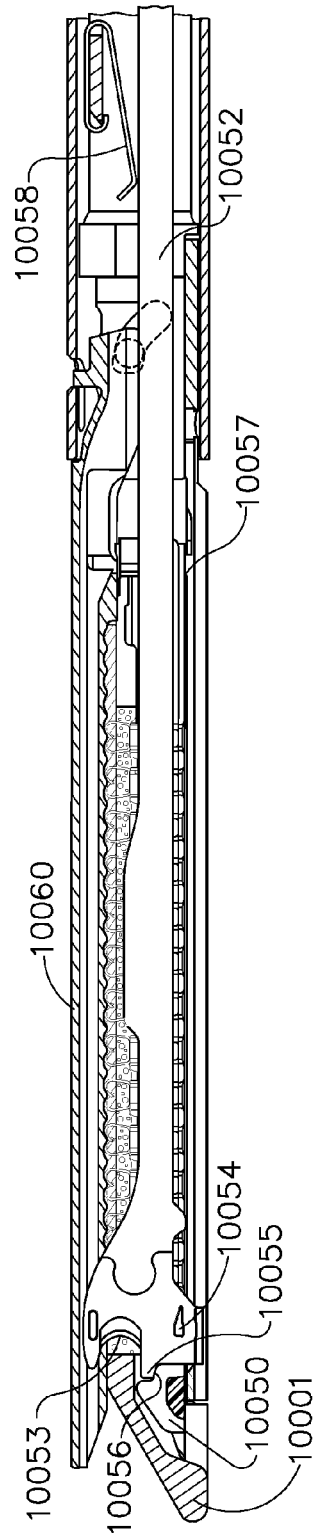


FIG. 58

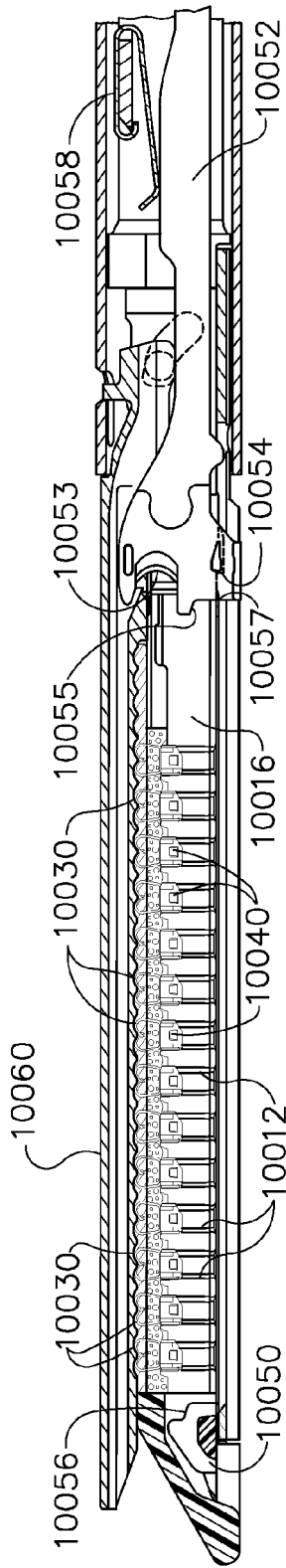


FIG. 59

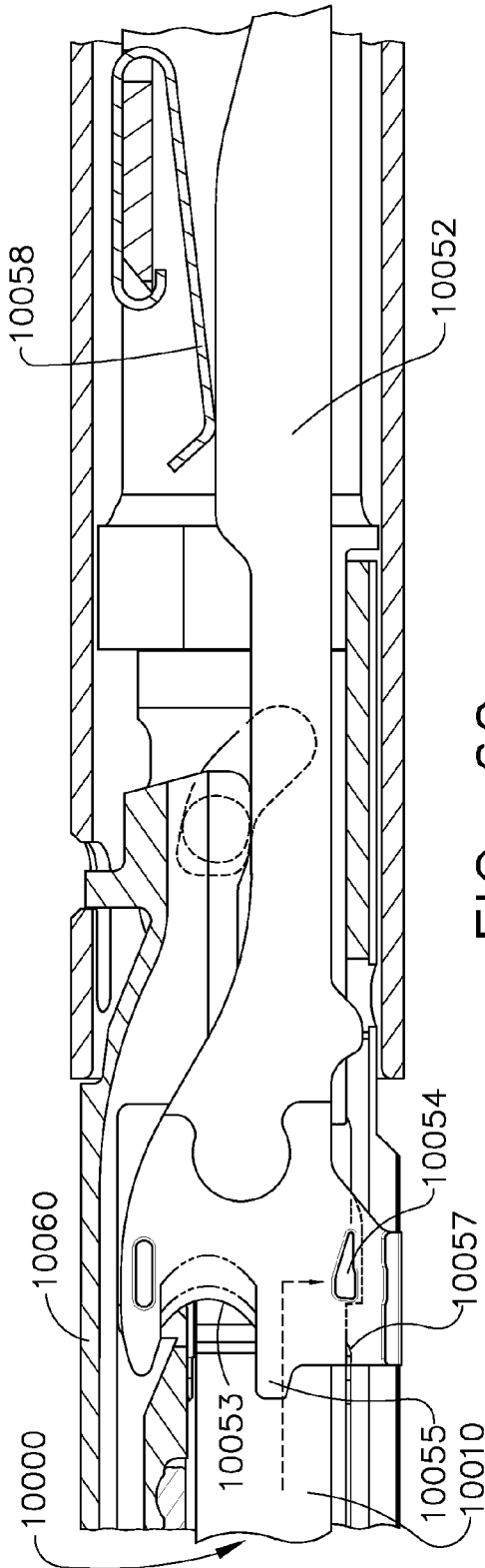
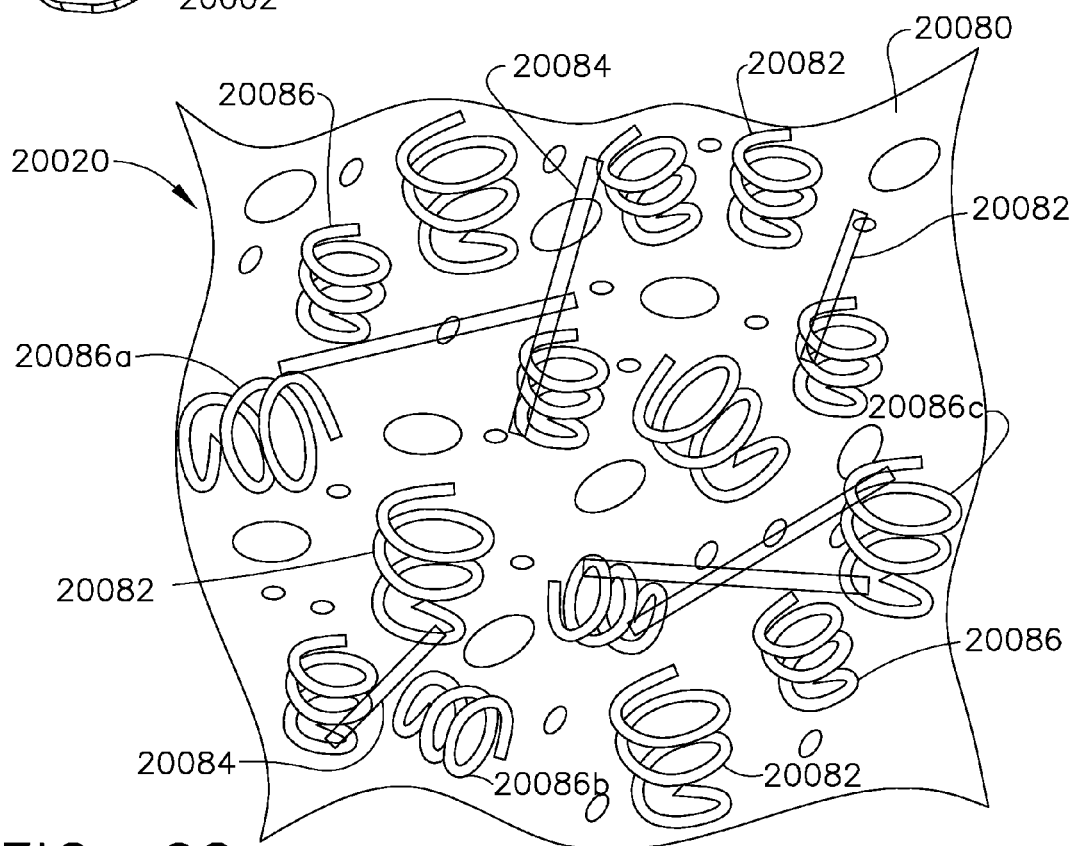
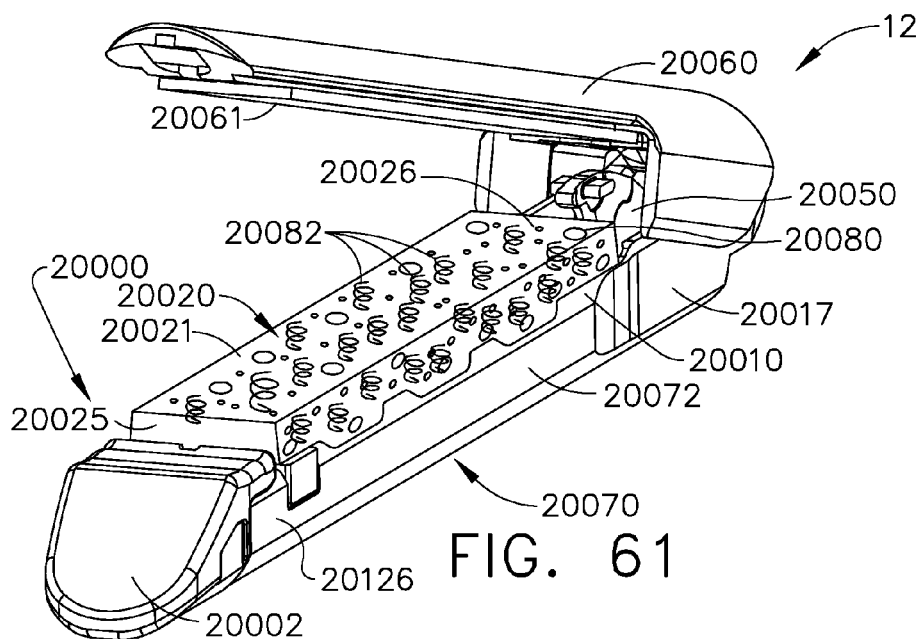


FIG. 60



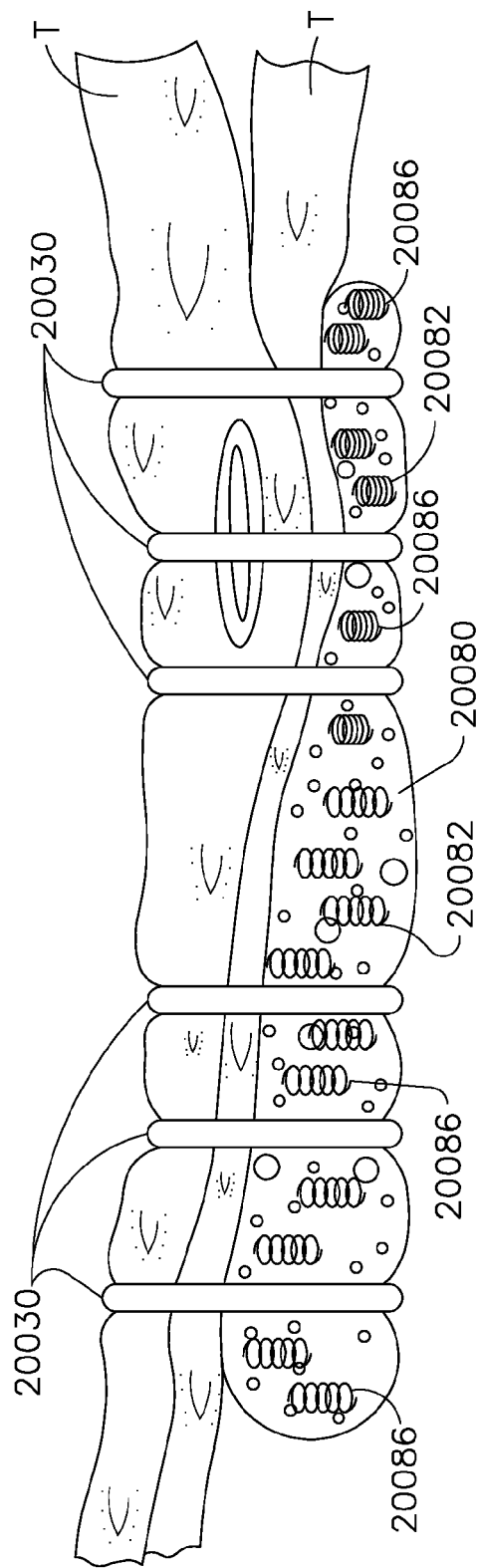


FIG. 63

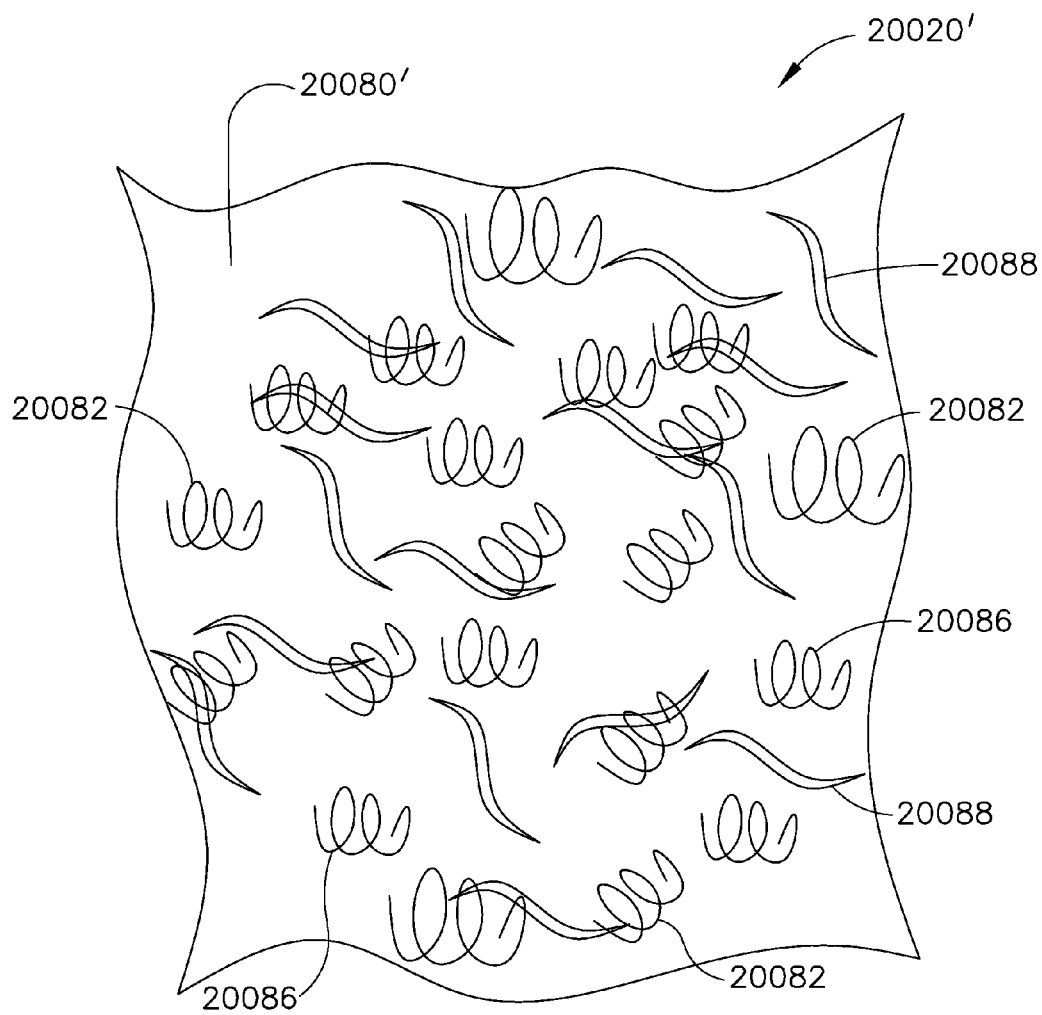


FIG. 64



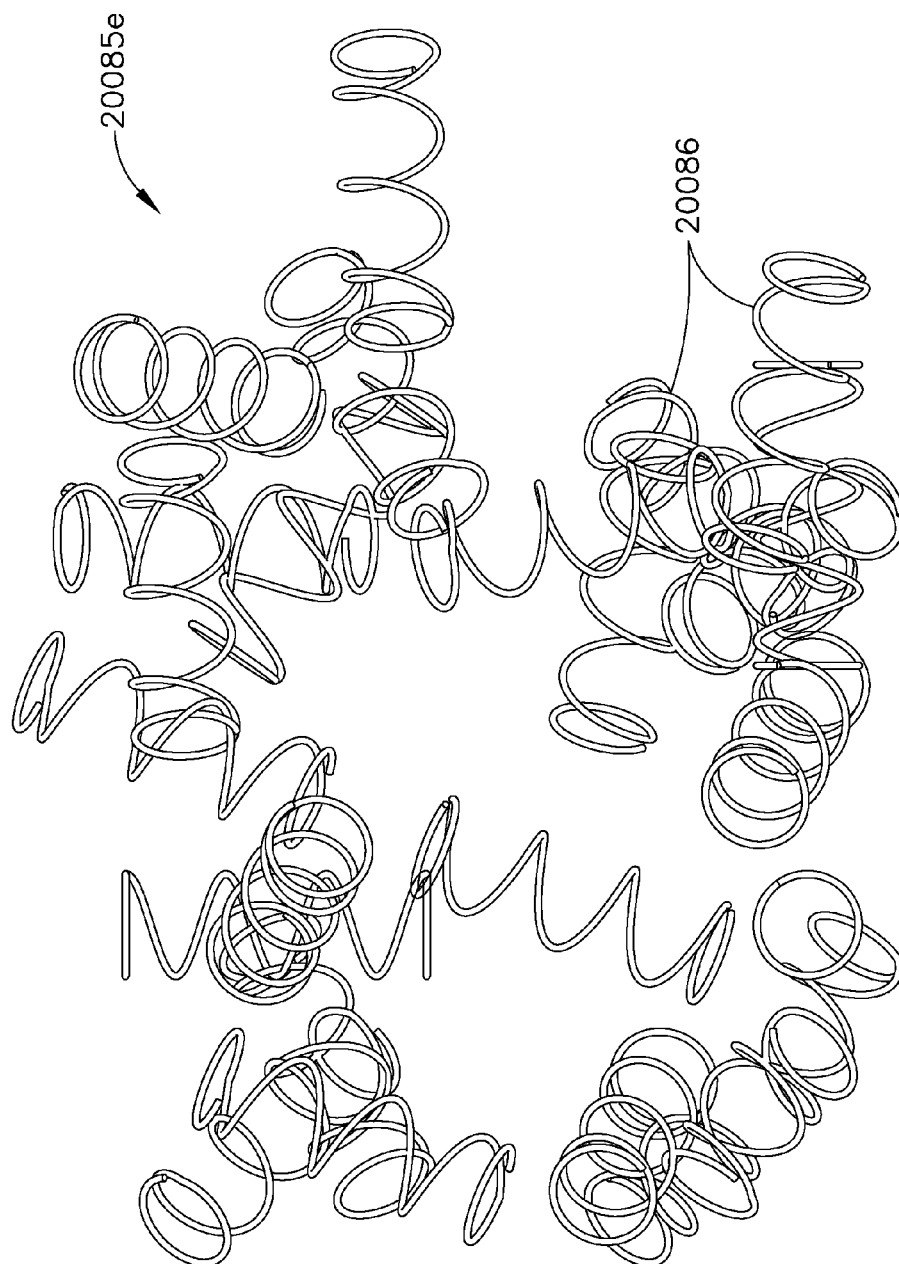


FIG. 66

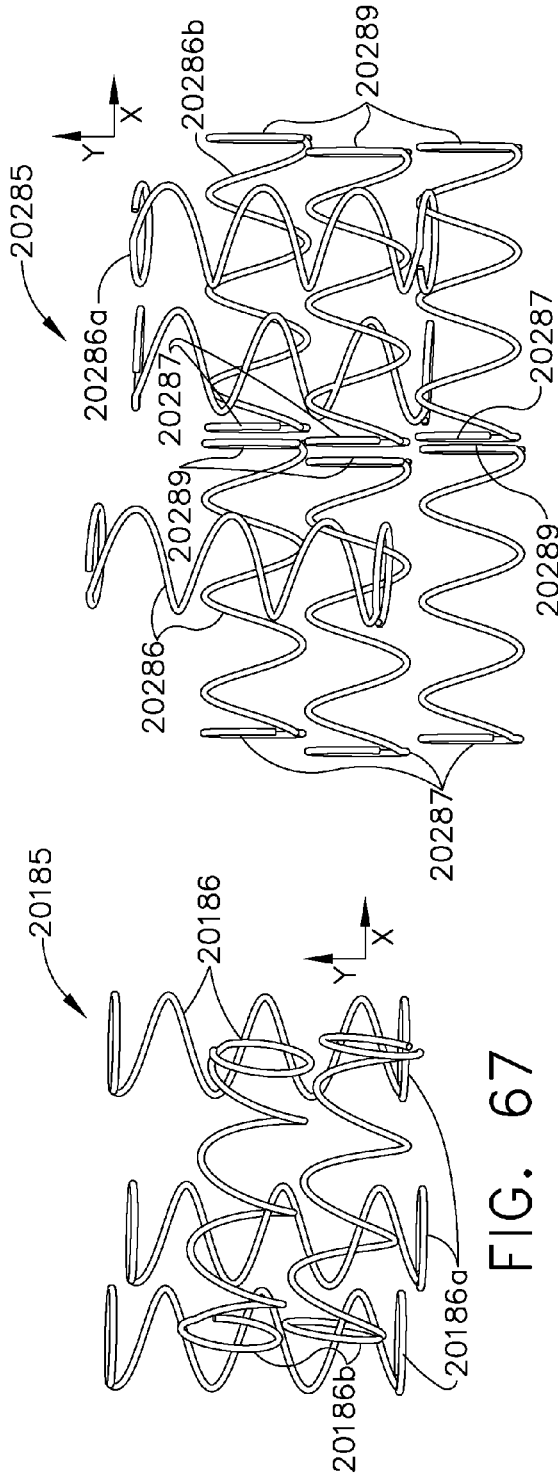


FIG. 67

FIG. 68

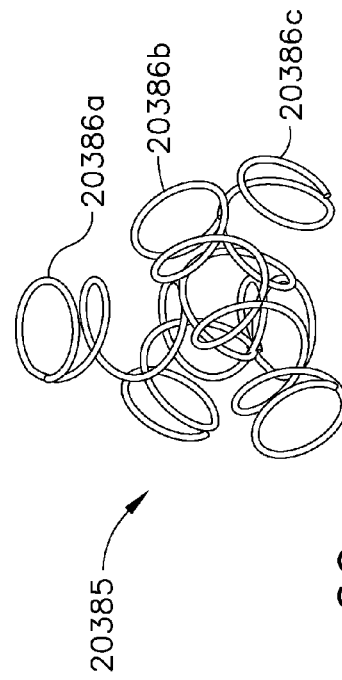


FIG. 69

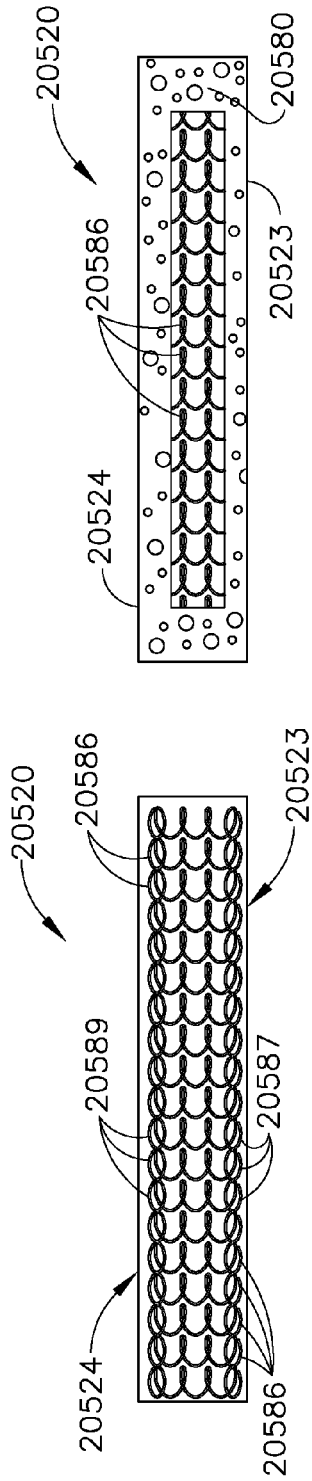


FIG. 70

FIG. 70A

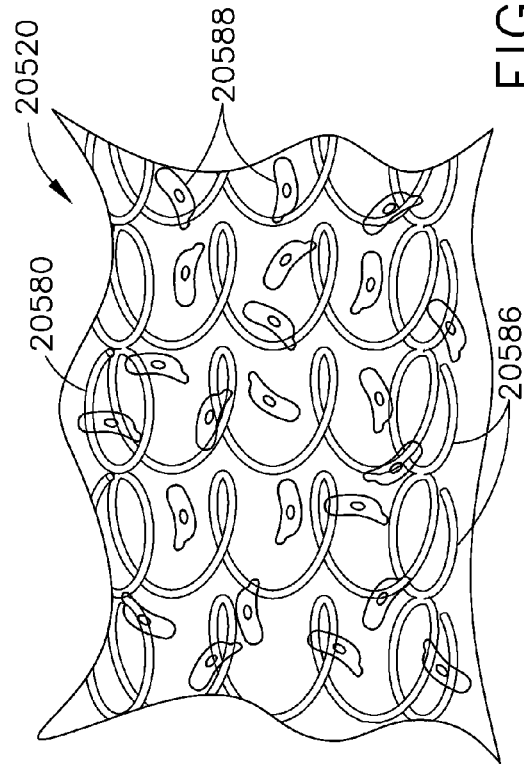


FIG. 70B

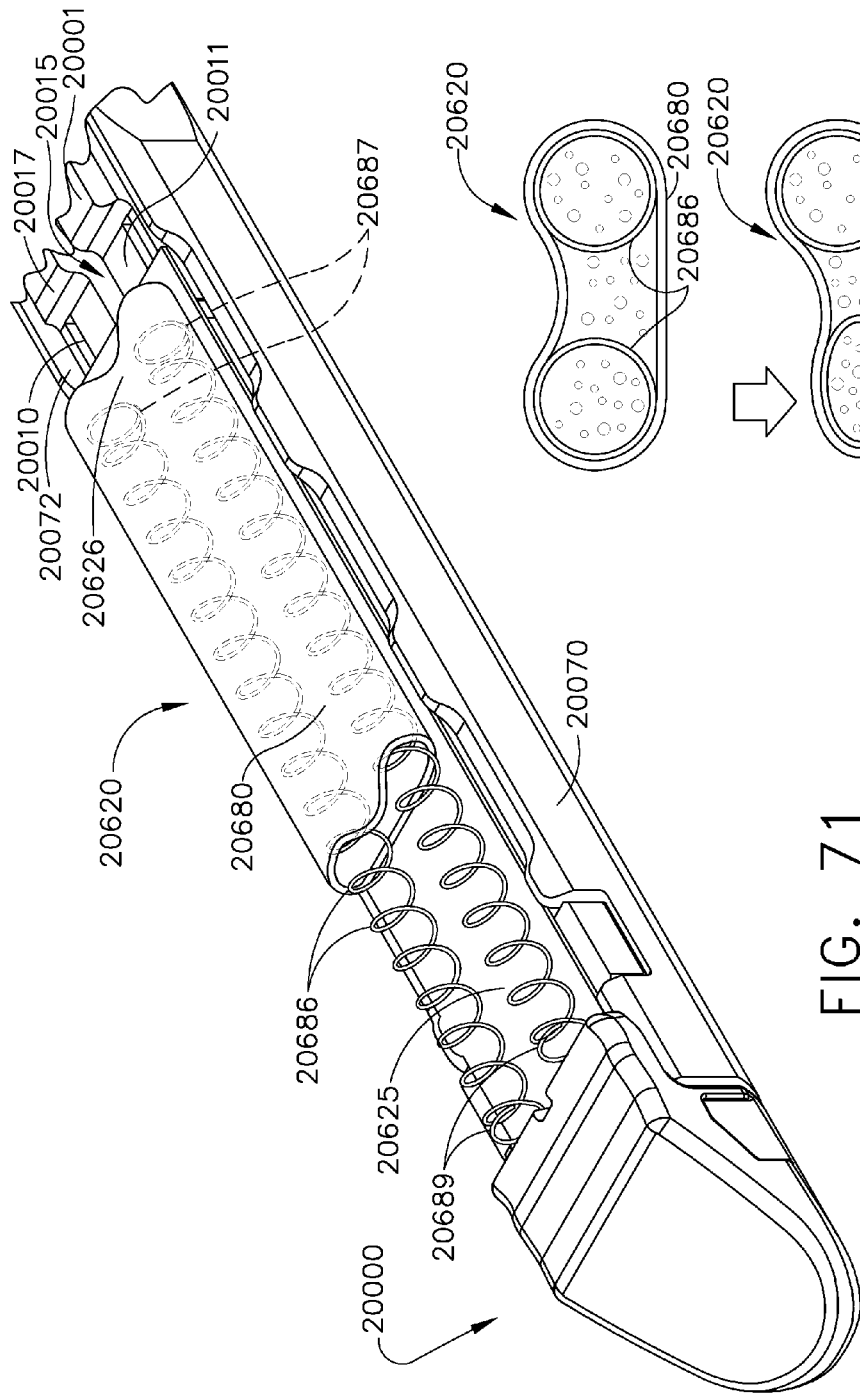


FIG. 71

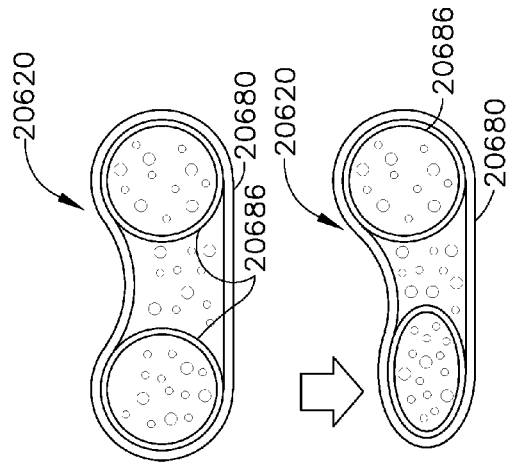


FIG. 72



FIG. 73

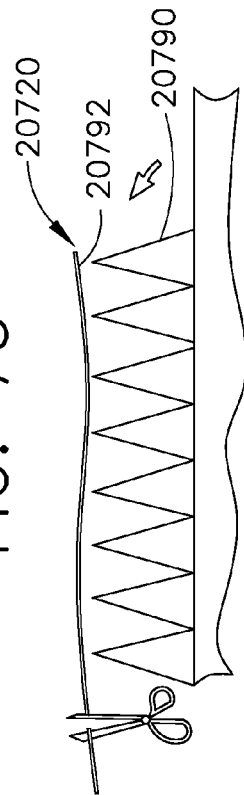


FIG. 74

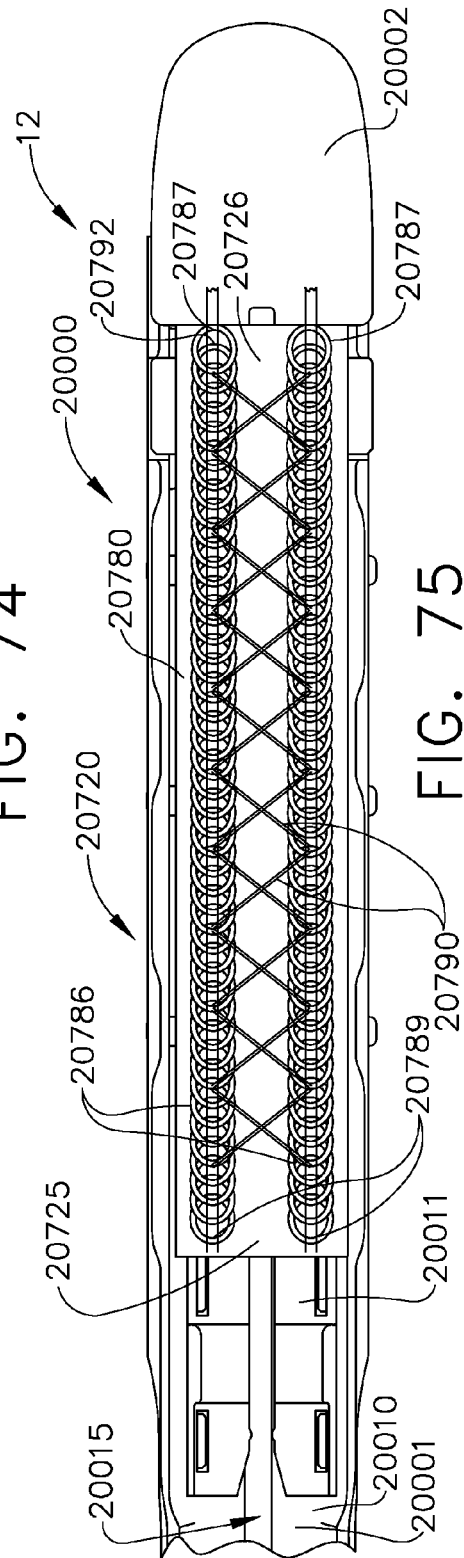


FIG. 75

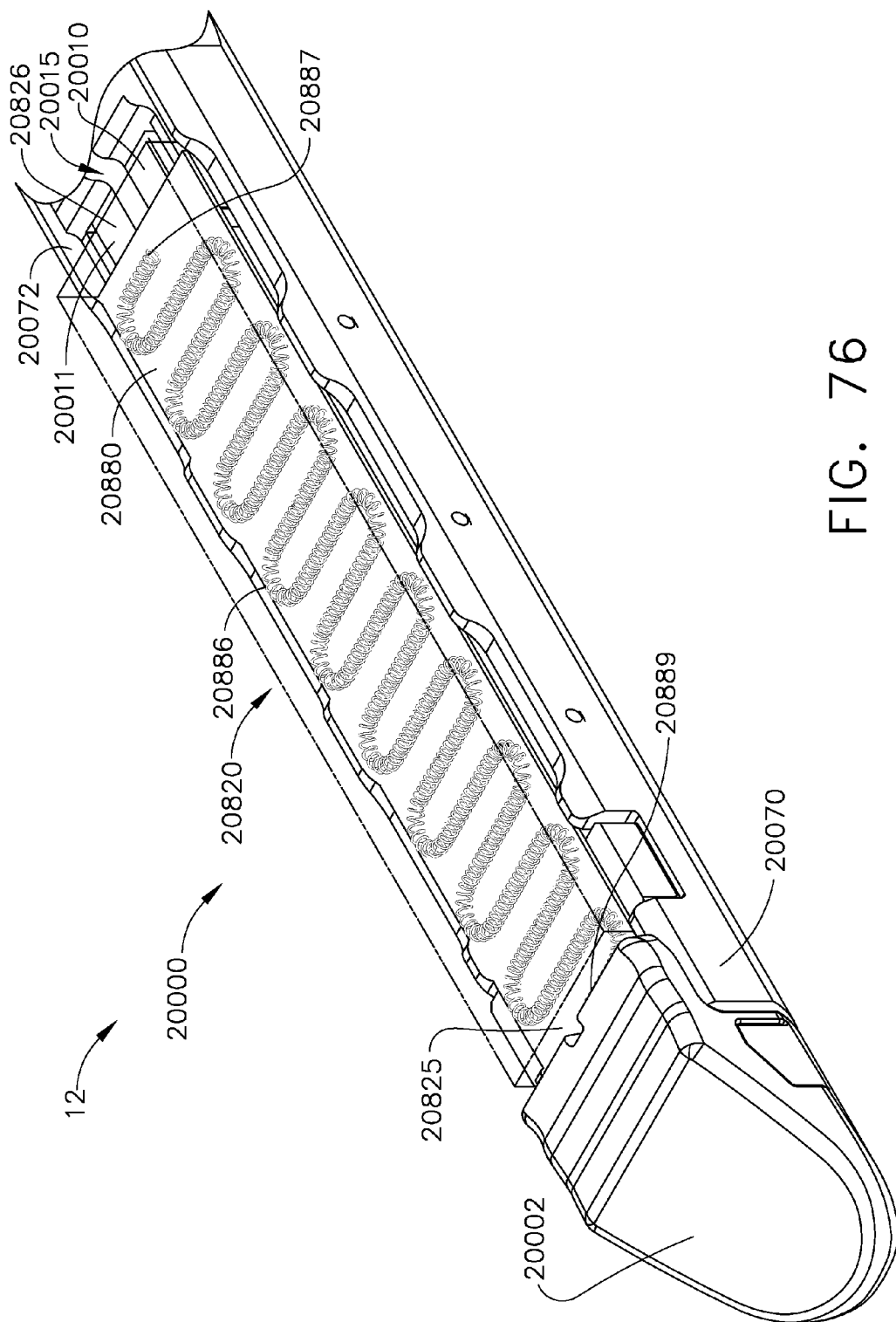


FIG. 76

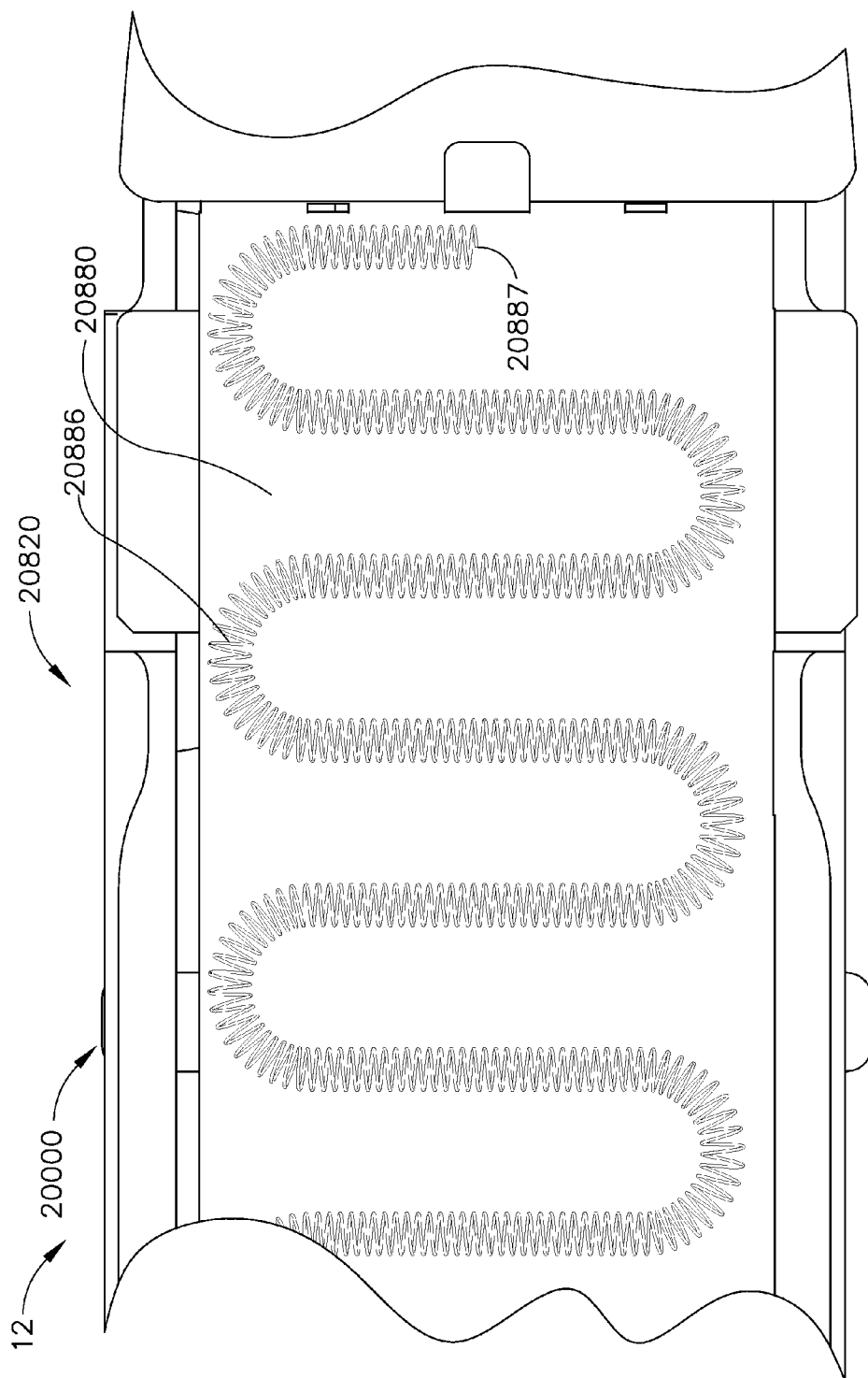


FIG. 77

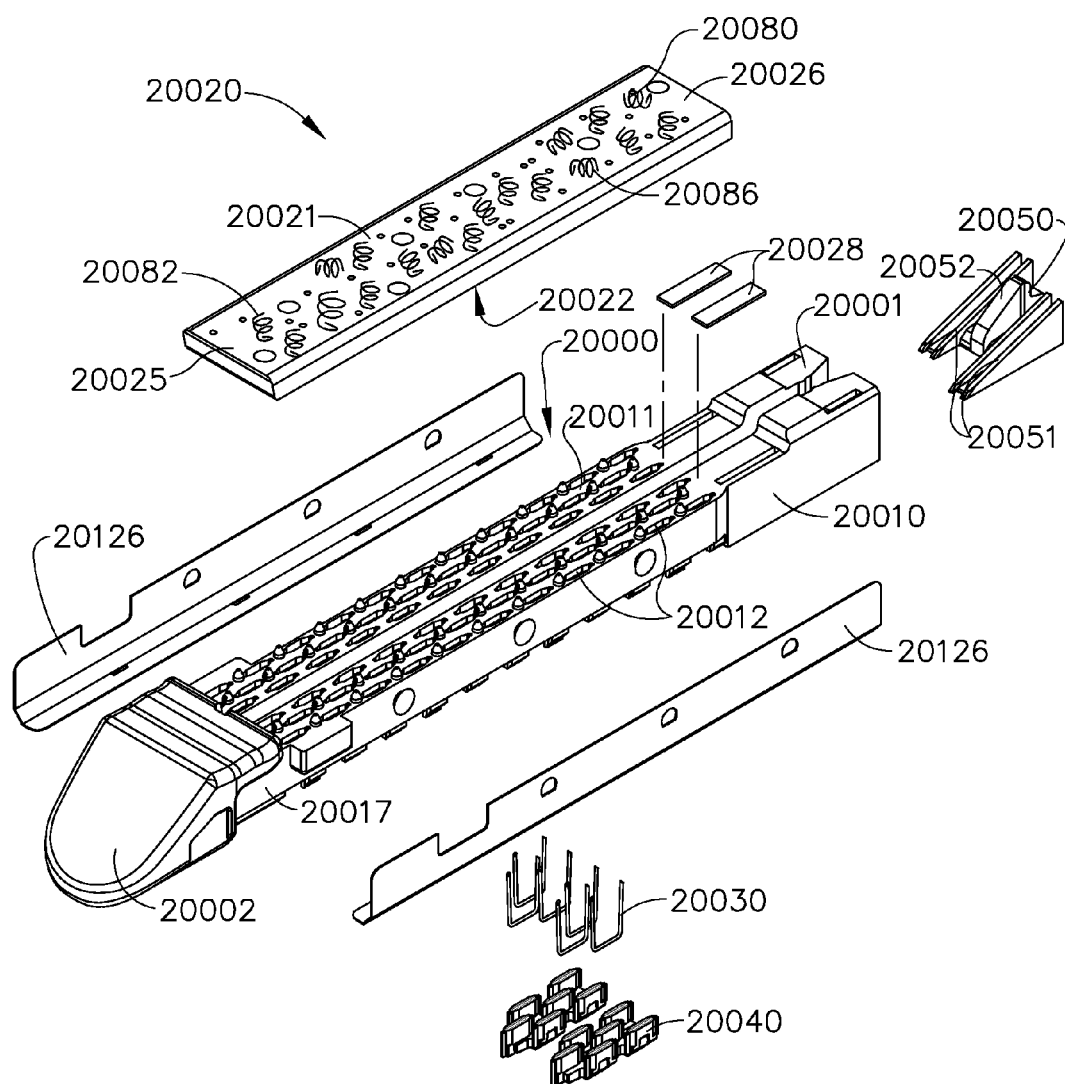


FIG. 78

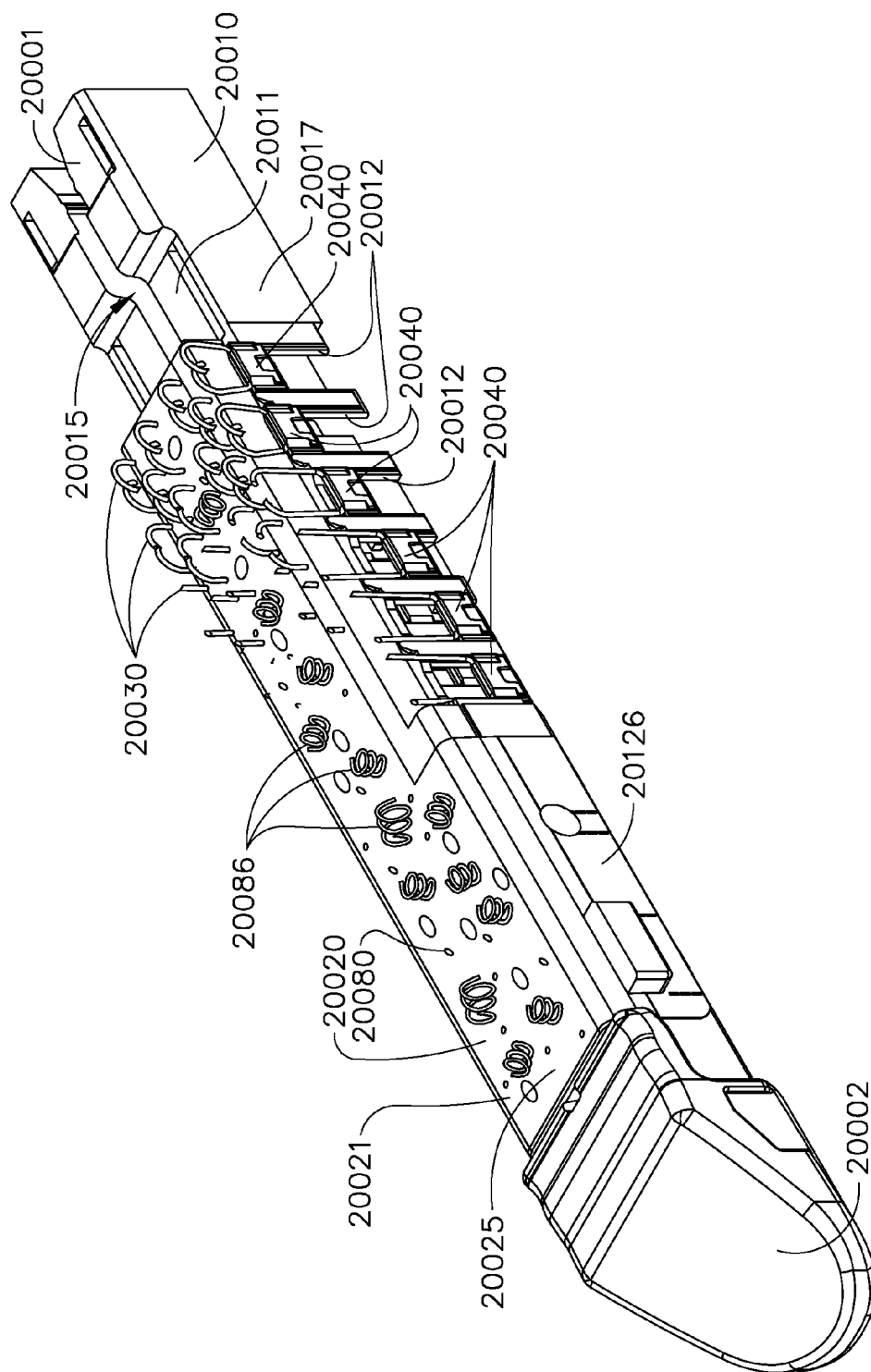


FIG. 79

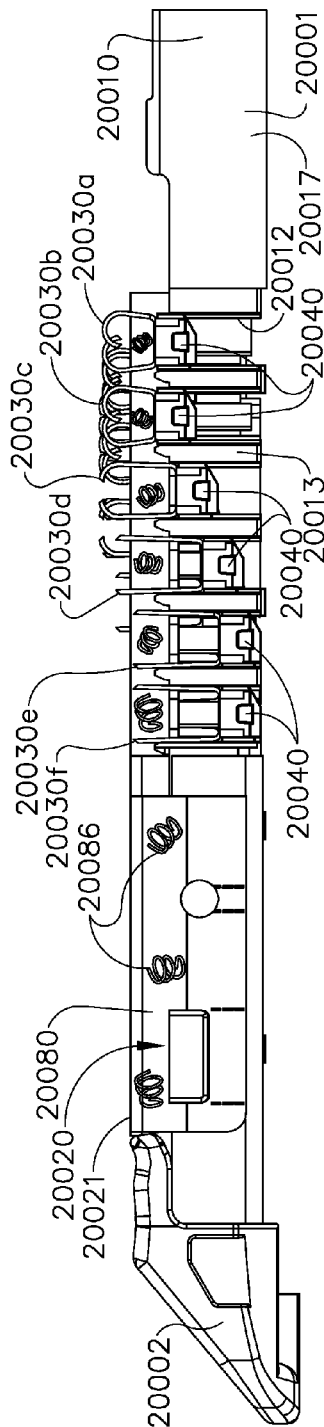


FIG. 80

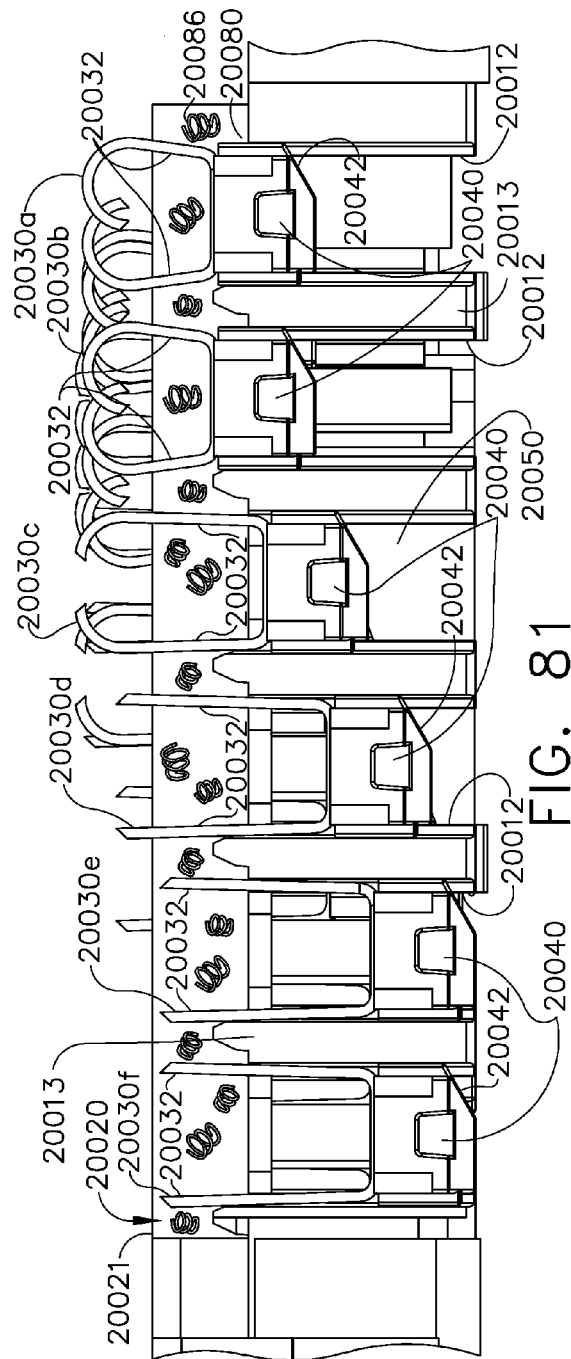


FIG. 81

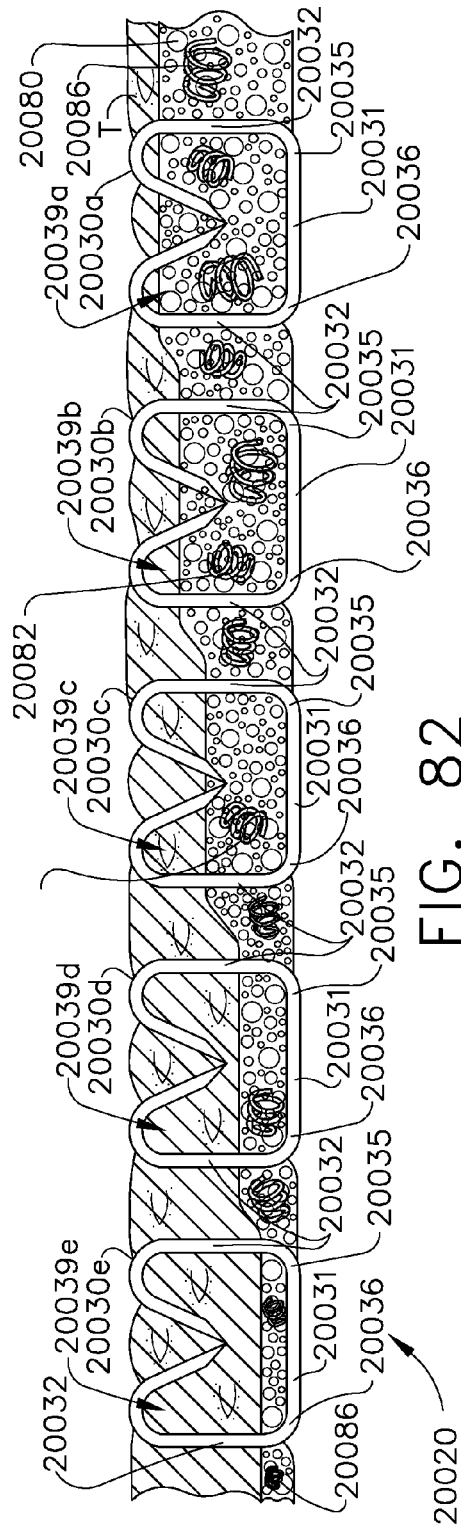


FIG. 82

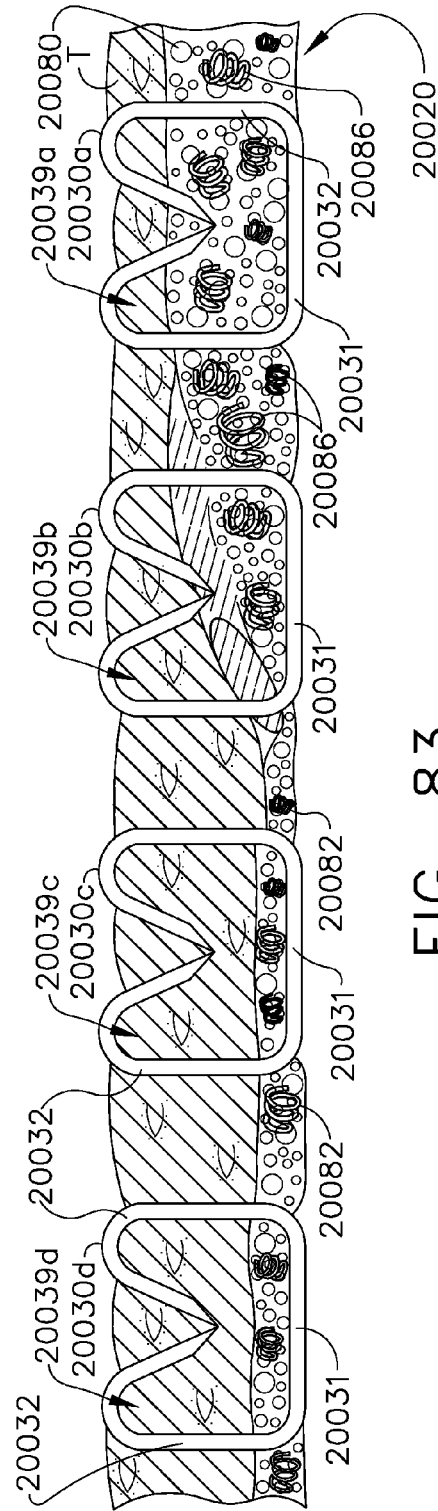
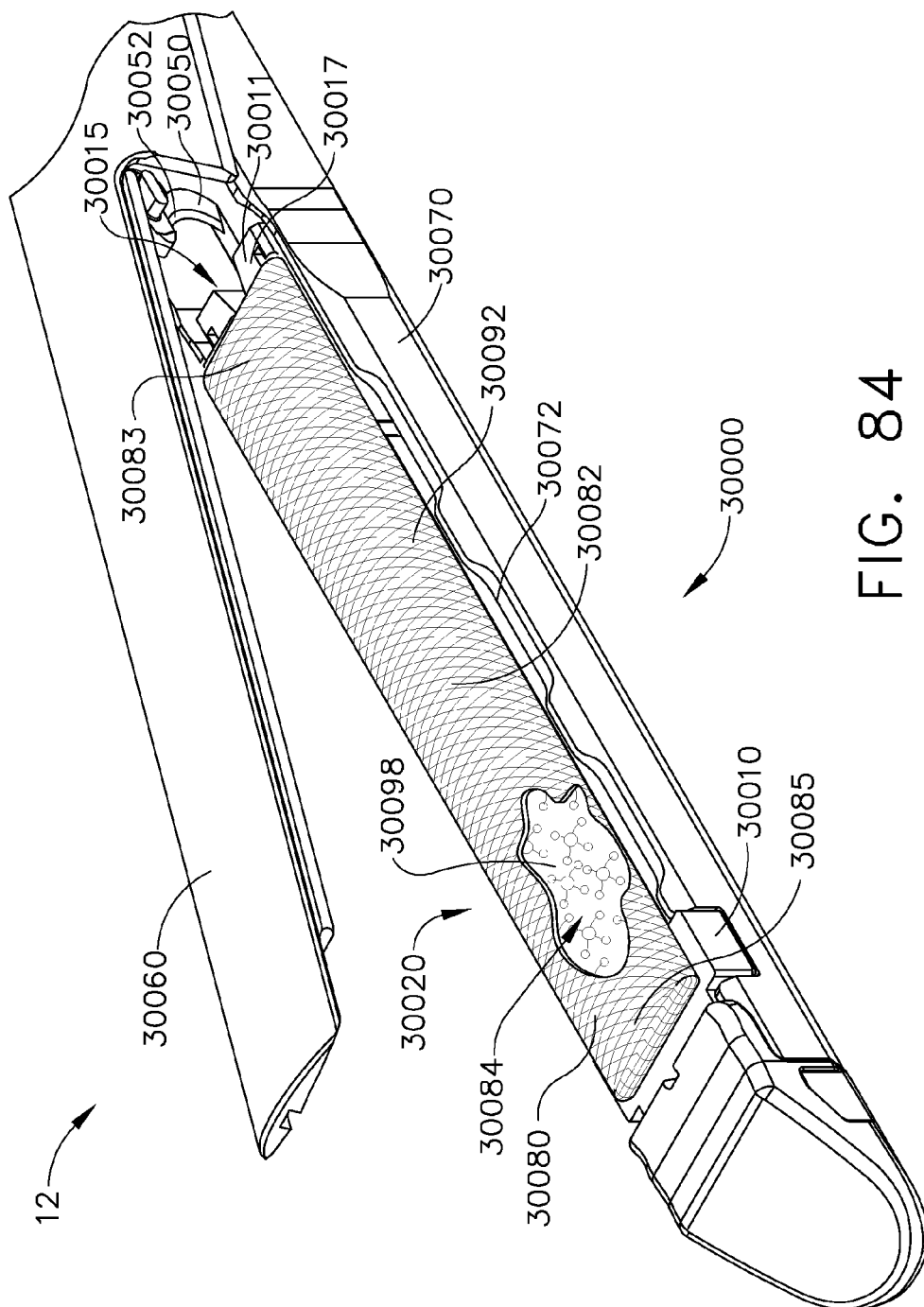


FIG. 83



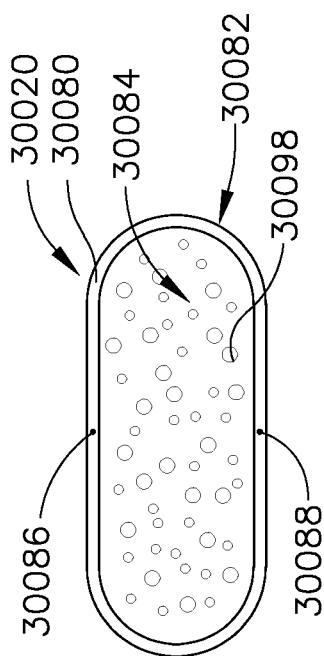
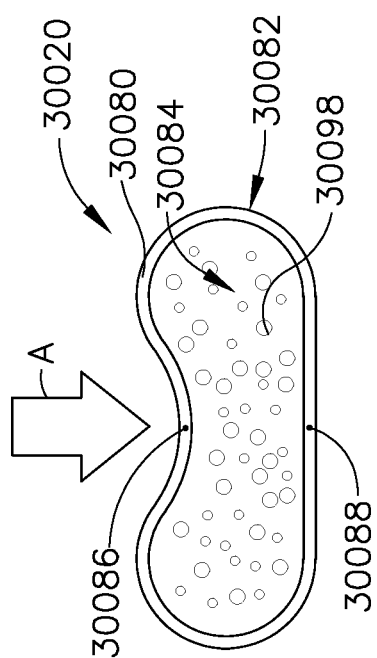


FIG. 85

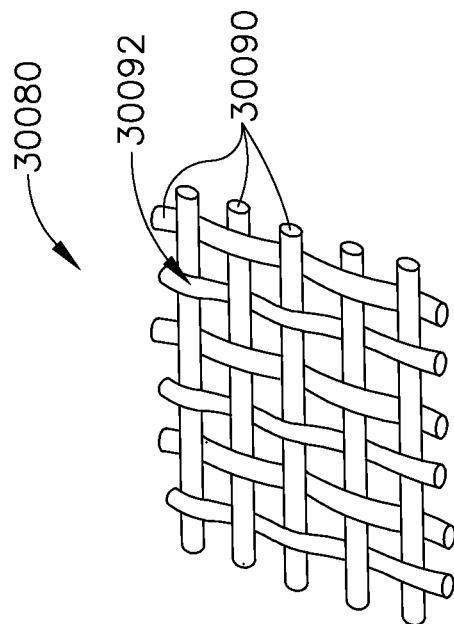


FIG. 86

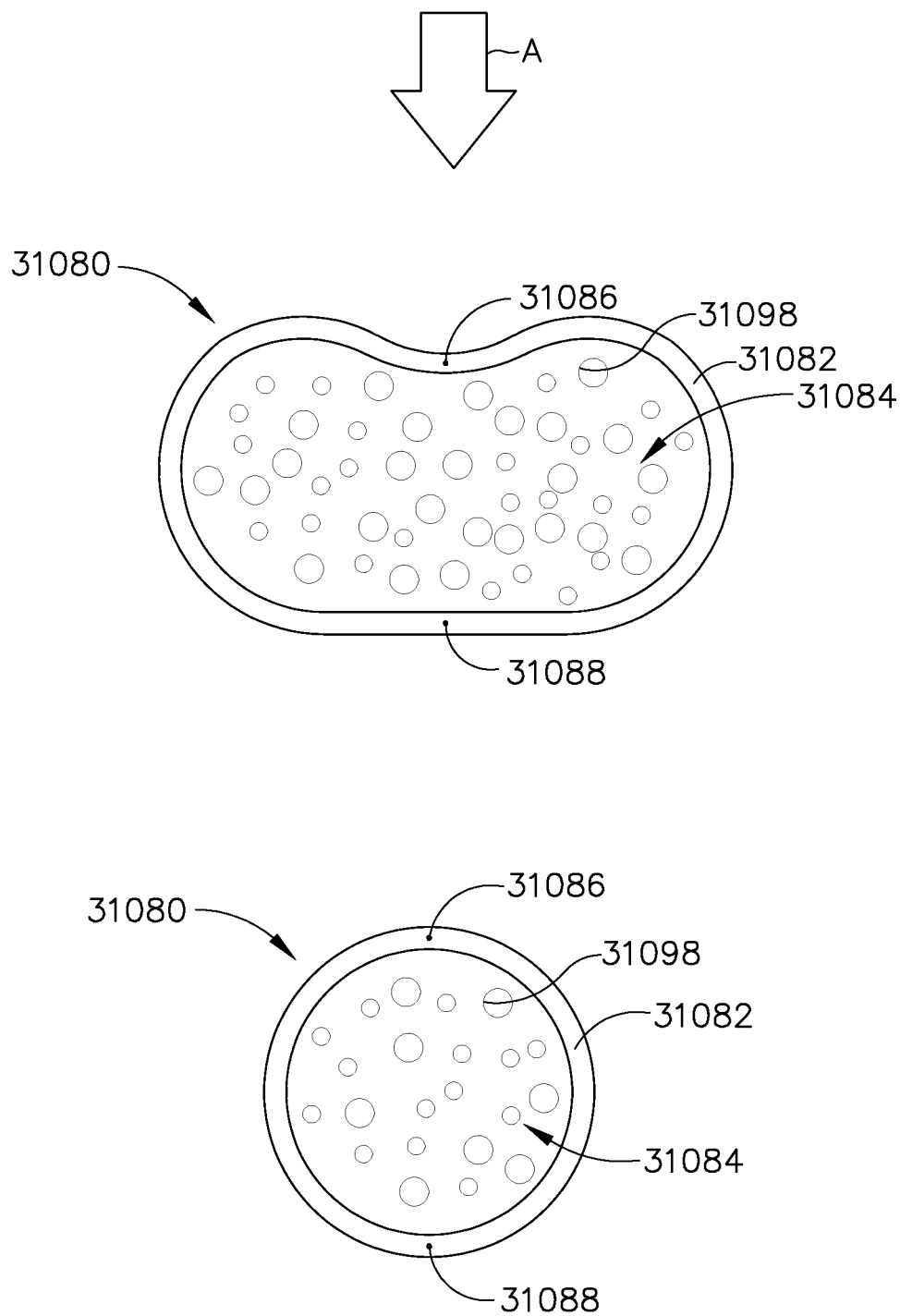


FIG. 87

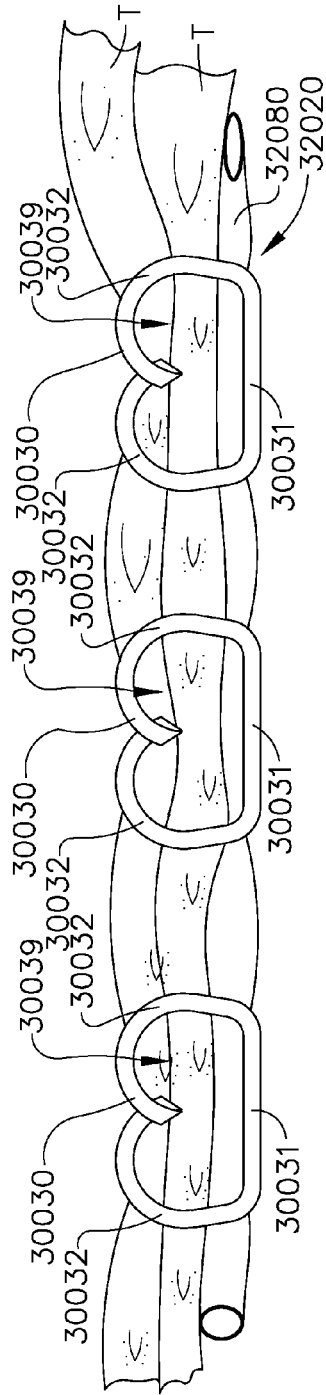


FIG. 88

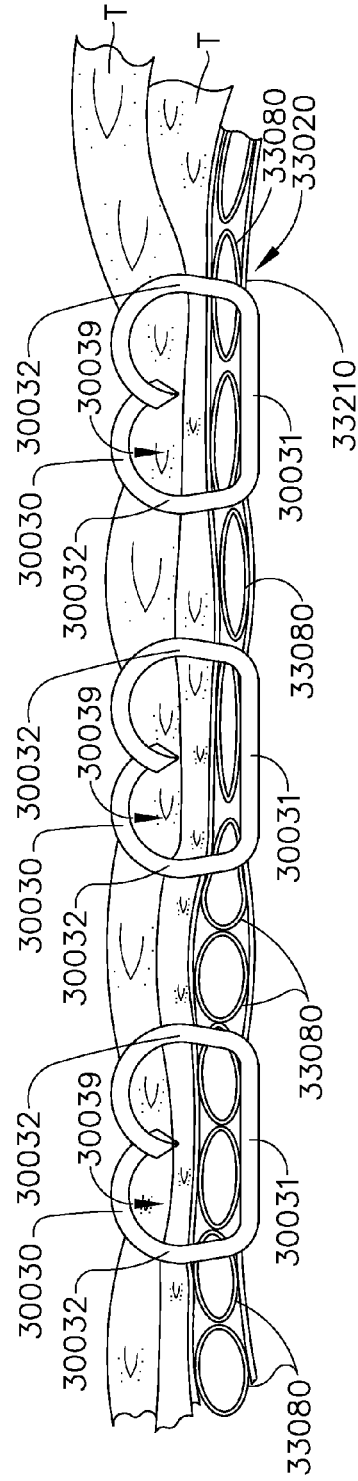


FIG. 89

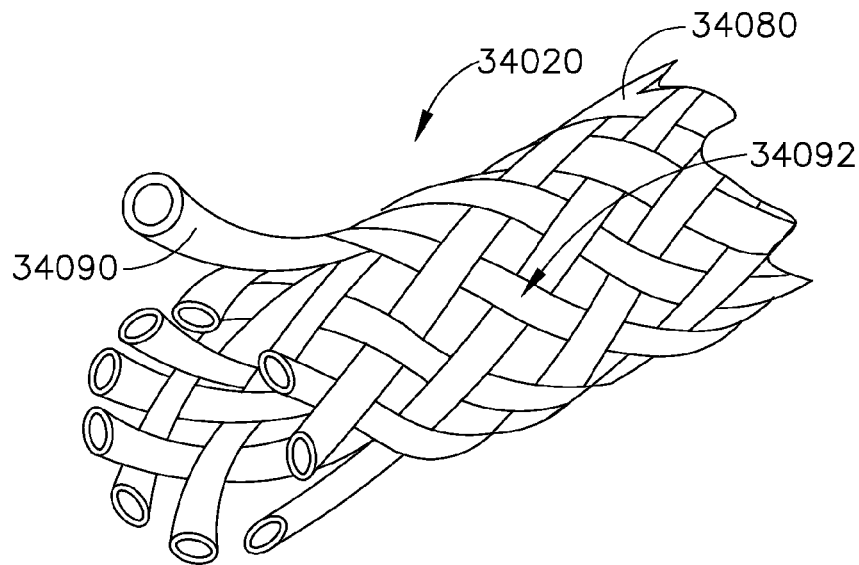


FIG. 90

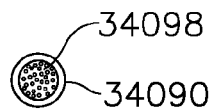


FIG. 91

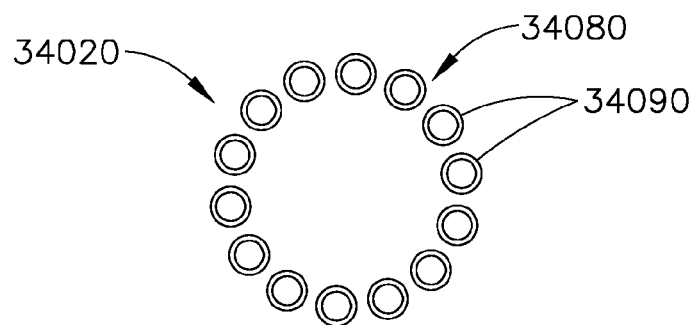


FIG. 92

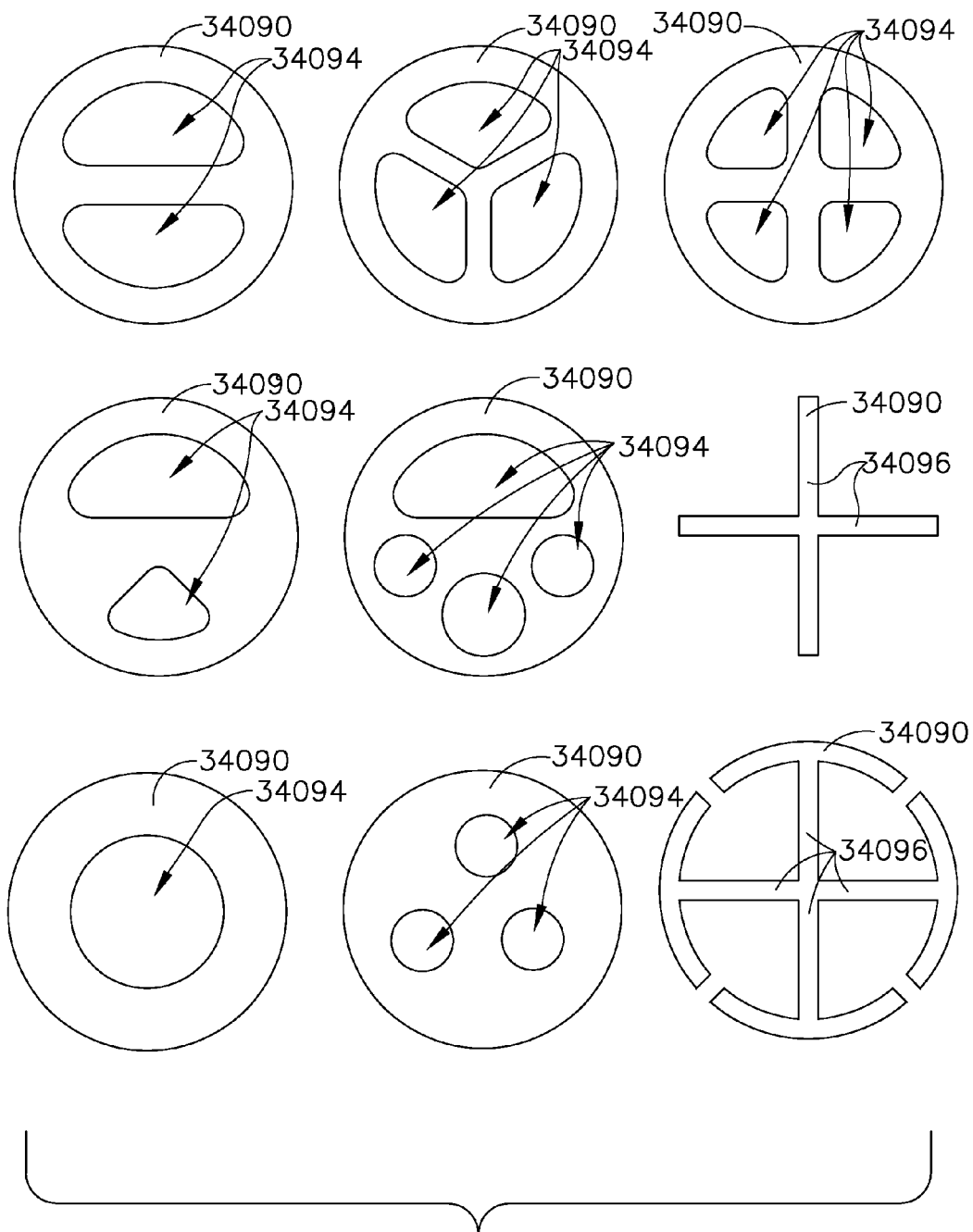


FIG. 93

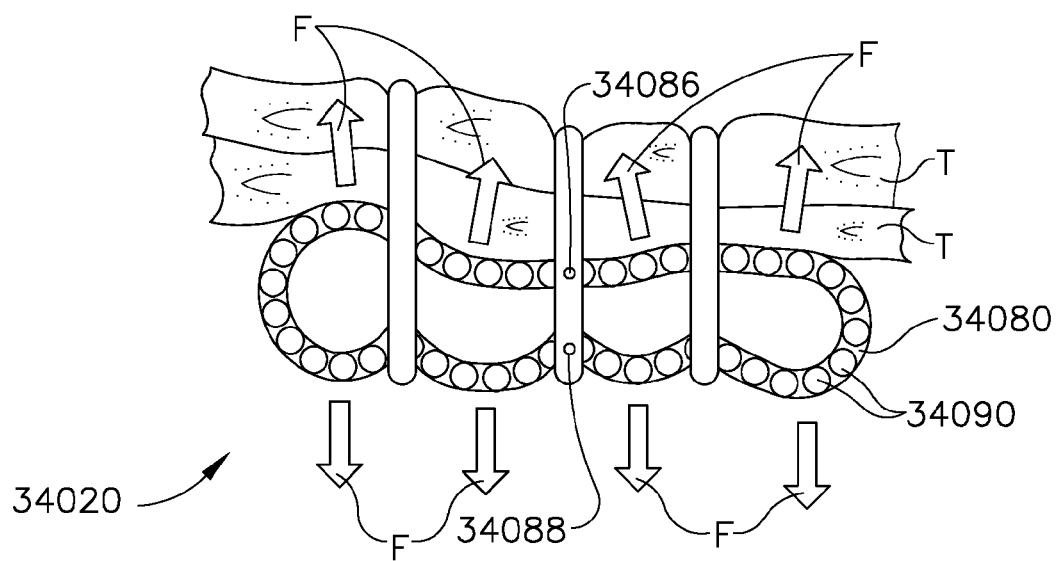
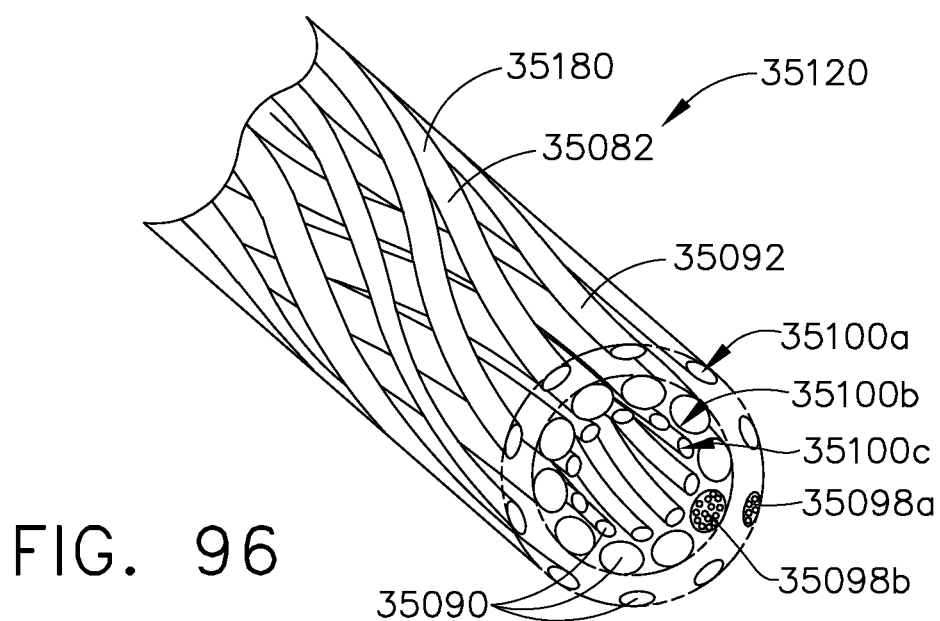
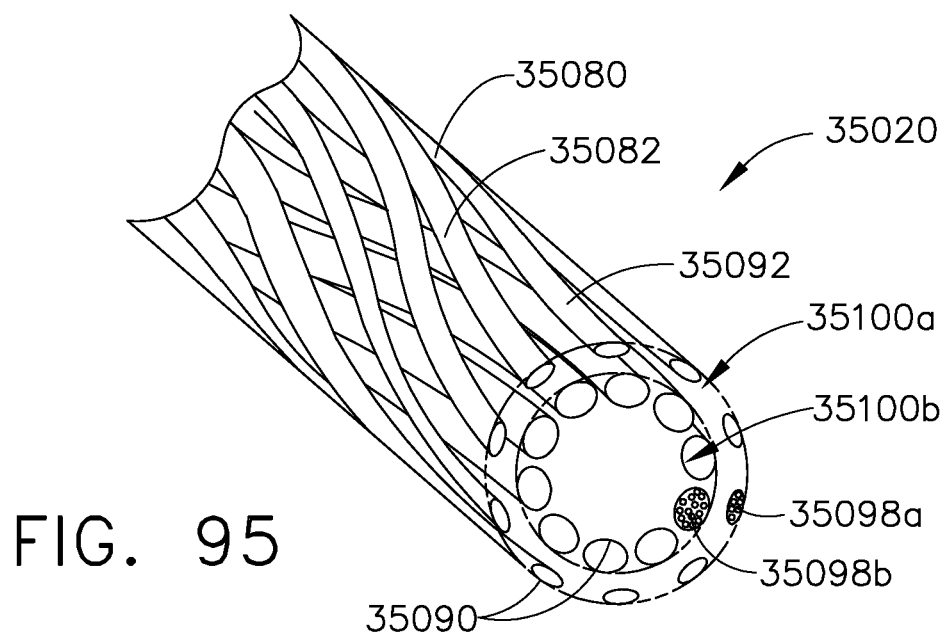


FIG.94



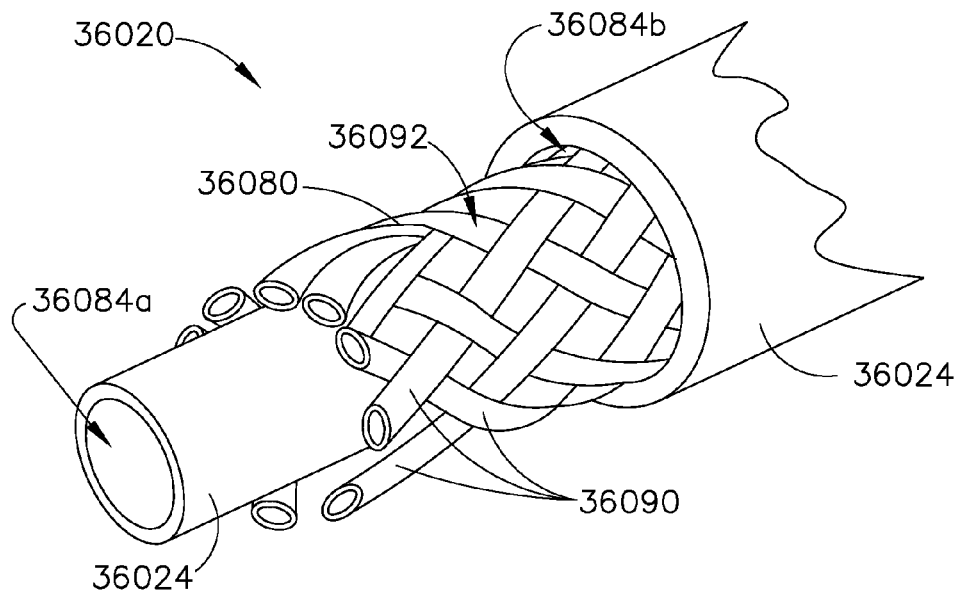


FIG. 97

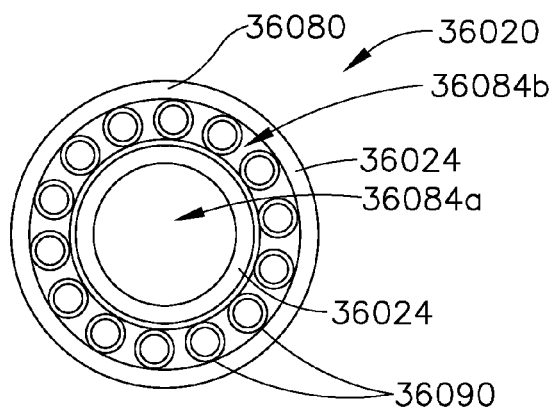
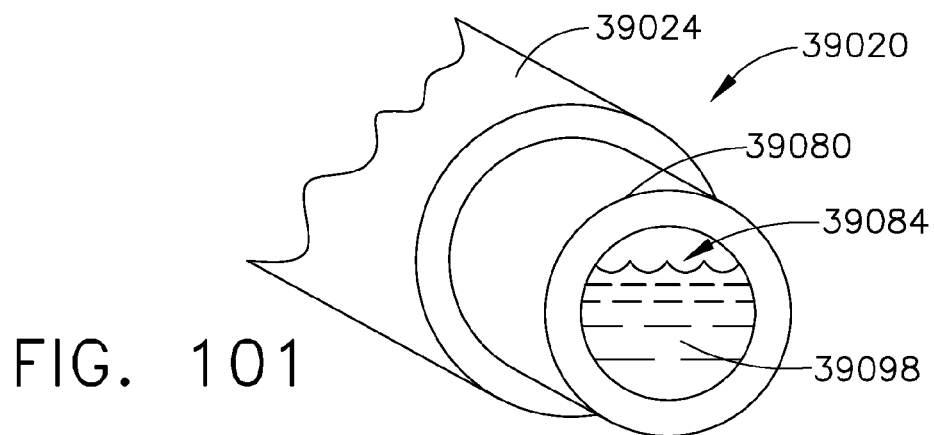
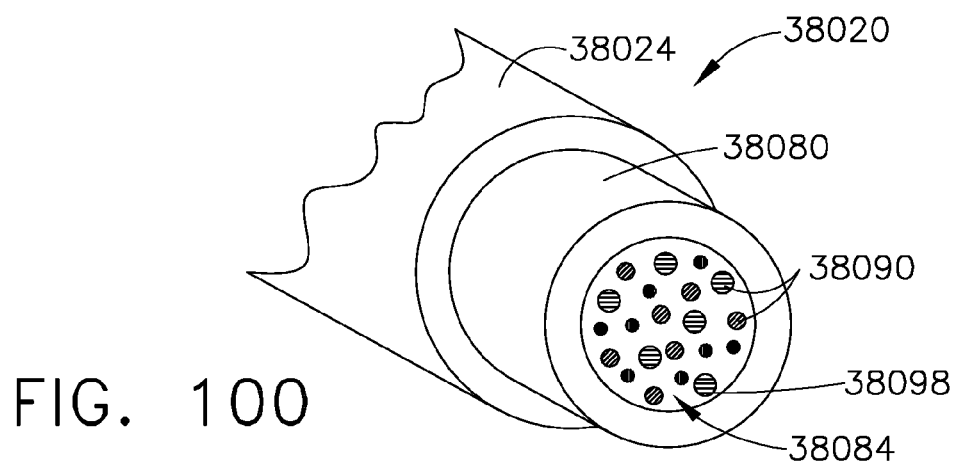
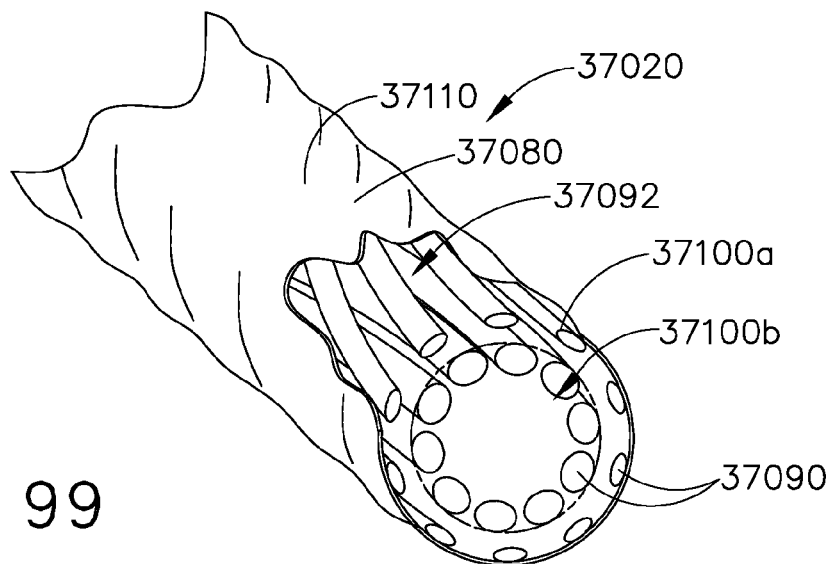


FIG. 98



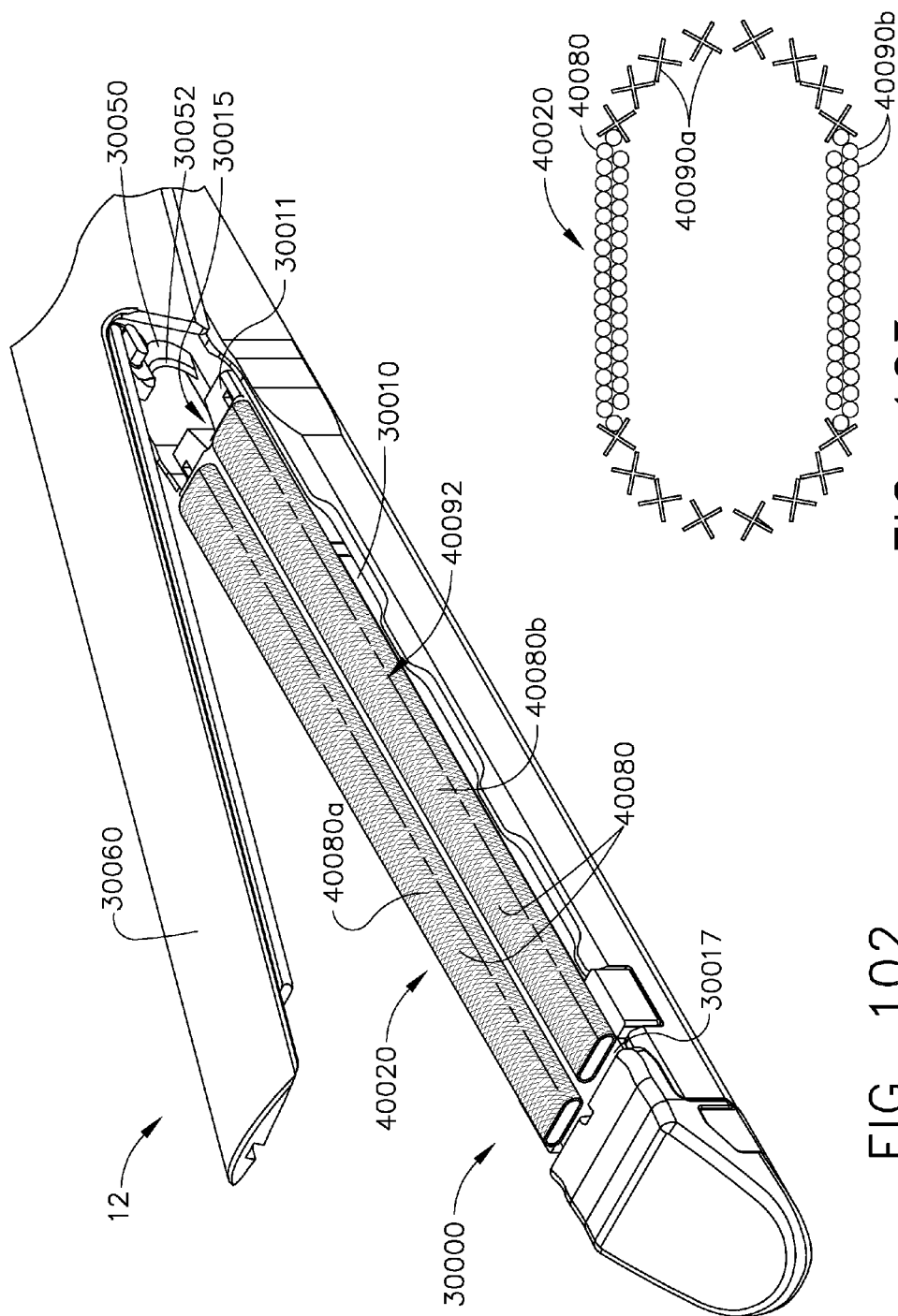


FIG. 103

FIG. 102

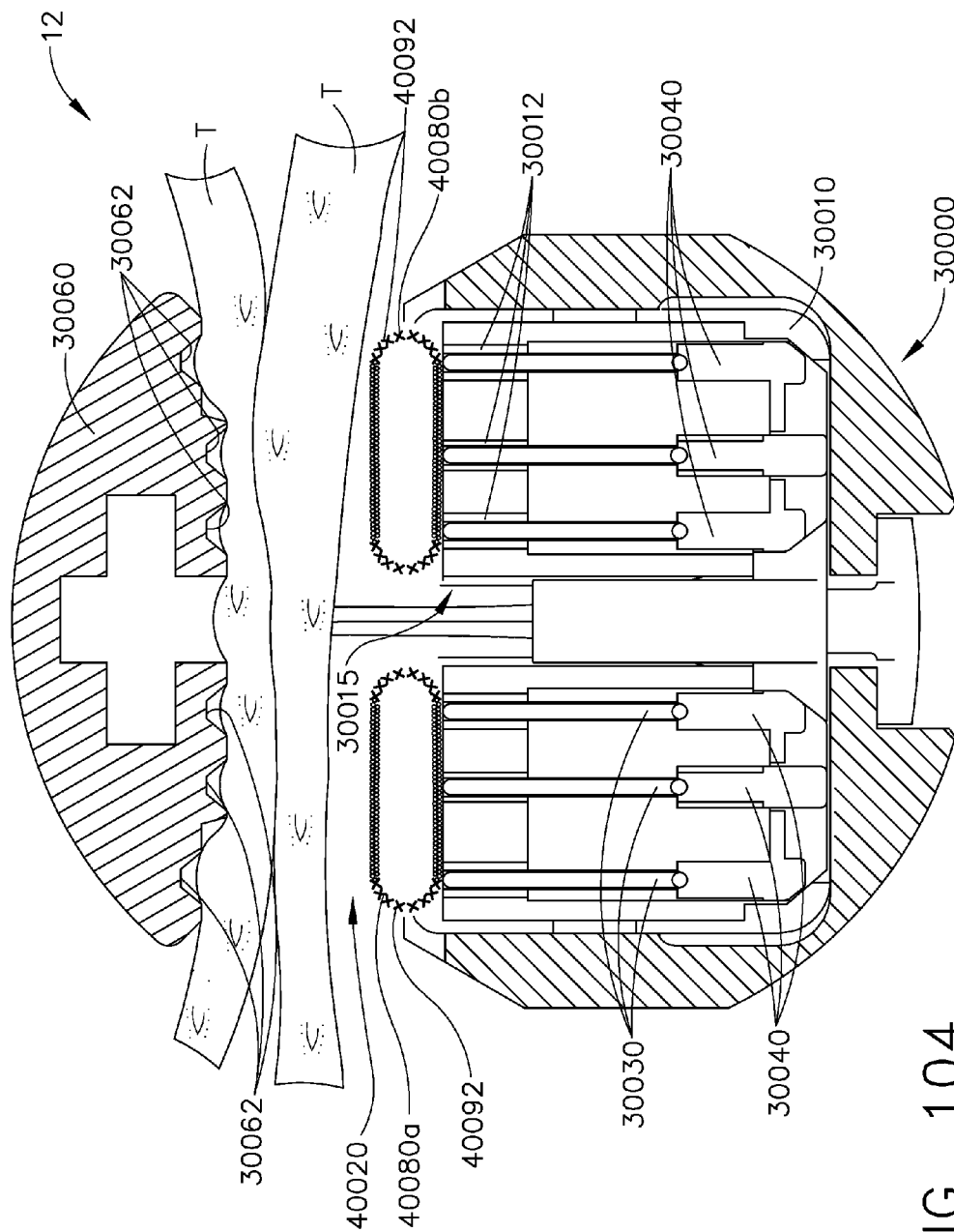


FIG. 104

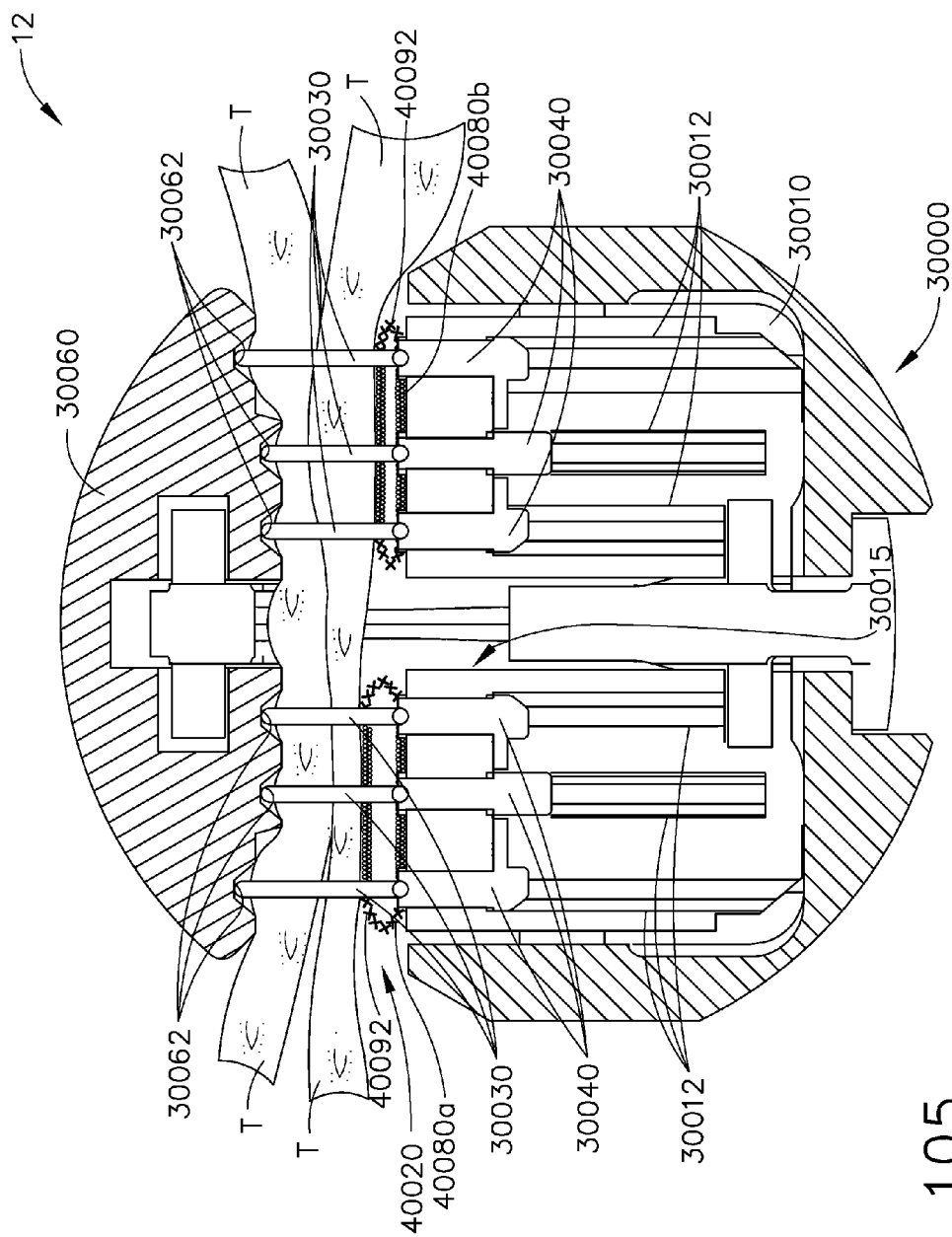


FIG. 105

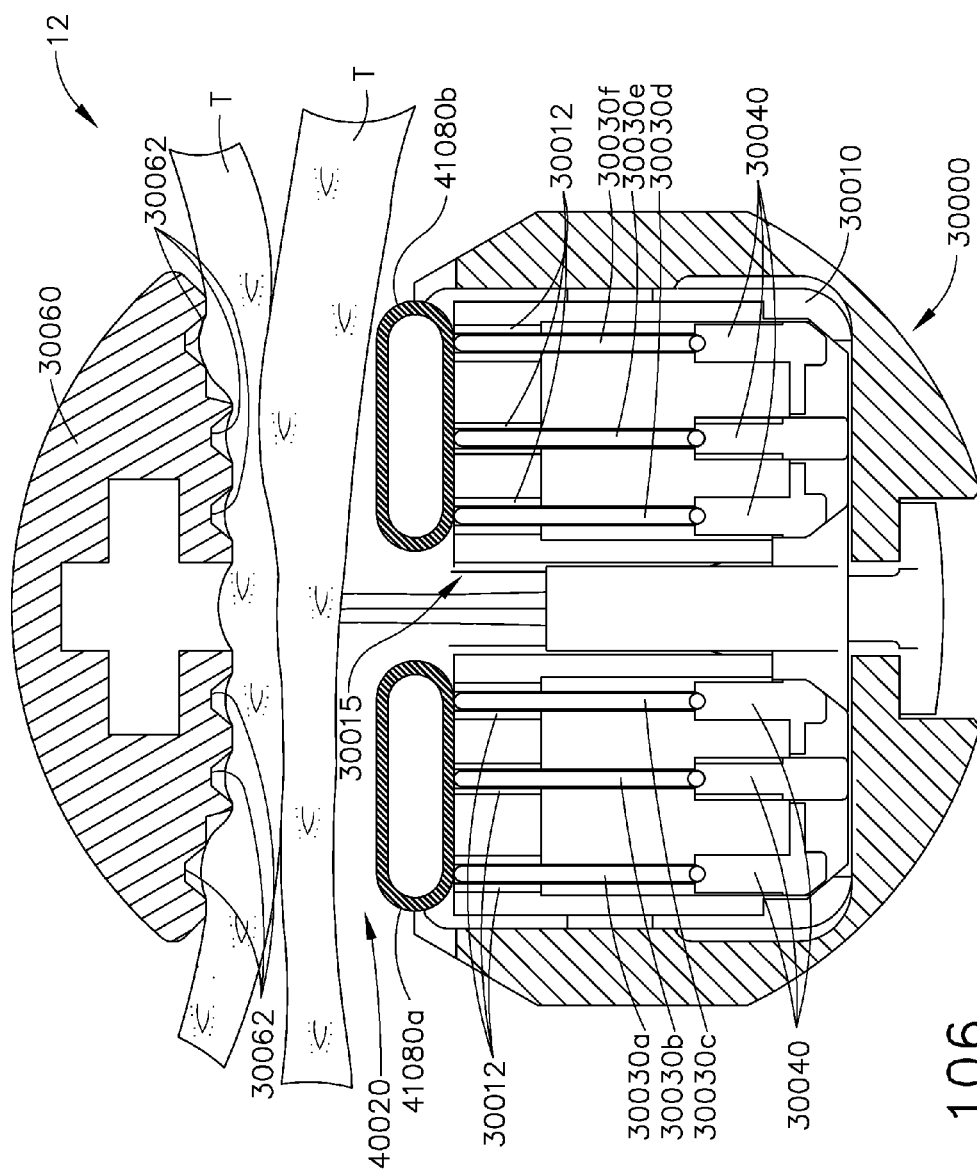


FIG. 106

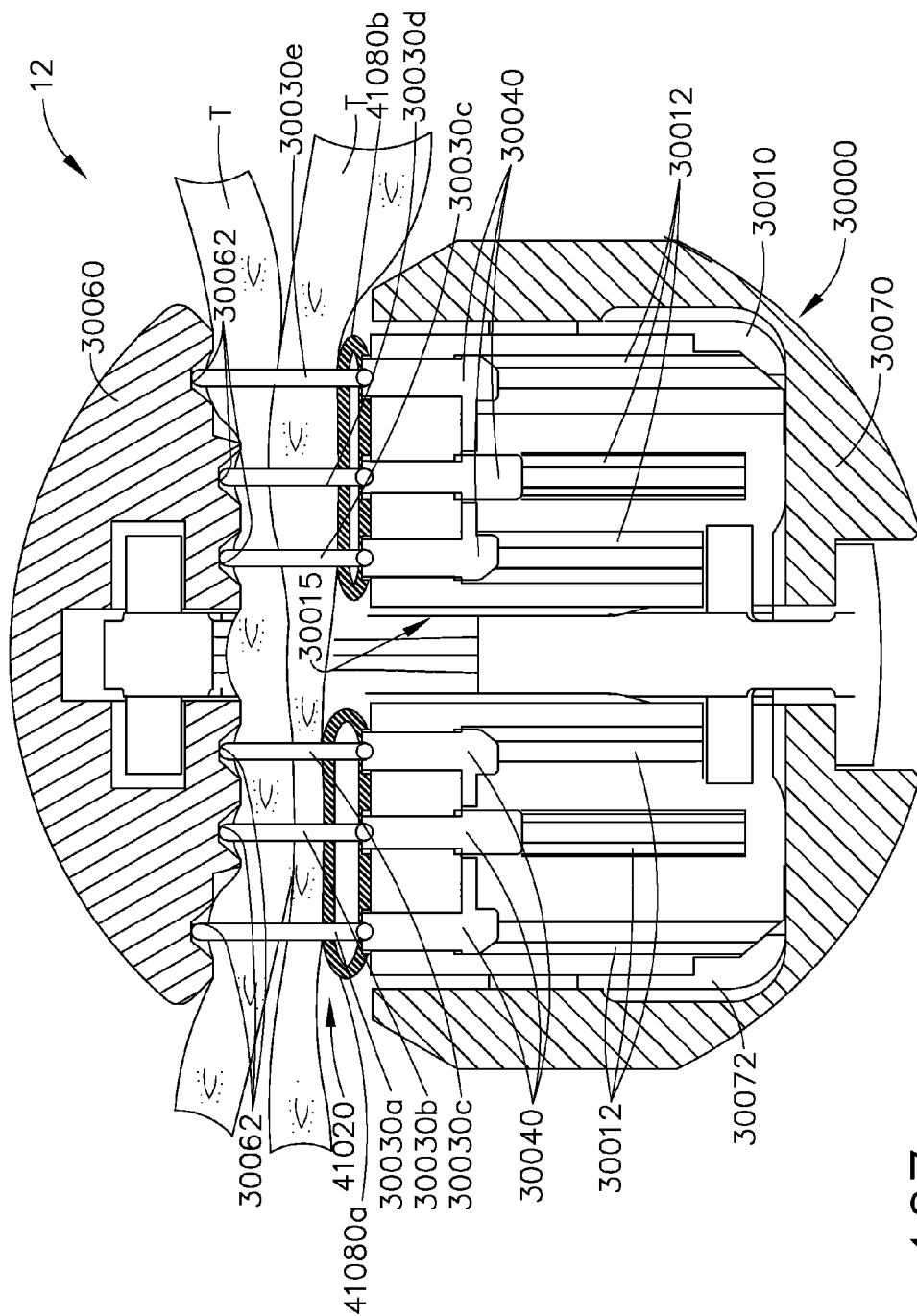


FIG. 107

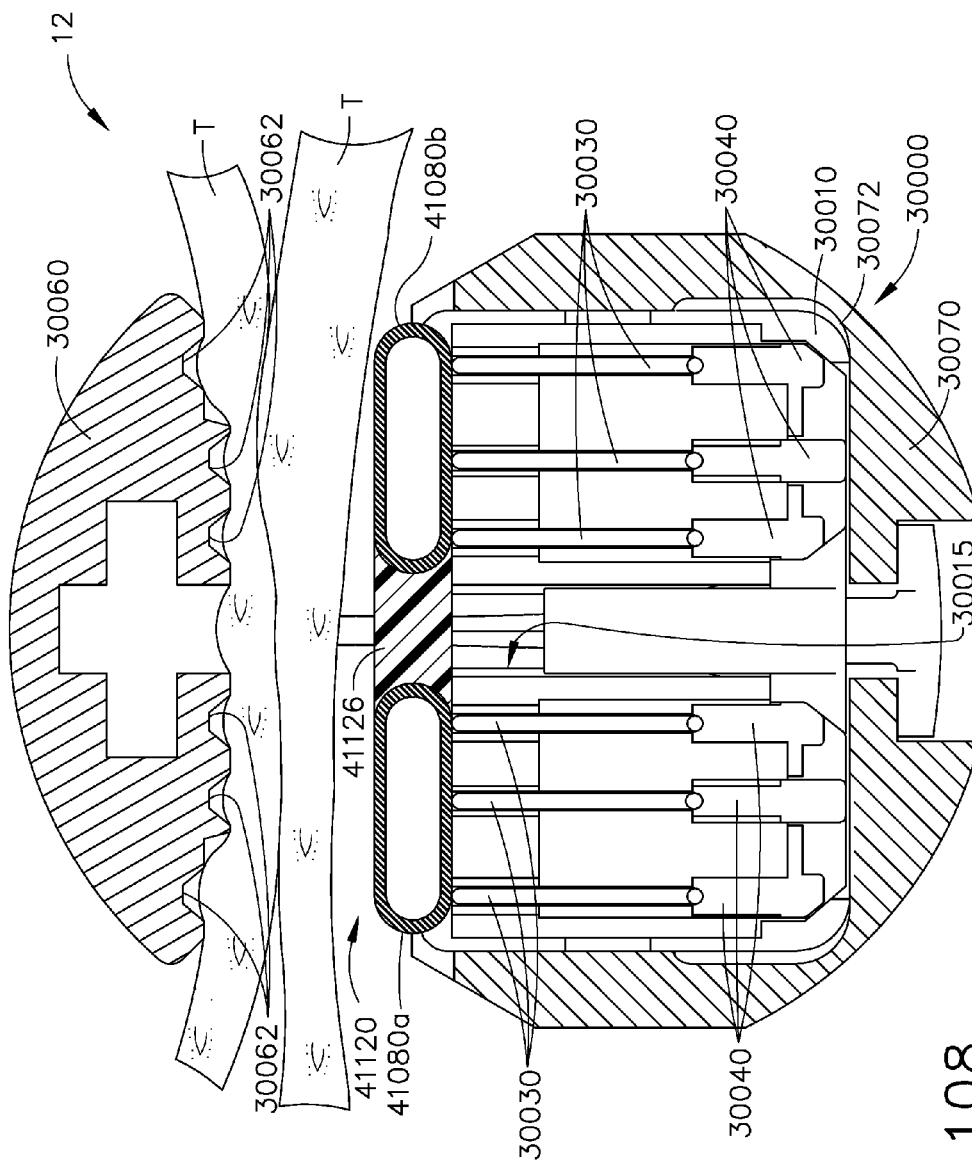


FIG. 108

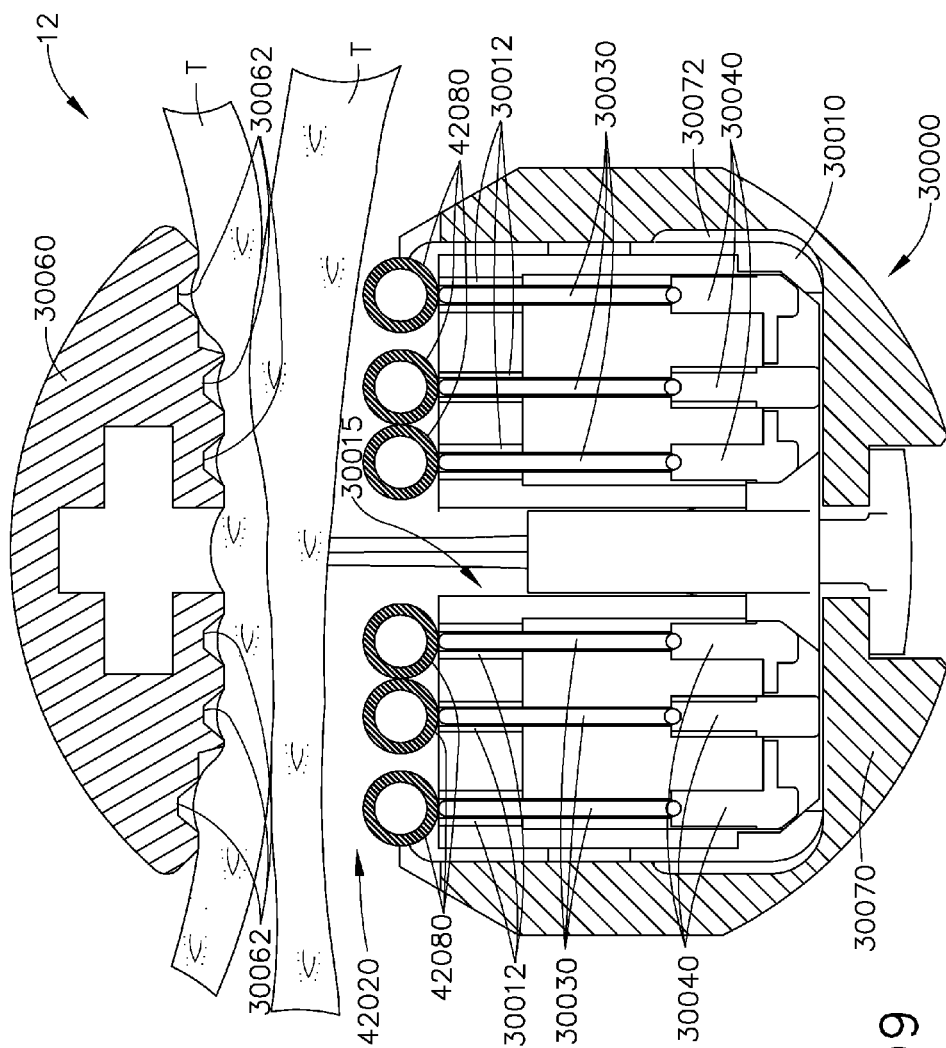


FIG. 109

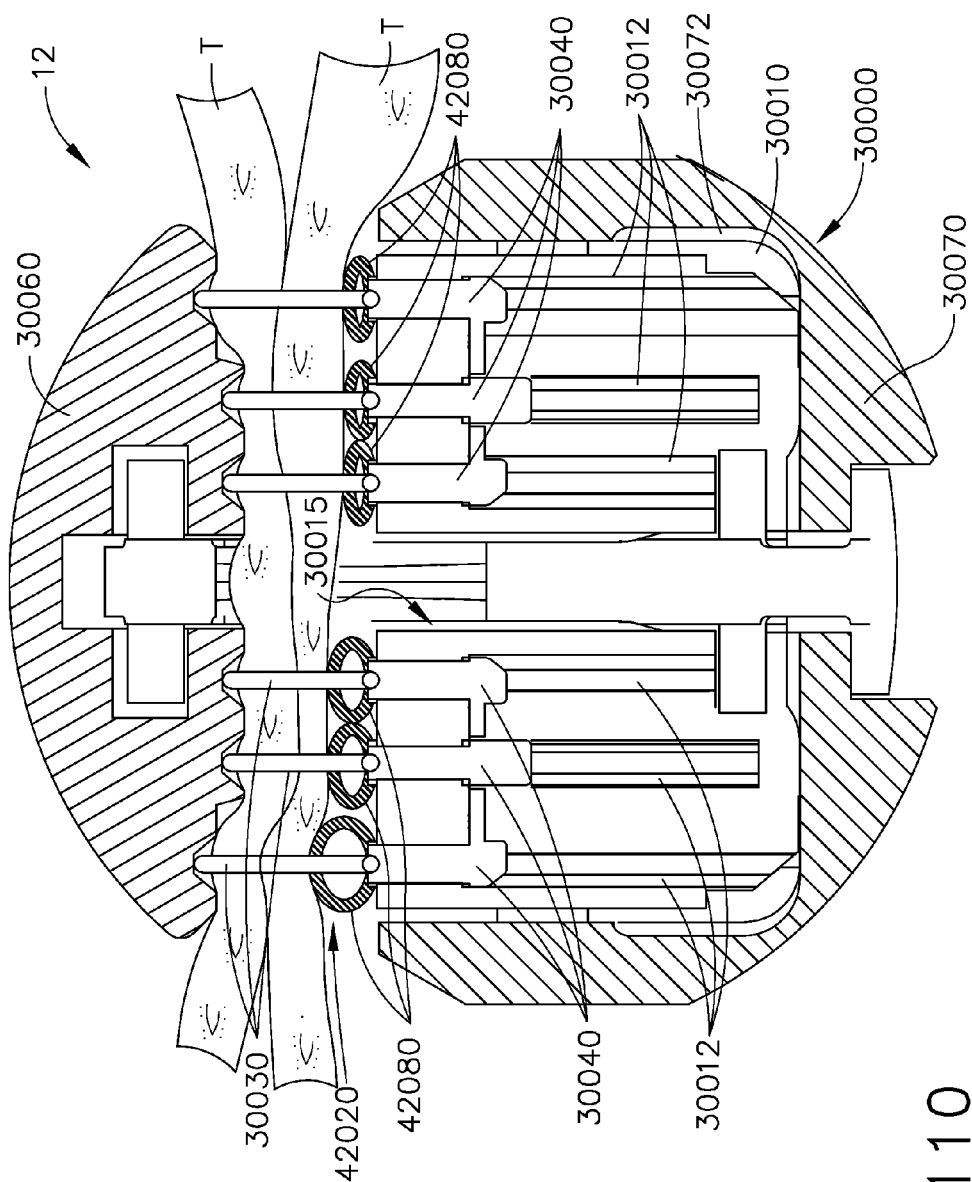
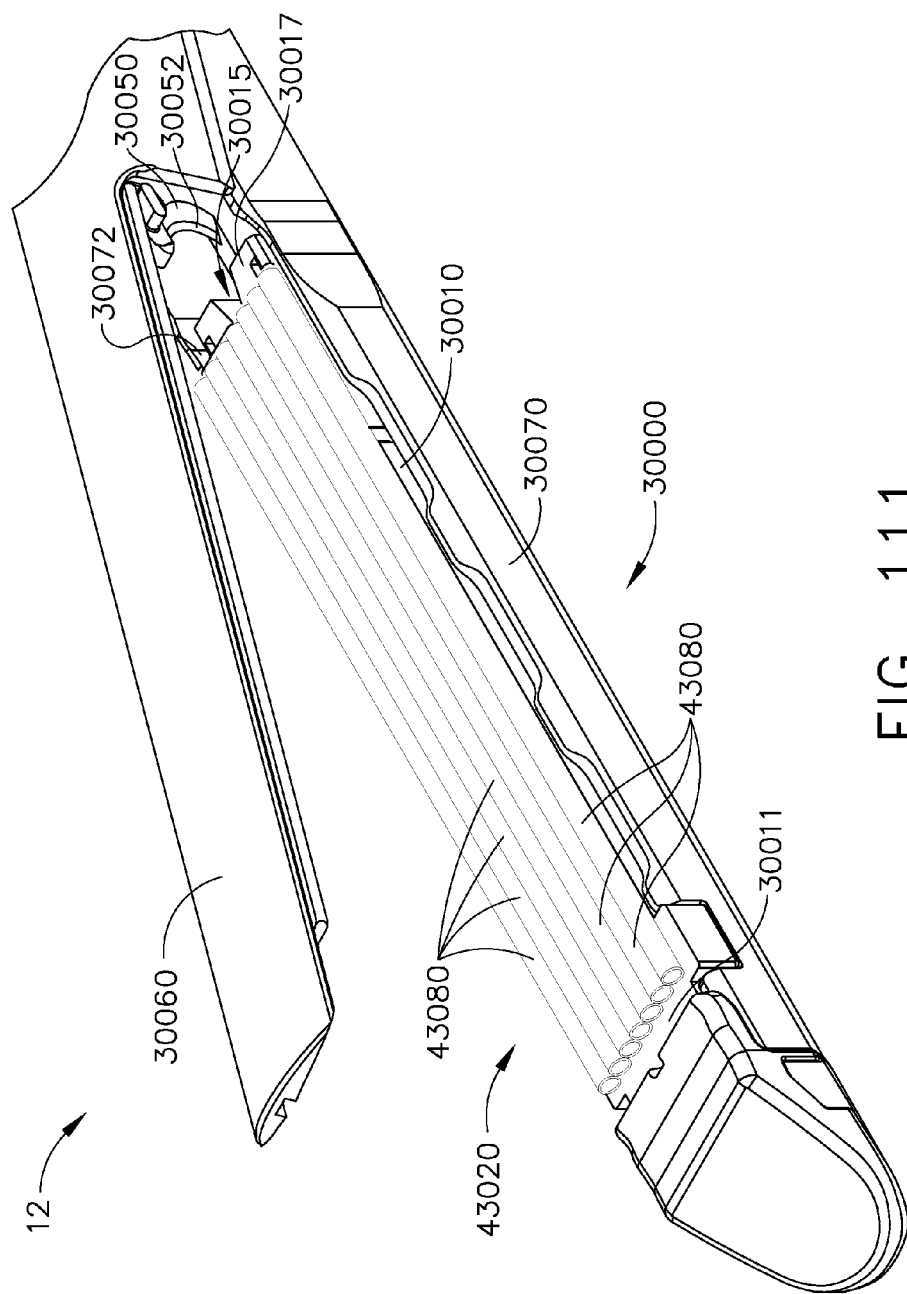


FIG. 110



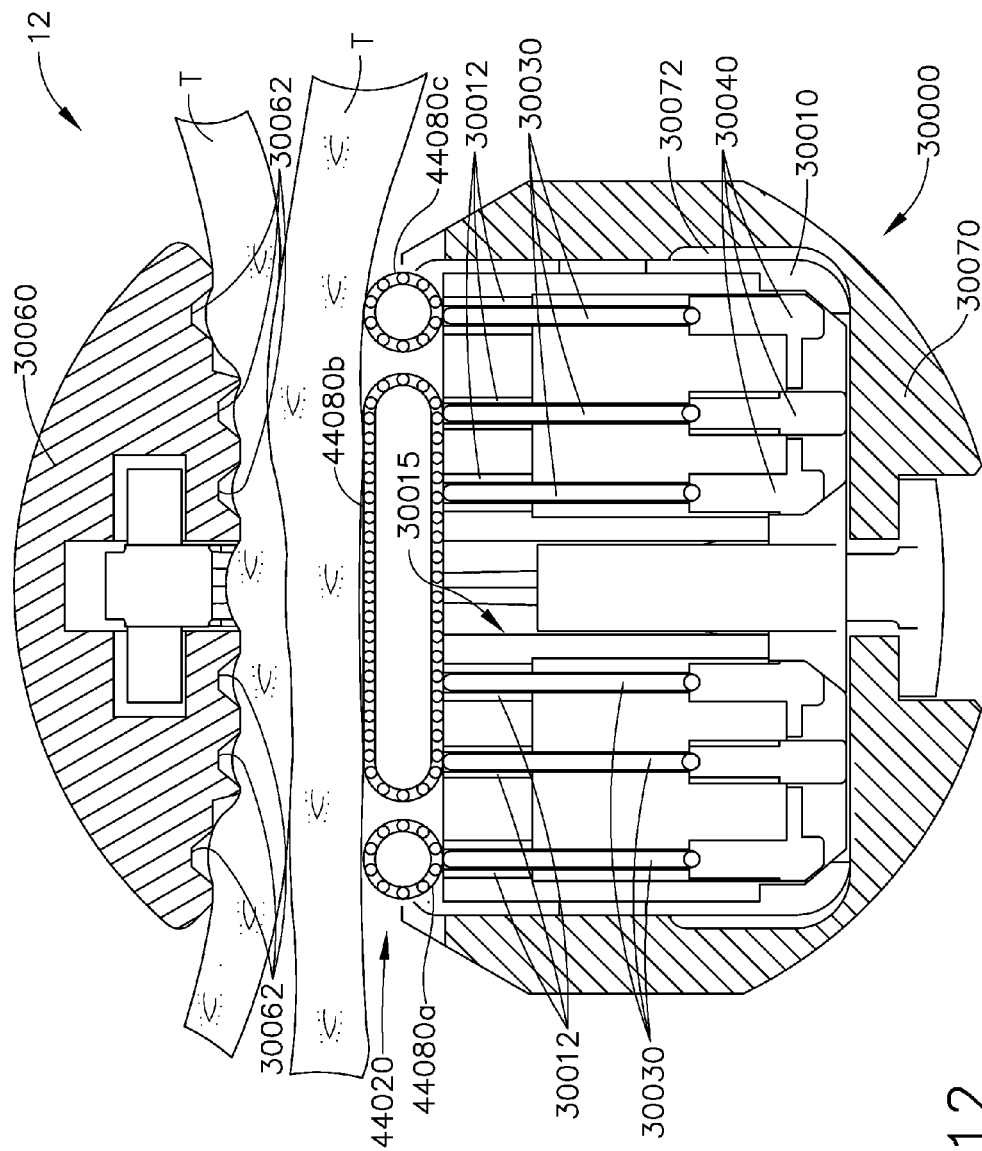


FIG. 112

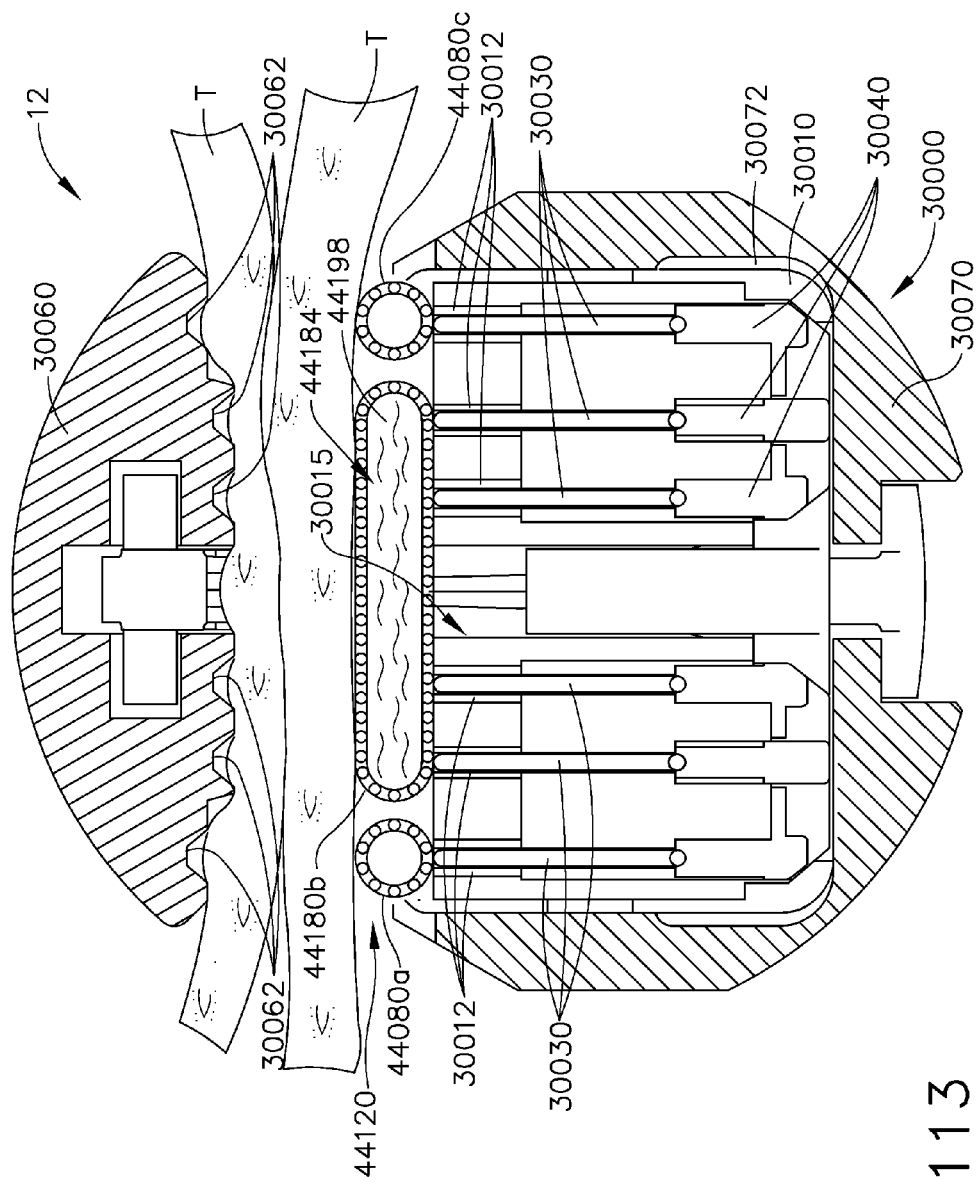


FIG. 113

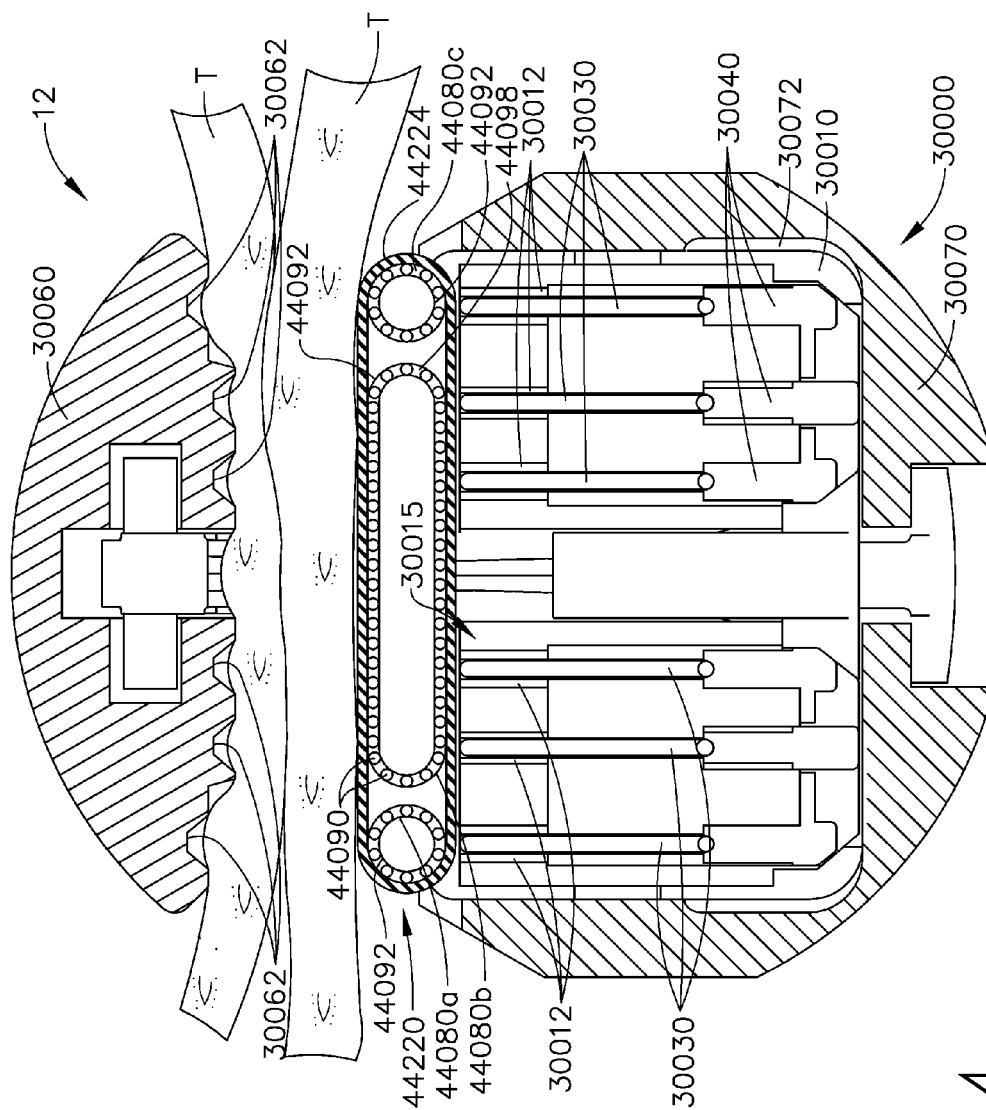


FIG. 114

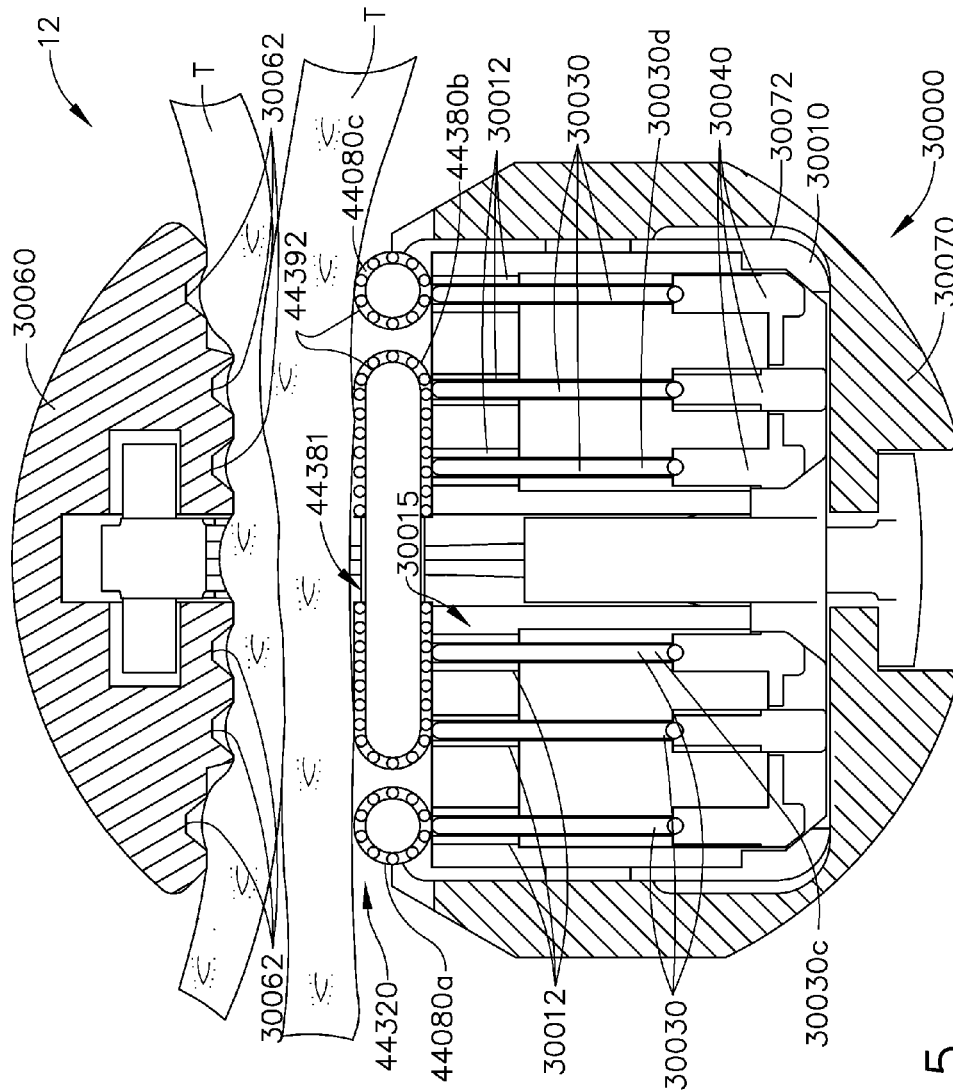


FIG. 115

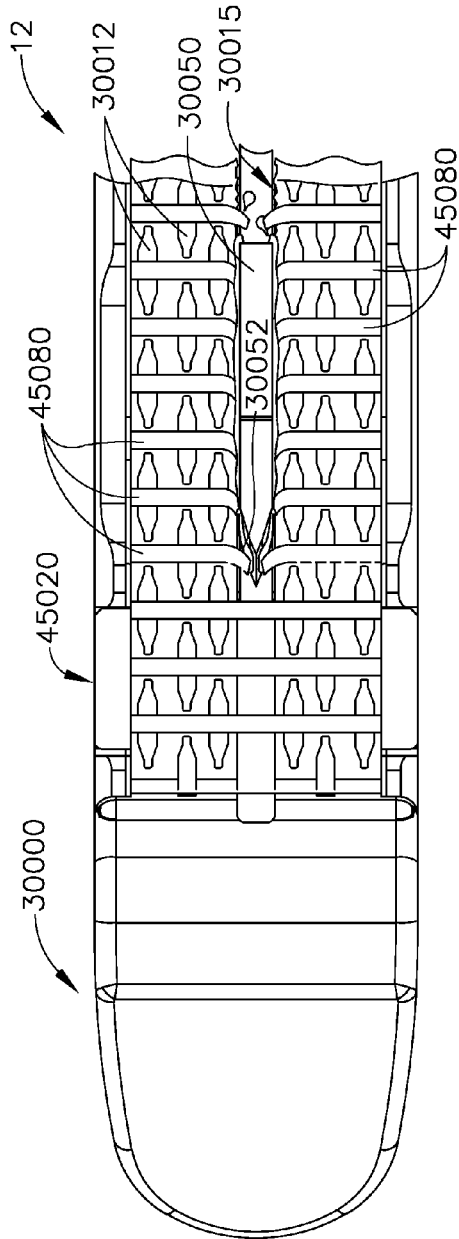


FIG. 116

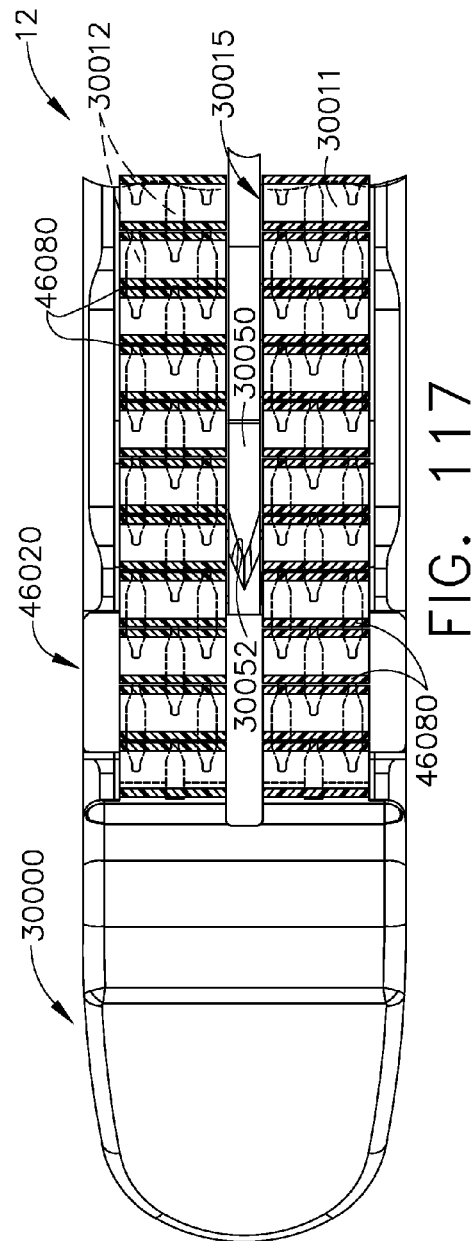
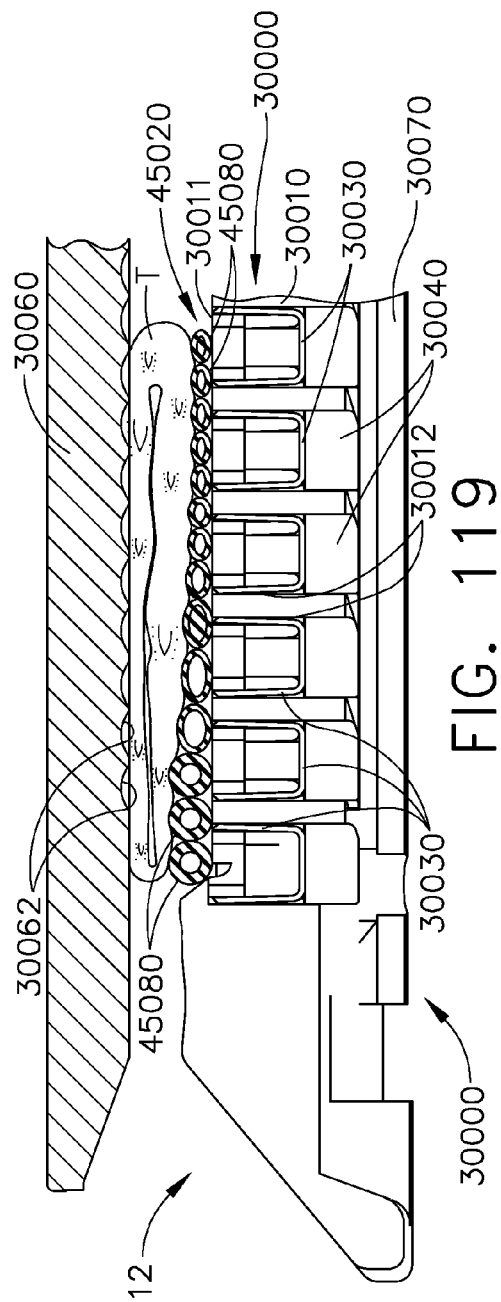
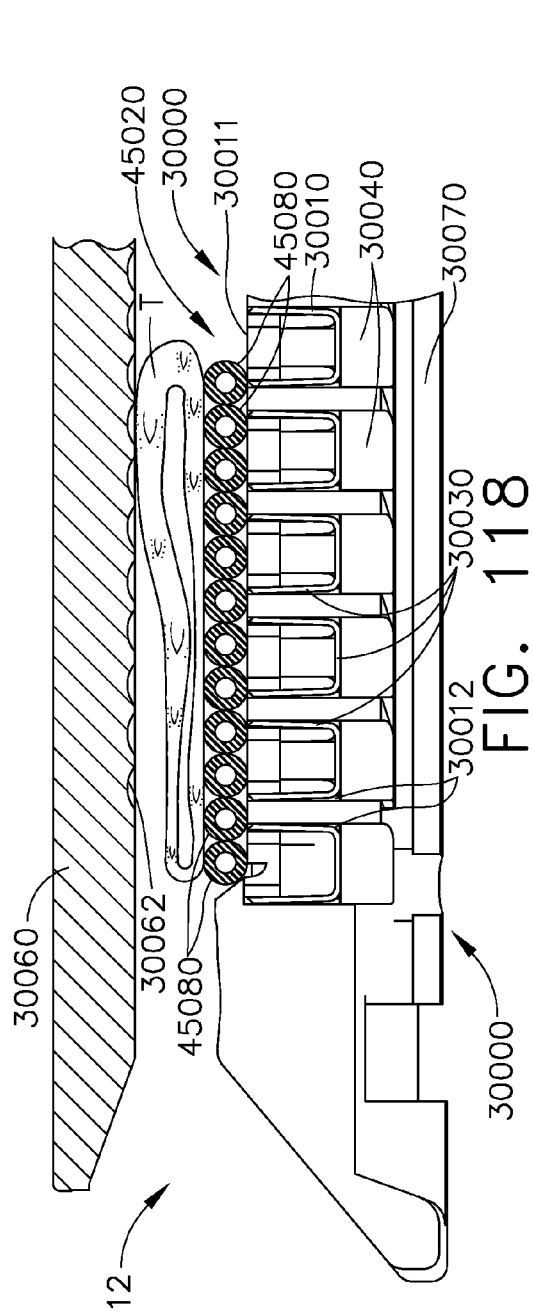
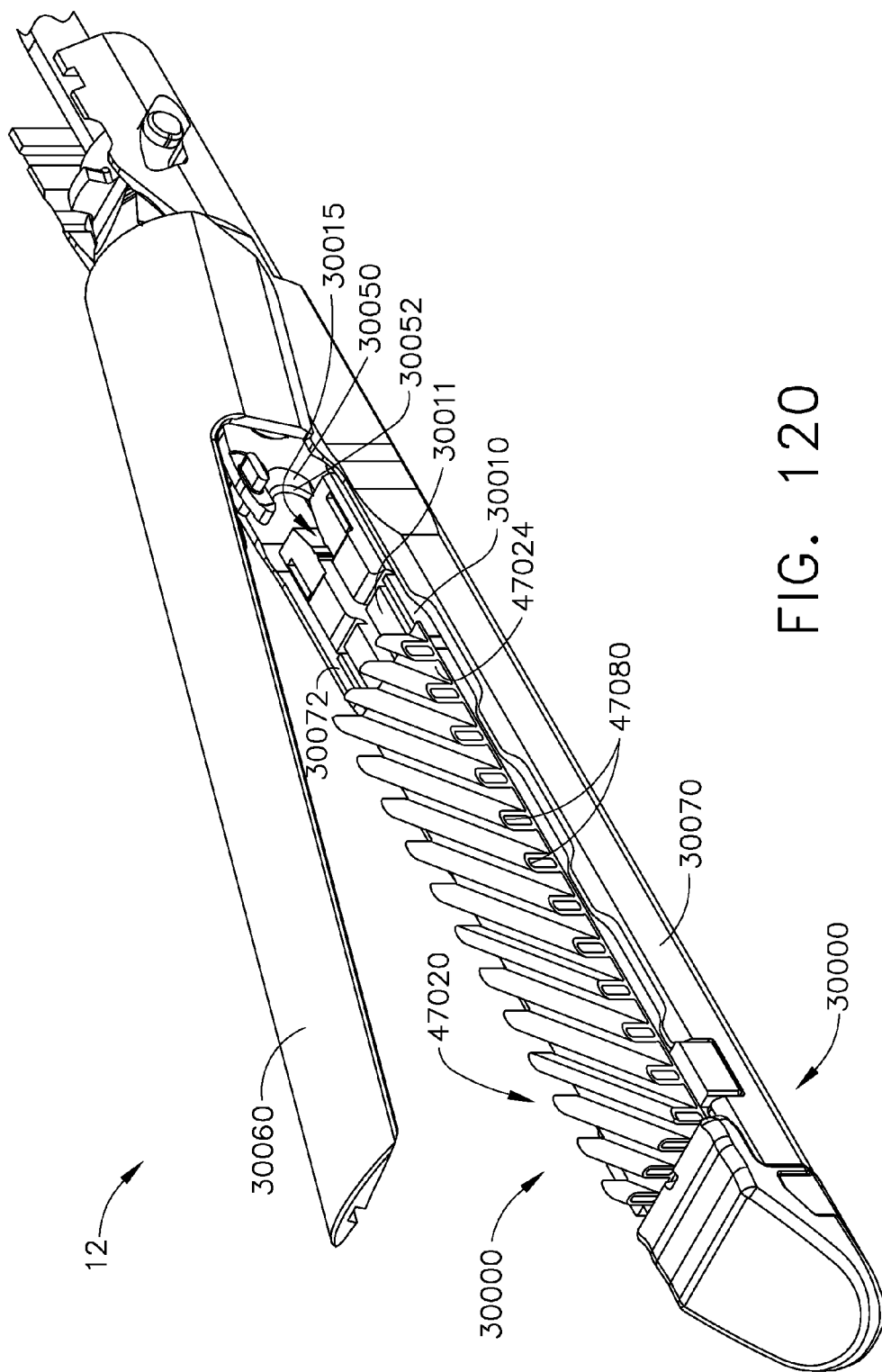


FIG. 117





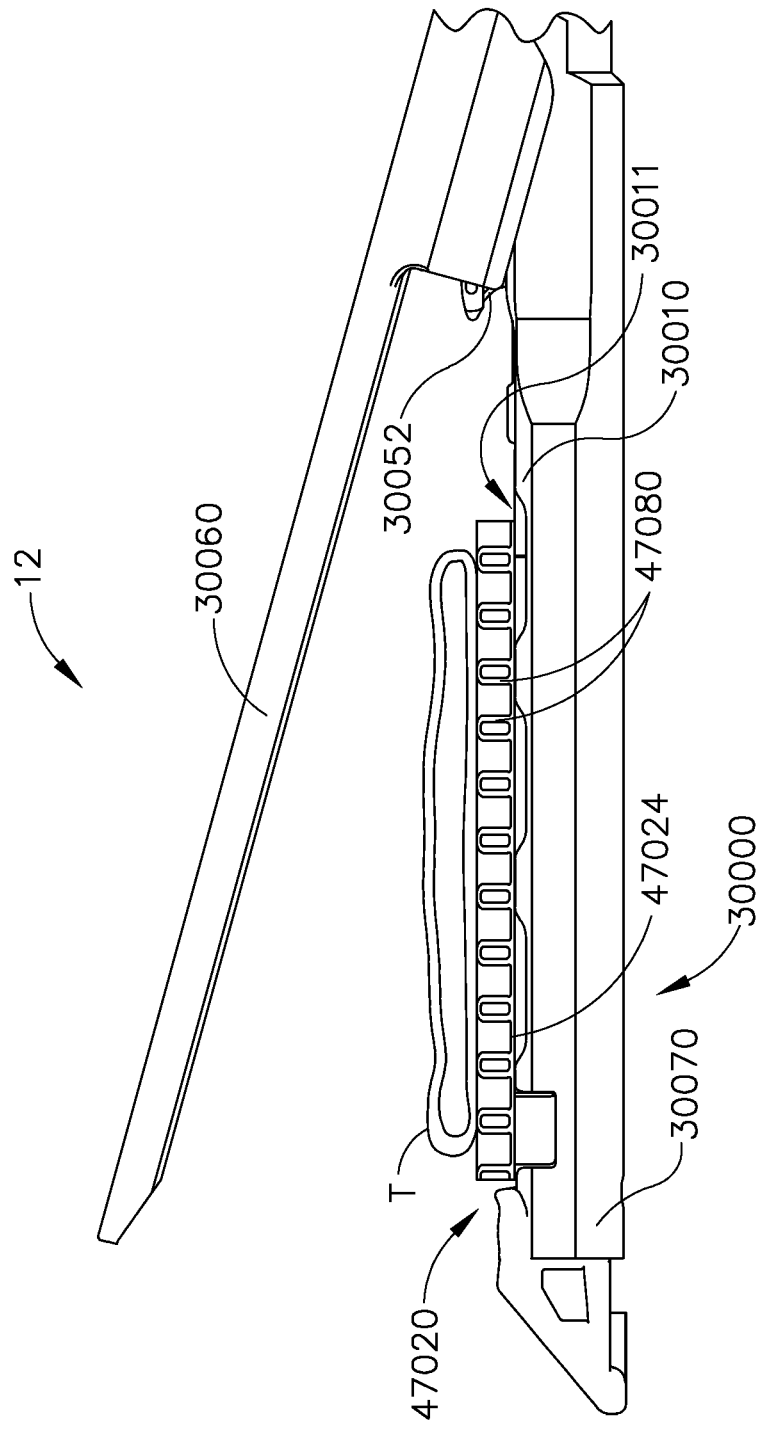
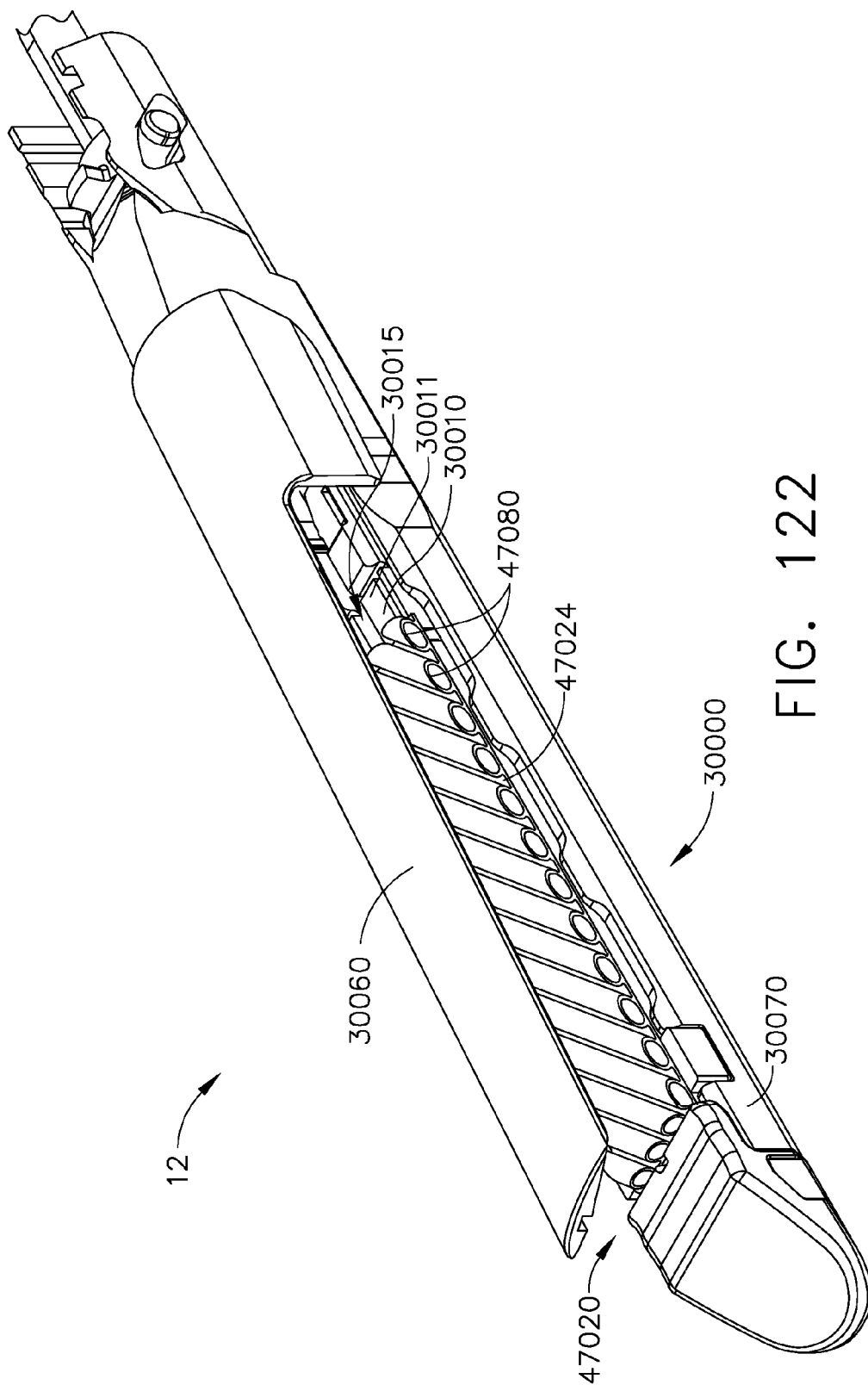


FIG. 121



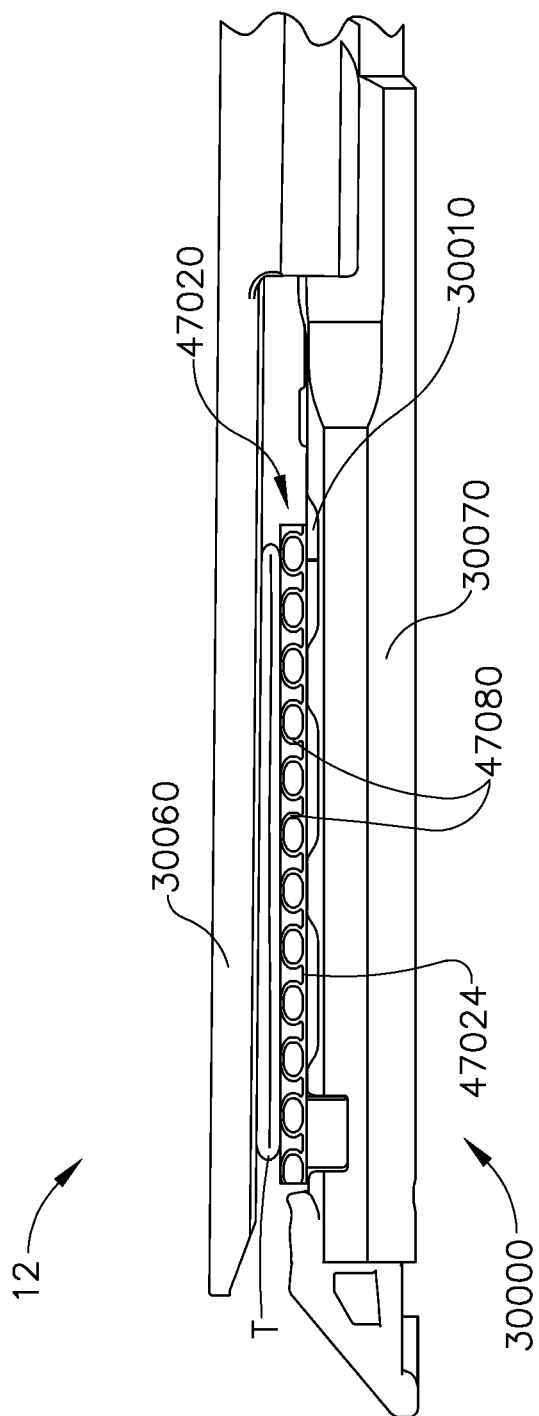


FIG. 123

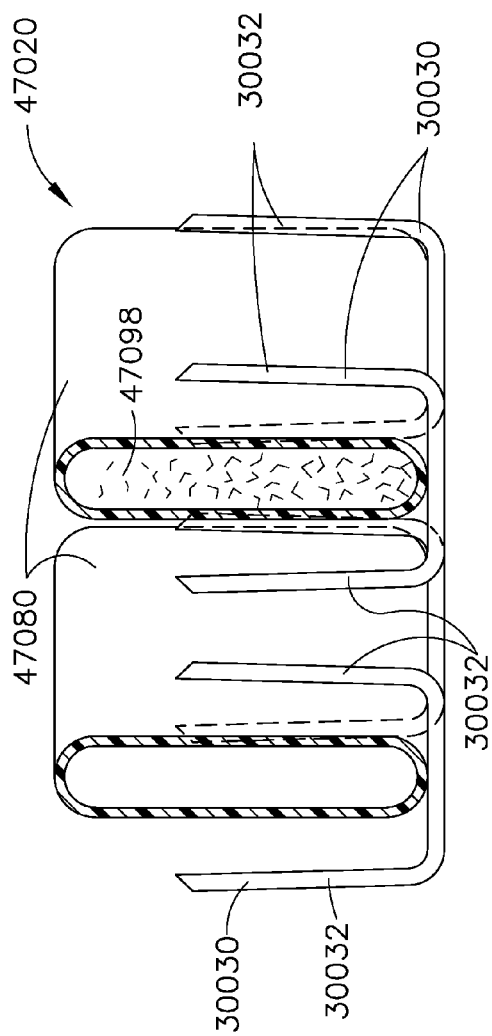


FIG. 124

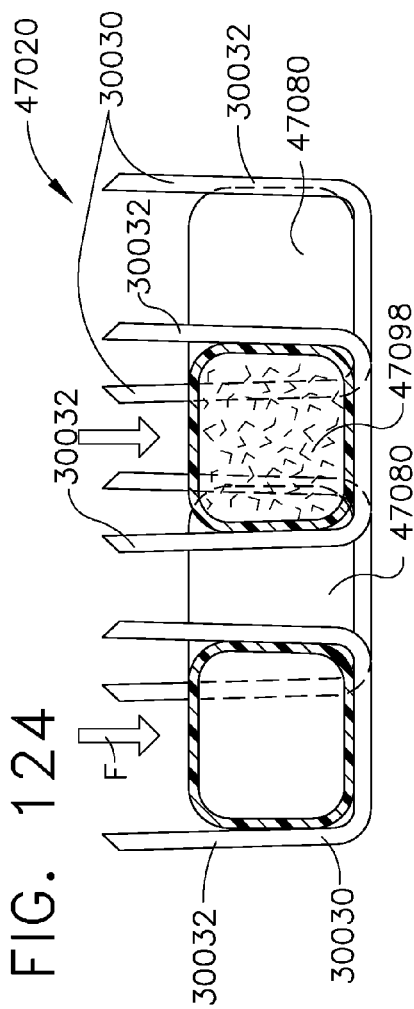


FIG. 125

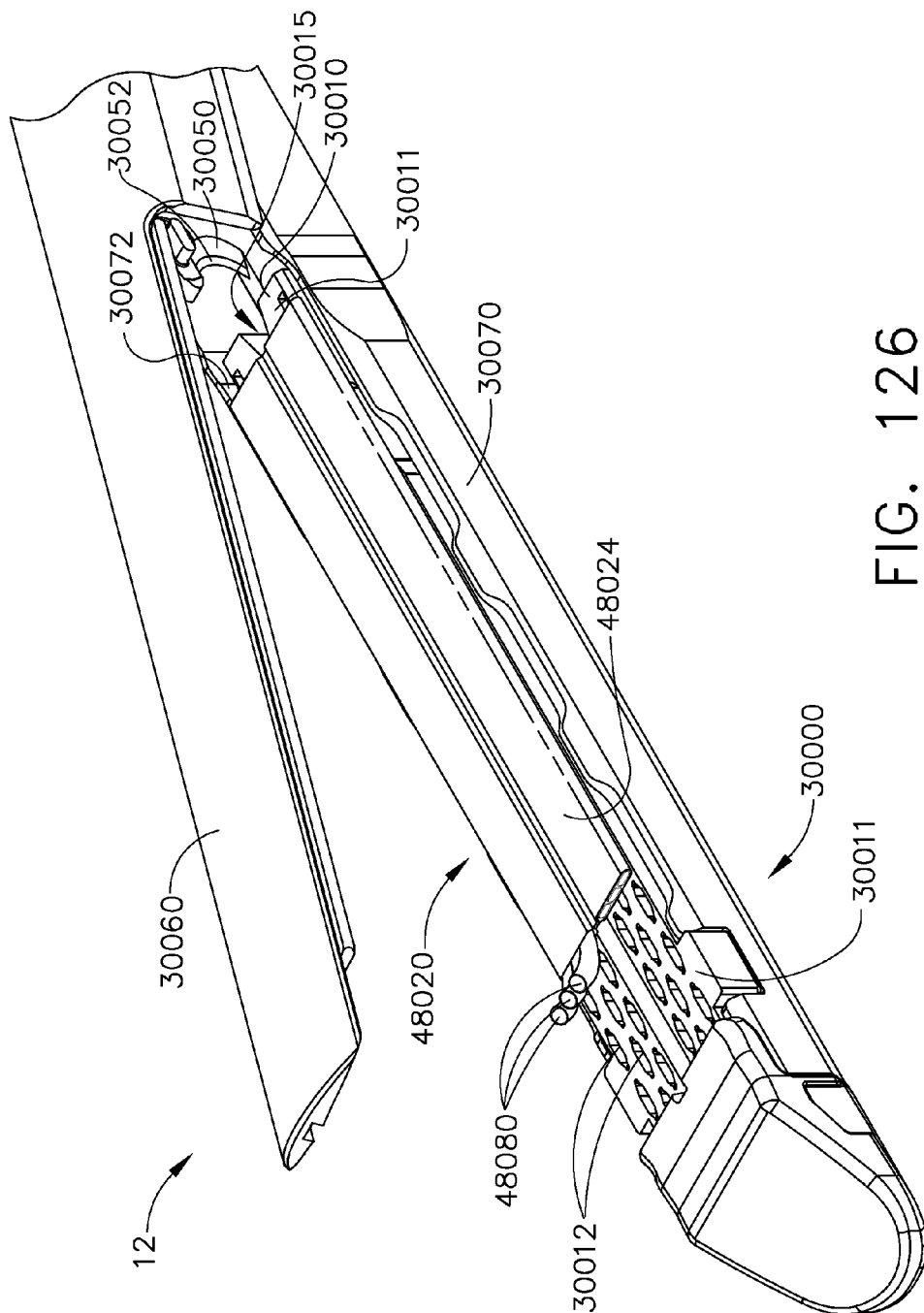


FIG. 126

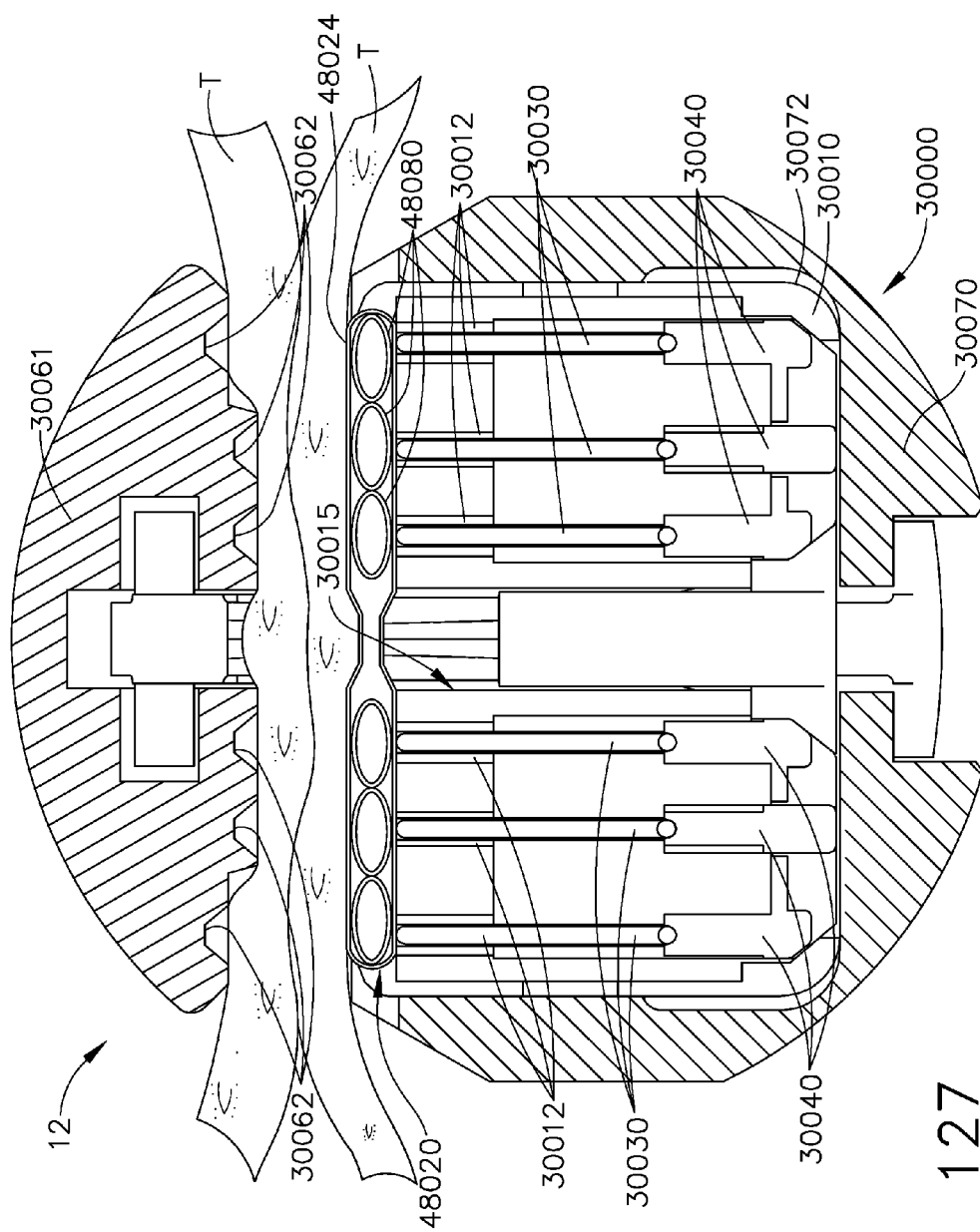


FIG. 127

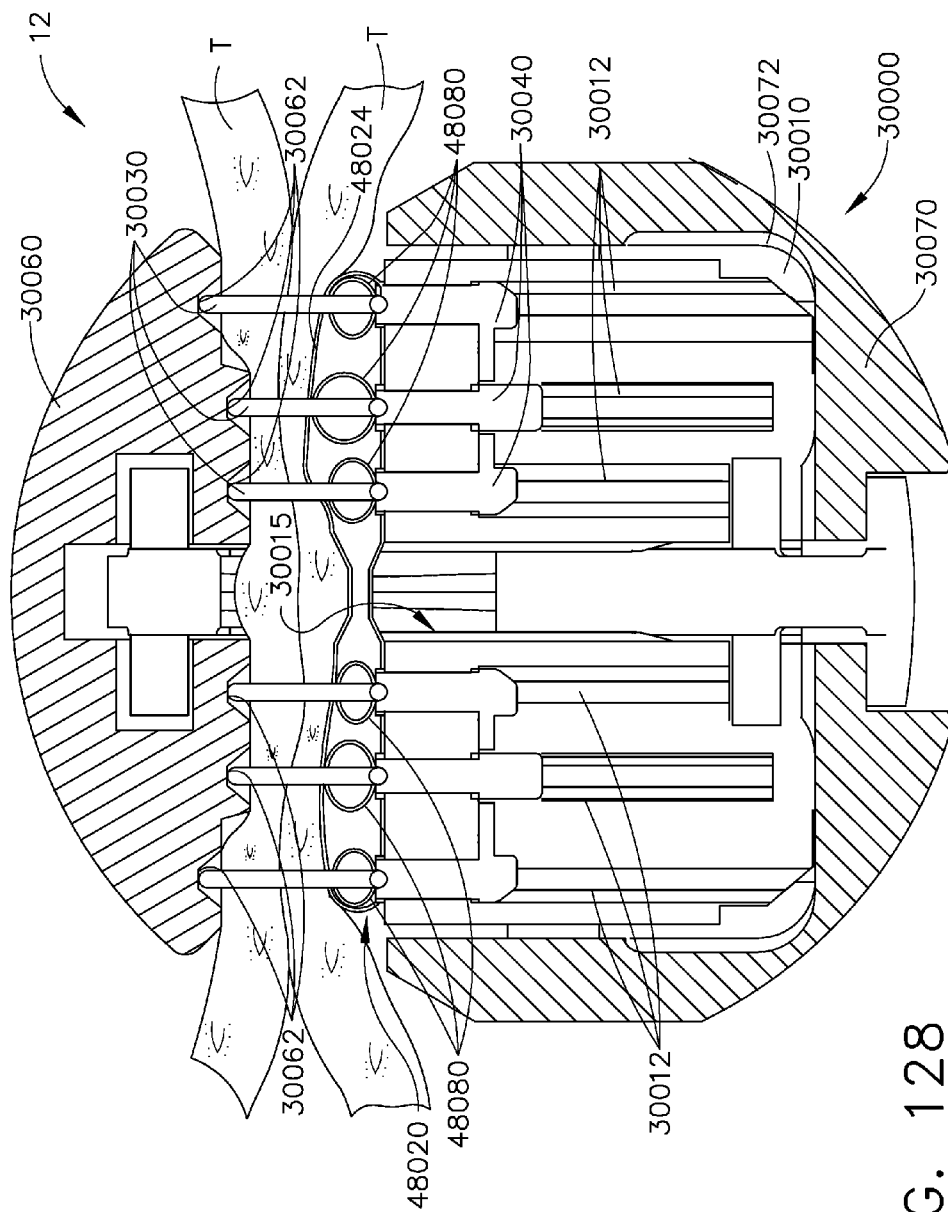


FIG. 128

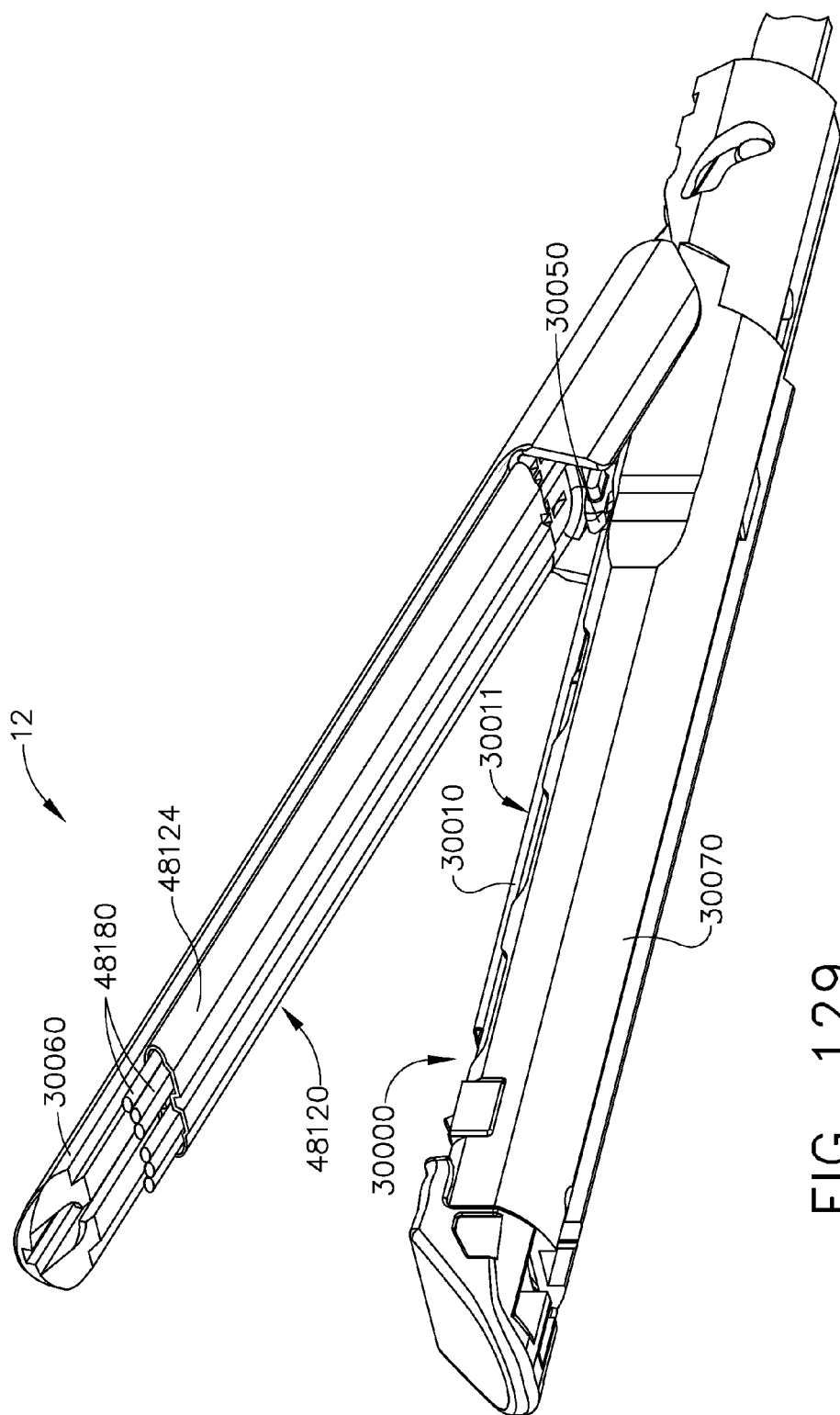


FIG. 129

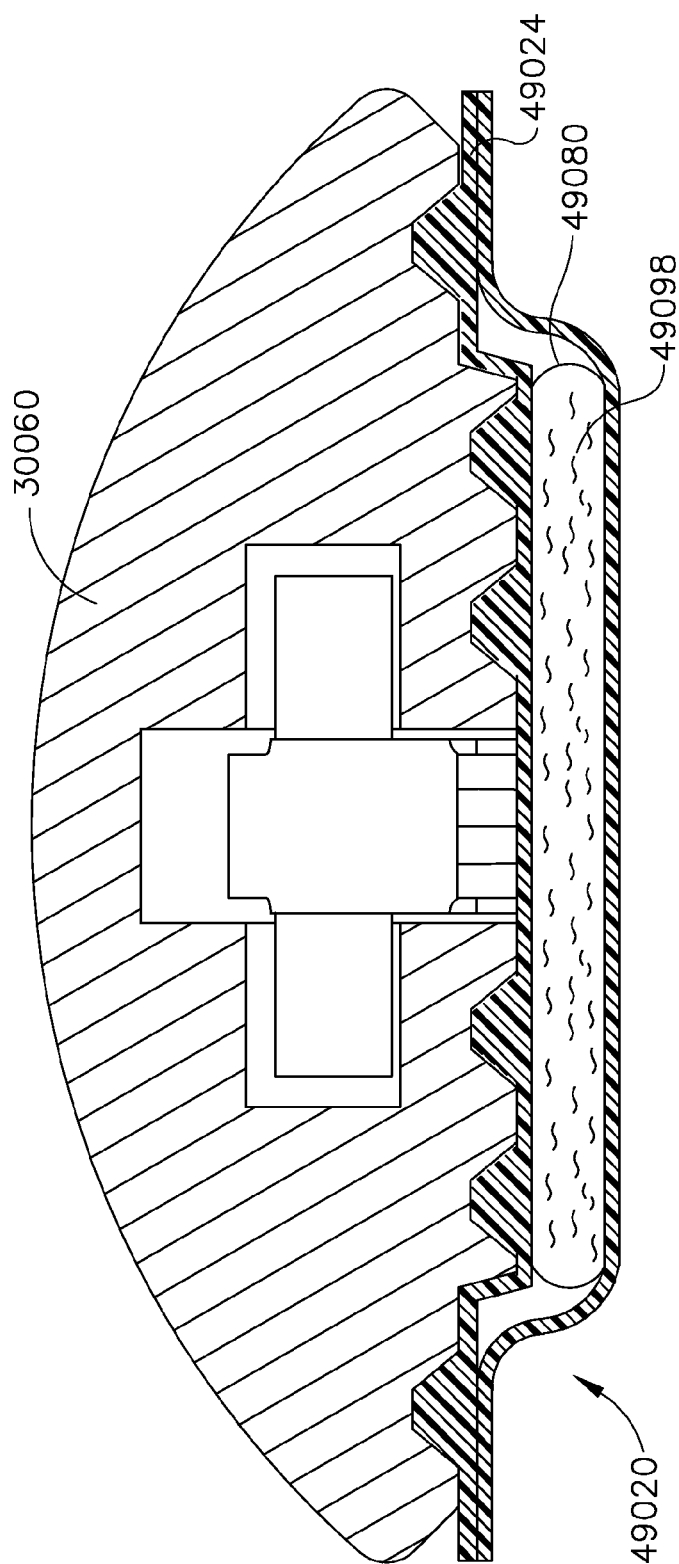


FIG. 130

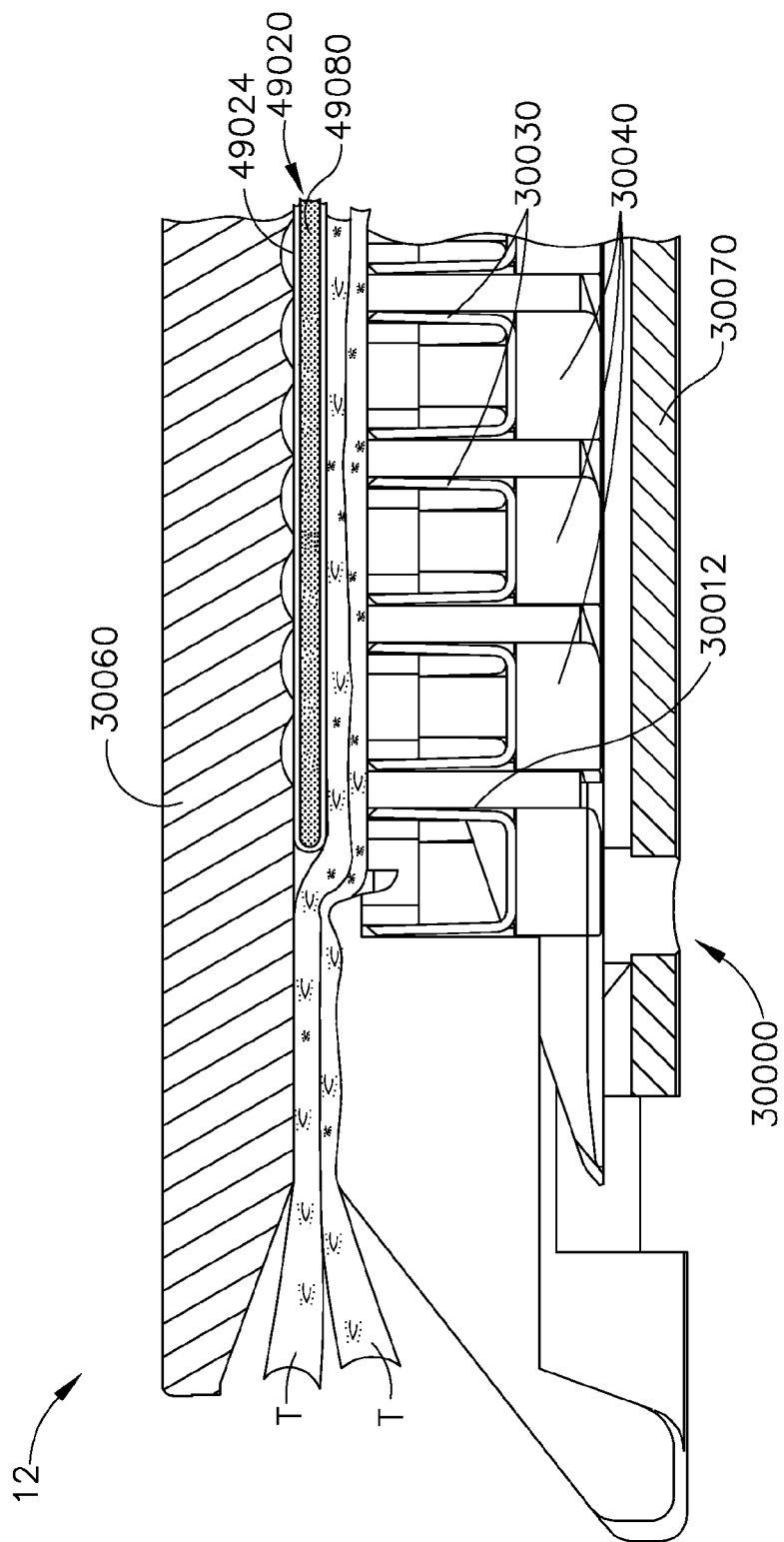


FIG. 131

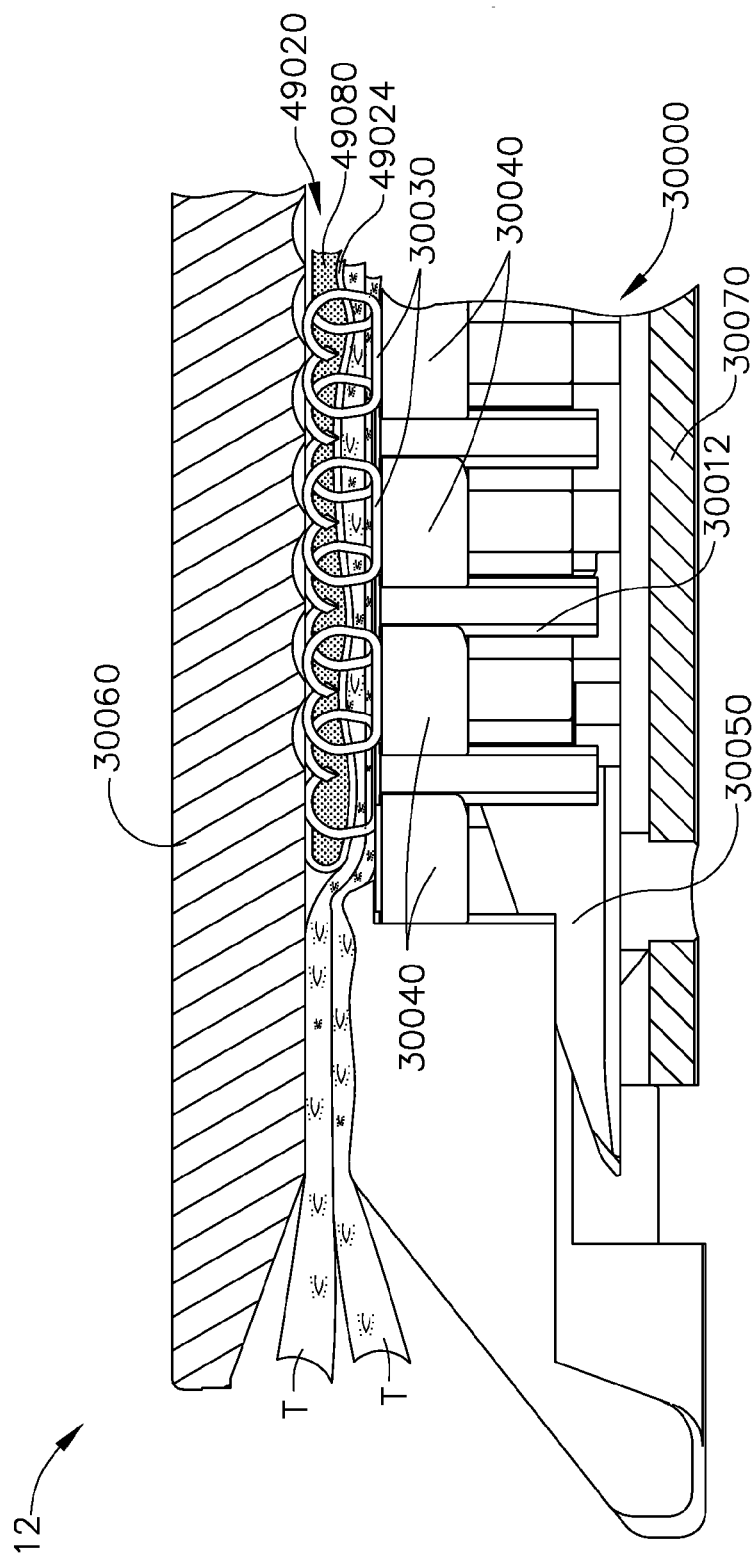


FIG. 132

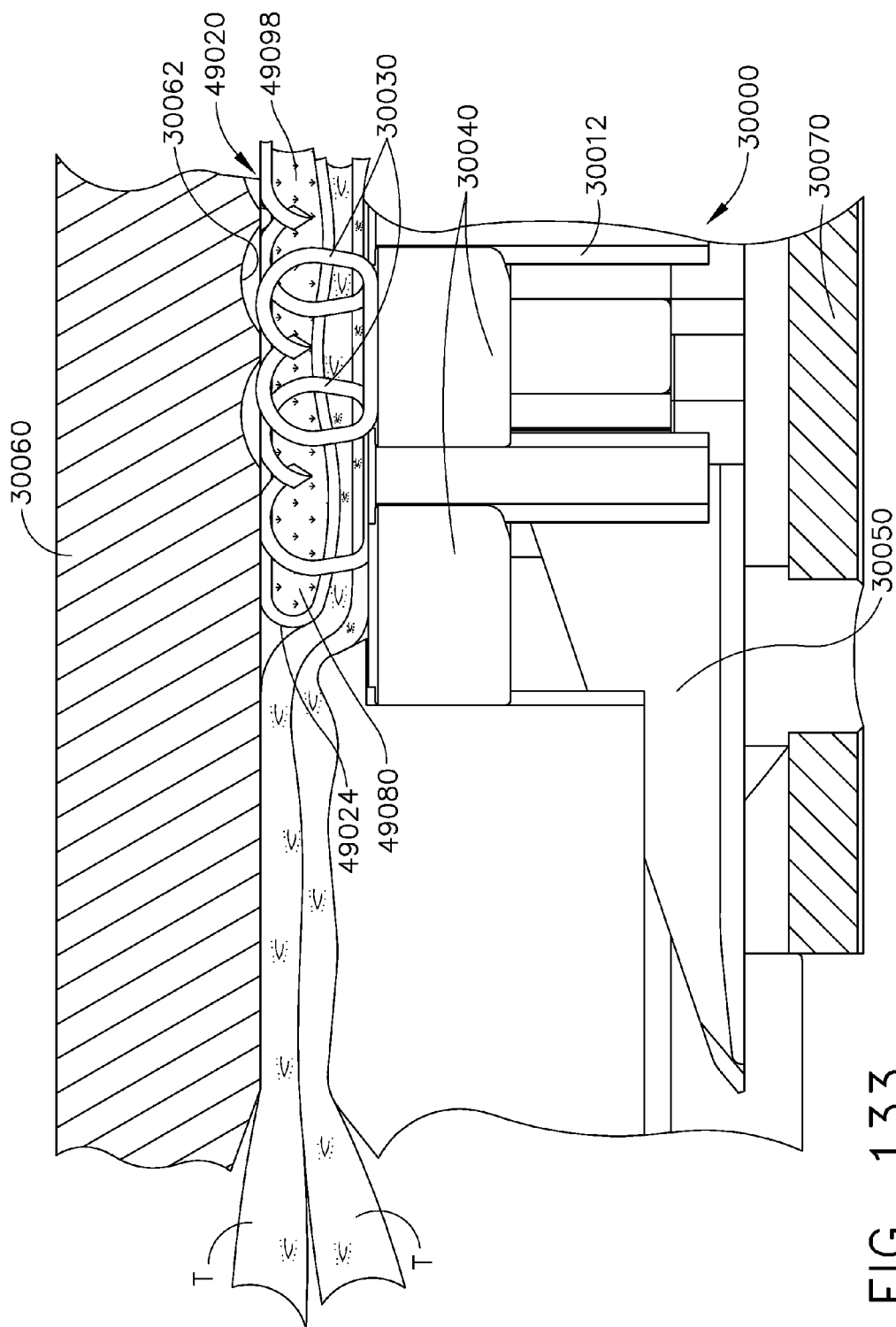


FIG. 133

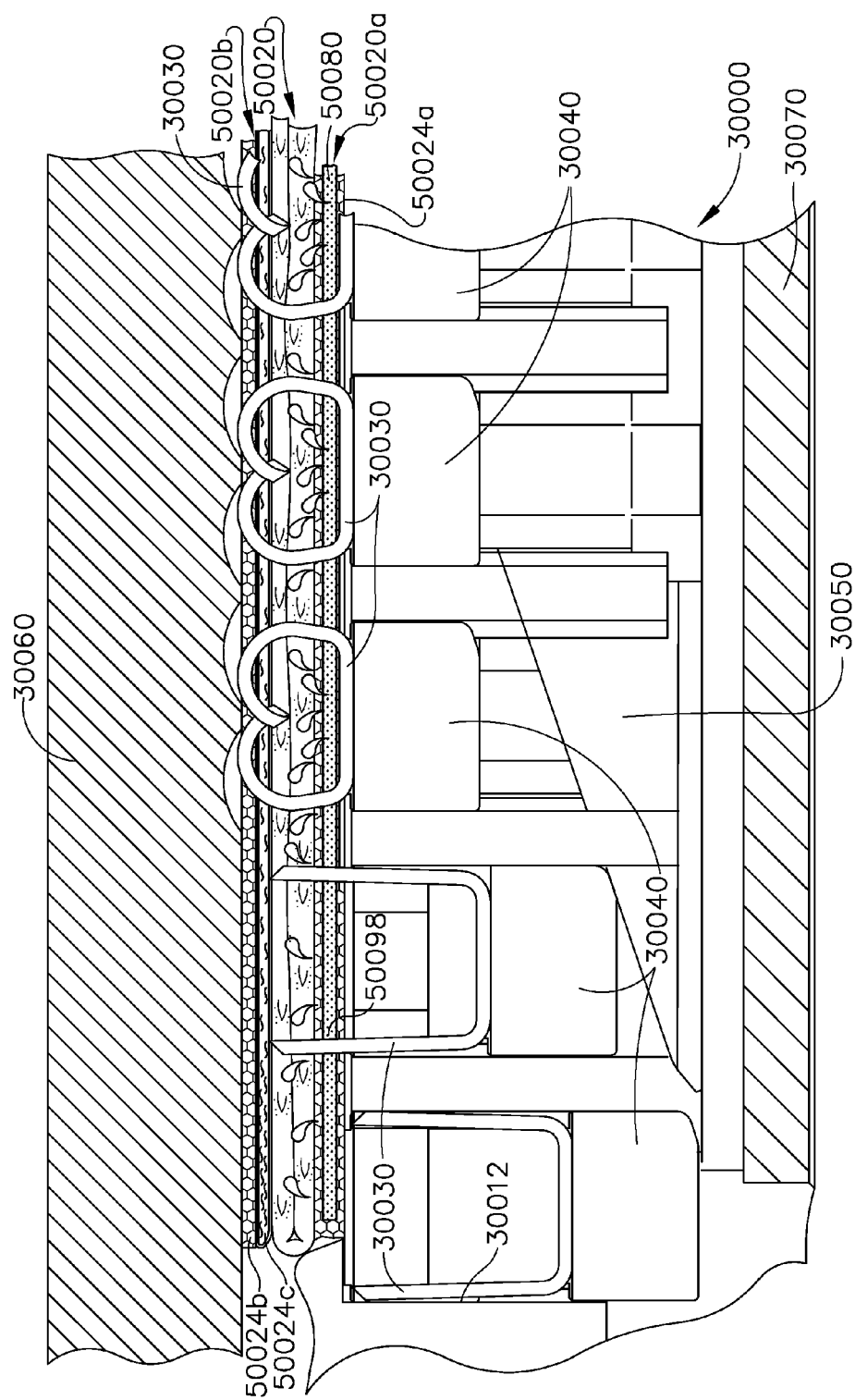


FIG. 134

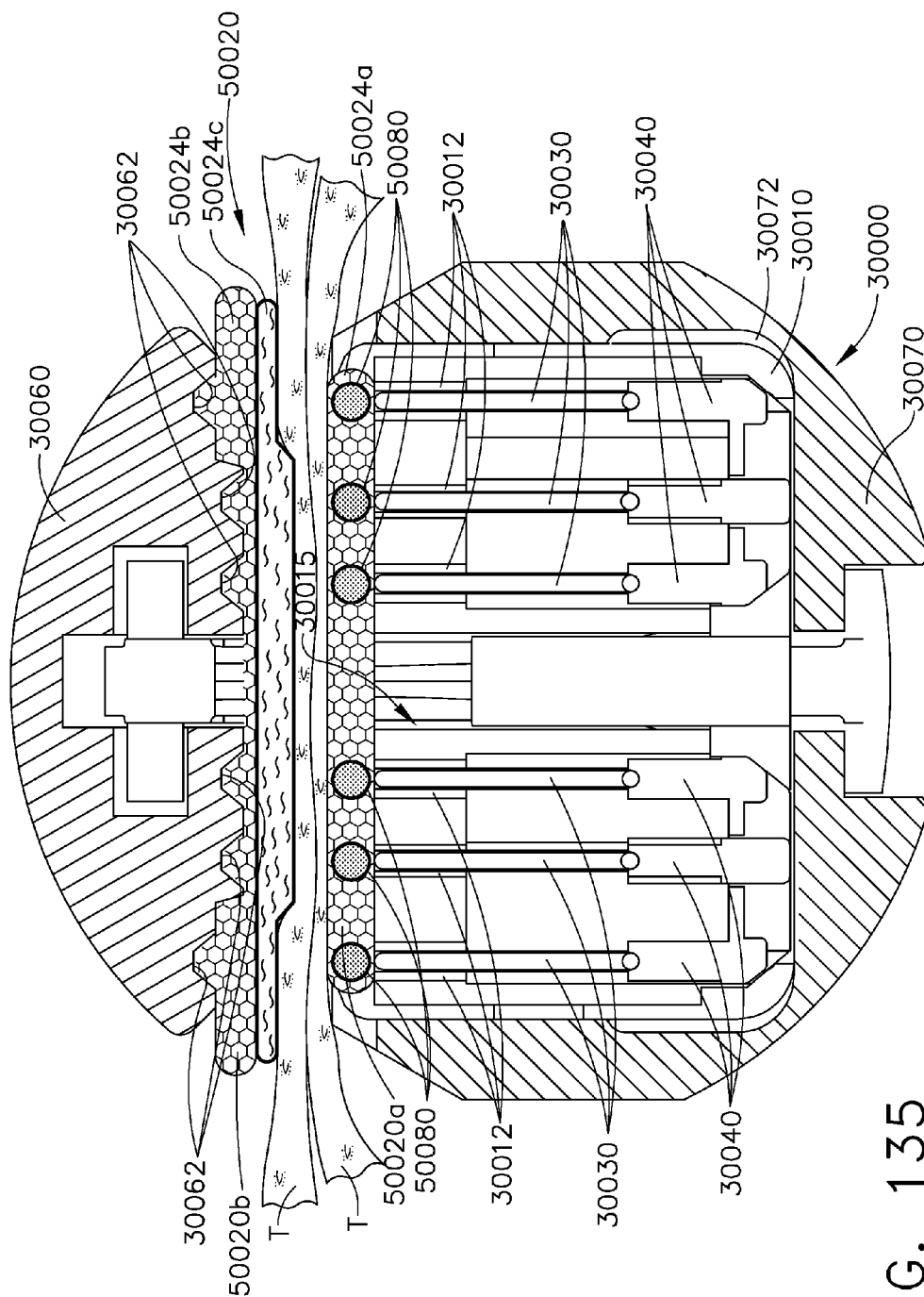


FIG. 135

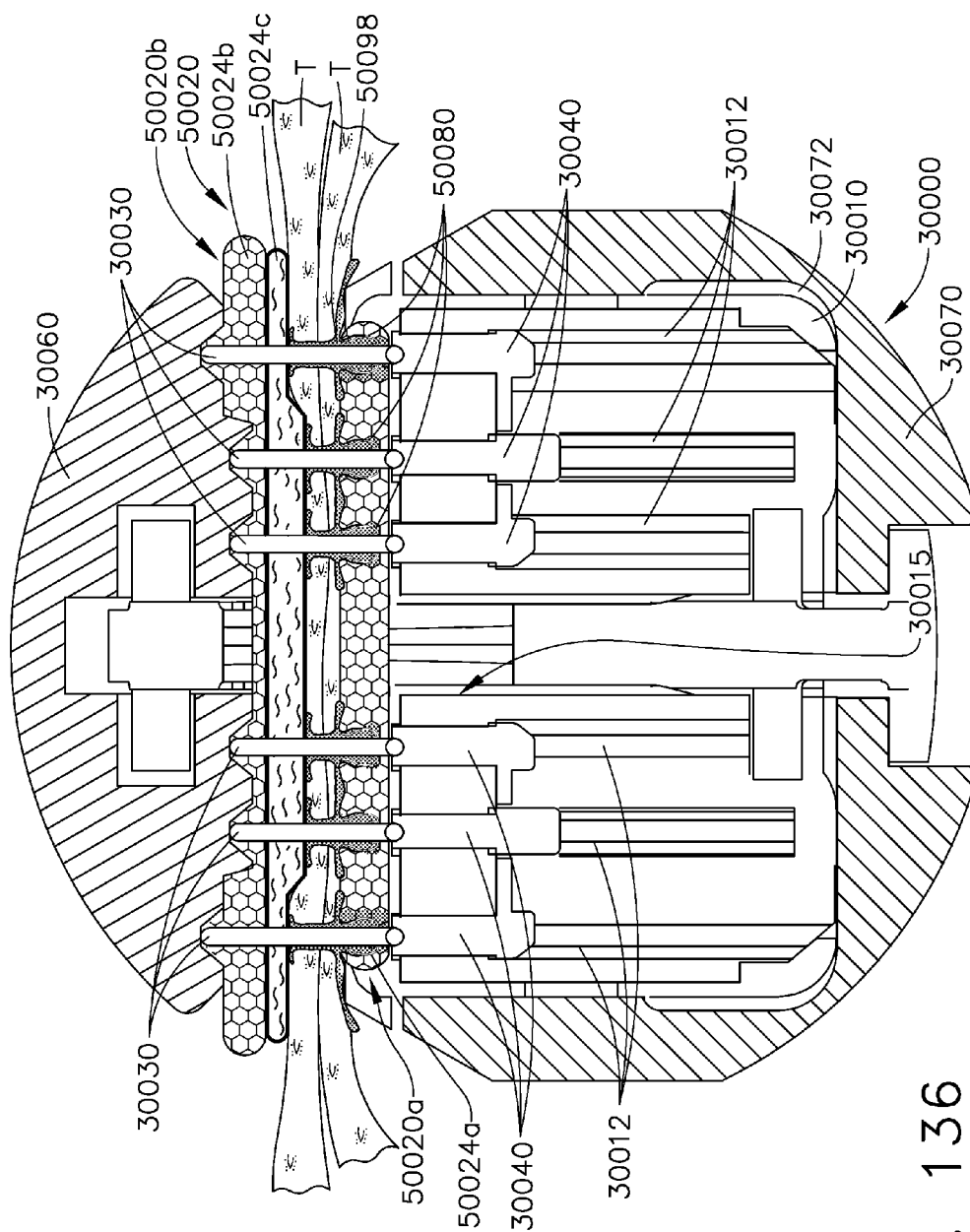


FIG. 136

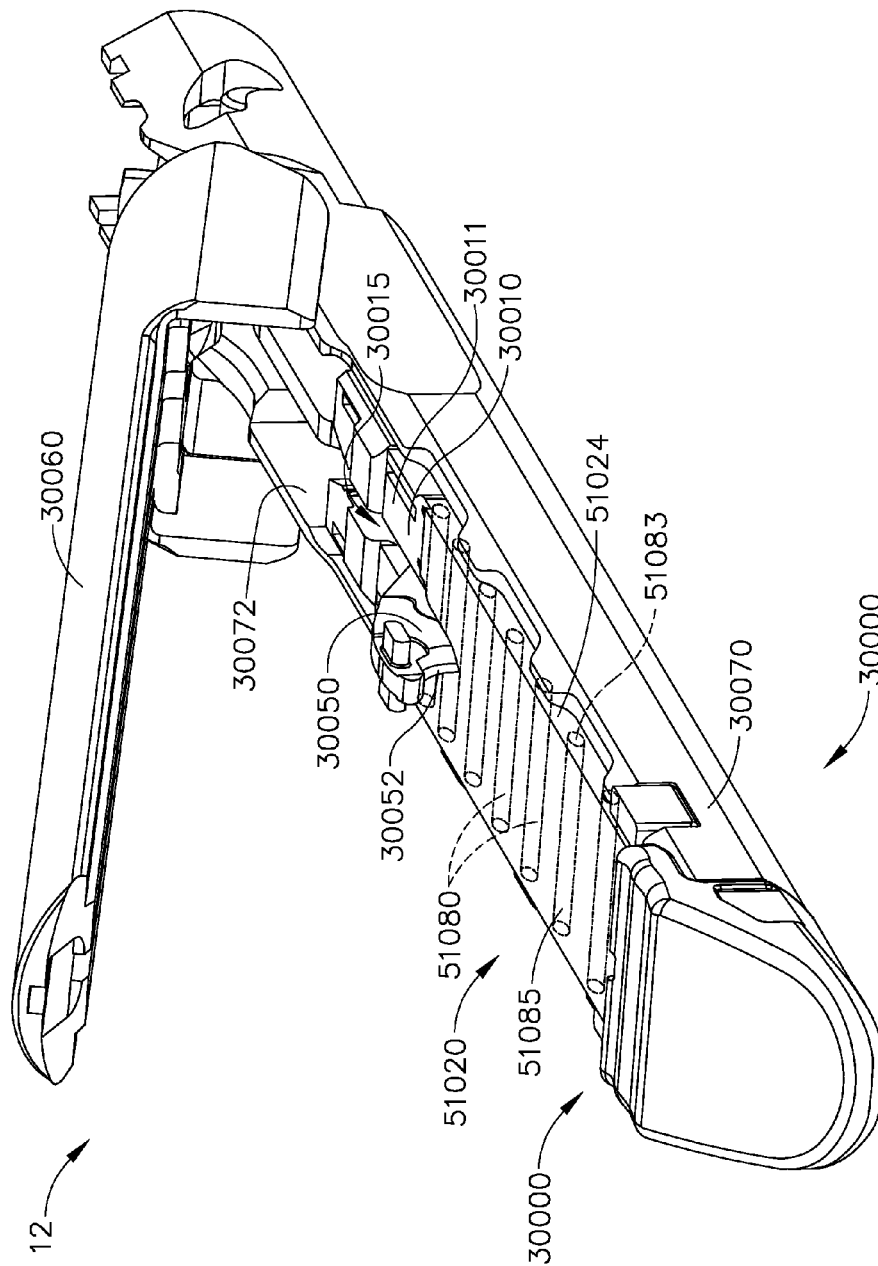


FIG. 137

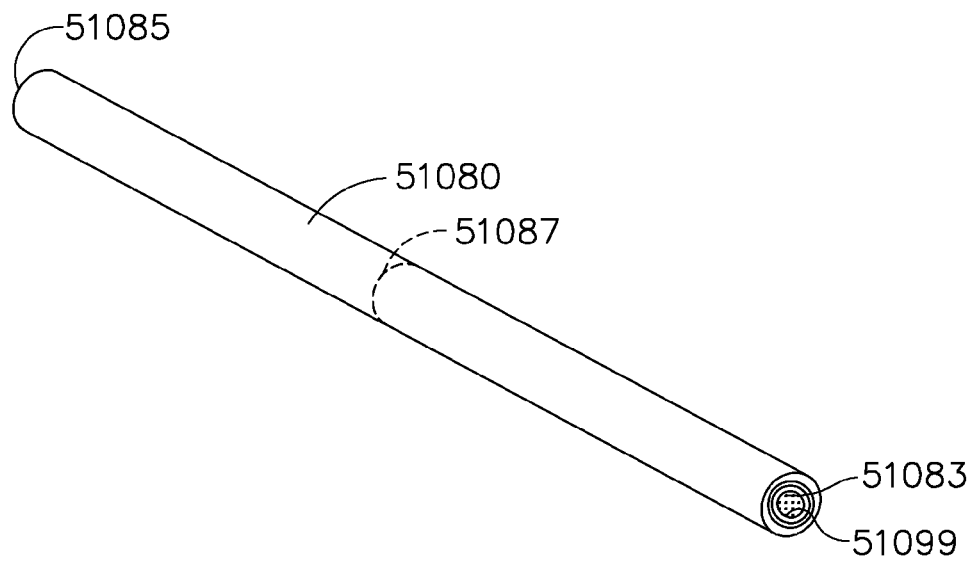


FIG. 138

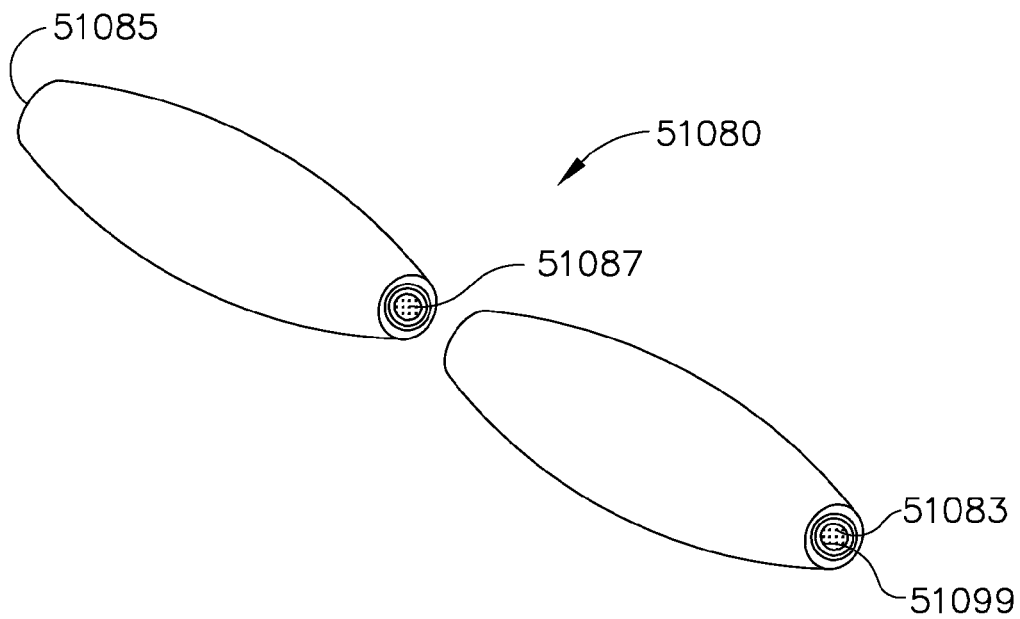


FIG. 139

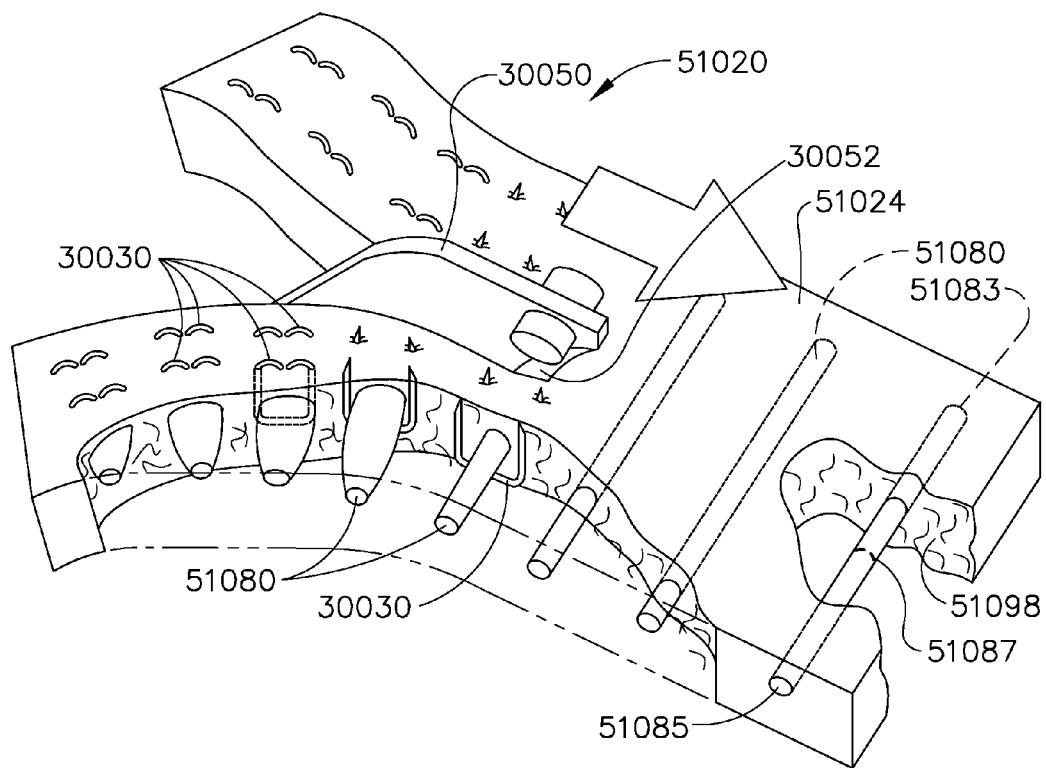


FIG. 140

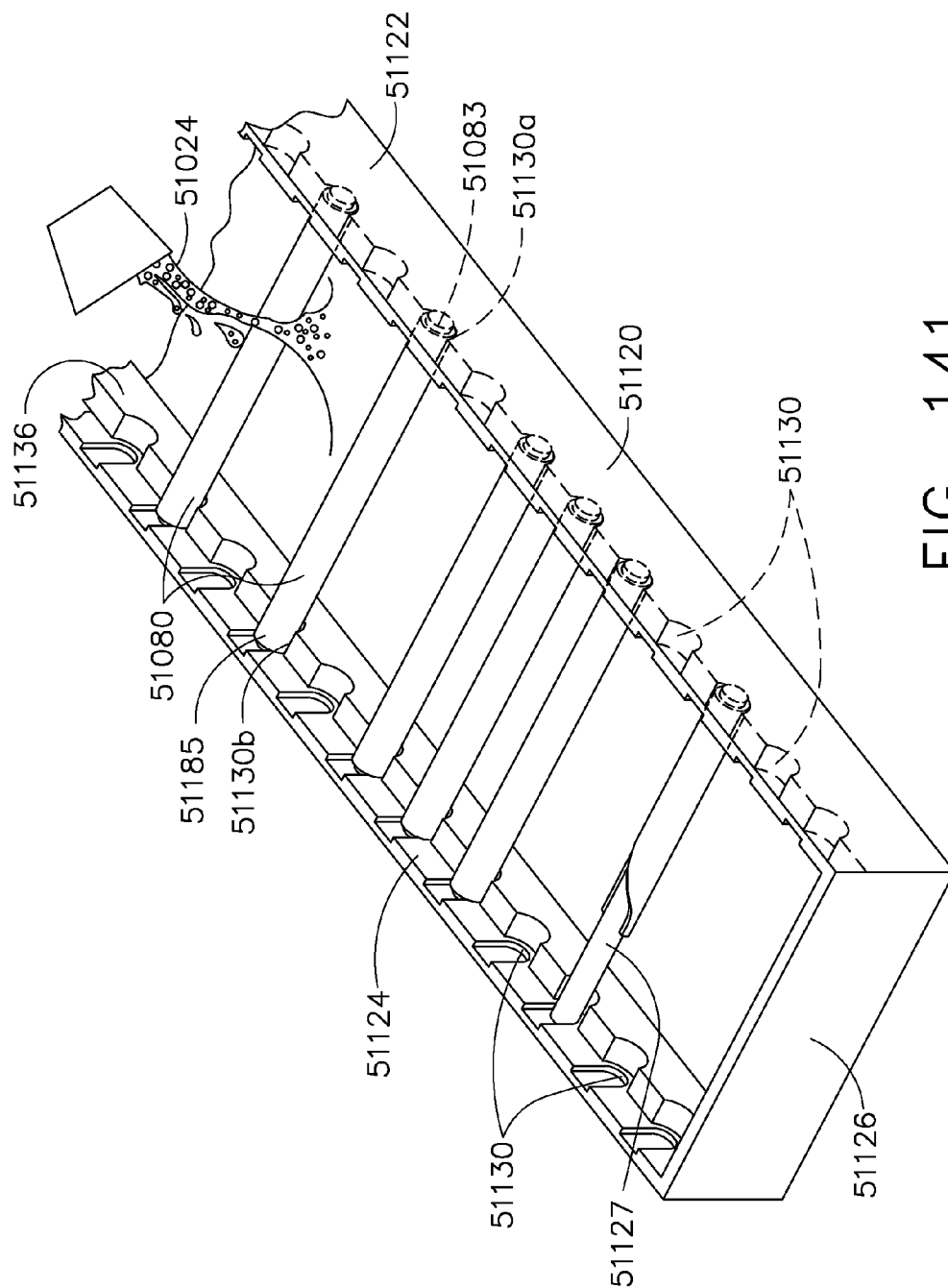


FIG. 141

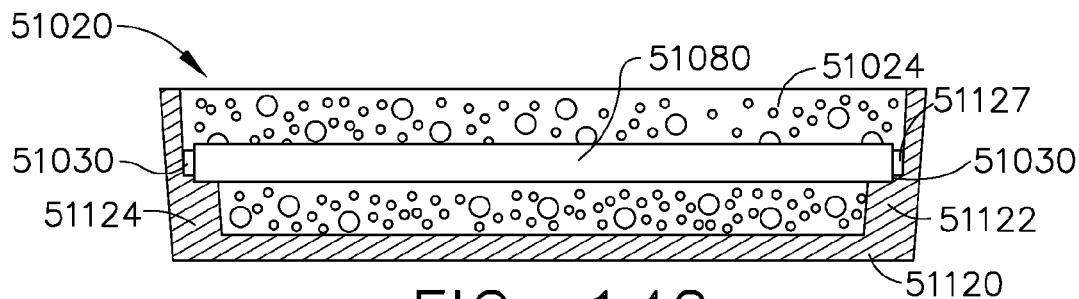


FIG. 142

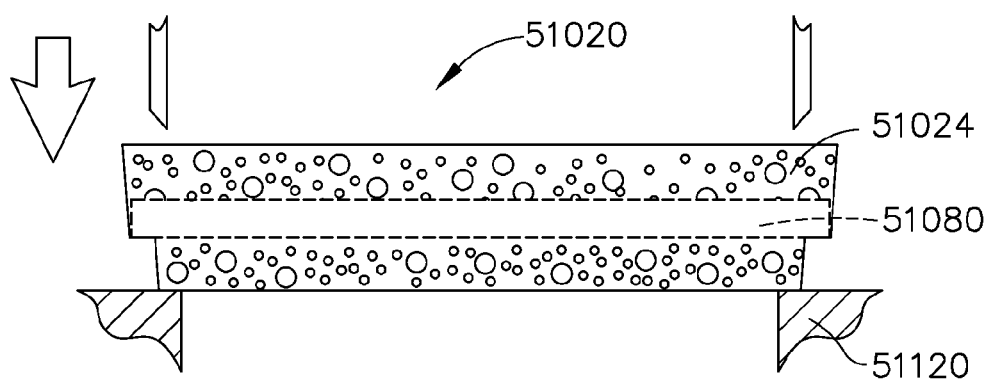


FIG. 143

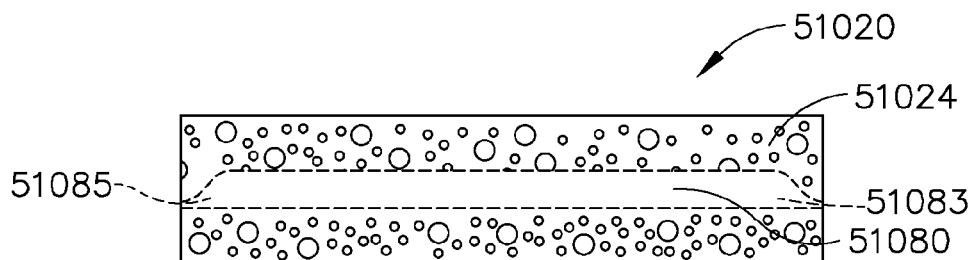


FIG. 144

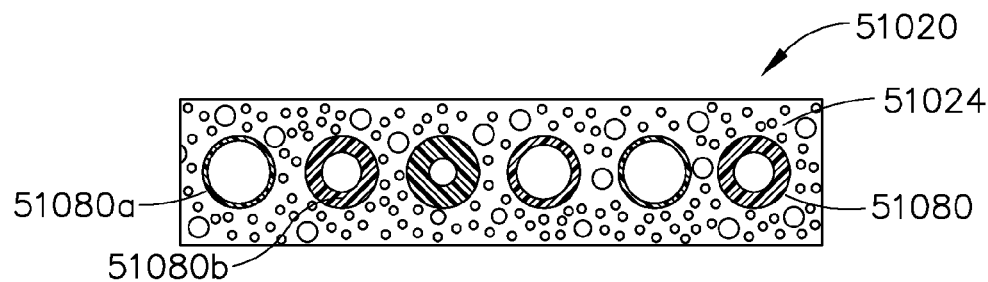


FIG. 145

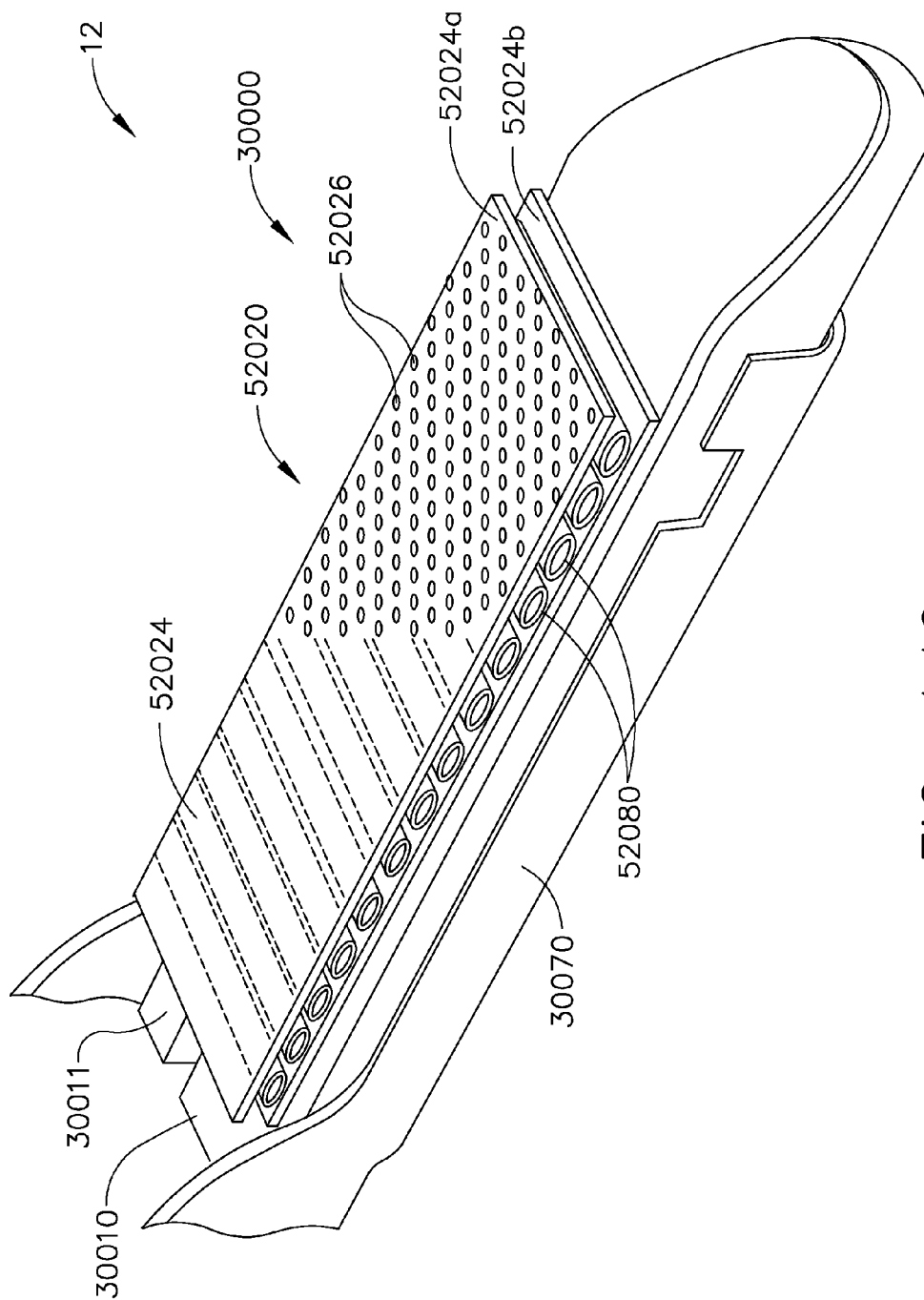


FIG. 146

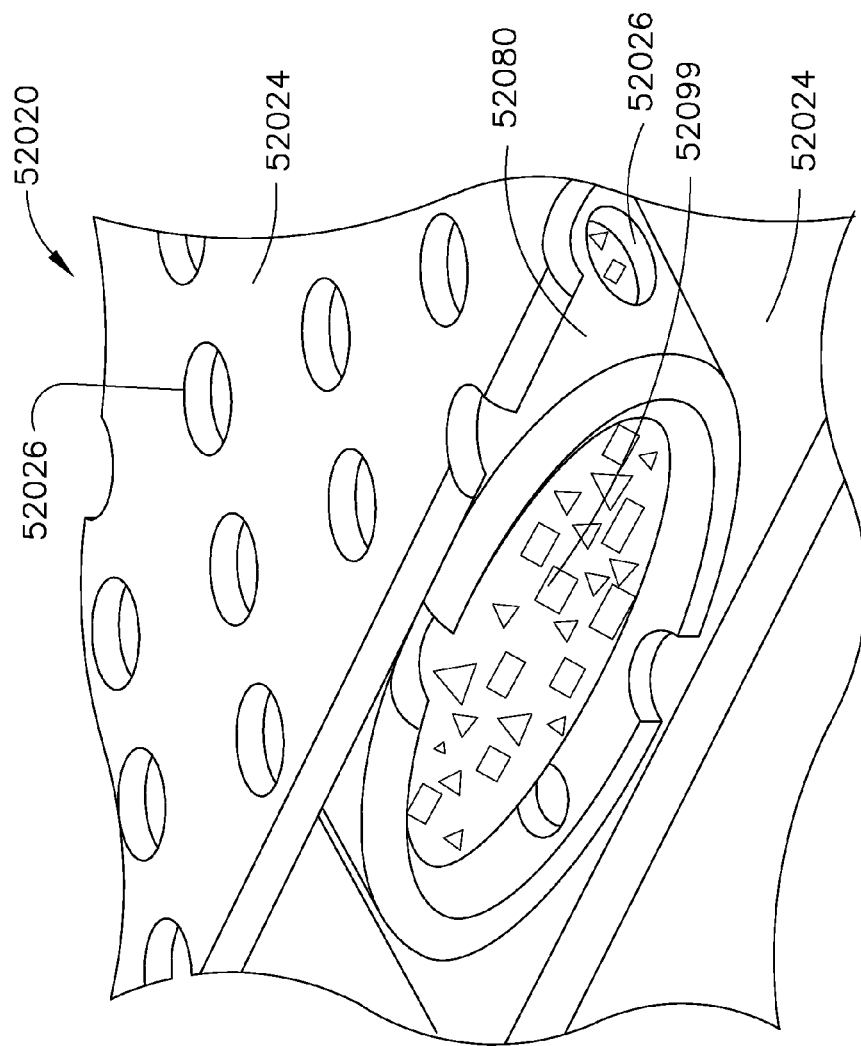


FIG. 147

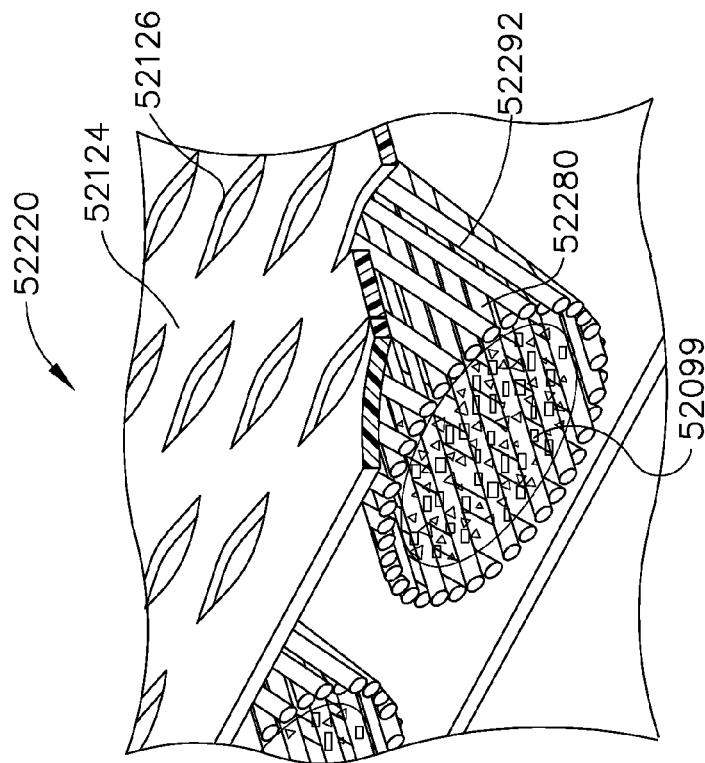


FIG. 149

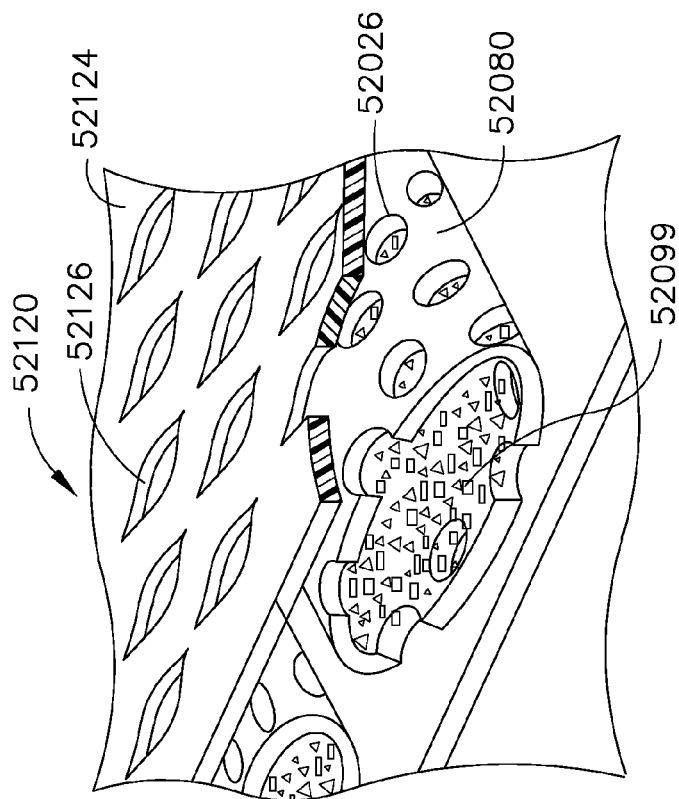


FIG. 148

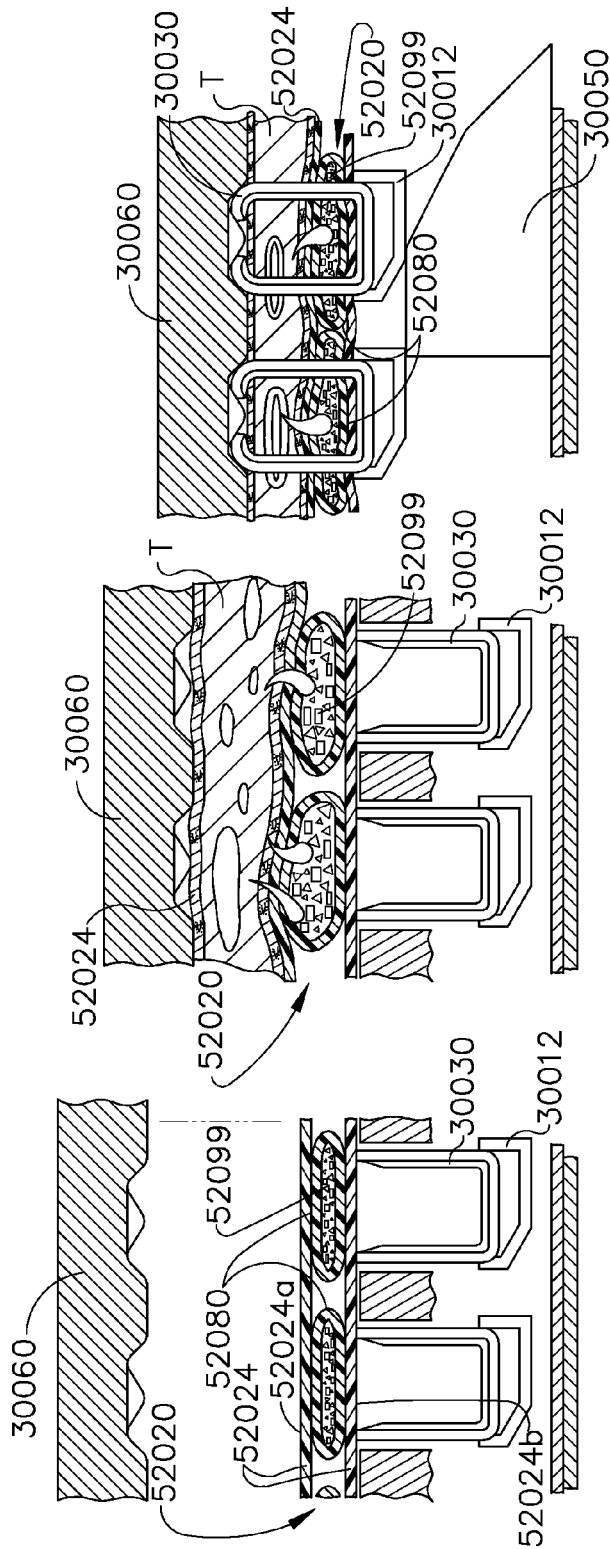


FIG. 150A

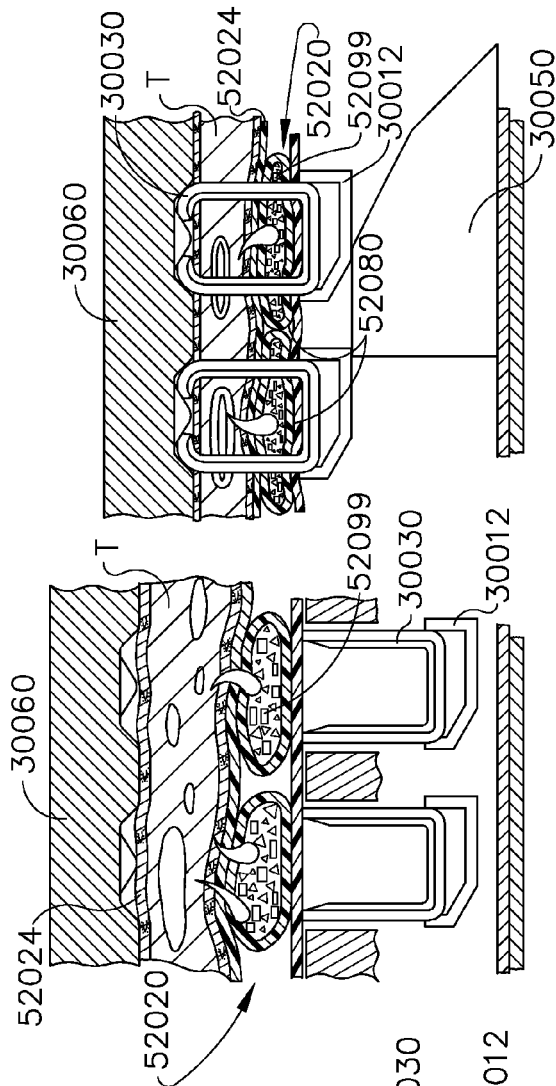


FIG. 150B

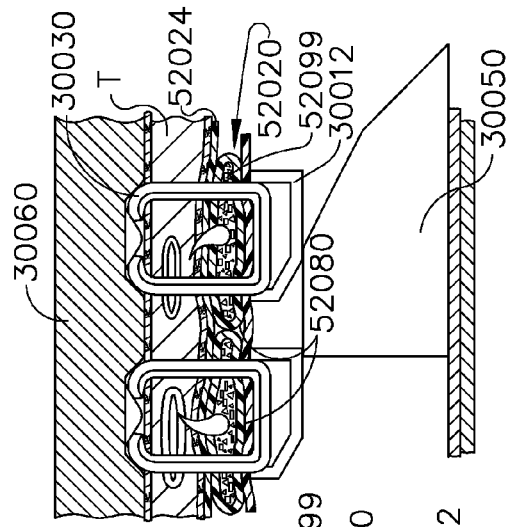


FIG. 150C

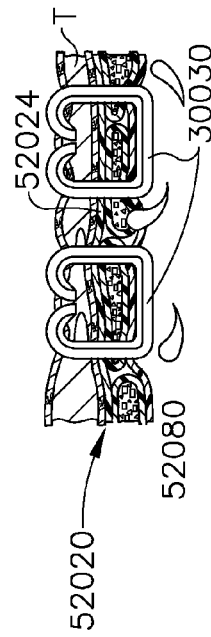


FIG. 150D

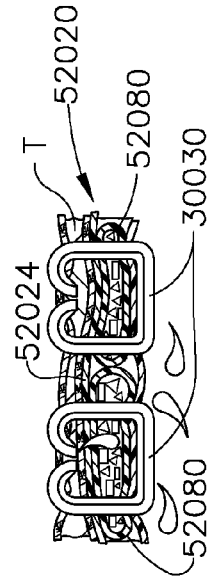
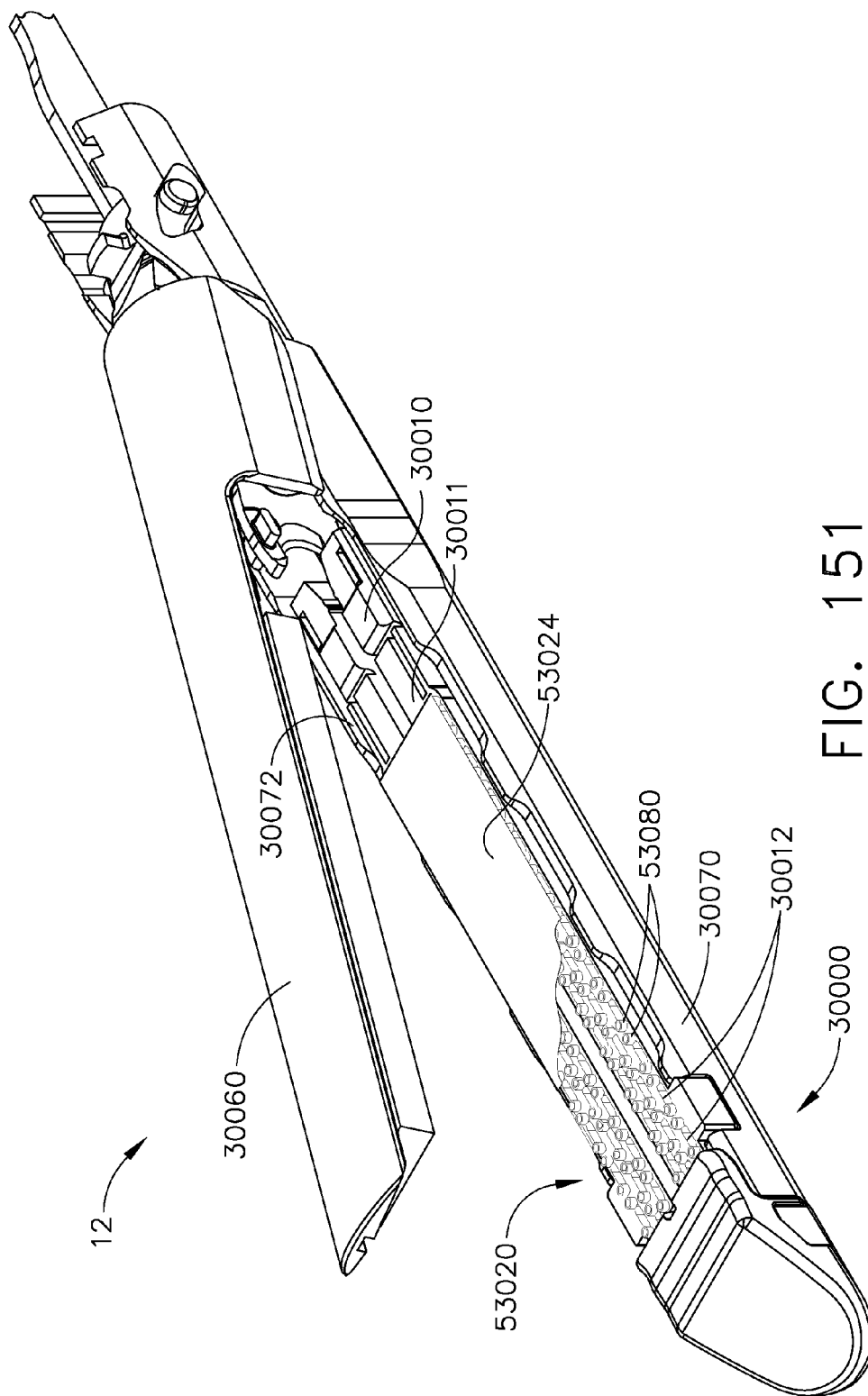


FIG. 150E



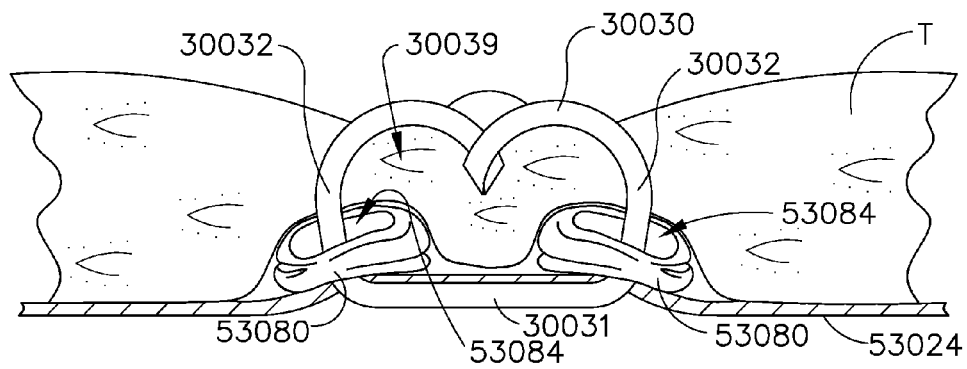


FIG. 152

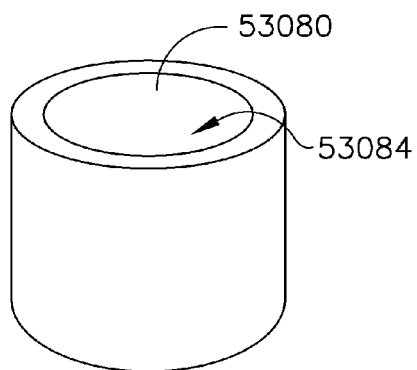


FIG. 153

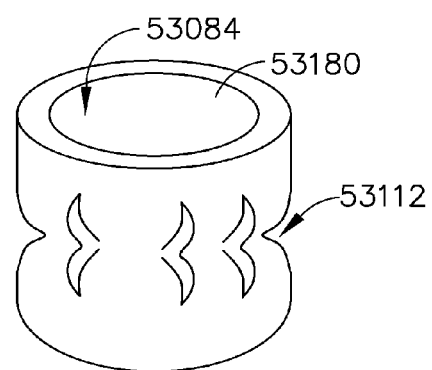


FIG. 154

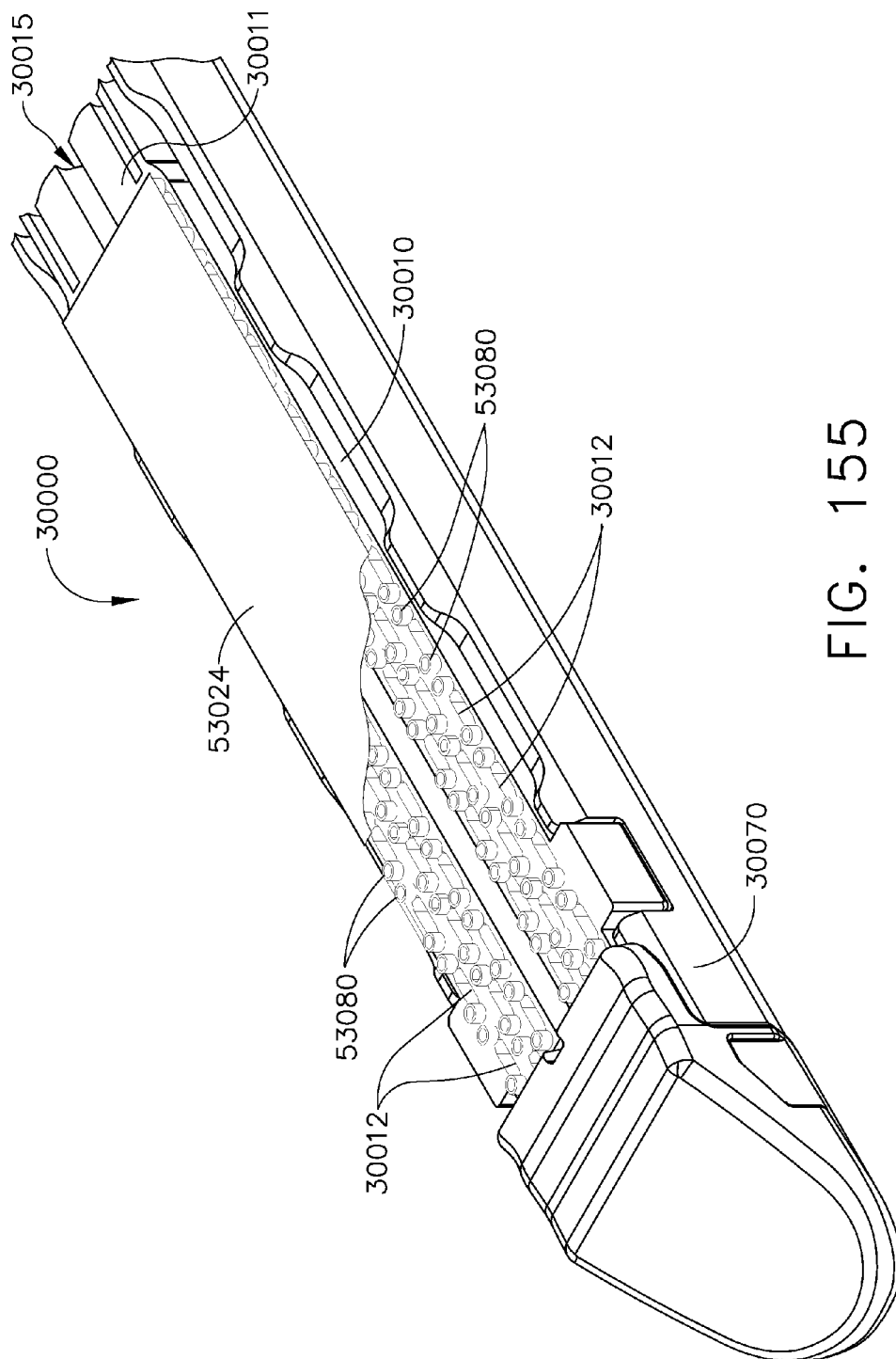


FIG. 155

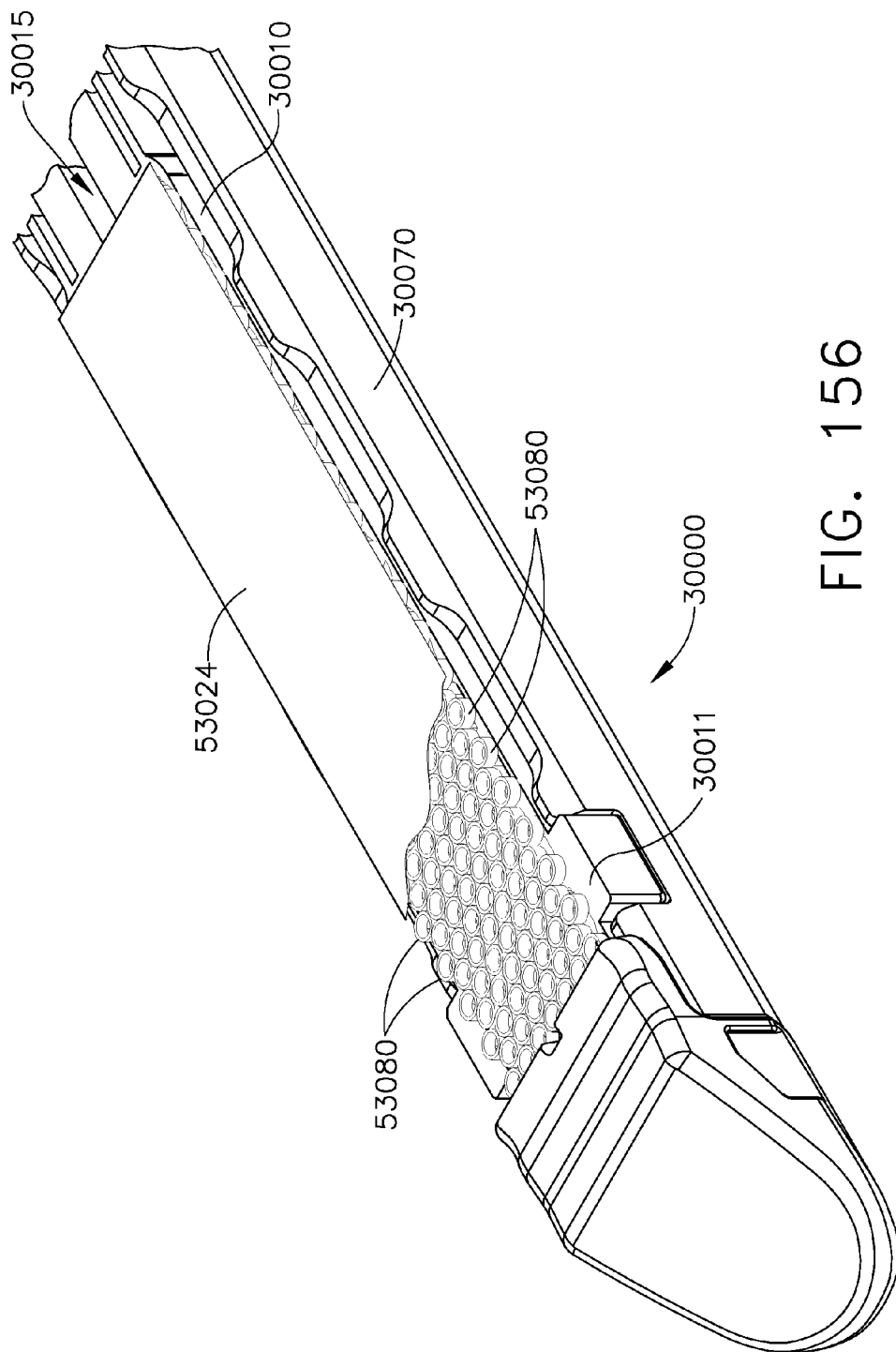


FIG. 156

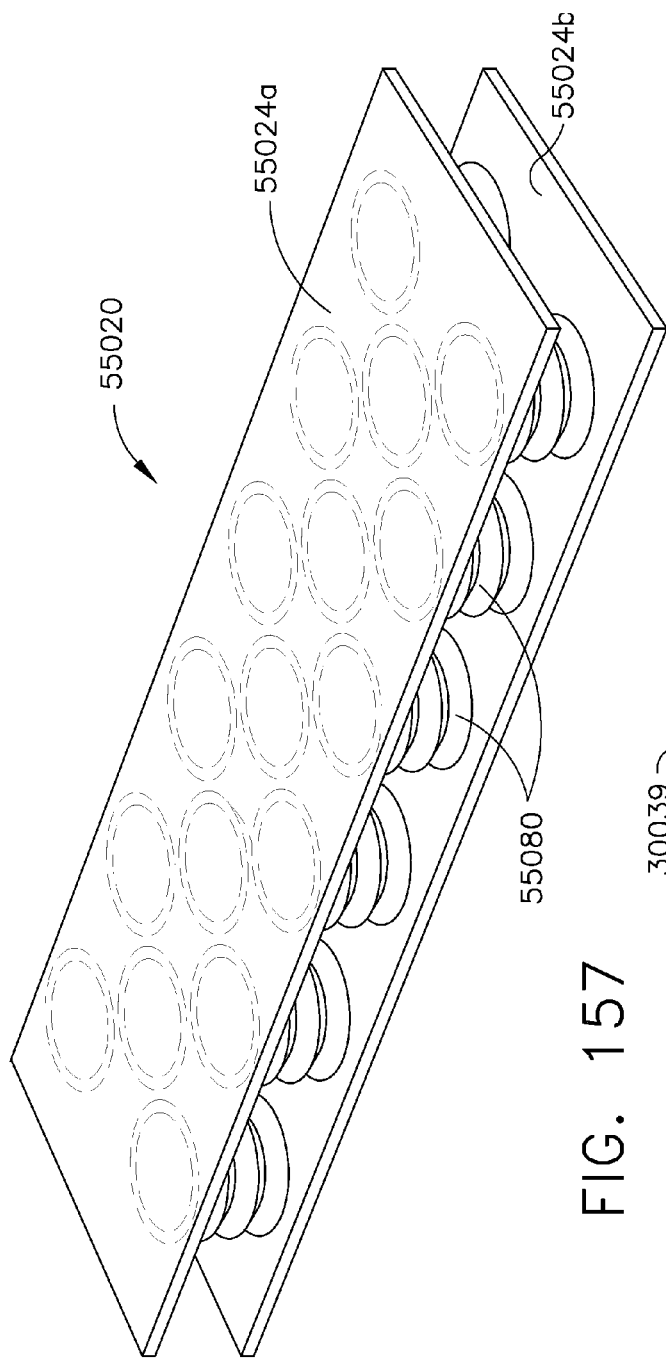


FIG. 157

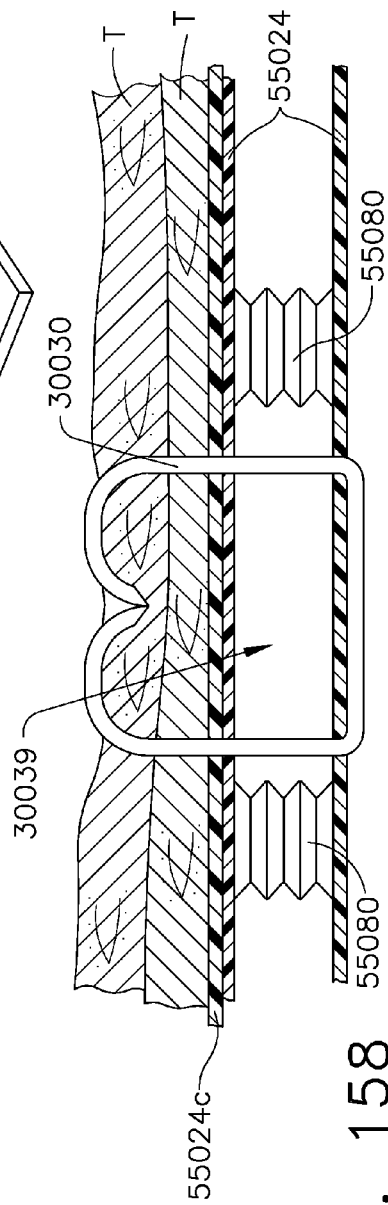


FIG. 158

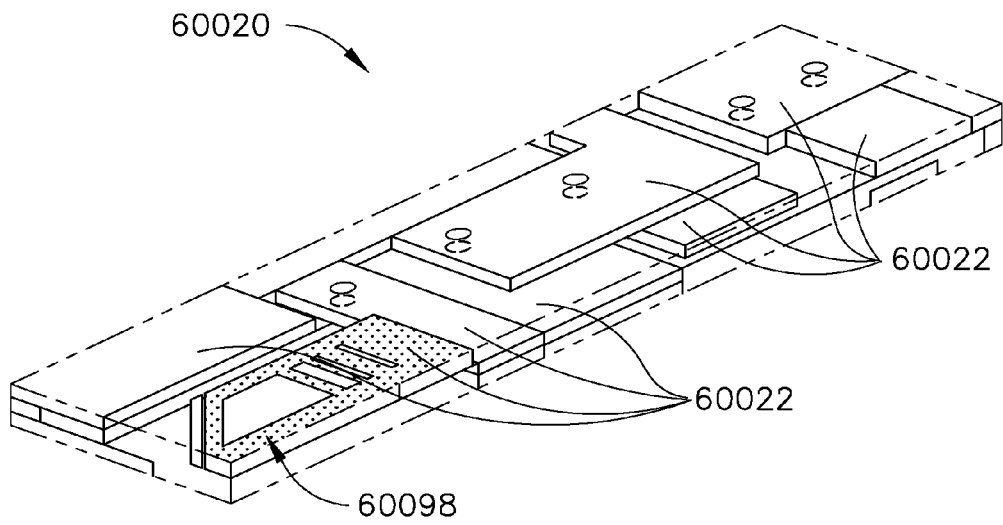


FIG. 159

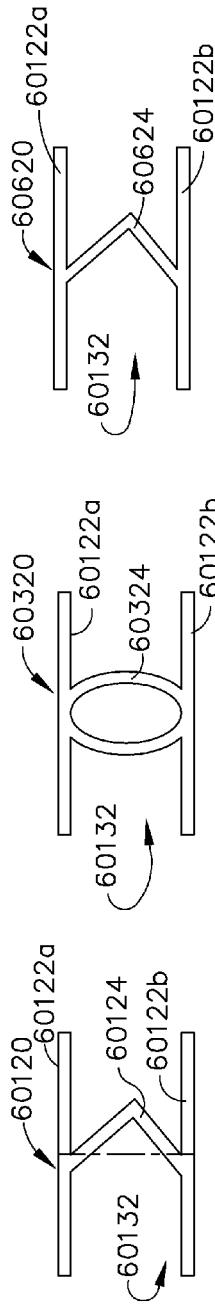


FIG. 160

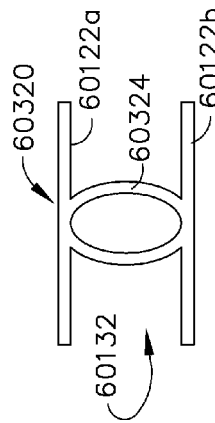


FIG. 163

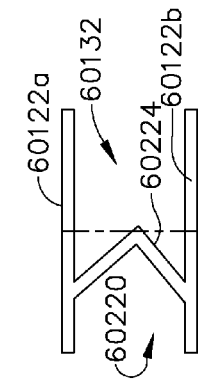


FIG. 161

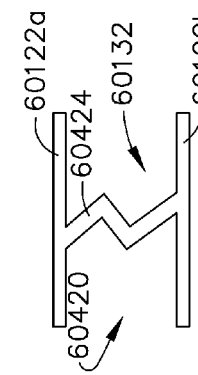


FIG. 164

FIG. 166

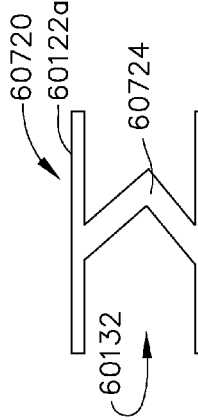
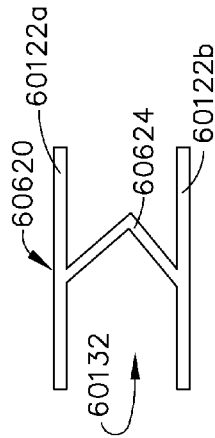


FIG. 167

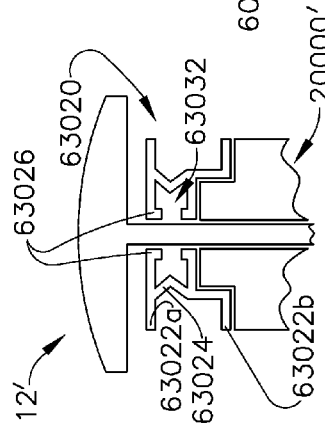


FIG. 162

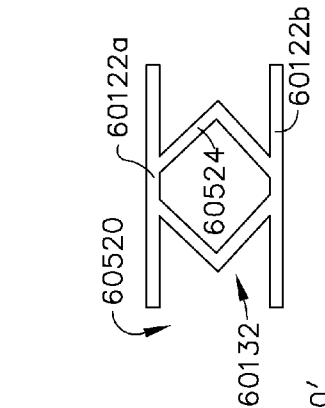


FIG. 165

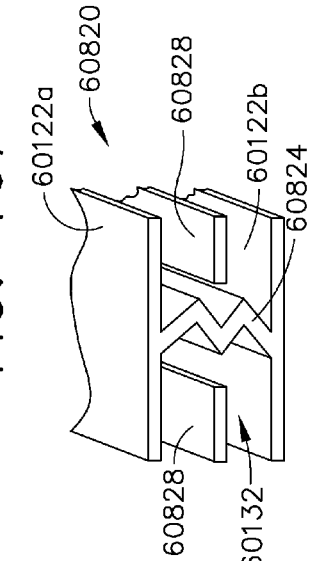


FIG. 168

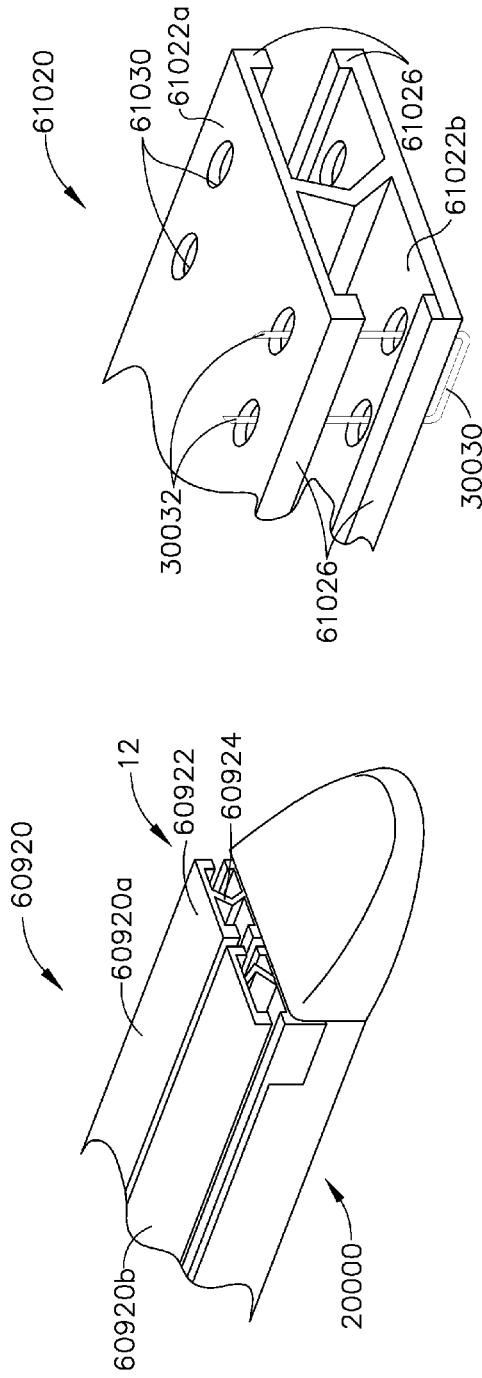


FIG. 169

FIG. 170

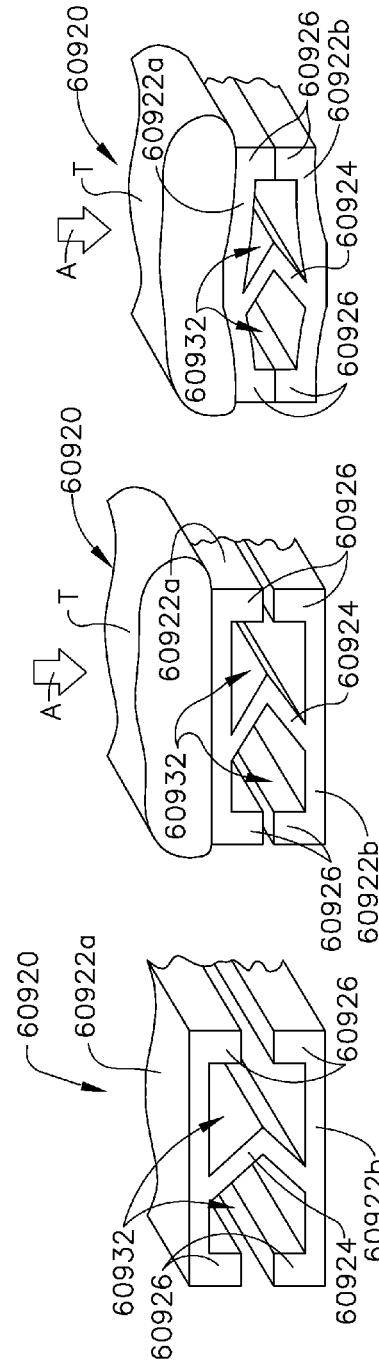


FIG. 171

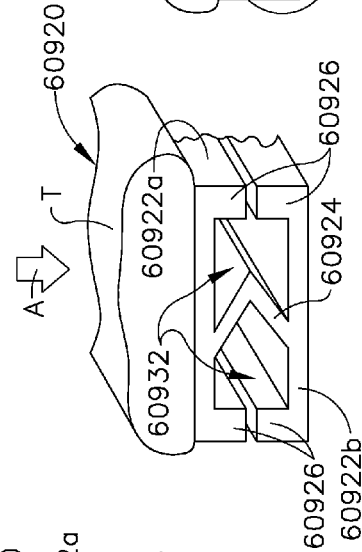


FIG. 172

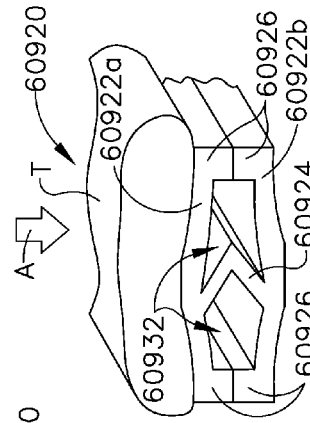
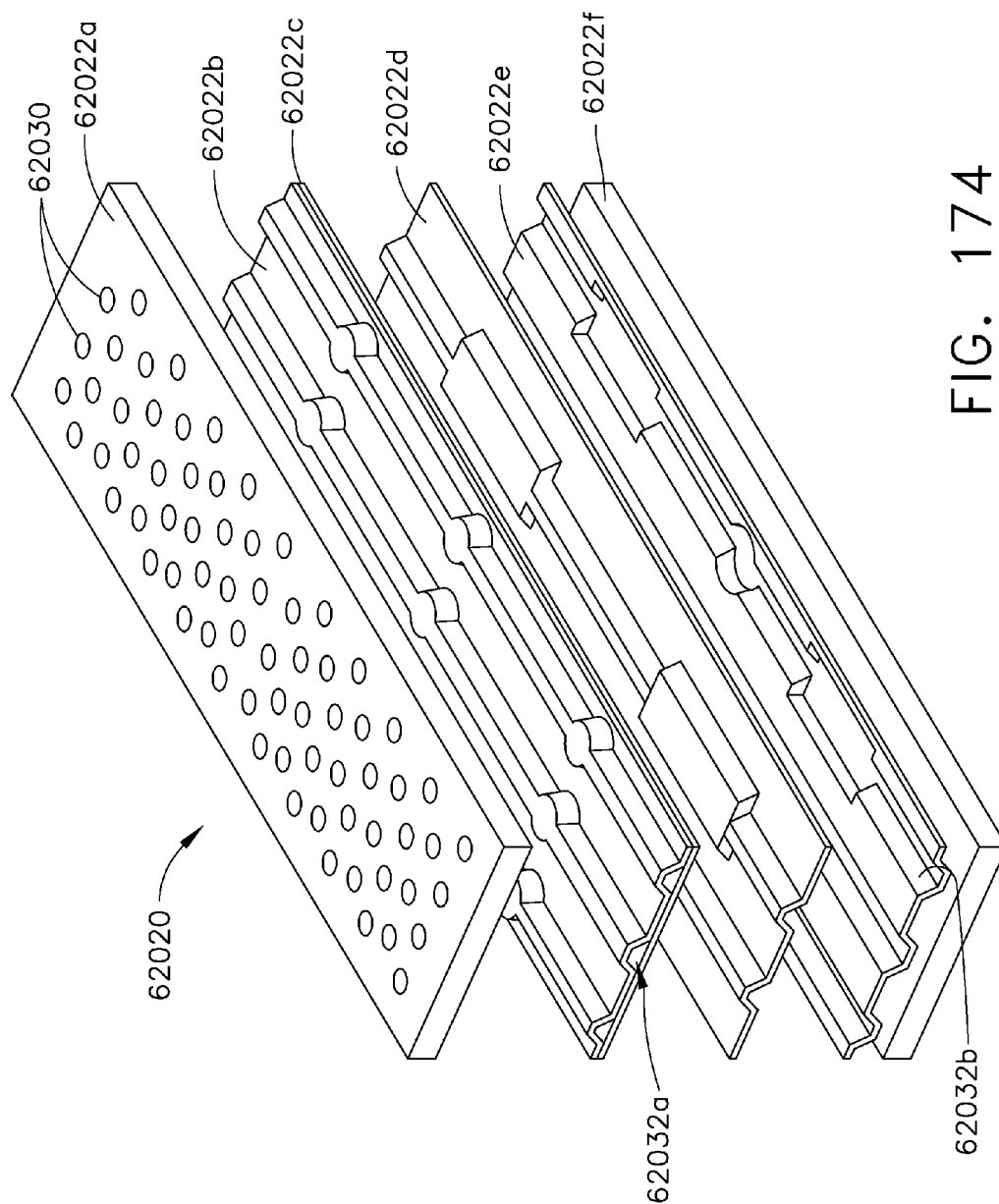


FIG. 173



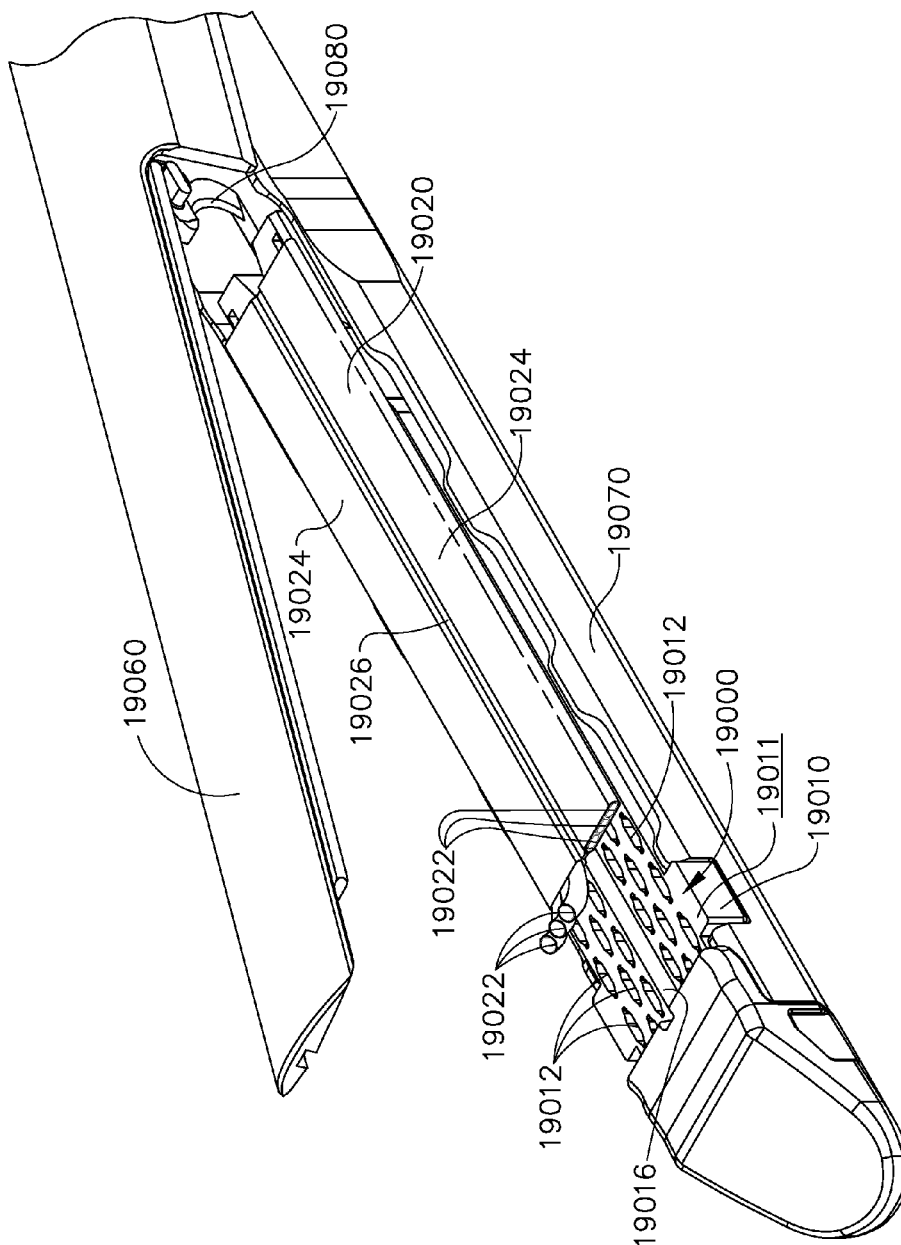


FIG. 175

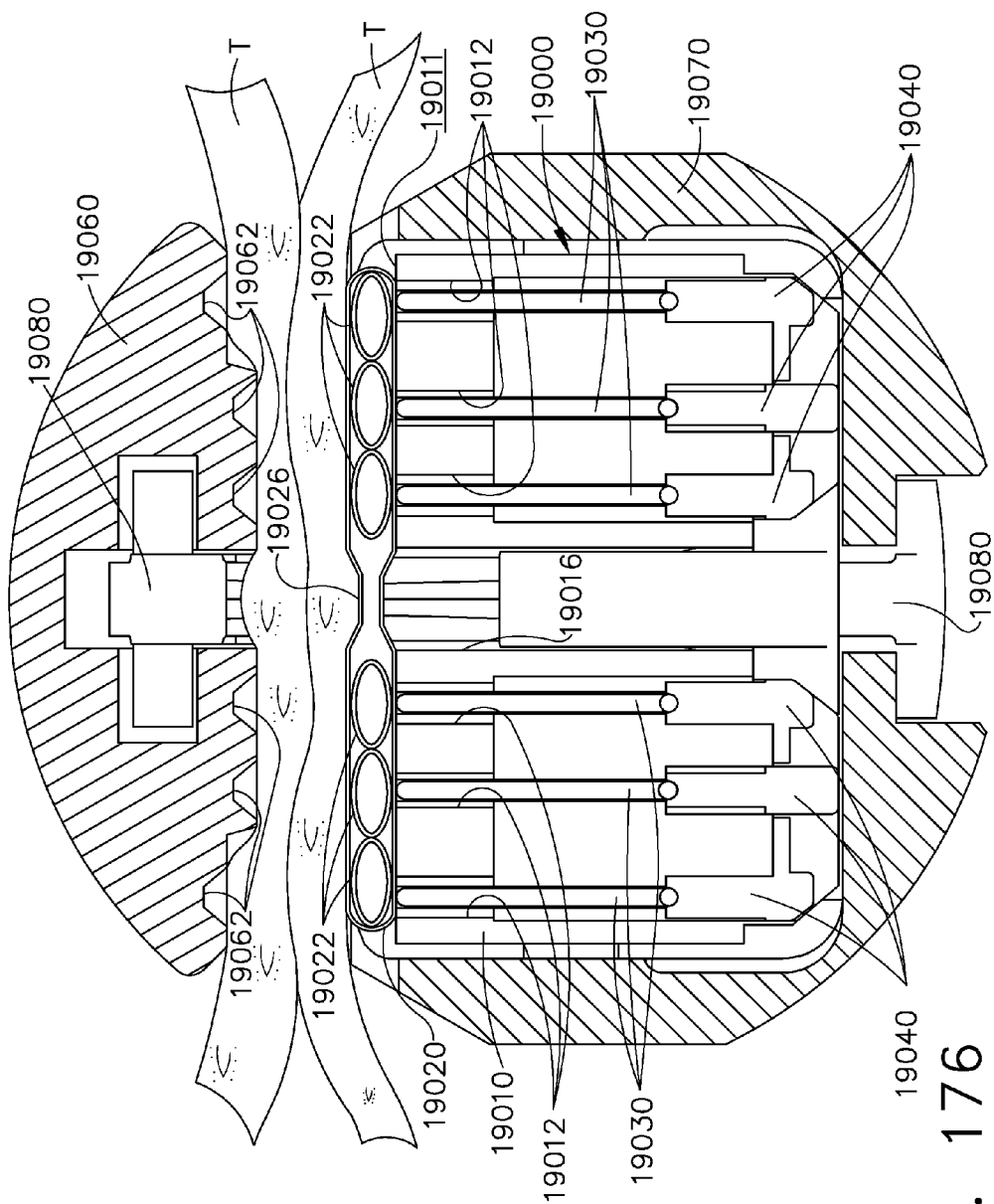


FIG. 176

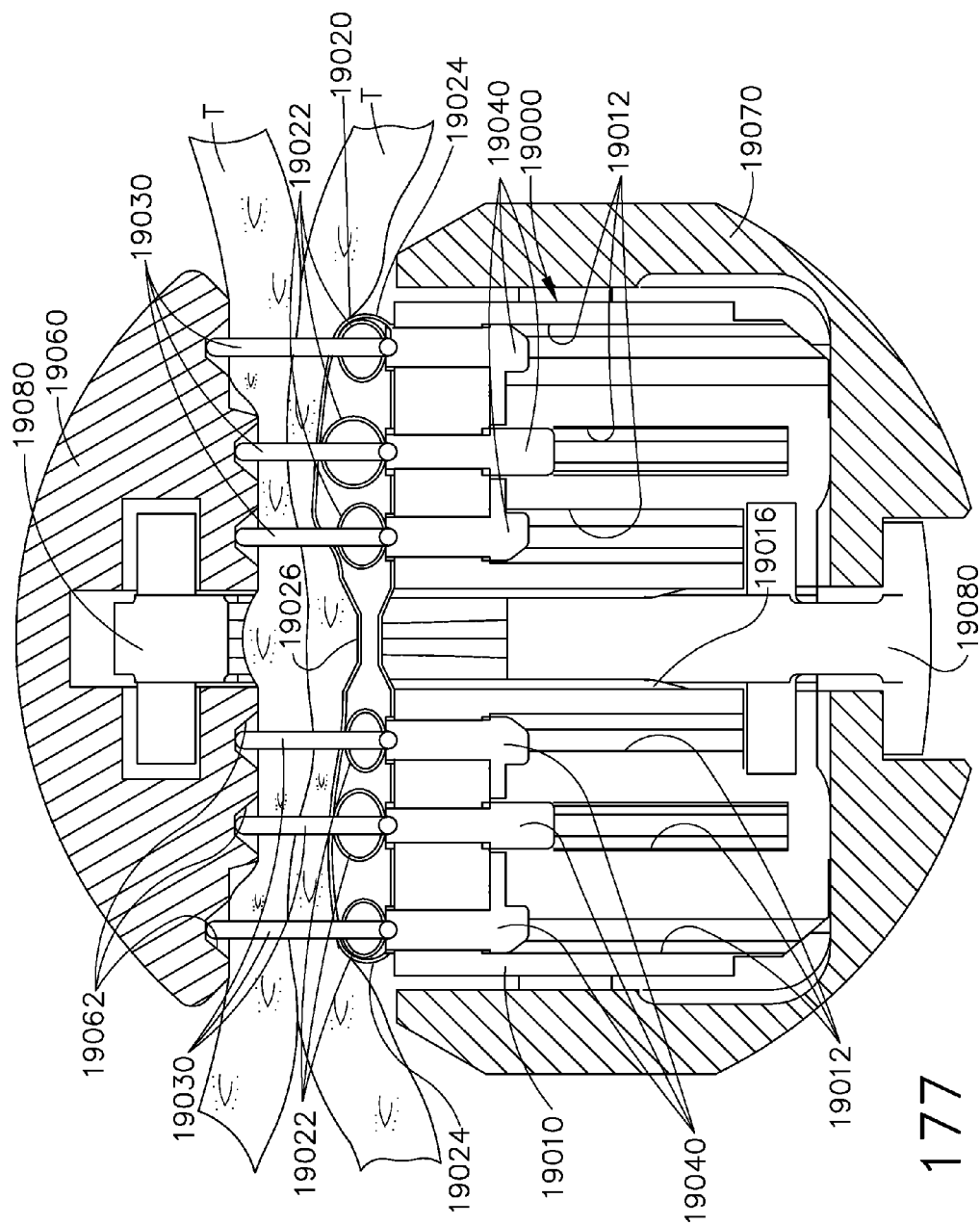


FIG. 177

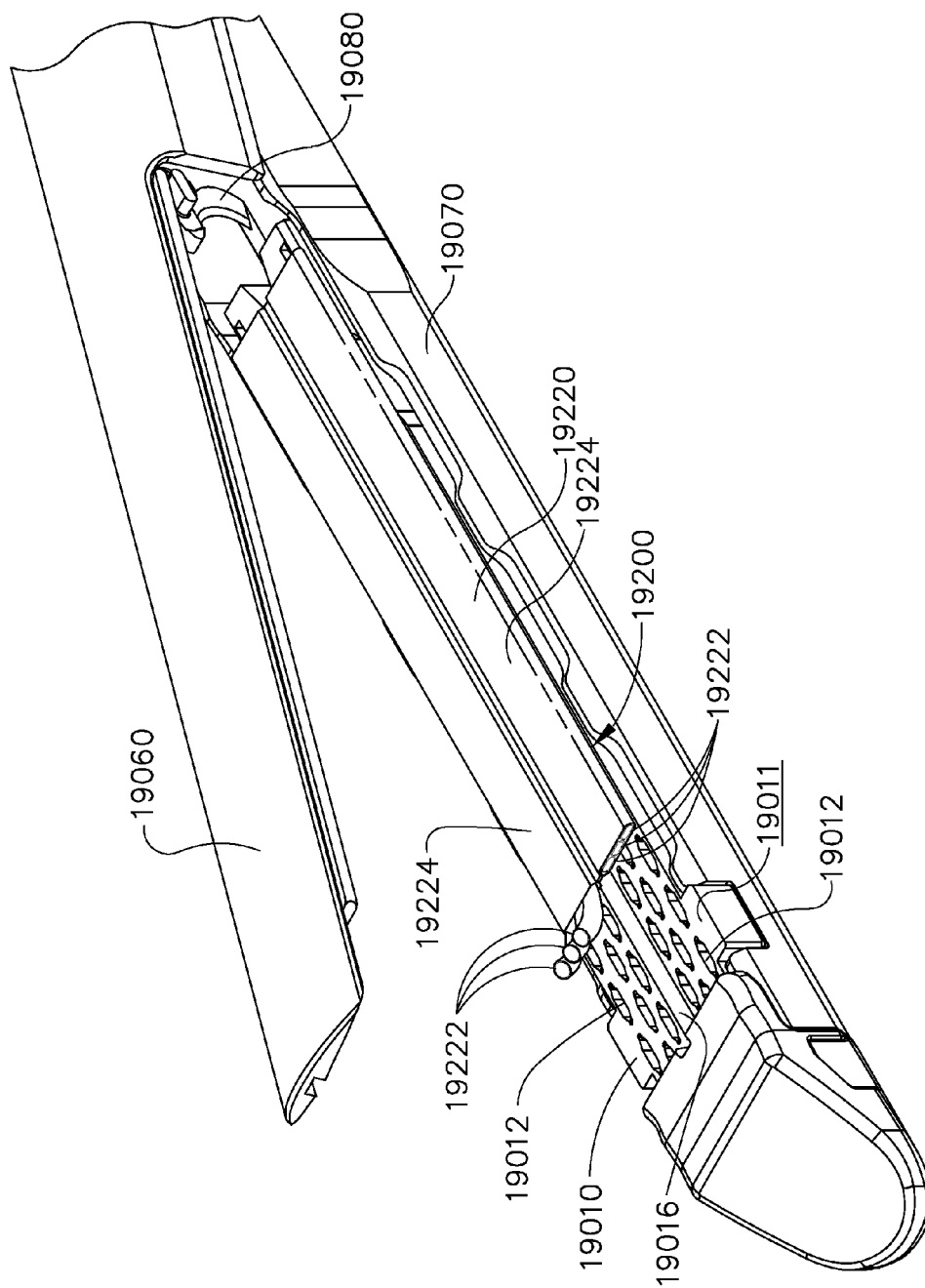


FIG. 178

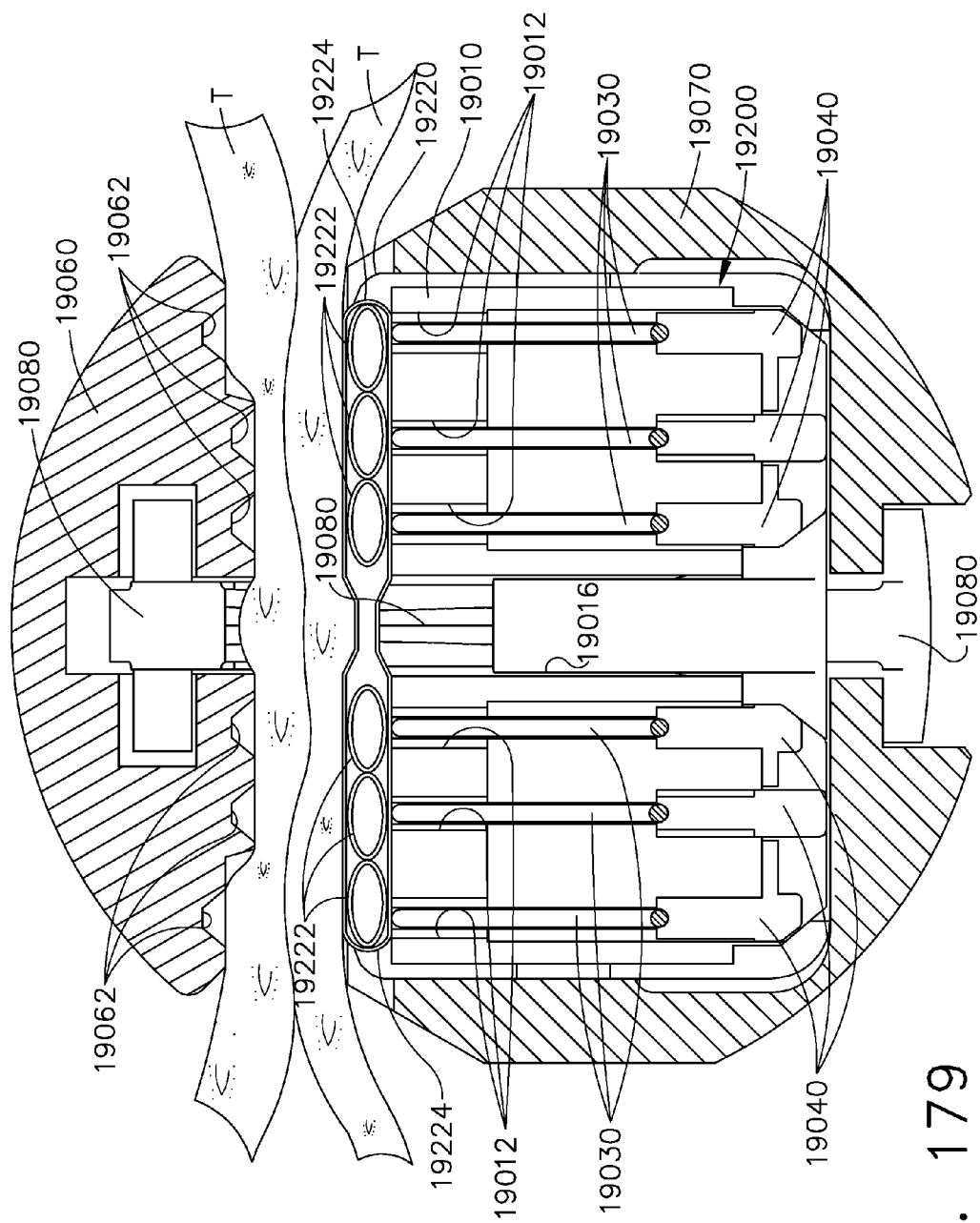


FIG. 179

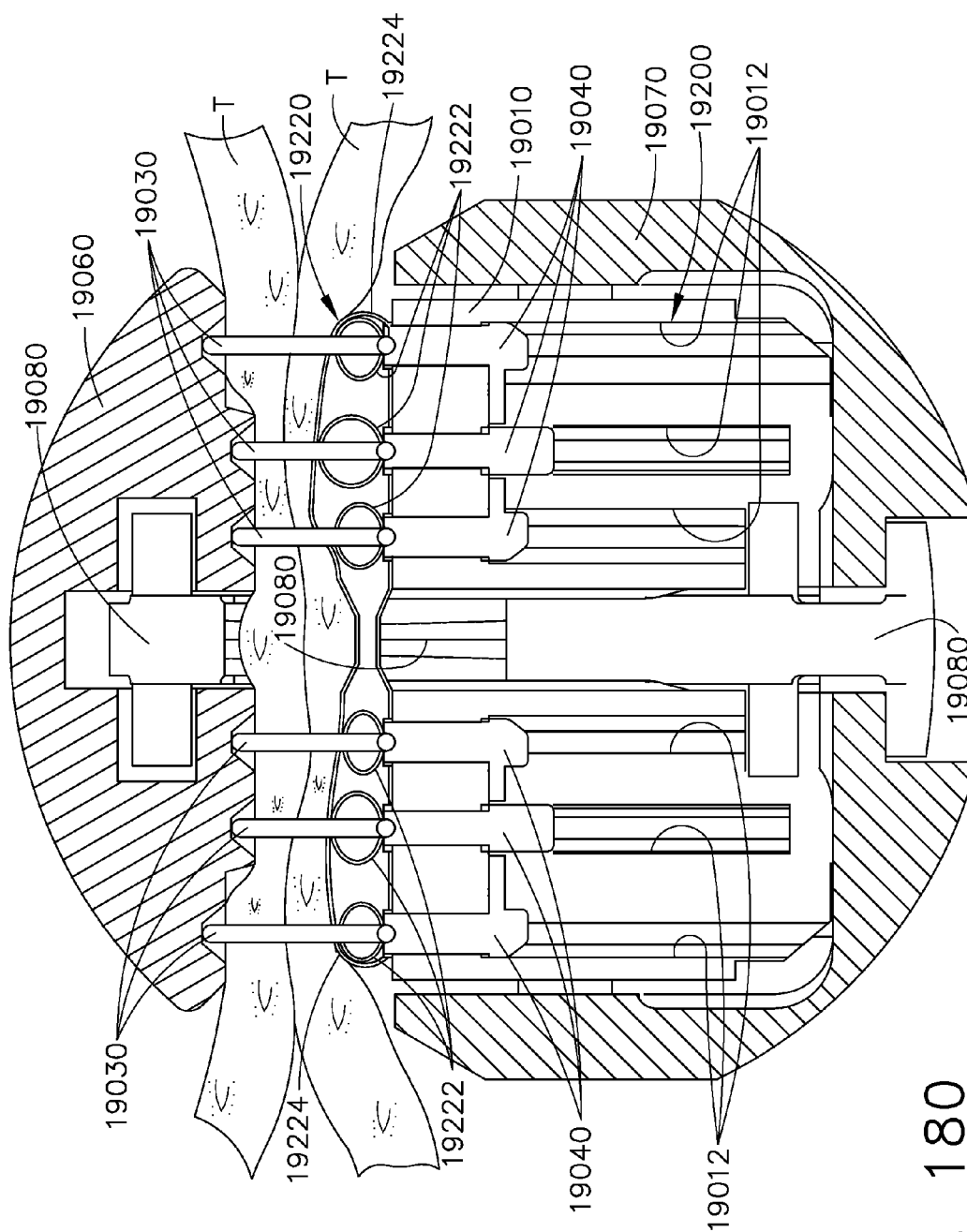


FIG. 180

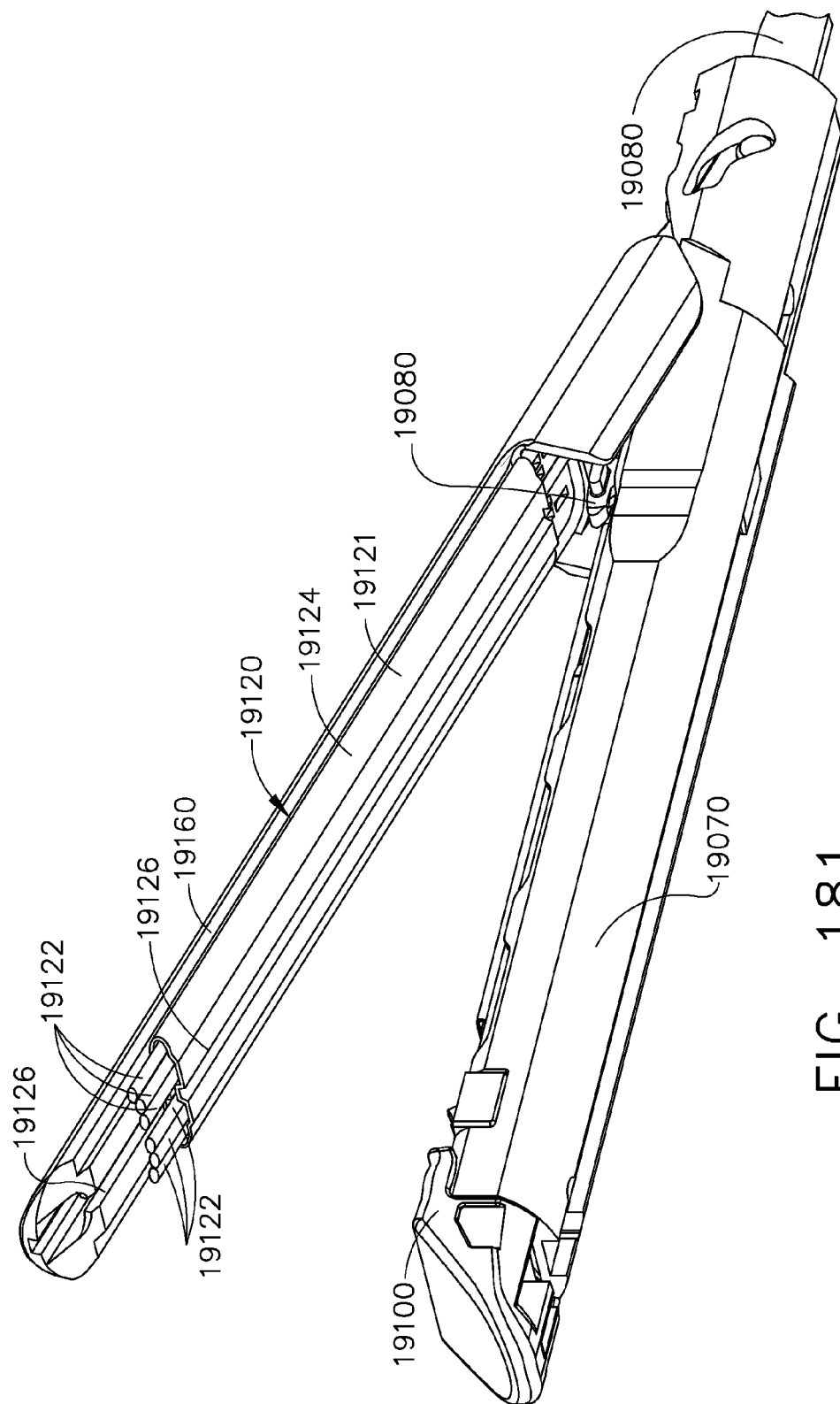


FIG. 181

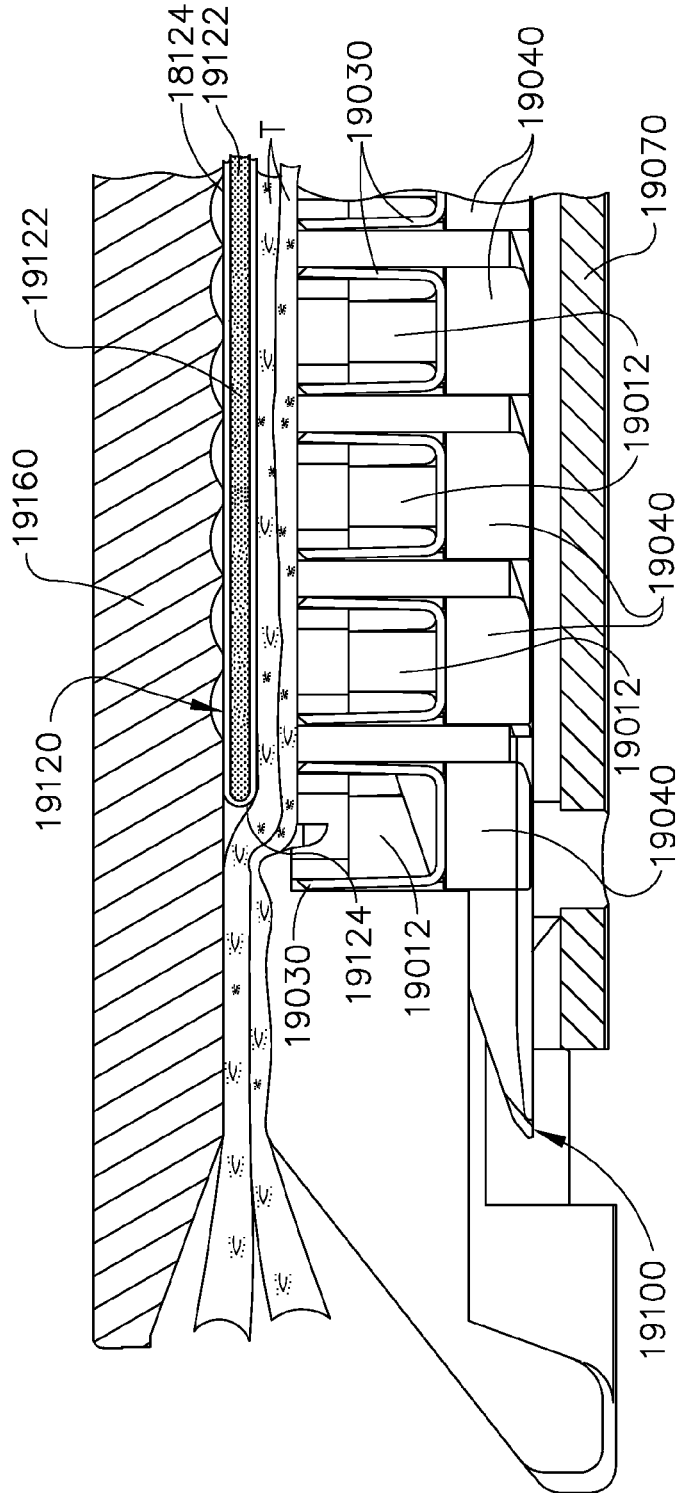


FIG. 182

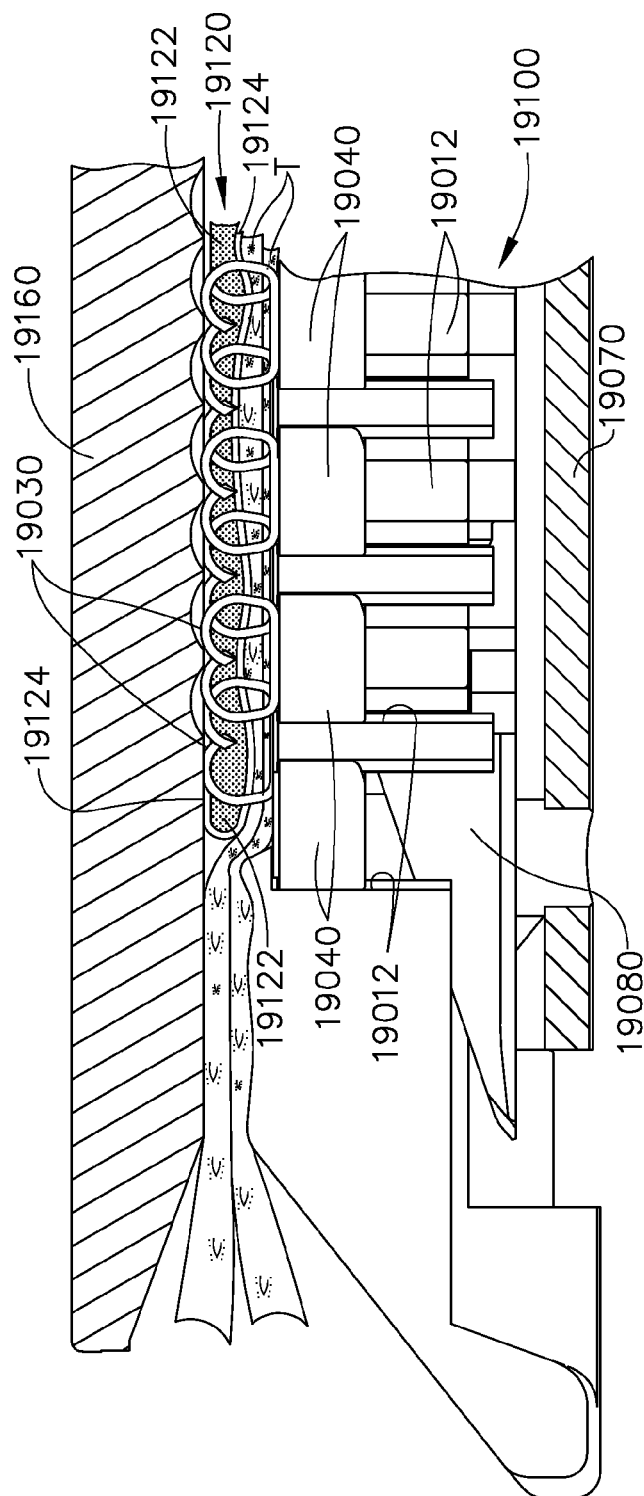


FIG. 183

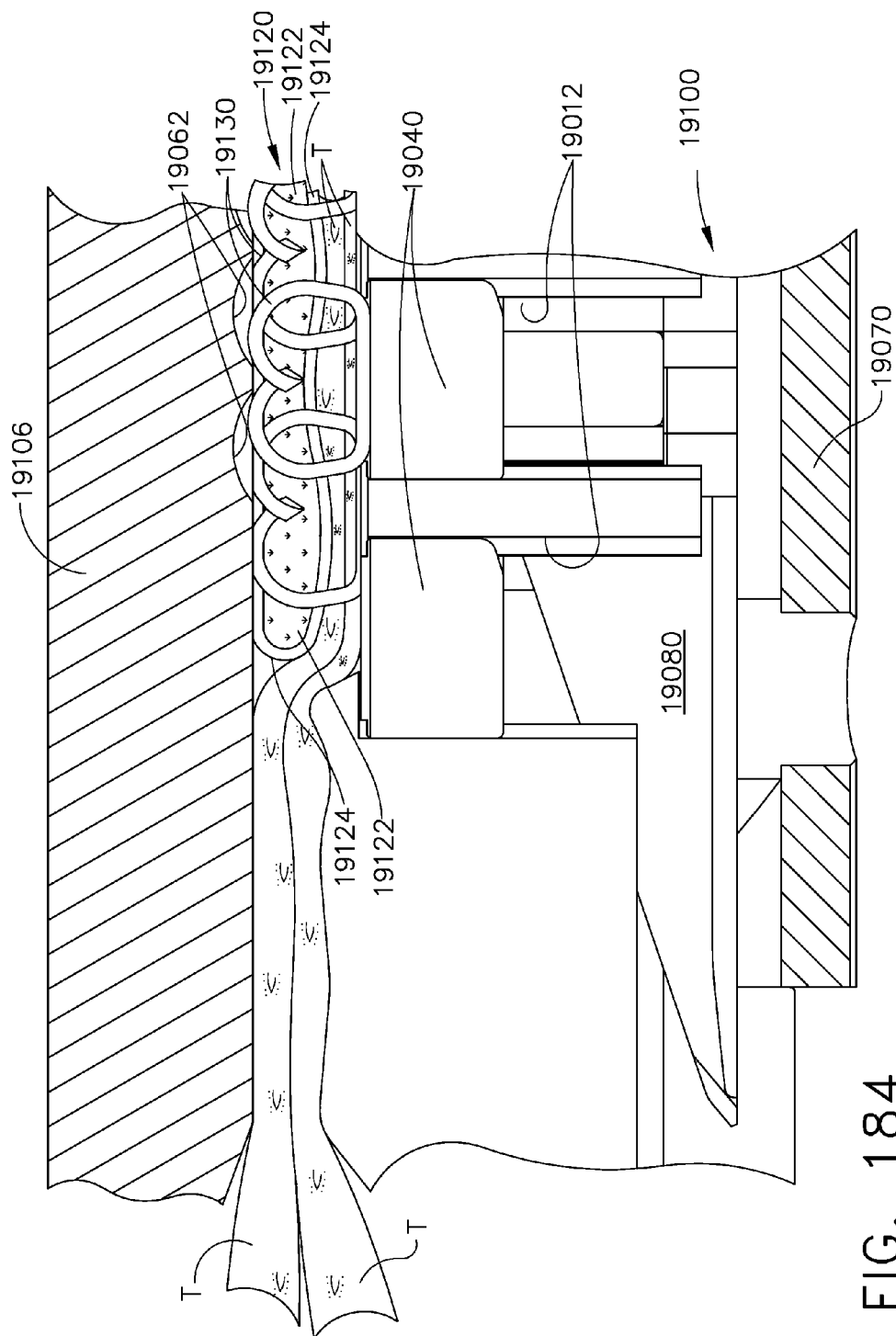


FIG. 184

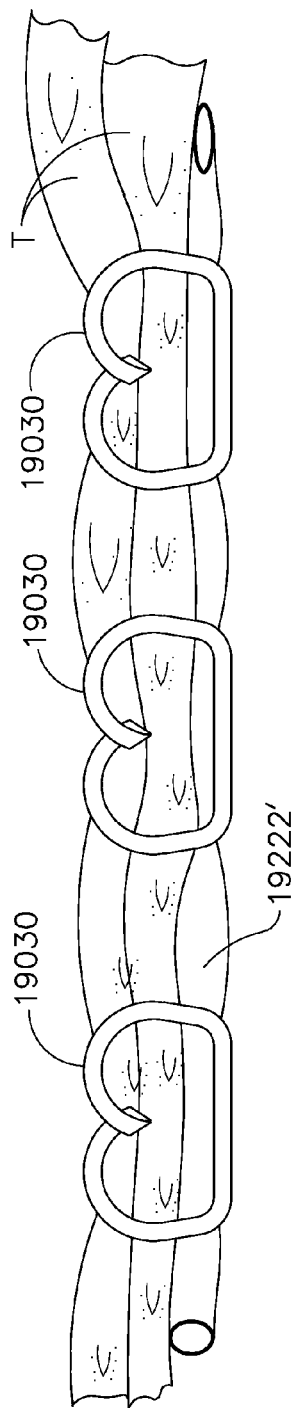


FIG. 185

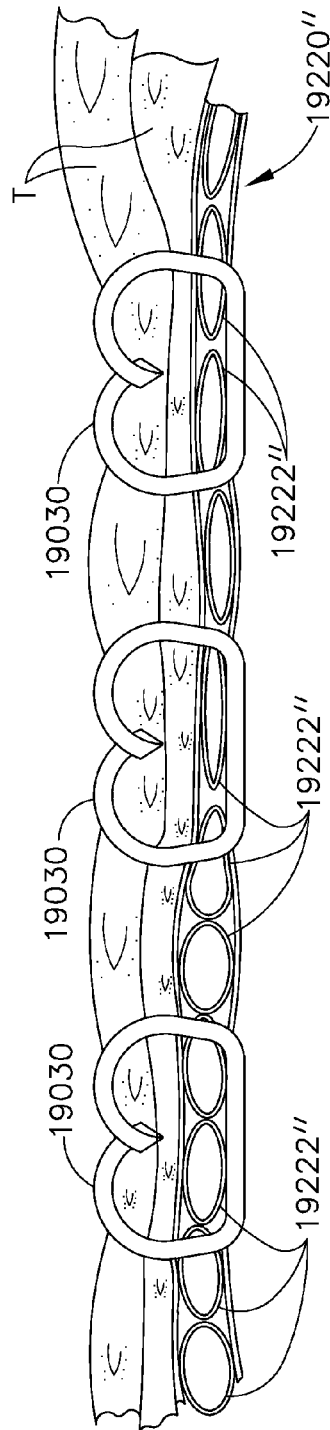


FIG. 186

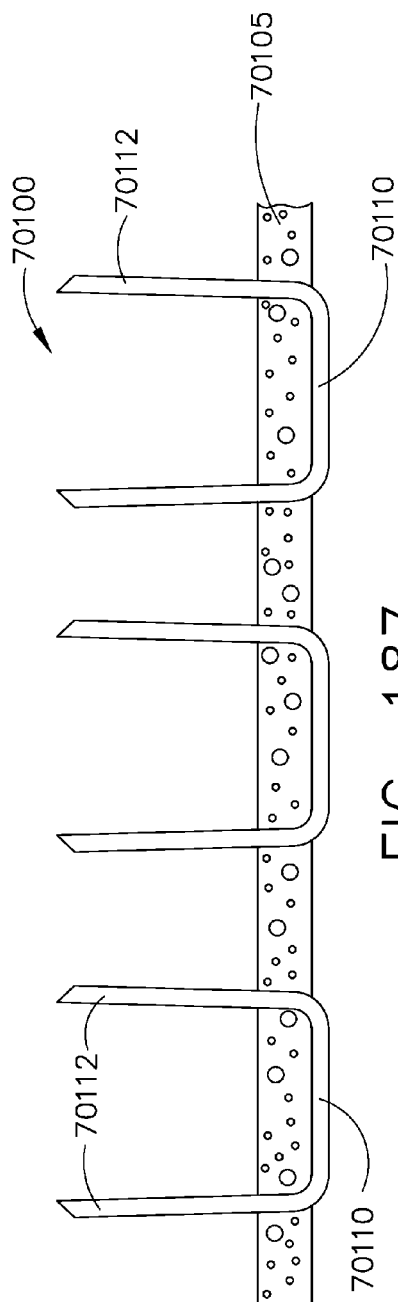


FIG. 187

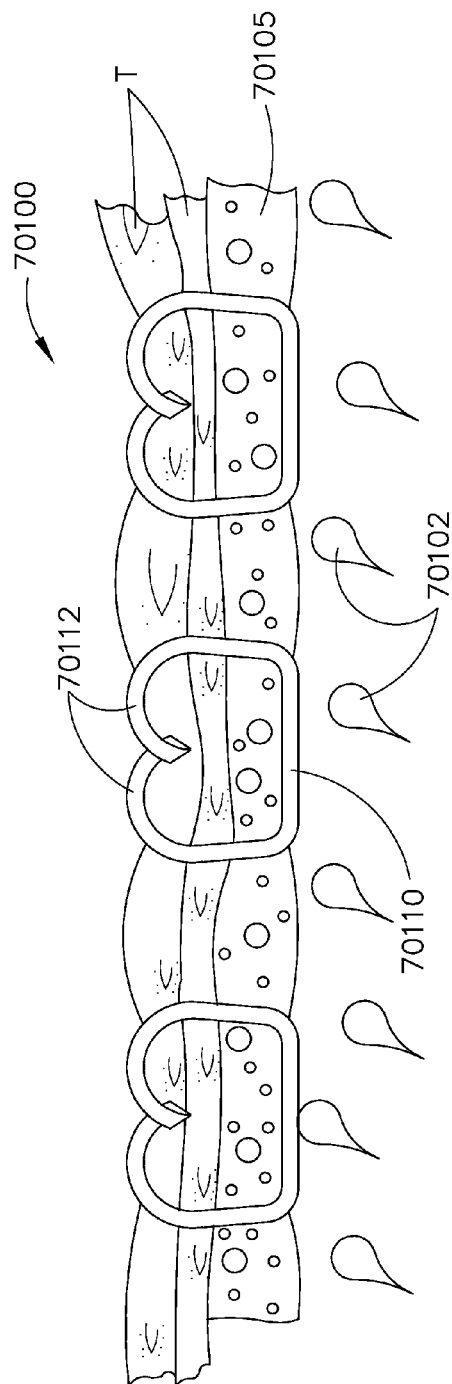


FIG. 188

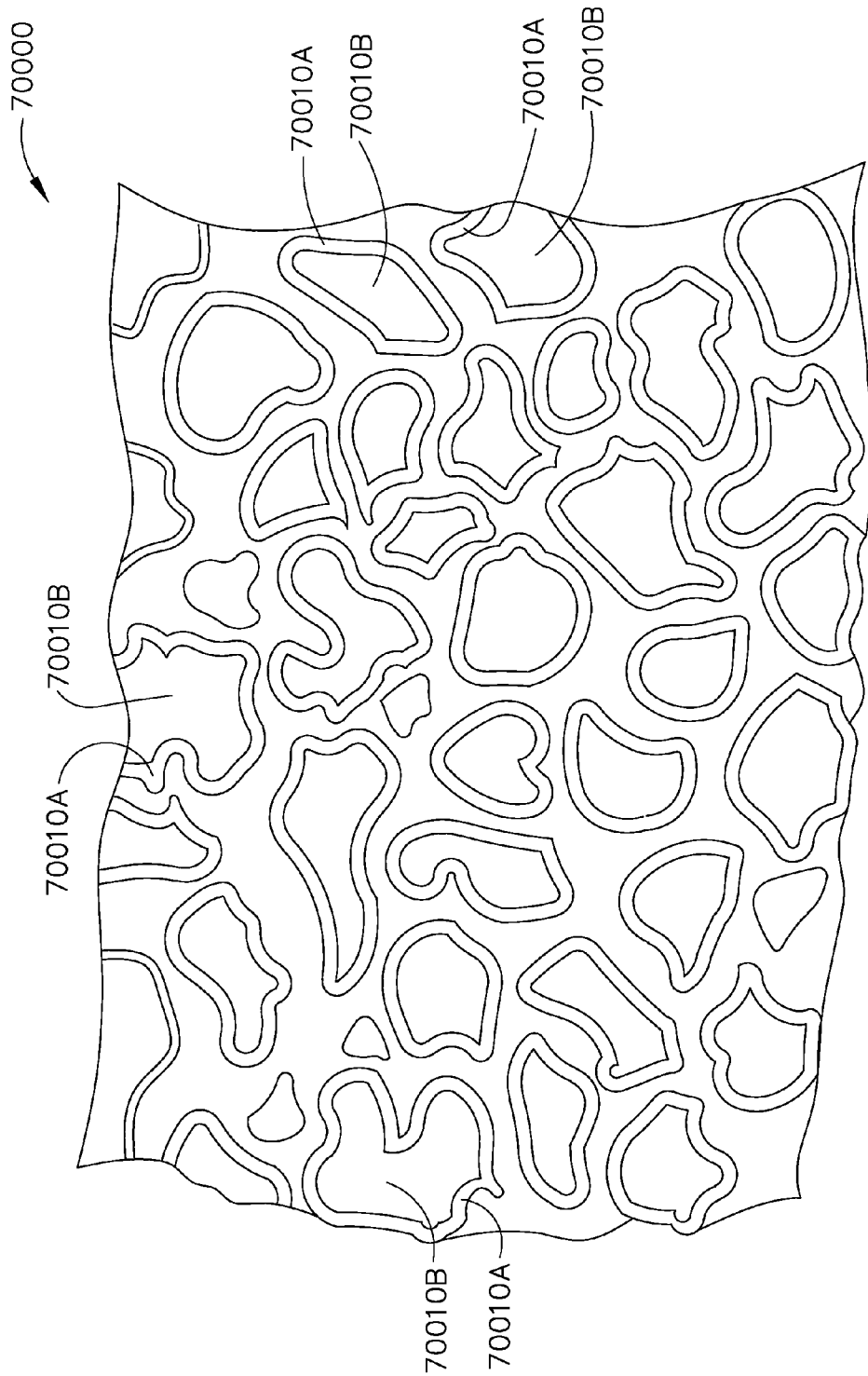


FIG. 189A

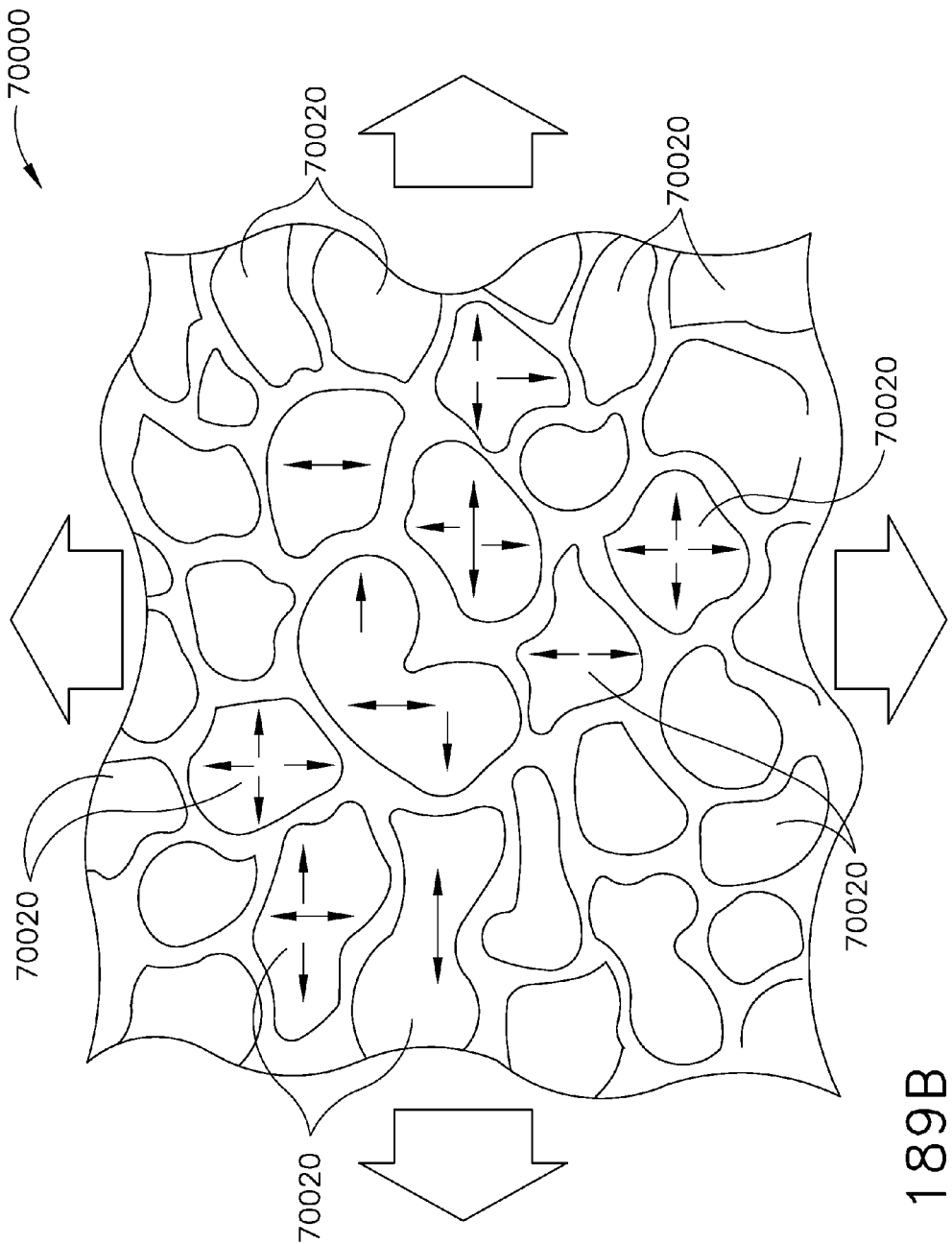


FIG. 189B

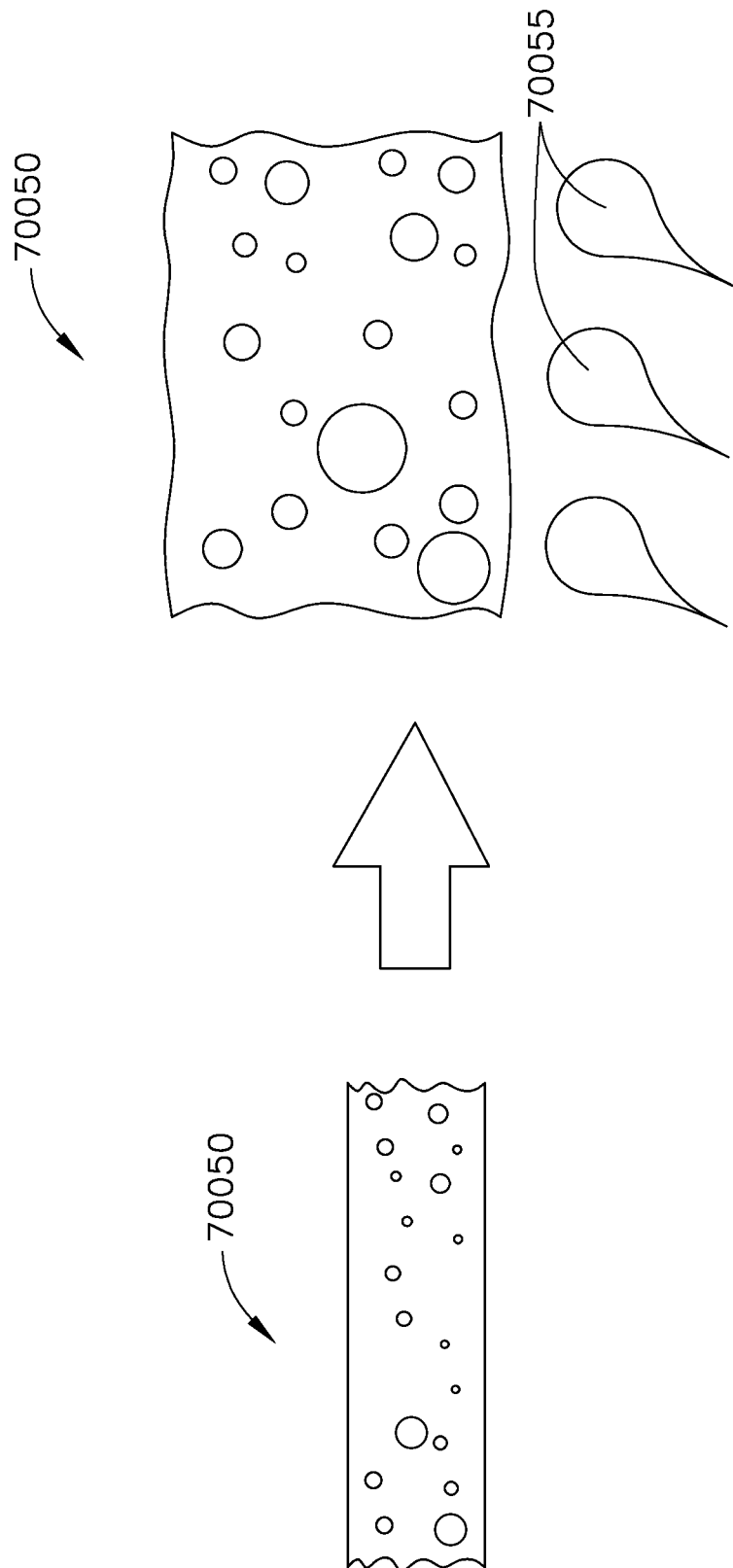


FIG. 190

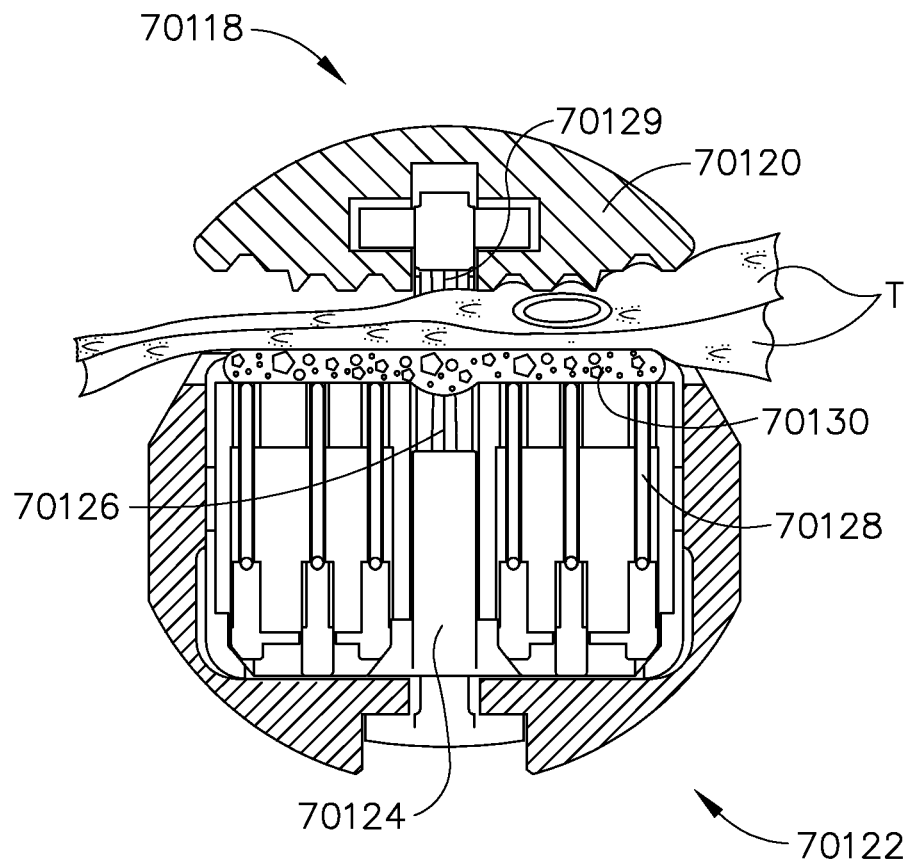


FIG. 191

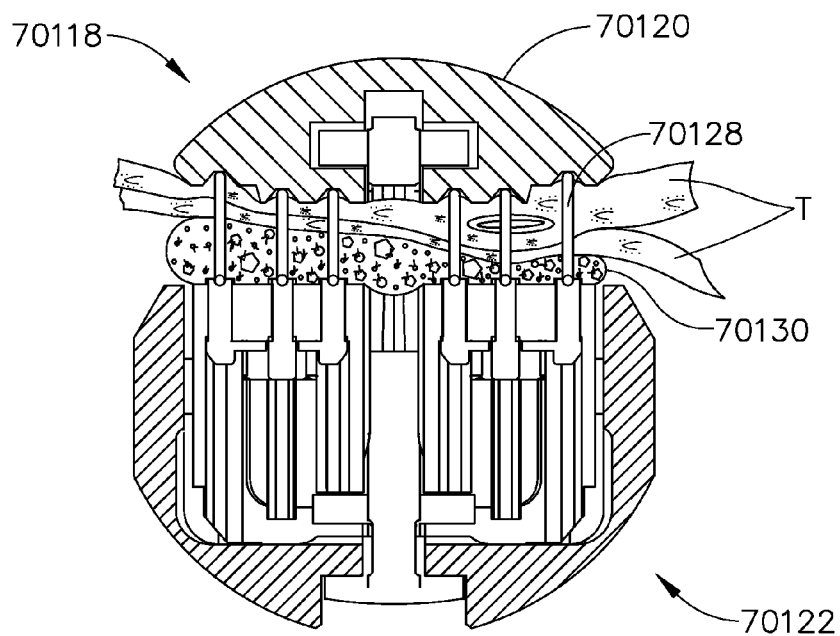


FIG. 192

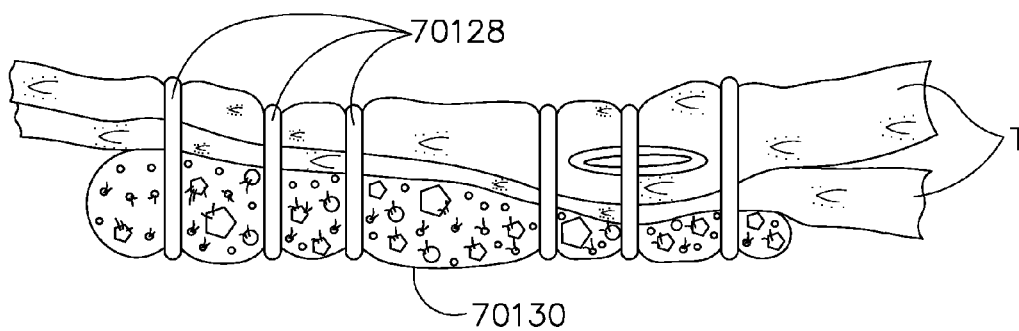


FIG. 193

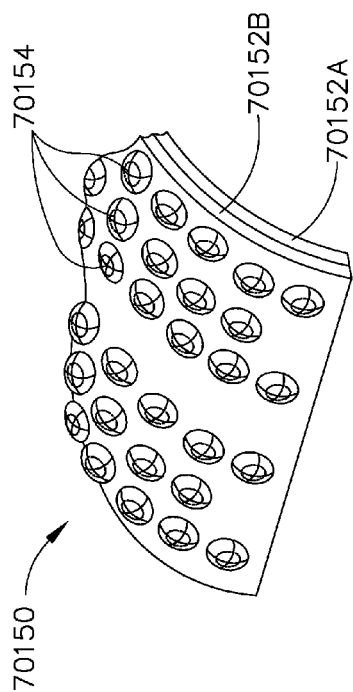


FIG. 194

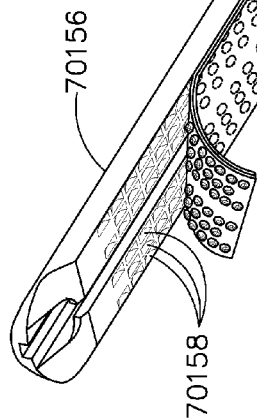


FIG. 195

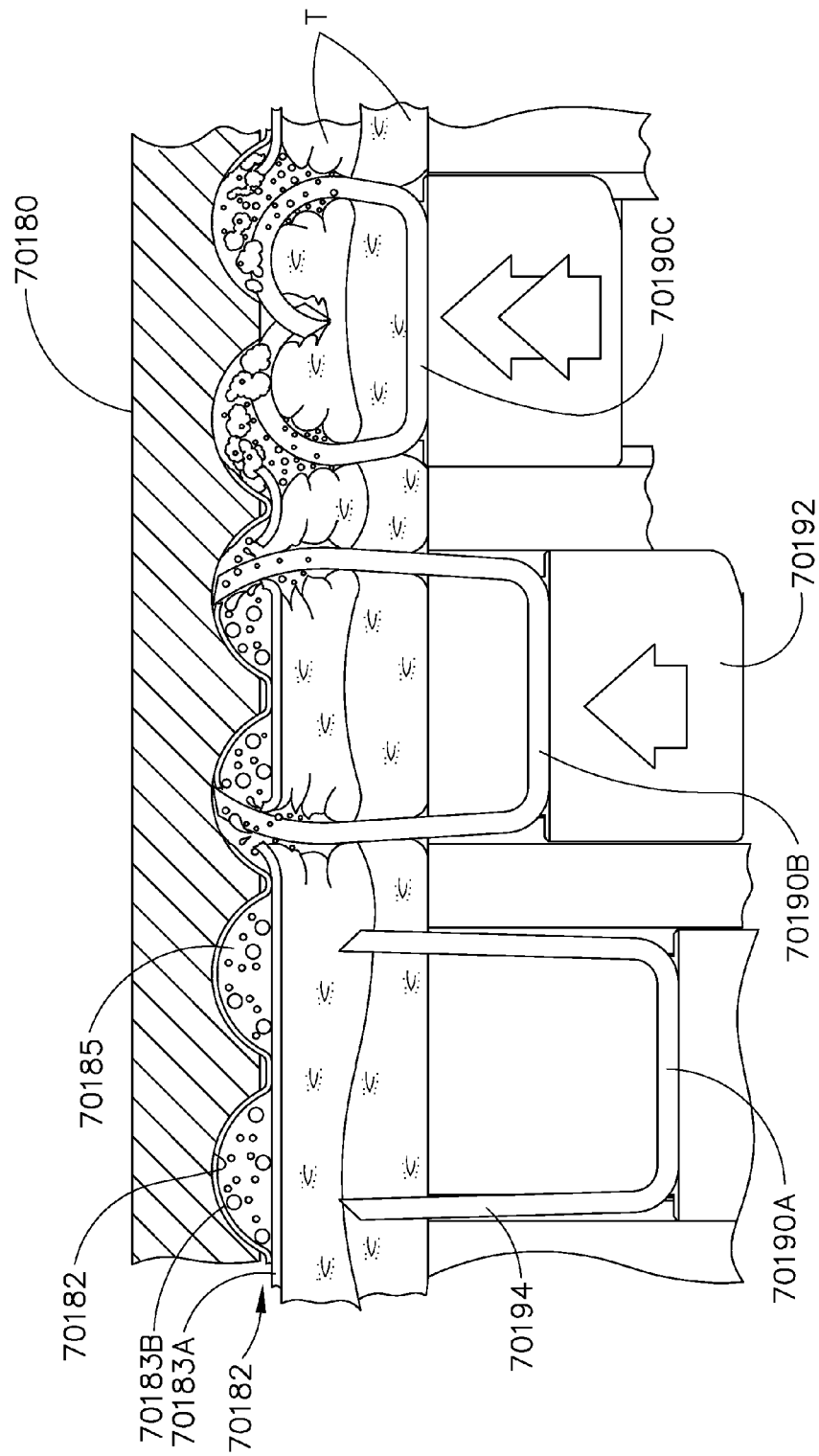


FIG. 196

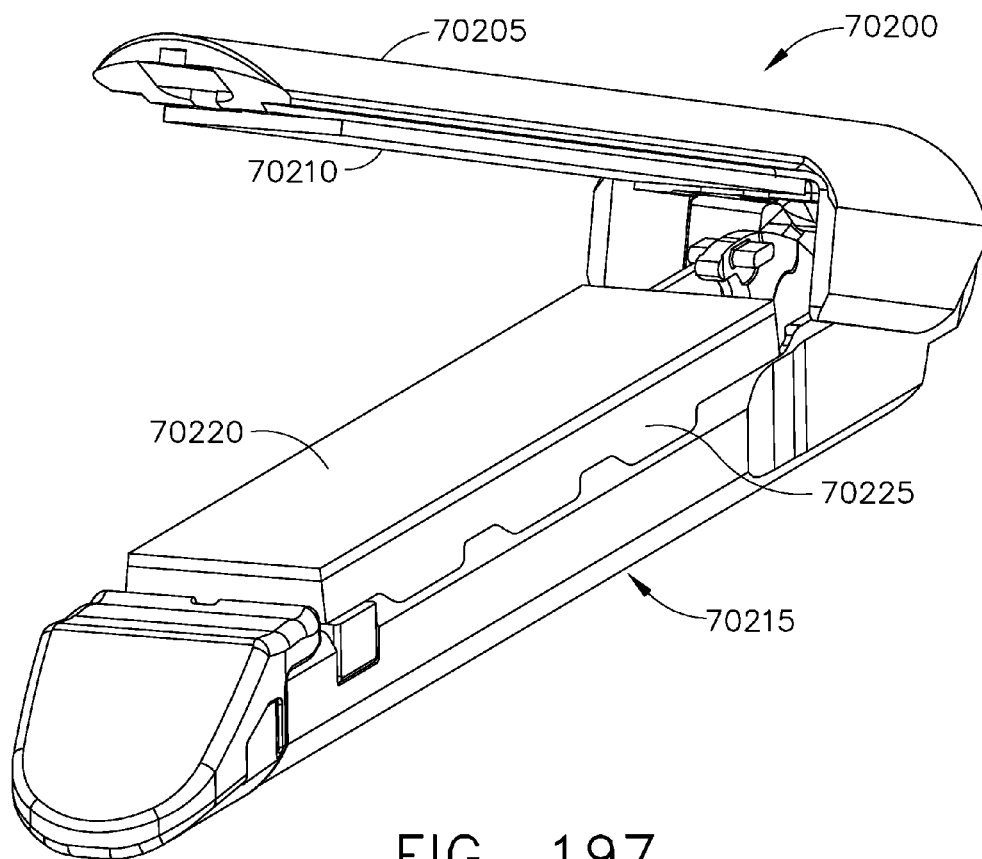


FIG. 197

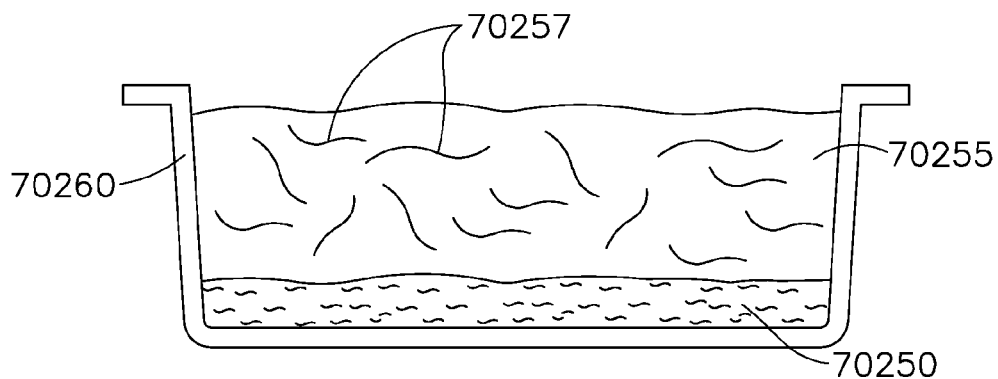


FIG. 198A

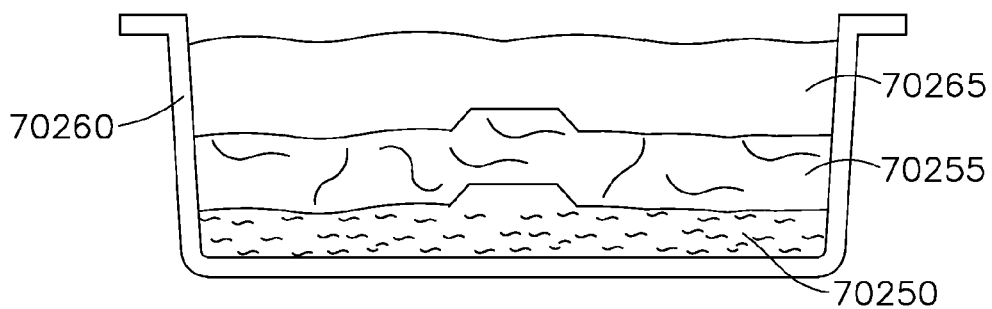


FIG. 198B

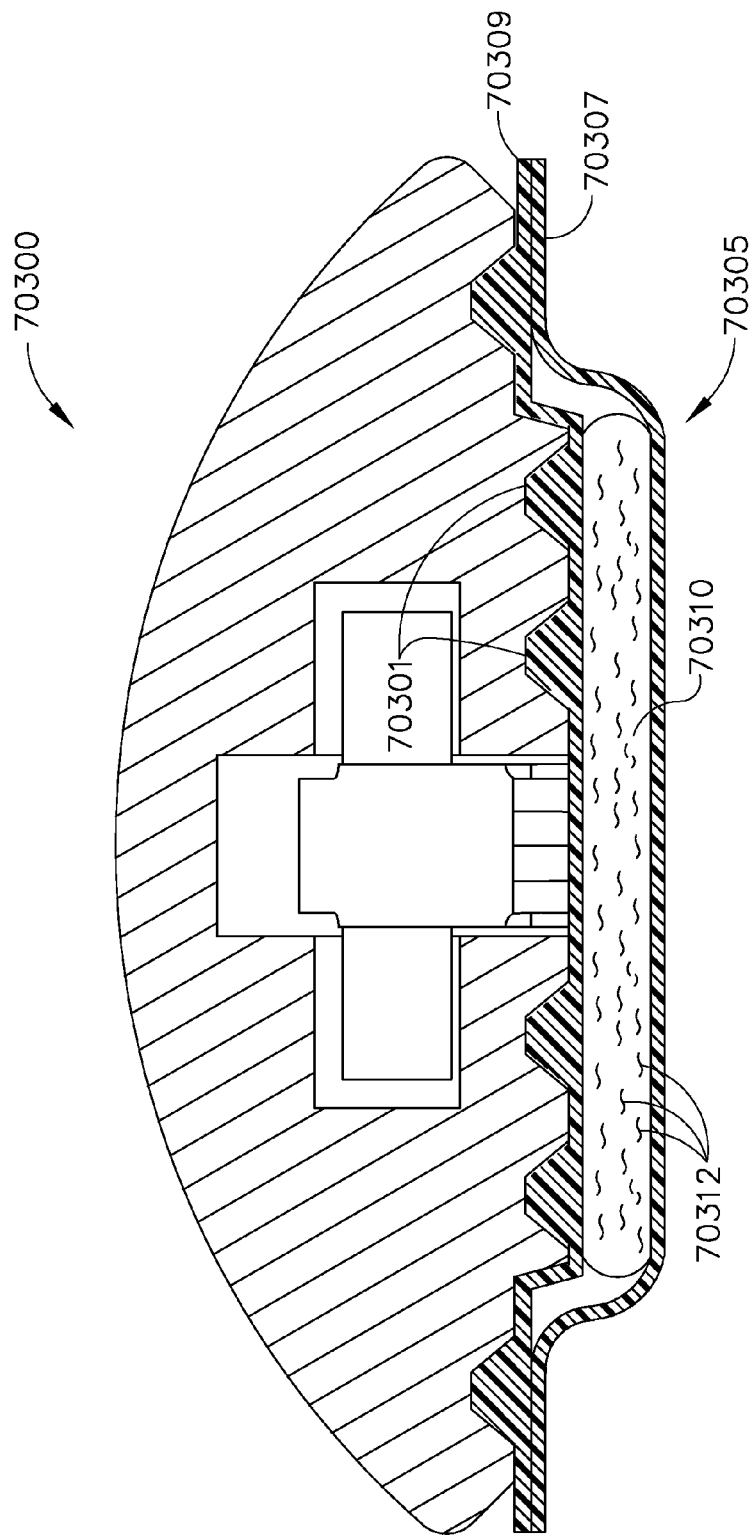


FIG. 199

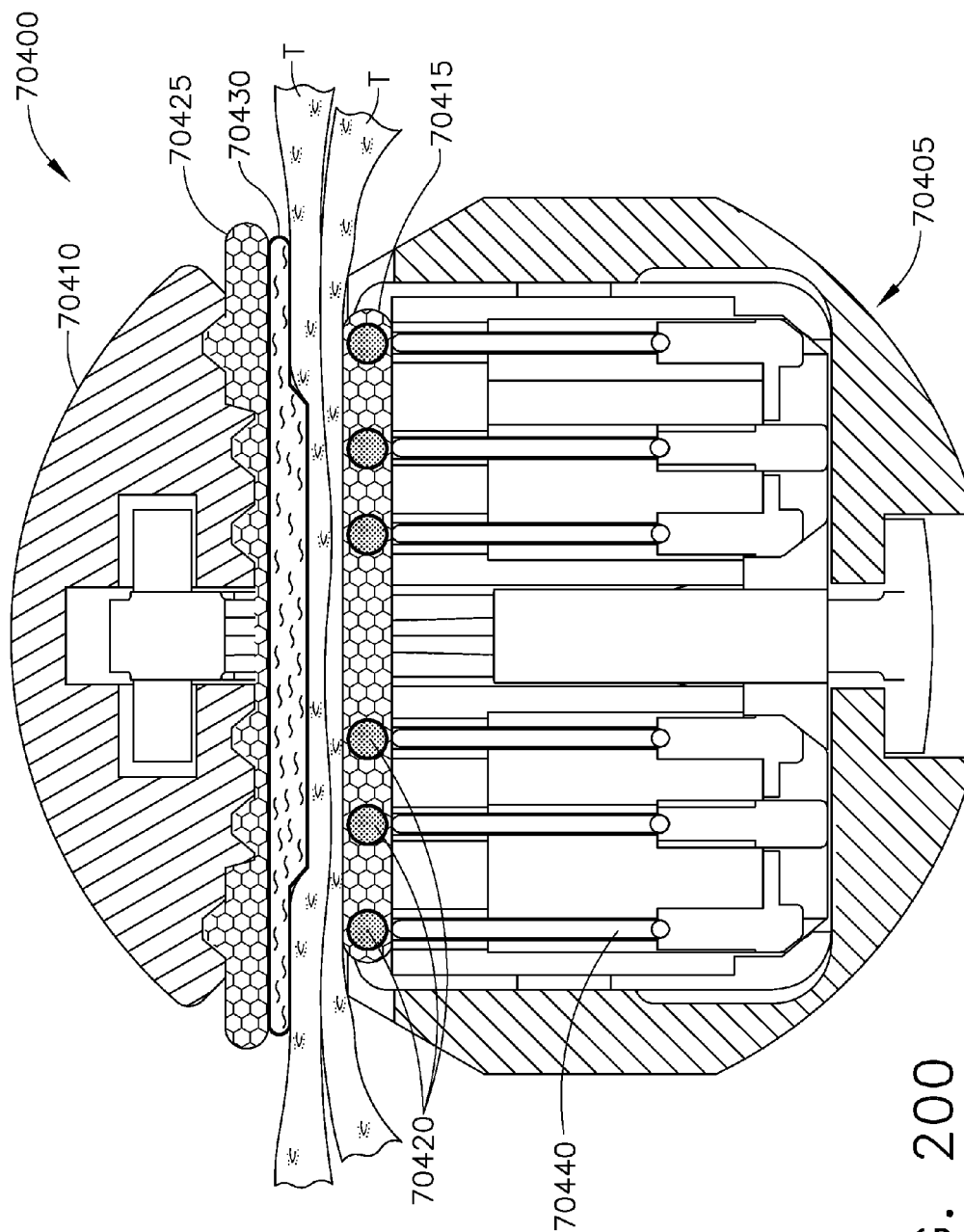


FIG. 200

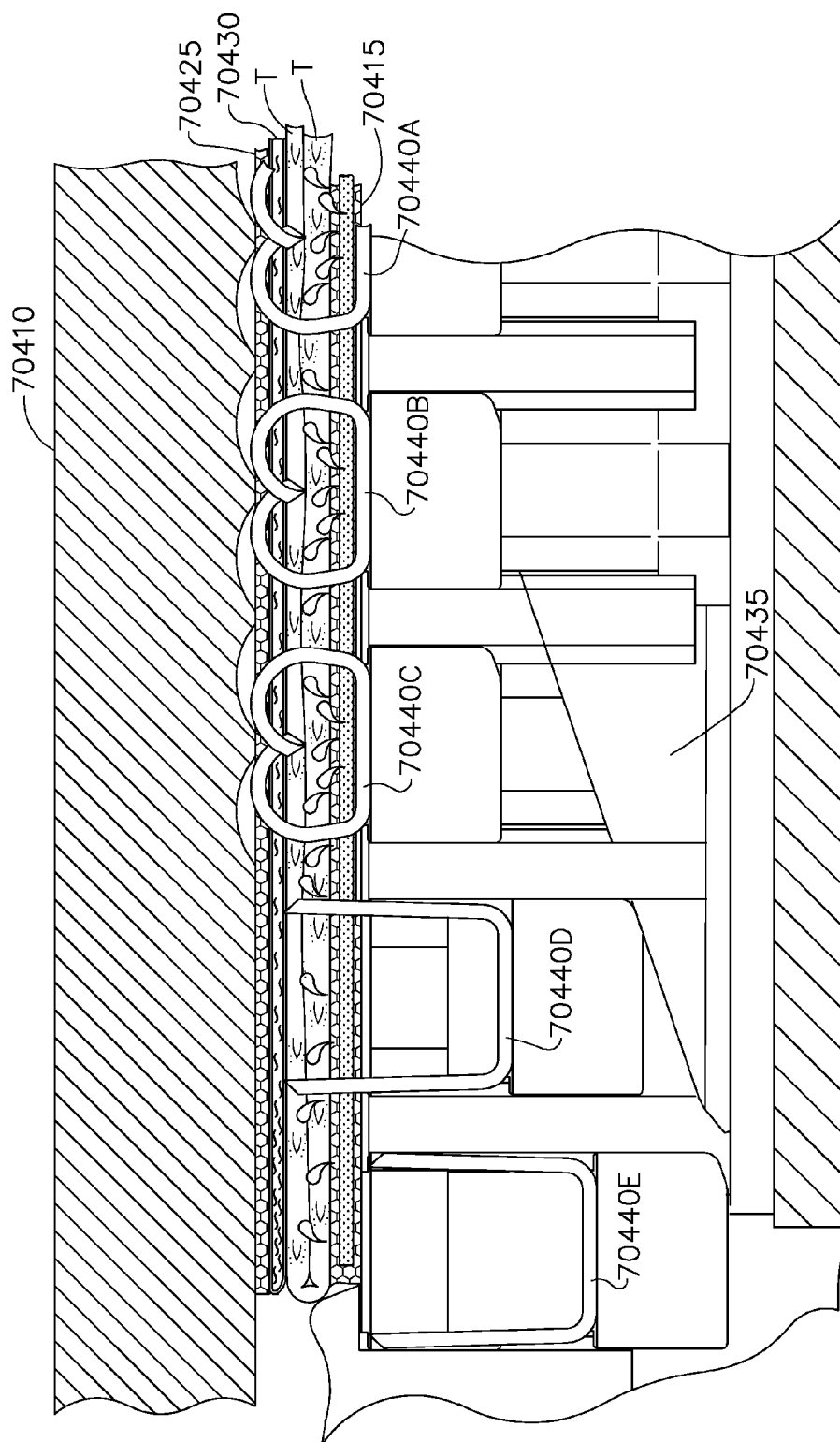


FIG. 201

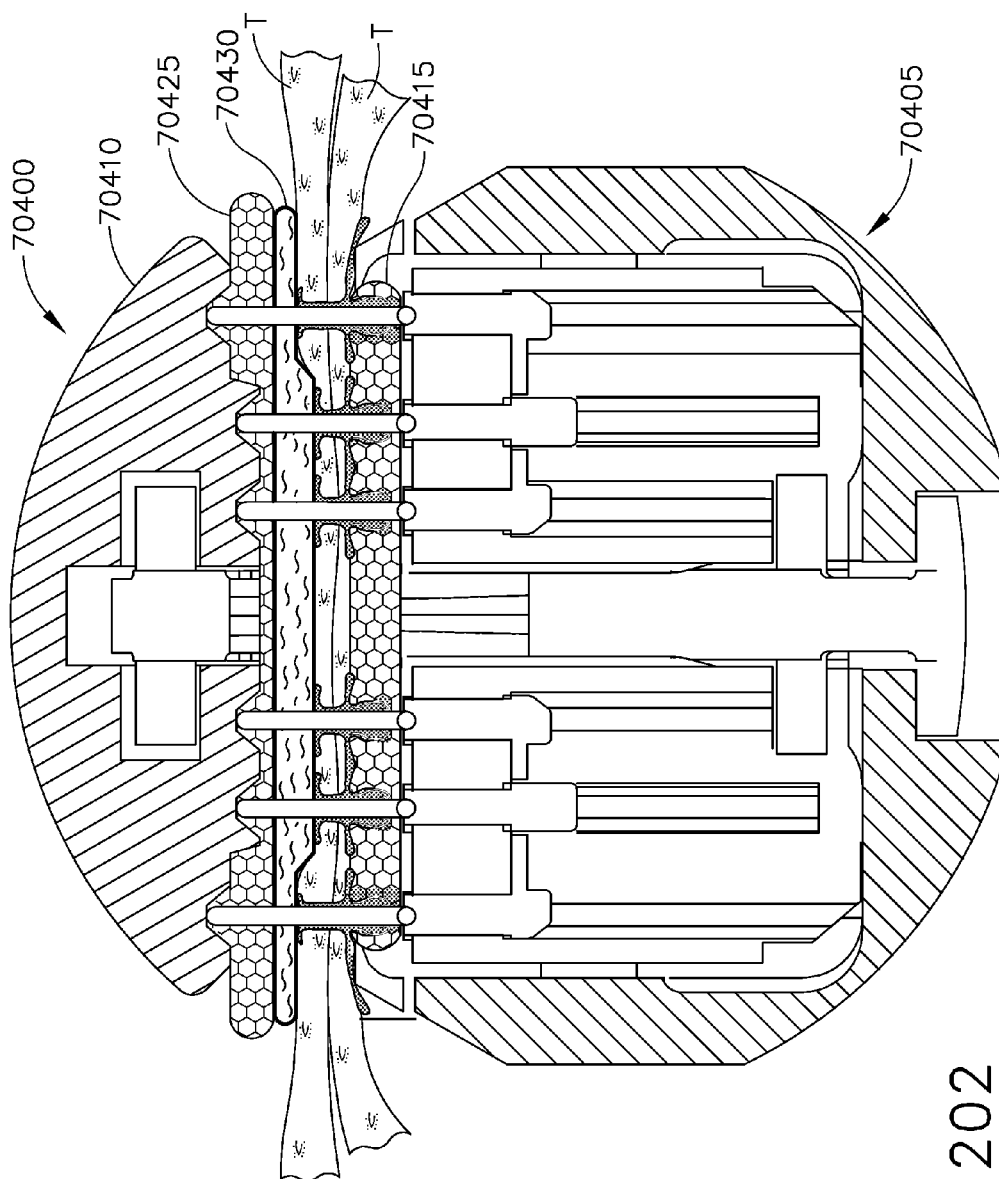


FIG. 202

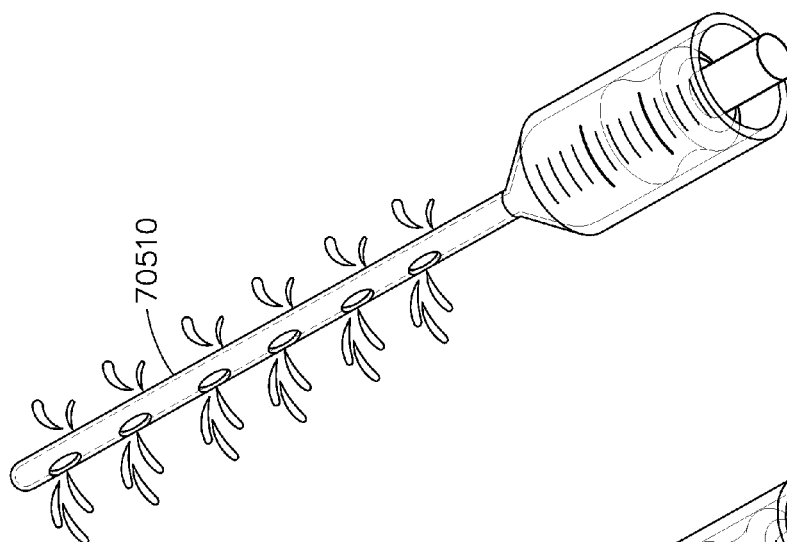


FIG. 203A

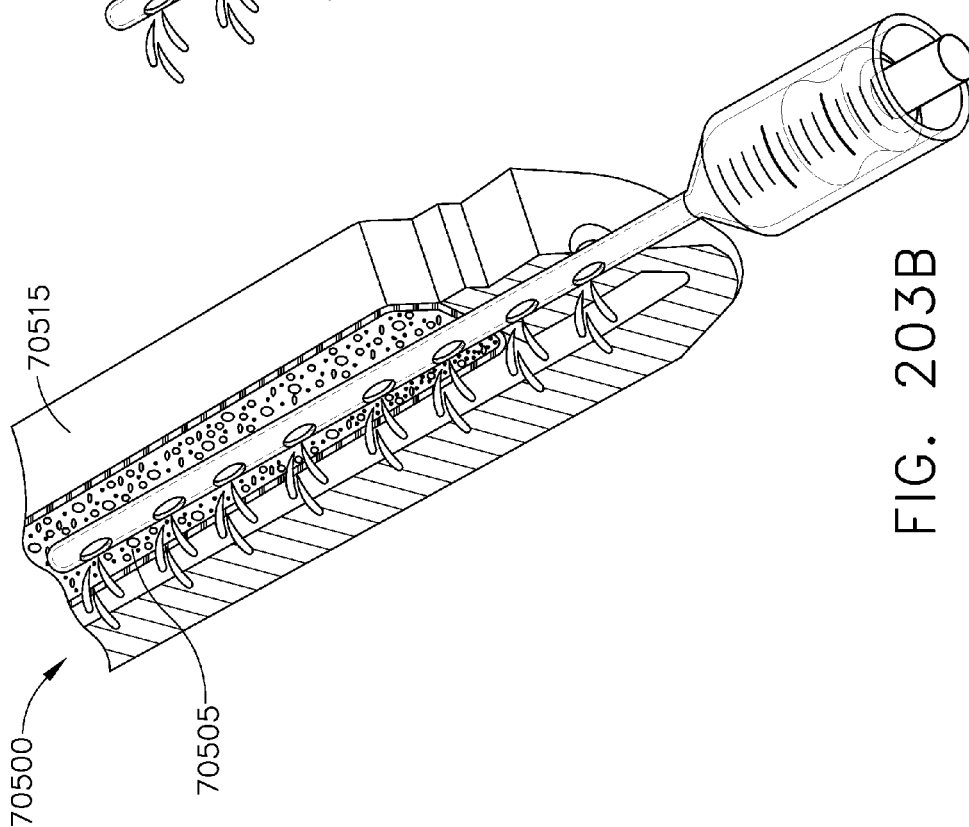


FIG. 203B

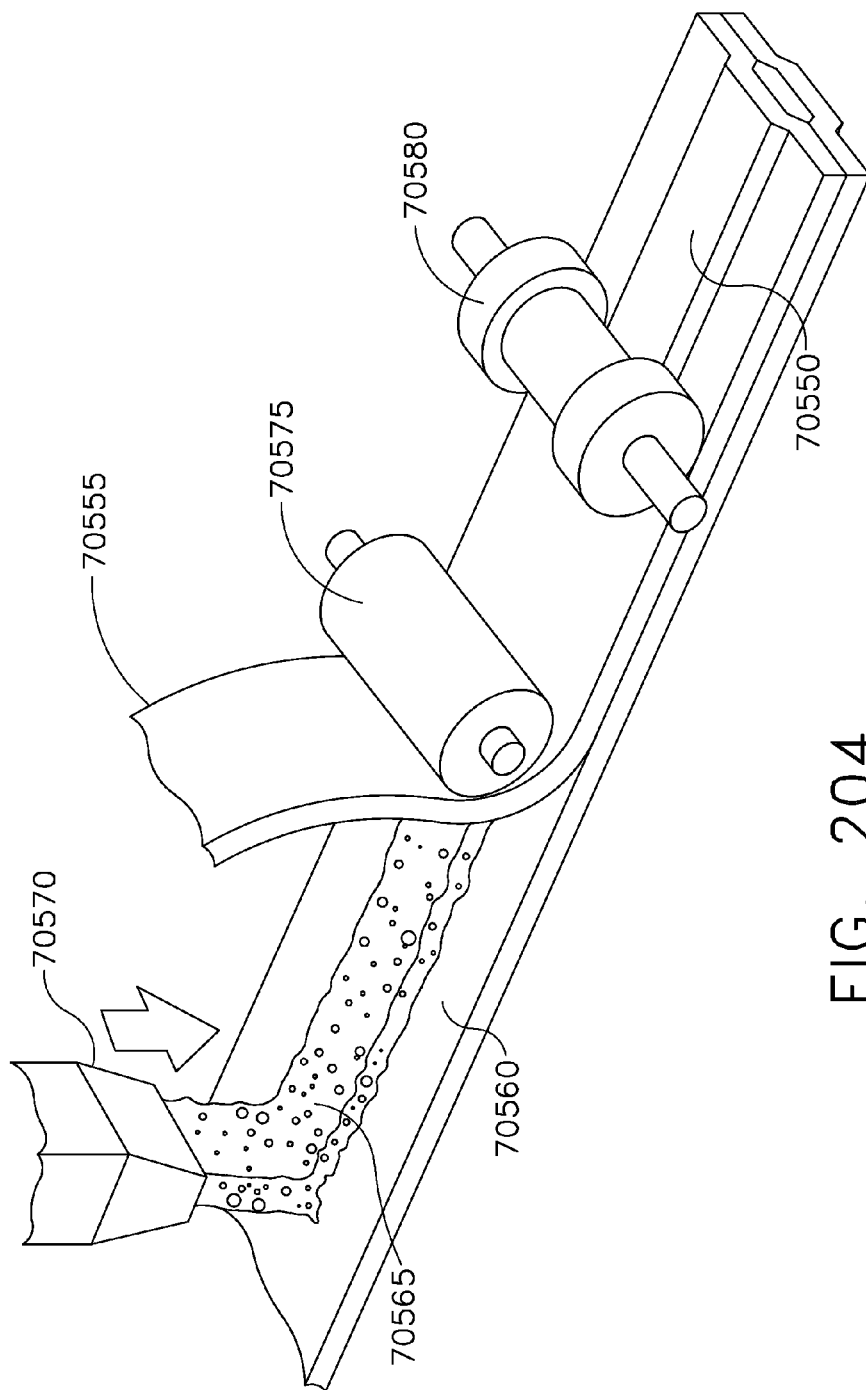


FIG. 204

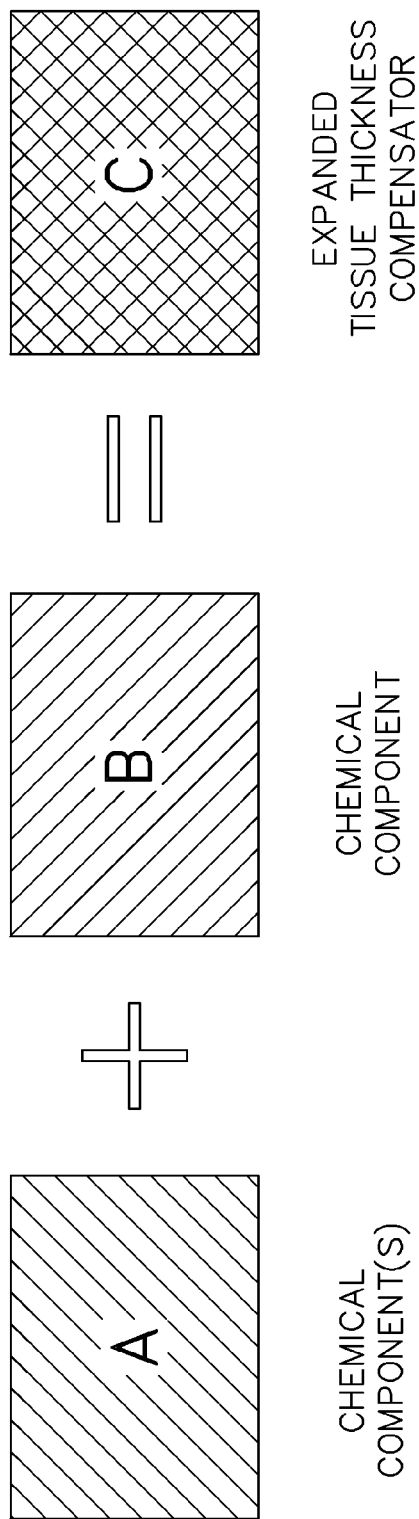


FIG. 205

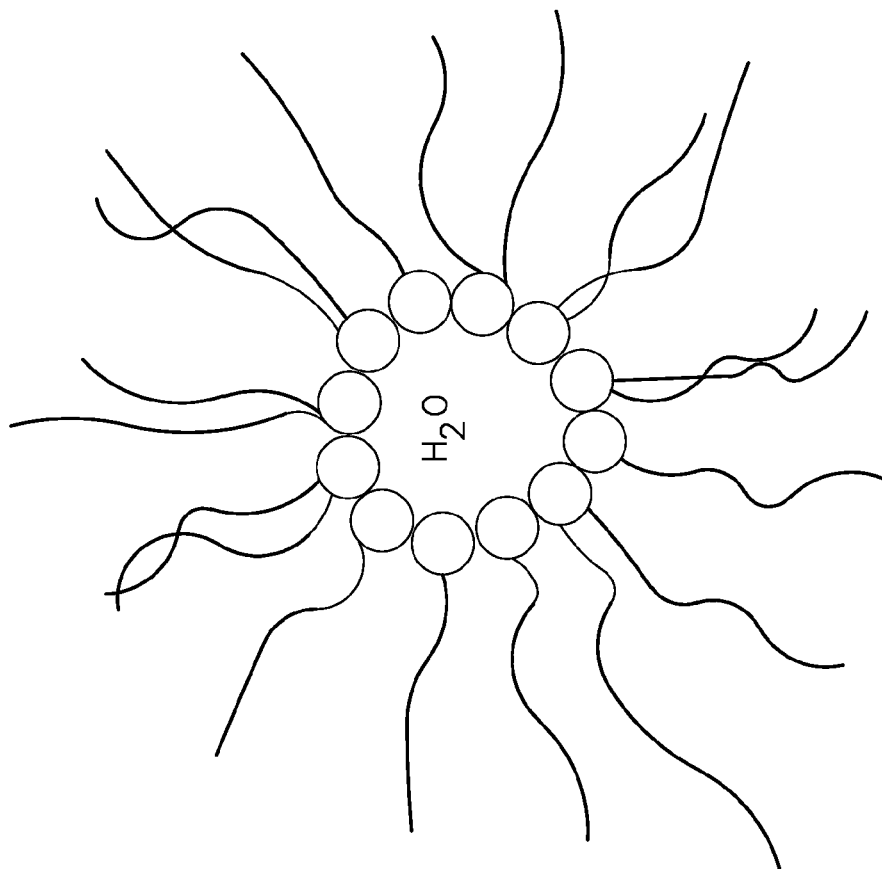


FIG. 206

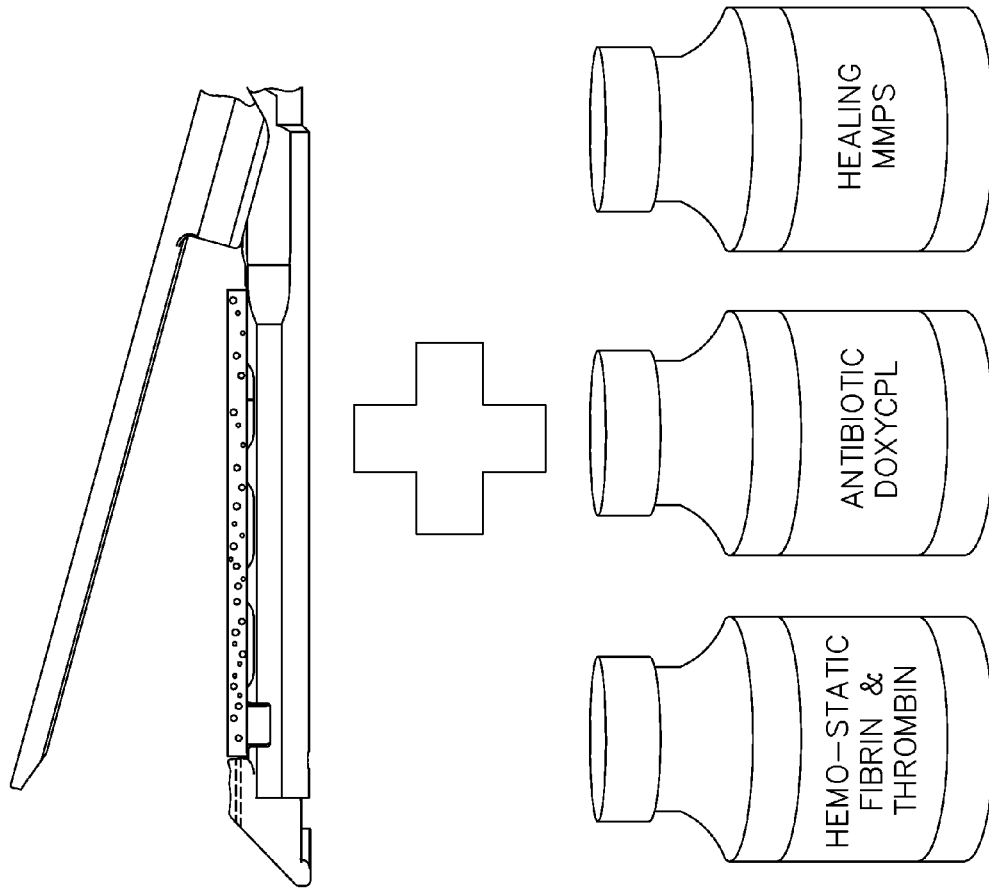


FIG. 207

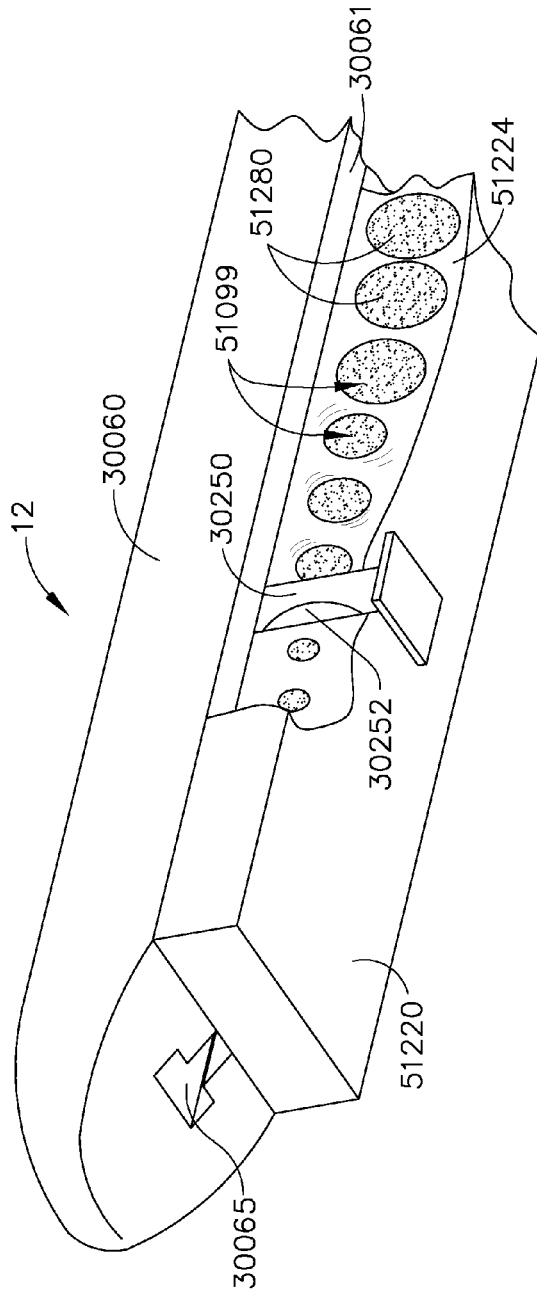


FIG. 208

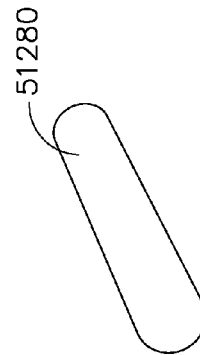


FIG. 209



FIG. 210

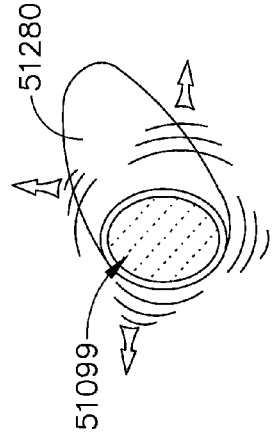


FIG. 211

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TISSUE THICKNESS COMPENSATOR COMPRISING STRUCTURE TO PRODUCE A RESILIENT LOAD

CROSS-REFERENCE TO RELATED APPLICATIONS

This non-provisional patent application is a continuation-in-part application under 35 U.S.C. §120 of U.S. patent application Ser. No. 13/097,891, entitled "Tissue Thickness Compensator For A Surgical Stapler Comprising An Adjustable Anvil, filed on Apr. 29, 2011, which issued on Oct. 21, 2014 as U.S. Pat. No. 8,864,009, which is a continuation-in-part application under 35 U.S.C. §120 of U.S. patent application Ser. No. 12/894,377, entitled "Selectively Orientable Implantable Fastener Cartridge", filed on Sep. 30, 2010, which issued on Mar. 12, 2013 as U.S. Pat. No. 8,393,514, the entire disclosures of which are hereby incorporated by reference herein.

BACKGROUND

The present invention relates to surgical instruments and, in various embodiments, to surgical cutting and stapling instruments and staple cartridges therefor that are designed to cut and staple tissue.

BRIEF DESCRIPTION OF THE DRAWINGS

The features and advantages of this invention, and the manner of attaining them, will become more apparent and the invention itself will be better understood by reference to the following description of embodiments of the invention taken in conjunction with the accompanying drawings, wherein:

FIG. 1 is a cross-sectional view of a surgical instrument embodiment;

FIG. 1A is a perspective view of one embodiment of an implantable staple cartridge;

FIGS. 1B-1E illustrate portions of an end effector clamping and stapling tissue with an implantable staple cartridge;

FIG. 2 is a partial cross-sectional side view of another end effector coupled to a portion of a surgical instrument with the end effector supporting a surgical staple cartridge and with the anvil thereof in an open position;

FIG. 3 is another partial cross-sectional side view of the end effector of FIG. 2 in a closed position;

FIG. 4 is another partial cross-sectional side view of the end effector of FIGS. 2 and 3 as the knife bar is starting to advance through the end effector;

FIG. 5 is another partial cross-sectional side view of the end effector of FIGS. 2-4 with the knife bar partially advanced therethrough;

FIGS. 6A-6D diagram the deformation of a surgical staple positioned within a collapsible staple cartridge body in accordance with at least one embodiment;

FIG. 7A is a diagram illustrating a staple positioned in a crushable staple cartridge body;

FIG. 7B is a diagram illustrating the crushable staple cartridge body of FIG. 7A being crushed by an anvil;

FIG. 7C is a diagram illustrating the crushable staple cartridge body of FIG. 7A being further crushed by the anvil;

FIG. 7D is a diagram illustrating the staple of FIG. 7A in a fully formed configuration and the crushable staple cartridge of FIG. 7A in a fully crushed condition;

FIG. 8 is a top view of a staple cartridge in accordance with at least one embodiment comprising staples embedded in a collapsible staple cartridge body;

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FIG. 9 is an elevational view of the staple cartridge of FIG. 8;

FIG. 10 is an exploded perspective view of an alternative embodiment of a compressible staple cartridge comprising staples therein and a system for driving the staples against an anvil;

FIG. 10A is a partial cut-away view of an alternative embodiment of the staple cartridge of FIG. 10;

FIG. 11 is a cross-sectional view of the staple cartridge of FIG. 10;

FIG. 12 is an elevational view of a sled configured to traverse the staple cartridge of FIG. 10 and move the staples toward the anvil;

FIG. 13 is a diagram of a staple driver which can be lifted toward the anvil by the sled of FIG. 12;

FIG. 14 is a perspective view of a staple cartridge comprising a rigid support portion and a compressible tissue thickness compensator for use with a surgical stapling instrument in accordance with at least one embodiment of the invention;

FIG. 15 is a partially exploded view of the staple cartridge of FIG. 14;

FIG. 16 is a fully exploded view of the staple cartridge of FIG. 14;

FIG. 17 is another exploded view of the staple cartridge of FIG. 14 without a warp covering the tissue thickness compensator;

FIG. 18 is a perspective view of a cartridge body, or support portion, of the staple cartridge of FIG. 14;

FIG. 19 is a top perspective view of a sled movable within the staple cartridge of FIG. 14 to deploy staples from the staple cartridge;

FIG. 20 is a bottom perspective view of the sled of FIG. 19;

FIG. 21 is an elevational view of the sled of FIG. 19;

FIG. 22 is a top perspective view of a driver configured to support one or more staples and to be lifted upwardly by the sled of FIG. 19 to eject the staples from the staple cartridge;

FIG. 23 is a bottom perspective view of the driver of FIG. 22;

FIG. 24 is a wrap configured to at least partially surround a compressible tissue thickness compensator of a staple cartridge;

FIG. 25 is a partial cut away view of a staple cartridge comprising a rigid support portion and a compressible tissue thickness compensator illustrated with staples being moved from an unfired position to a fired position during a first sequence;

FIG. 26 is an elevational view of the staple cartridge of FIG. 25;

FIG. 27 is a detail elevational view of the staple cartridge of FIG. 25;

FIG. 28 is a cross-sectional end view of the staple cartridge of FIG. 25;

FIG. 29 is a bottom view of the staple cartridge of FIG. 25;

FIG. 30 is a detail bottom view of the staple cartridge of FIG. 25;

FIG. 31 is a longitudinal cross-sectional view of an anvil in a closed position and a staple cartridge comprising a rigid support portion and a compressible tissue thickness compensator illustrated with staples being moved from an unfired position to a fired position during a first sequence;

FIG. 32 is another cross-sectional view of the anvil and the staple cartridge of FIG. 31 illustrating the anvil in an open position after the firing sequence has been completed;

FIG. 33 is a partial detail view of the staple cartridge of FIG. 31 illustrating the staples in an unfired position;

FIG. 34 is a cross-sectional elevational view of a staple cartridge comprising a rigid support portion and a compressible tissue thickness compensator illustrating the staples in an unfired position;

FIG. 35 is a detail view of the staple cartridge of FIG. 34;

FIG. 36 is an elevational view of an anvil in an open position and a staple cartridge comprising a rigid support portion and a compressible tissue thickness compensator illustrating the staples in an unfired position;

FIG. 37 is an elevational view of an anvil in a closed position and a staple cartridge comprising a rigid support portion and a compressible tissue thickness compensator illustrating the staples in an unfired position and tissue captured between the anvil and the tissue thickness compensator;

FIG. 38 is a detail view of the anvil and staple cartridge of FIG. 37;

FIG. 39 is an elevational view of an anvil in a closed position and a staple cartridge comprising a rigid support portion and a compressible tissue thickness compensator illustrating the staples in an unfired position illustrating thicker tissue positioned between the anvil and the staple cartridge;

FIG. 40 is a detail view of the anvil and staple cartridge of FIG. 39;

FIG. 41 is an elevational view of the anvil and staple cartridge of FIG. 39 illustrating tissue having different thicknesses positioned between the anvil and the staple cartridge;

FIG. 42 is a detail view of the anvil and staple cartridge of FIG. 39 as illustrated in FIG. 41;

FIG. 43 is a diagram illustrating a tissue thickness compensator which is compensating for different tissue thickness captured within different staples;

FIG. 44 is a diagram illustrating a tissue thickness compensator applying a compressive pressure to one or more vessels that have been transected by a staple line;

FIG. 45 is a diagram illustrating a circumstance wherein one or more staples have been improperly formed;

FIG. 46 is a diagram illustrating a tissue thickness compensator which could compensate for improperly formed staples;

FIG. 47 is a diagram illustrating a tissue thickness compensator positioned in a region of tissue in which multiple staples lines have intersected;

FIG. 48 is a diagram illustrating tissue captured within a staple;

FIG. 49 is a diagram illustrating tissue and a tissue thickness compensator captured within a staple;

FIG. 50 is a diagram illustrating tissue captured within a staple;

FIG. 51 is a diagram illustrating thick tissue and a tissue thickness compensator captured within a staple;

FIG. 52 is a diagram illustrating thin tissue and a tissue thickness compensator captured within a staple;

FIG. 53 is a diagram illustrating tissue having an intermediate thickness and a tissue thickness compensator captured within a staple;

FIG. 54 is a diagram illustrating tissue having another intermediate thickness and a tissue thickness compensator captured within a staple;

FIG. 55 is a diagram illustrating thick tissue and a tissue thickness compensator captured within a staple;

FIG. 56 is a partial cross-sectional view of an end effector of a surgical stapling instrument illustrating a firing bar and staple-firing sled in a retracted, unfired position;

FIG. 57 is another partial cross-sectional view of the end effector of FIG. 56 illustrating the firing bar and the staple-firing sled in a partially advanced position;

FIG. 58 is a cross-sectional view of the end effector of FIG. 56 illustrating the firing bar in a fully advanced, or fired, position;

FIG. 59 is a cross-sectional view of the end effector of FIG. 56 illustrating the firing bar in a retracted position after being fired and the staple-firing sled left in its fully fired position;

FIG. 60 is a detail view of the firing bar in the retracted position of FIG. 59;

FIG. 61 is a perspective view of a tissue thickness compensator in an end effector of a surgical instrument according to at least one embodiment;

FIG. 62 is a detail view of nonwoven material of the tissue thickness compensator of FIG. 61;

FIG. 63 is an elevational view depicting the tissue thickness compensator of FIG. 61 implanted against tissue and released from the end effector;

FIG. 64 is a detail view of nonwoven material of a tissue thickness compensator according to at least one embodiment;

FIG. 65 is a schematic depicting clusters of randomly oriented crimped fibers according to at least one embodiment;

FIG. 66 is a schematic depicting a cluster of randomly oriented crimped fibers according to at least one embodiment;

FIG. 67 is a schematic depicting an arrangement of crimped fibers according to at least one embodiment;

FIG. 68 is a schematic depicting an arrangement of crimped fibers according to at least one embodiment;

FIG. 69 is a schematic depicting an arrangement of crimped fibers according to at least one embodiment;

FIG. 70 is a plan cross-sectional view of coiled fibers in a tissue thickness compensator according to at least one embodiment;

FIG. 70A is a plan cross-sectional view of the coiled fibers of FIG. 70;

FIG. 70B is a cross-sectional detail view of the tissue thickness compensator of FIG. 70;

FIG. 71 is a perspective view of a tissue thickness compensator in an end effector of a surgical instrument according to at least one embodiment;

FIG. 72 is a diagram depicting deformation of the tissue thickness compensator of FIG. 71;

FIG. 73 is a schematic of woven suture for a tissue thickness compensator depicting the woven suture in a loaded configuration according to at least one embodiment;

FIG. 74 is a schematic of the woven suture of FIG. 73 depicting the woven suture in a released configuration;

FIG. 75 is a plan view of a tissue thickness compensator having the woven suture of FIG. 73 in an end effector of a surgical instrument;

FIG. 76 is a perspective view of a tissue thickness compensator in an end effector of a surgical instrument according to at least one embodiment;

FIG. 77 is a partial plan view of the tissue thickness compensator of FIG. 76;

FIG. 78 is an exploded view of the fastener cartridge assembly of the end effector and tissue thickness compensator of FIG. 61;

FIG. 79 is a partial cross-sectional view of the fastener cartridge assembly of FIG. 78 depicting unfired, partially fired, and fired fasteners;

FIG. 80 is an elevational view of the fastener cartridge assembly of FIG. 78 depicting a driver firing fasteners from staple cavities of the fastener cartridge assembly into the tissue thickness compensator;

FIG. 81 is a detail view of the fastener cartridge assembly of FIG. 80;

FIG. 82 is an elevational view of the tissue thickness compensator of FIG. 61 and tissue captured within fired fasteners;

FIG. 83 is an elevational view of the tissue thickness compensator of FIG. 61 and tissue captured within fired fasteners;

FIG. 84 is a perspective view of a tissue thickness compensator in an end effector of a surgical instrument according to at least one embodiment;

FIG. 85 is a diagram depicting deformation of a deformable tube of the tissue thickness compensator of FIG. 84;

FIG. 86 is a detail view of the deformable tube of the tissue thickness compensator of FIG. 84;

FIG. 87 is a diagram depicting deformation of a deformable tube of a tissue thickness compensator according to at least one embodiment;

FIG. 88 is an elevational view of a tissue thickness compensator comprising a tubular element implanted against tissue according to at least one embodiment;

FIG. 89 is an elevational view of a tissue thickness compensator comprising tubular elements implanted against tissue according to at least one embodiment;

FIG. 90 is a partial perspective view of a deformable tube comprising a tubular lattice according to at least one embodiment;

FIG. 91 is an elevational view of a tubular strand of the deformable tube of FIG. 90.

FIG. 92 is an elevational view of the deformable tube of FIG. 90;

FIG. 93 is an elevational view of multiple tubular strands for the deformable tube of FIG. 90 according to various embodiments;

FIG. 94 is an elevational view of the tubular lattice of FIG. 90 implanted against tissue;

FIG. 95 is a partial perspective view of a deformable tube according to at least one embodiment;

FIG. 96 is a partial perspective view of a deformable tube according to at least one embodiment;

FIG. 97 is a partial perspective view of a deformable tube according to at least one embodiment;

FIG. 98 is an elevational view of the deformable tube of FIG. 97;

FIG. 99 is a partial perspective view of a deformable tube according to at least one embodiment;

FIG. 100 is a partial perspective view of a deformable tube according to at least one embodiment;

FIG. 101 is a partial perspective view of a deformable tube according to at least one embodiment;

FIG. 102 is a perspective view of a tissue thickness compensator positioned in an end effector of a surgical instrument according to at least one embodiment;

FIG. 103 is an elevational view of a tubular element of the tissue thickness compensator of FIG. 102;

FIG. 104 is an elevational cross-sectional view of the tissue thickness compensator and the end effector of FIG. 102 depicting the end effector in an unclamped configuration;

FIG. 105 is an elevational cross-sectional view of the tissue thickness compensator and the end effector of FIG. 102 depicting the end effector in a clamped and fired configuration;

FIG. 106 is an elevational cross-sectional view of a tissue thickness compensator positioned in an end effector of a surgical instrument according to at least one embodiment;

FIG. 107 is an elevational cross-sectional view of the tissue thickness compensator and the end effector of FIG. 106 depicting the end effector in a clamped and fired configuration;

FIG. 108 is an elevational cross-sectional view of a tissue thickness compensator in the end effector of a surgical instrument according to at least one embodiment;

FIG. 109 is a cross-sectional elevational view of a tissue thickness compensator positioned in an end effector of a surgical instrument according to at least one embodiment;

FIG. 110 is a cross-sectional elevational view of the tissue thickness compensator and the end effector of FIG. 109 depicting the end effector in a clamped and fired configuration;

FIG. 111 is a perspective view of a tissue thickness compensator positioned in an end effector of a surgical instrument according to at least one embodiment;

FIG. 112 is an elevational cross-sectional view of a tissue thickness compensator positioned in an end effector of a surgical instrument according to at least one embodiment;

FIG. 113 is an elevational cross-sectional view of a tissue thickness compensator positioned in an end effector of a surgical instrument according to at least one embodiment;

FIG. 114 is an elevational cross-sectional view of a tissue thickness compensator positioned in an end effector of a surgical instrument according to at least one embodiment;

FIG. 115 is an elevational cross-sectional view of a tissue thickness compensator positioned in an end effector of a surgical instrument according to at least one embodiment;

FIG. 116 is a partial plan view of a tissue thickness compensator positioned in an end effector of a surgical instrument according to at least one embodiment;

FIG. 117 is a partial plan view of a tissue thickness compensator positioned in an end effector of a surgical instrument according to at least one embodiment;

FIG. 118 is a partial elevational cross-sectional view of the tissue thickness compensator and the end effector of FIG. 116 depicting the end effector in an unclamped configuration;

FIG. 119 is a partial elevational cross-sectional view of the tissue thickness compensator and the end effector of FIG. 116 depicting the end effector in a clamped configuration;

FIG. 120 is a perspective view of a tissue thickness compensator in an end effector of a surgical instrument according to at least one embodiment;

FIG. 121 is an elevational view of the tissue thickness compensator and the end effector of FIG. 120;

FIG. 122 is a perspective view of the tissue thickness compensator and the end effector of FIG. 120 depicting the anvil of the end effector moving towards a clamped configuration;

FIG. 123 is an elevational view of the tissue thickness compensator and the end effector of FIG. 120 depicting the end effector in a clamped configuration;

FIG. 124 is an elevational cross-sectional view of tubular elements of the tissue thickness compensator of FIG. 120 in an undeformed configuration;

FIG. 125 is an elevational cross-sectional view of tubular elements of the tissue thickness compensator of FIG. 120 in a deformed configuration;

FIG. 126 is a perspective view of a tissue thickness compensator in an end effector of a surgical instrument according to at least one embodiment;

FIG. 127 is an elevational cross-sectional view of the tissue thickness compensator and the end effector of FIG. 126 depicting the end effector in a clamped configuration;

FIG. 128 is an elevational cross-sectional view of the tissue thickness compensator and the end effector of FIG. 126 depicting the end effector in a fired and partially unclamped configuration;

FIG. 129 is a perspective view of a tissue thickness compensator positioned in an end effector of a surgical instrument according to at least one embodiment;

FIG. 130 is an elevational cross-sectional view of a tissue thickness compensator secured to an anvil of an end effector of a surgical instrument according to at least one embodiment;

FIG. 131 is an elevational cross-sectional view of the tissue thickness compensator and the end effector of FIG. 130 depicting the end effector in a clamped configuration;

FIG. 132 is an elevational cross-sectional view of the tissue thickness compensator and the end effector of FIG. 130 depicting the end effector in a fired and partially unclamped configuration;

FIG. 133 is a detail view of the tissue thickness compensator and the end effector of FIG. 132;

FIG. 134 is an elevational cross-sectional view of a tissue thickness compensator clamped in an end effector of a surgical instrument depicting deployment of staples by a staple-firing sled according to at least one embodiment;

FIG. 135 is an elevational cross-sectional view of the tissue thickness compensator and the end effector of FIG. 134 depicting the end effector in a clamped configuration;

FIG. 136 is an elevational cross-sectional view of the tissue thickness compensator and the end effector of FIG. 134 depicting the end effector in a fired configuration;

FIG. 137 is a perspective view of a tissue thickness compensator in an end effector of a surgical instrument according to at least one embodiment;

FIG. 138 is a perspective view of a tubular element of the tissue thickness compensator of FIG. 137;

FIG. 139 is a perspective view of the tubular element of FIG. 138 severed between a first and second end;

FIG. 140 is a perspective view of the tissue thickness compensator of FIG. 137 depicting a cutting element severing the tissue thickness compensator and staples engaging the tissue thickness compensator;

FIG. 141 is perspective view of a frame configured to make the tissue thickness compensator of FIG. 137 according to at least one embodiment;

FIG. 142 is an elevational cross-sectional view of the frame of FIG. 141 depicting the tissue thickness compensator of FIG. 137 curing in the frame;

FIG. 143 is an elevational cross-sectional view of the tissue thickness compensator removed from the frame of FIG. 142 and prepared for trimming by at least one cutting instrument;

FIG. 144 is an elevational cross-sectional view of the tissue thickness compensator of FIG. 143 after at least one cutting instrument has trimmed the tissue thickness compensator;

FIG. 145 is an elevational cross-sectional view of the tissue thickness compensator formed in the frame of FIG. 142 depicting severable tubes having various cross-sectional geometries;

FIG. 146 is a perspective view of a tissue thickness compensator in an end effector of a surgical instrument according to at least one embodiment;

FIG. 147 is a detail view of the tissue thickness compensator of FIG. 146 according to at least one embodiment;

FIG. 148 is a partial perspective view of a tissue thickness compensator according to at least one embodiment;

FIG. 149 is a partial perspective view of a tissue thickness compensator according to at least one embodiment;

FIG. 150A is an elevational cross-sectional view of the tissue thickness compensator and the end effector of FIG. 146 depicting the end effector in an unclamped configuration;

FIG. 150B is an elevational cross-sectional view of the tissue thickness compensator and the end effector of FIG. 146 depicting the end effector in a clamped configuration;

FIG. 150C is an elevational cross-sectional view of the tissue thickness compensator and the end effector of FIG. 146 depicting the end effector in a clamped and fired configuration;

FIG. 150D is an elevational cross-sectional view of the tissue thickness compensator of FIG. 146 captured in fired staples;

FIG. 150E is an elevational cross-sectional view of the tissue thickness compensator of FIG. 146 captured in fired staples depicting further expansion of the tissue thickness compensator;

FIG. 151 is a perspective cross-sectional view of a tissue thickness compensator in an end effector of a surgical instrument according to at least one embodiment;

FIG. 152 is a partial elevational view of the tissue thickness compensator of FIG. 151 captured in a fired staple;

FIG. 153 is an elevational view of a deformable tube of the tissue thickness compensator of FIG. 151;

FIG. 154 is an elevational view of a deformable tube according to at least one embodiment;

FIG. 155 is a perspective cross-sectional view of the tissue thickness compensator of FIG. 151;

FIG. 156 is a perspective cross-sectional view of a tissue thickness compensator in an end effector of a surgical instrument according to at least one embodiment;

FIG. 157 is a perspective view of a tissue thickness compensator according to at least one embodiment;

FIG. 158 is a partial elevational cross-sectional view of the tissue thickness compensator of FIG. 157 depicting a fastener engaged with tissue and with the tissue thickness compensator;

FIG. 159 is a perspective cross-sectional view of a tissue thickness compensator according to at least one embodiment;

FIG. 160 is an elevational view of a tissue thickness compensator according to at least one embodiment;

FIG. 161 is an elevational view of a tissue thickness compensator according to at least one embodiment;

FIG. 162 is an elevational view of a tissue thickness compensator positioned in a circular end effector of a surgical instrument according to at least one embodiment;

FIG. 163 is an elevational view of a tissue thickness compensator according to at least one embodiment;

FIG. 164 is an elevational view of a tissue thickness compensator according to at least one embodiment;

FIG. 165 is an elevational view of a tissue thickness compensator according to at least one embodiment;

FIG. 166 is an elevational view of a tissue thickness compensator according to at least one embodiment;

FIG. 167 is an elevational view of a tissue thickness compensator according to at least one embodiment;

FIG. 168 is a partial perspective view of a tissue thickness compensator according to at least one embodiment;

FIG. 169 is a partial perspective view of a tissue thickness compensator positioned in an end effector of a surgical instrument according to at least one embodiment;

FIG. 170 is a partial perspective view of a tissue thickness compensator with a fastener positioned in the apertures thereof according to at least one embodiment;

FIG. 171 is a partial perspective view of the tissue thickness compensator of FIG. 169 depicting the tissue thickness compensator in an undeformed configuration;

FIG. 172 is a partial perspective view of the tissue thickness compensator of FIG. 169 depicting the tissue thickness compensator in a partially deformed configuration;

FIG. 173 is a partial perspective view of the tissue thickness compensator of FIG. 169 depicting the tissue thickness compensator in a deformed configuration;

FIG. 174 is a perspective view of a tissue thickness compensator according to at least one embodiment;

FIG. 175 is a perspective view of an end effector of a stapling instrument comprising an anvil and a staple cartridge in accordance with at least one embodiment;

FIG. 176 is a cross-sectional view of the end effector of FIG. 175 illustrating staples positioned within the staple cartridge in an unfired state and a tissue thickness compensator comprising a sealed vessel in an unpunctured state, wherein the vessel is depicted with portions thereof removed for the purposes of illustration;

FIG. 177 is a cross-sectional view of the end effector of FIG. 175 illustrating the staples of FIG. 176 in an at least partially fired state and the vessel in an at least partially punctured state;

FIG. 178 is a perspective view of an end effector of a stapling instrument comprising an anvil and a staple cartridge in accordance with at least one embodiment;

FIG. 179 is a cross-sectional view of the end effector of FIG. 178 illustrating staples positioned within the staple cartridge in an unfired state and sealed vessels positioned within a tissue thickness compensator of the staple cartridge in an unpunctured state, wherein the vessels are depicted with portions thereof removed for the purposes of illustration;

FIG. 180 is a cross-sectional view of the end effector of FIG. 178 illustrating the staples of FIG. 179 in an at least partially fired state and the vessels in the staple cartridge in an at least partially punctured state;

FIG. 181 is a perspective view of an end effector of a stapling instrument comprising an anvil and a sealed vessel attached to the anvil in accordance with at least one alternative embodiment wherein the vessel is depicted with portions thereof removed for the purposes of illustration;

FIG. 182 is a cross-sectional view of the end effector of FIG. 181 illustrating staples at least partially fired from a staple cartridge and the vessels attached to the anvil in an at least partially punctured state;

FIG. 183 is a cross-sectional view of the vessel attached to the anvil of FIG. 181 illustrated in an expanded state;

FIG. 184 is a detail view of the vessel attached to the anvil of FIG. 183 illustrated in an expanded state;

FIG. 185 illustrates a vessel extending in a direction transverse to a line of staples;

FIG. 186 illustrates a plurality of vessels extending in directions which are transverse to a line of staples;

FIG. 187 is a cross-sectional view of a staple cartridge in accordance with various embodiments;

FIG. 188 is a partial cross-section view of FIG. 187 in an implanted condition;

FIG. 189A is a partial perspective view of a tissue thickness compensator prior to expansion;

FIG. 189B is a partial perspective view of a tissue thickness compensator of FIG. 189 during expansion;

FIG. 190 is a partial perspective view of a tissue thickness compensator comprising a fluid swellable composition according to various embodiments;

FIG. 191 is a cross-sectional view of tissue positioned adjacent a tissue thickness compensator according to various embodiments;

FIG. 192 is a partial cross-sectional view of FIG. 191 after the staple cartridge has been fired;

FIG. 193 is a diagram illustrating the tissue thickness compensator of FIG. 191 implanted adjacent the tissue;

FIG. 194 is a partial perspective view of a tissue thickness compensator according to various embodiments;

FIG. 195 is a perspective view of a jaw configured to receive the tissue thickness compensator of FIG. 194;

FIG. 196 is a partial cross-sectional view of a staple cartridge illustrating staples being deployed from the staple cartridge;

FIG. 197 is a perspective view of an upper tissue thickness compensator and a lower tissue thickness compensator positioned within an effector of a disposable loading unit;

FIG. 198A is a cross-sectional view of the lower tissue thickness compensator of FIG. 197 being manufactured in a mold in accordance with various embodiments;

FIG. 198B is a cross-sectional view of a trilayer tissue thickness compensator being manufactured in a mold in accordance with various embodiments;

FIG. 199 is a cross-sectional view of an anvil comprising a tissue thickness compensator comprising reinforcement material in accordance with various embodiments;

FIG. 200 is cross-sectional view of a tissue positioned intermediate the upper tissue thickness compensator and lower tissue thickness compensator in accordance with various embodiments;

FIG. 201 is a cross-sectional view of FIG. 200 illustrating staples being deployed from the staple cartridge;

FIG. 202 is a cross-sectional view of FIG. 200 after the staple cartridge has been fired;

FIG. 203A illustrates a needle configured to deliver a fluid to a tissue thickness compensator attached to a staple cartridge according to various embodiments;

FIG. 203B is a cross-sectional view of a staple cartridge comprising a tissue thickness compensator configured to receive the needle of FIG. 203A;

FIG. 204 illustrates a method of manufacturing a tissue thickness compensator according to various embodiments;

FIG. 205 is a diagram and a method of forming an expanding thickness compensator according to various embodiments;

FIG. 206 illustrates a micelle comprising a hydrogel precursor; and

FIG. 207 is a diagram of a surgical instrument comprising a tissue thickness compensator and fluids that may be delivered to the tissue thickness compensator according to various embodiments.

FIG. 208 is a partial perspective view of a tissue thickness compensator secured to an anvil of an end effector of a surgical instrument according to at least one embodiment.

FIG. 209 is a perspective view of a tubular element of the tissue thickness compensator of FIG. 208.

FIG. 210 is a perspective view of the tubular element of FIG. 209 depicting the tubular element severed into two halves and fluid contacting the hydrophilic substance within each half.

FIG. 211 is a perspective view of a half of the severed tubular element of FIG. 210 depicting expansion of the severed tubular element.

Corresponding reference characters indicate corresponding parts throughout the several views. The exemplifications set out herein illustrate certain embodiments of the invention, in one form, and such exemplifications are not to be construed as limiting the scope of the invention in any manner.

DETAILED DESCRIPTION

The Applicant of the present application also owns the U.S. Patent Applications identified below which are each herein incorporated by reference in their respective entirety:

U.S. patent application Ser. No. 12/894,311, entitled SURGICAL INSTRUMENTS WITH RECONFIGURABLE SHAFT SEGMENTS, now U.S. Patent Application Publication No. 2012/0080496;

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U.S. patent application Ser. No. 12/894,340, entitled SURGICAL STAPLE CARTRIDGES SUPPORTING NON-LINEARLY ARRANGED STAPLES AND SURGICAL STAPLING INSTRUMENTS WITH COMMON STAPLE-FORMING POCKETS, now U.S. Patent Application Publication No. 2012/0080482;

U.S. patent application Ser. No. 12/894,327, entitled JAW CLOSURE ARRANGEMENTS FOR SURGICAL INSTRUMENTS, now U.S. Patent Application Publication No. 2012/0080499;

U.S. patent application Ser. No. 12/894,351, entitled SURGICAL CUTTING AND FASTENING INSTRUMENTS WITH SEPARATE AND DISTINCT FASTENER DEPLOYMENT AND TISSUE CUTTING SYSTEMS, now U.S. Patent Application Publication No. 2012/0080502;

U.S. patent application Ser. No. 12/894,338, entitled IMPLANTABLE FASTENER CARTRIDGE HAVING A NON-UNIFORM ARRANGEMENT, now U.S. Patent Application Publication No. 2012/0080481;

U.S. patent application Ser. No. 12/894,369, entitled IMPLANTABLE FASTENER CARTRIDGE COMPRISING A SUPPORT RETAINER, now U.S. Patent Application Publication No. 2012/0080344;

U.S. patent application Ser. No. 12/894,312, entitled IMPLANTABLE FASTENER CARTRIDGE COMPRISING MULTIPLE LAYERS, now U.S. Patent Application Publication No. 2012/0080479;

U.S. patent application Ser. No. 12/894,377, entitled SELECTIVELY ORIENTABLE IMPLANTABLE FASTENER CARTRIDGE, now U.S. Pat. No. 8,393,514;

U.S. patent application Ser. No. 12/894,339, entitled SURGICAL STAPLING INSTRUMENT WITH COMPACT ARTICULATION CONTROL ARRANGEMENT, now U.S. Patent Application Publication No. 2012/0080500;

U.S. patent application Ser. No. 12/894,360, entitled SURGICAL STAPLING INSTRUMENT WITH A VARIABLE STAPLE FORMING SYSTEM, now U.S. Patent Application Publication No. 2012/0080484;

U.S. patent application Ser. No. 12/894,322, entitled SURGICAL STAPLING INSTRUMENT WITH INTERCHANGEABLE STAPLE CARTRIDGE ARRANGEMENTS, now U.S. Patent Application Publication No. 2012/0080501;

U.S. patent application Ser. No. 12/894,350, entitled SURGICAL STAPLE CARTRIDGES WITH DETACHABLE SUPPORT STRUCTURES AND SURGICAL STAPLING INSTRUMENTS WITH SYSTEMS FOR PREVENTING ACTUATION MOTIONS WHEN A CARTRIDGE IS NOT PRESENT, now U.S. Patent Application No. 2012/0080478;

U.S. patent application Ser. No. 12/894,383, entitled IMPLANTABLE FASTENER CARTRIDGE COMPRISING BIOABSORBABLE LAYERS, now U.S. Patent Application No. 2012/0080345;

U.S. patent application Ser. No. 12/894,389, entitled COMPRESSIBLE FASTENER CARTRIDGE, now U.S. Patent Application Publication No. 2012/0080335;

U.S. patent application Ser. No. 12/894,345, entitled FASTENERS SUPPORTED BY A FASTENER CARTRIDGE SUPPORT, now U.S. Patent Application Publication No. 2012/0080483;

U.S. patent application Ser. No. 12/894,306, entitled COLLAPSIBLE FASTENER CARTRIDGE, now U.S. Patent Application Publication No. 2012/0080332;

U.S. patent application Ser. No. 12/894,318, entitled FASTENER SYSTEM COMPRISING A PLURALITY OF CONNECTED RETENTION MATRIX ELEMENTS, now U.S. Patent Application Publication No. 2012/0080480;

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U.S. patent application Ser. No. 12/894,330, entitled FASTENER SYSTEM COMPRISING A RETENTION MATRIX AND AN ALIGNMENT MATRIX, now U.S. Patent Application Publication No. 2012/0080503;

U.S. patent application Ser. No. 12/894,361, entitled FASTENER SYSTEM COMPRISING A RETENTION MATRIX, now U.S. Pat. No. 8,529,600;

U.S. patent application Ser. No. 12/894,367, entitled FASTENING INSTRUMENT FOR DEPLOYING A FASTENER SYSTEM COMPRISING A RETENTION MATRIX, now U.S. Patent Application Publication No. 2012/0080485;

U.S. patent application Ser. No. 12/894,388, entitled FASTENER SYSTEM COMPRISING A RETENTION MATRIX AND A COVER, now U.S. Pat. No. 8,474,677;

U.S. patent application Ser. No. 12/894,376, entitled FASTENER SYSTEM COMPRISING A PLURALITY OF FASTENER CARTRIDGES, now U.S. Patent Application Publication No. 2012/0080486;

U.S. patent application Ser. No. 13/097,865, entitled SURGICAL STAPLER ANVIL COMPRISING A PLURALITY OF FORMING POCKETS, now U.S. Patent Application Publication No. 2012/0080488;

U.S. patent application Ser. No. 13/097,936, entitled TISSUE THICKNESS COMPENSATOR FOR A SURGICAL STAPLER, now U.S. Patent Application Publication No. 2012/0080339;

U.S. patent application Ser. No. 13/097,954, entitled STAPLE CARTRIDGE COMPRISING A VARIABLE THICKNESS COMPRESSIBLE PORTION, now U.S. Patent Application Publication No. 2012/0080340;

U.S. patent application Ser. No. 13/097,856, entitled STAPLE CARTRIDGE COMPRISING STAPLES POSITIONED WITHIN A COMPRESSIBLE PORTION THEREOF, now U.S. Patent Application Publication No. 2012/0080336;

U.S. patent application Ser. No. 13/097,928, entitled TISSUE THICKNESS COMPENSATOR COMPRISING DETACHABLE PORTIONS, now U.S. Patent Application Publication No. 2012/0080490;

U.S. patent application Ser. No. 13/097,891, entitled TISSUE THICKNESS COMPENSATOR FOR A SURGICAL STAPLER COMPRISING AN ADJUSTABLE ANVIL, now U.S. Patent Application Publication No. 2012/0080489;

U.S. patent application Ser. No. 13/097,948, entitled STAPLE CARTRIDGE COMPRISING AN ADJUSTABLE DISTAL PORTION, now U.S. Patent Application Publication No. 2012/0083836;

U.S. patent application Ser. No. 13/097,907, entitled COMPRESSIBLE STAPLE CARTRIDGE ASSEMBLY, now U.S. Patent Application Publication No. 2012/0080338;

U.S. patent application Ser. No. 13/097,861, entitled TISSUE THICKNESS COMPENSATOR COMPRISING PORTIONS HAVING DIFFERENT PROPERTIES, U.S. Patent Application Publication No. 2012/0080337;

U.S. patent application Ser. No. 13/097,869, entitled STAPLE CARTRIDGE LOADING ASSEMBLY, now U.S. Patent Application Publication No. 2012/0160721;

U.S. patent application Ser. No. 13/097,917, entitled COMPRESSIBLE STAPLE CARTRIDGE COMPRISING ALIGNMENT MEMBERS, now U.S. Patent Application No. 2012/0083834;

U.S. patent application Ser. No. 13/097,873, entitled STAPLE CARTRIDGE COMPRISING A RELEASABLE PORTION, now U.S. Patent Application Publication No. 2012/0083833;

U.S. patent application Ser. No. 13/097,938, entitled STAPLE CARTRIDGE COMPRISING COMPRESSIBLE DISTORTION RESISTANT COMPONENTS, now U.S. Patent Application Publication No. 2012/0080491;

U.S. patent application Ser. No. 13/097,924, entitled STAPLE CARTRIDGE COMPRISING A TISSUE THICKNESS COMPENSATOR, now U.S. Patent Application Publication No. 2012/0083835;

U.S. patent application Ser. No. 13/242,029, entitled SURGICAL STAPLER WITH FLOATING ANVIL, now U.S. Patent Application Publication No. 2012/0080493;

U.S. patent application Ser. No. 13/242,066, entitled CURVED END EFFECTOR FOR A STAPLING INSTRUMENT, now U.S. Patent Application Publication No. 2012/0080498;

U.S. patent application Ser. No. 13/242,086, entitled STAPLE CARTRIDGE INCLUDING COLLAPSIBLE DECK, now U.S. Patent Application Publication No. 2013/0075450;

U.S. patent application Ser. No. 13/241,912, entitled STAPLE CARTRIDGE INCLUDING COLLAPSIBLE DECK ARRANGEMENT, now U.S. Patent Application Publication No. 2013/0075448;

U.S. patent application Ser. No. 13/241,922, entitled SURGICAL STAPLER WITH STATIONARY STAPLE DRIVERS, now U.S. Patent Application Publication No. 2013/0075449;

U.S. patent application Ser. No. 13/241,637, entitled SURGICAL INSTRUMENT WITH TRIGGER ASSEMBLY FOR GENERATING MULTIPLE ACTUATION MOTIONS, now U.S. Patent Application Publication No. 2012/0074201; and

U.S. patent application Ser. No. 13/241,629, entitled SURGICAL INSTRUMENT WITH SELECTIVELY ARTICULATABLE END EFFECTOR, now U.S. Patent Application Publication No. 2012/0074200.

The Applicant of the present application also owns the U.S. Patent Applications identified below which were filed on Mar. 28, 2012 and which are each herein incorporated by reference in their respective entirety:

U.S. patent application Ser. No. 13/433,096, entitled TISSUE THICKNESS COMPENSATOR COMPRISING A PLURALITY OF CAPSULES, now U.S. Patent Application Publication No. 2012/0241496;

U.S. patent application Ser. No. 13/433,103, entitled TISSUE THICKNESS COMPENSATOR COMPRISING A PLURALITY OF LAYERS, now U.S. Patent Application Publication No. 2012/0241498;

U.S. patent application Ser. No. 13/433,098, entitled EXPANDABLE TISSUE THICKNESS COMPENSATOR, now U.S. Patent Application Publication No. 2012/0241491;

U.S. patent application Ser. No. 13/433,102, entitled TISSUE THICKNESS COMPENSATOR COMPRISING A RESERVOIR, now U.S. Patent Application Publication No. 2012/0241497;

U.S. patent application Ser. No. 13/433,114, entitled RETAINER ASSEMBLY INCLUDING A TISSUE THICKNESS COMPENSATOR, now U.S. Patent Application Publication No. 2012/0241499;

U.S. patent application Ser. No. 13/433,136, entitled TISSUE THICKNESS COMPENSATOR COMPRISING AT LEAST ONE MEDICAMENT, now U.S. Patent Application Publication No. 2012/0241492;

U.S. patent application Ser. No. 13/433,141, entitled TISSUE THICKNESS COMPENSATOR COMPRISING CONTROLLED RELEASE AND EXPANSION, now U.S. Patent Application Publication No. 2012/0241493;

U.S. patent application Ser. No. 13/433,144, entitled TISSUE THICKNESS COMPENSATOR COMPRISING FIBERS TO PRODUCE A RESILIENT LOAD, now U.S. Patent Application Publication Serial No. 2012/0241500;

U.S. patent application Ser. No. 13/433,155, entitled TISSUE THICKNESS COMPENSATOR COMPRISING RESILIENT MEMBERS, now U.S. Patent Application Publication No. 2012/0241502;

U.S. patent application Ser. No. 13/433,163, entitled METHODS FOR FORMING TISSUE THICKNESS COMPENSATOR ARRANGEMENTS FOR SURGICAL STAPLERS, now U.S. Patent Application Publication No. 2012/0248169;

U.S. patent application Ser. No. 13/433,167, entitled TISSUE THICKNESS COMPENSATORS, now U.S. Patent Application Publication No. 2012/0241503;

U.S. patent application Ser. No. 13/433,175, entitled LAYERED TISSUE THICKNESS COMPENSATOR, now U.S. Patent Application Publication No. 2012/0253298;

U.S. patent application Ser. No. 13/433,179, entitled TISSUE THICKNESS COMPENSATORS FOR CIRCULAR SURGICAL STAPLERS, now U.S. Patent Application Publication No. 2012/0241505;

U.S. patent application Ser. No. 13/433,115, entitled TISSUE THICKNESS COMPENSATOR COMPRISING CAPSULES DEFINING A LOW PRESSURE ENVIRONMENT, now U.S. Patent Application Publication No. 2013/0256372;

U.S. patent application Ser. No. 13/433,118, entitled TISSUE THICKNESS COMPENSATOR COMPRISED OF A PLURALITY OF MATERIALS, now U.S. Patent Application Publication No. 2013/0256365;

U.S. patent application Ser. No. 13/433,135, entitled MOVABLE MEMBER FOR USE WITH A TISSUE THICKNESS COMPENSATOR, U.S. Patent Application Publication No. 2013/0256382;

U.S. patent application Ser. No. 13/433,129, entitled TISSUE THICKNESS COMPENSATOR COMPRISING A PLURALITY OF MEDICAMENTS, now U.S. Patent Application Publication No. 2013/0256367;

U.S. patent application Ser. No. 13/433,140, entitled TISSUE THICKNESS COMPENSATOR AND METHOD FOR MAKING THE SAME, now U.S. Patent Application Publication No. 2013/0256368;

U.S. patent application Ser. No. 13/433,147, entitled TISSUE THICKNESS COMPENSATOR COMPRISING CHANNELS, now U.S. Patent Application Publication No. 2013/0256369;

U.S. patent application Ser. No. 13/433,126, entitled TISSUE THICKNESS COMPENSATOR COMPRISING TISSUE INGROWTH FEATURES, now U.S. Patent Application Publication No. 2013/0256366; and

U.S. patent application Ser. No. 13/433,132, entitled DEVICES AND METHODS FOR ATTACHING TISSUE THICKNESS COMPENSATING MATERIALS TO SURGICAL STAPLING INSTRUMENTS, now U.S. Patent Application Publication No. 2013/0256373.

Certain exemplary embodiments will now be described to provide an overall understanding of the principles of the structure, function, manufacture, and use of the devices and methods disclosed herein. One or more examples of these embodiments are illustrated in the accompanying drawings. Those of ordinary skill in the art will understand that the devices and methods specifically described herein and illustrated in the accompanying drawings are non-limiting exemplary embodiments and that the scope of the various embodiments of the present invention is defined solely by the claims. The features illustrated or described in connection with one

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exemplary embodiment may be combined with the features of other embodiments. Such modifications and variations are intended to be included within the scope of the present invention.

Reference throughout the specification to “various embodiments,” “some embodiments,” “one embodiment,” or “an embodiment,” or the like, means that a particular feature, structure, or characteristic described in connection with the embodiment is included in at least one embodiment. Thus, appearances of the phrases “in various embodiments,” “in some embodiments,” “in one embodiment,” or “in an embodiment,” or the like, in places throughout the specification are not necessarily all referring to the same embodiment. Furthermore, the particular features, structures, or characteristics may be combined in any suitable manner in one or more embodiments. Thus, the particular features, structures, or characteristics illustrated or described in connection with one embodiment may be combined, in whole or in part, with the features structures, or characteristics of one or more other embodiments without limitation. Such modifications and variations are intended to be included within the scope of the present invention.

The terms “proximal” and “distal” are used herein with reference to a clinician manipulating the handle portion of the surgical instrument. The term “proximal” referring to the portion closest to the clinician and the term “distal” referring to the portion located away from the clinician. It will be further appreciated that, for convenience and clarity, spatial terms such as “vertical,” “horizontal,” “up,” and “down” may be used herein with respect to the drawings. However, surgical instruments are used in many orientations and positions, and these terms are not intended to be limiting and/or absolute.

Various exemplary devices and methods are provided for performing laparoscopic and minimally invasive surgical procedures. However, the person of ordinary skill in the art will readily appreciate that the various methods and devices disclosed herein can be used in numerous surgical procedures and applications including, for example, in connection with open surgical procedures. As the present Detailed Description proceeds, those of ordinary skill in the art will further appreciate that the various instruments disclosed herein can be inserted into a body in any way, such as through a natural orifice, through an incision or puncture hole formed in tissue, etc. The working portions or end effector portions of the instruments can be inserted directly into a patient's body or can be inserted through an access device that has a working channel through which the end effector and elongated shaft of a surgical instrument can be advanced.

Turning to the Drawings wherein like numerals denote like components throughout the several views, FIG. 1 depicts a surgical instrument 10 that is capable of practicing several unique benefits. The surgical stapling instrument 10 is designed to manipulate and/or actuate various forms and sizes of end effectors 12 that are operably attached thereto. In the embodiment depicted in FIGS. 1-1E, for example, the end effector 12 includes an elongated channel 14 that forms a lower jaw 13 of the end effector 12. The elongated channel 14 is configured to support an “implantable” staple cartridge 30 and also movably support an anvil 20 that functions as an upper jaw 15 of the end effector 12.

In various embodiments, the elongated channel 14 may be fabricated from, for example, 300 & 400 Series, 17-4 & 17-7 stainless steel, titanium, etc. and be formed with spaced side walls 16. The anvil 20 may be fabricated from, for example, 300 & 400 Series, 17-4 & 17-7 stainless steel, titanium, etc. and have a staple forming undersurface, generally labeled as

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22 that has a plurality of staple forming pockets 23 formed therein. See FIGS. 1B-1E. In addition, the anvil 20 has a bifurcated ramp assembly 24 that protrudes proximally therefrom. An anvil pin 26 protrudes from each lateral side of the ramp assembly 24 to be received within a corresponding slot or opening 18 in the side walls 16 of the elongated channel 14 to facilitate its movable or pivotable attachment thereto.

Various forms of implantable staple cartridges may be employed with the various embodiments of the surgical instruments disclosed herein. Specific staple cartridge configurations and constructions will be discussed in further detail below. However, in the embodiment depicted in FIG. 1A, an implantable staple cartridge 30 is shown. In at least one embodiment, the staple cartridge 30 has a body portion 31 that consists of a compressible hemostat material such as, for example, oxidized regenerated cellulose (“ORC”) or a bioabsorbable foam in which lines of unformed metal staples 32 are supported. In at least some embodiments, in order to prevent the staple from being affected and the hemostat material from being activated during the introduction and positioning process, the entire cartridge may be coated or wrapped in a biodegradable film 38 such as a polydioxanone film sold under the trademark PDS® or with a Polyglycerol sebacate (PGS) film or other biodegradable films formed from PGA (Polyglycolic acid, marketed under the trade mark Vicryl), PCL (Polycaprolactone), PLA or PLLA (Polylactic acid), PHA (polyhydroxyalkanoate), PGCL (poliglecaprone 25, sold under the trademark Monocryl) or a composite of PGA, PCL, PLA, PDS that would be impermeable until ruptured. The body 31 of staple cartridge 30 is sized to be removably supported within the elongated channel 14 as shown such that each staple 32 therein is aligned with corresponding staple forming pockets 23 in the anvil when the anvil 20 is driven into forming contact with the staple cartridge 30.

In use, once the end effector 12 has been positioned adjacent the target tissue, the end effector 12 is manipulated to capture or clamp the target tissue between an upper face 36 of the staple cartridge 30 and the staple forming surface 22 of the anvil 20. The staples 32 are formed by moving the anvil 20 in a path that is substantially parallel to the elongated channel 14 to bring the staple forming surface 22 and, more particularly, the staple forming pockets 23 therein into substantially simultaneous contact with the upper face 36 of the staple cartridge 30. As the anvil 20 continues to move into the staple cartridge 30, the legs 34 of the staples 32 contact a corresponding staple forming pocket 23 in anvil 20 which serves to bend the staple legs 34 over to form the staples 32 into a “B shape”. Further movement of the anvil 20 toward the elongated channel 14 will further compress and form the staples 32 to a desired final formed height “FF”.

The above-described staple forming process is generally depicted in FIGS. 1B-1E. For example, FIG. 1B illustrates the end effector 12 with target tissue “T” between the anvil 20 and the upper face 36 of the implantable staple cartridge 30. FIG. 1C illustrates the initial clamping position of the anvil 20 wherein the anvil has 20 been closed onto the target tissue “T” to clamp the target tissue “T” between the anvil 20 and the upper face 36 of the staple cartridge 30. FIG. 1D illustrates the initial staple formation wherein the anvil 20 has started to compress the staple cartridge 30 such that the legs 34 of the staples 32 are starting to be formed by the staple forming pockets 23 in the anvil 20. FIG. 1E illustrates the staple 32 in its final formed condition through the target tissue “T” with the anvil 20 removed for clarity purposes. Once the staples 32 have been formed and fastened to the target tissue “T”, the surgeon will move the anvil 20 to the open position to enable the cartridge body 31 and the staples 32 to remain affixed to

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the target tissue while the end effector **12** is being withdrawn from the patient. The end effector **12** forms all of the staples simultaneously as the two jaws **13**, **15** are clamped together. The remaining “crushed” body materials **31** act as both a hemostat (the ORC) and a staple line reinforcement (PGA, PDS or any of the other film compositions mentioned above **38**). Also, since the staples **32** never have to leave the cartridge body **31** during forming, the likelihood of the staples **32** being malformed during forming is minimized. As used herein the term “implantable” means that, in addition to the staples, the cartridge body materials that support the staples will also remain in the patient and may eventually be absorbed by the patient’s body. Such implantable staple cartridges are distinguishable from prior cartridge arrangements that remain positioned within the end effector in their entirety after they have been fired.

In various implementations, the end effector **12** is configured to be coupled to an elongated shaft assembly **40** that protrudes from a handle assembly **100**. The end effector **12** (when closed) and the elongated shaft assembly **40** may have similar cross-sectional shapes and be sized to operably pass through a trocar tube or working channel in another form of access instrument. As used herein, the term “operably pass” means that the end effector and at least a portion of the elongated shaft assembly may be inserted through or passed through the channel or tube opening and can be manipulated therein as needed to complete the surgical stapling procedure. In some embodiments, when in a closed position, the jaws **13** and **15** of the end effector **12** may provide the end effector with a roughly circular cross-sectional shape that facilitates its passage through a circular passage/opening. However, the end effectors of various embodiments of the present invention, as well as the elongated shaft assembly embodiments, could conceivably be provided with other cross-sectional shapes that could otherwise pass through access passages and openings that have non-circular cross-sectional shapes. Thus, an overall size of a cross-section of a closed end effector will be related to the size of the passage or opening through which it is intended to pass. Thus, one end effector for example, may be referred to as a “5 mm” end effector which means it can operably pass through an opening that is at least approximately 5 mm in diameter.

In various embodiments, the elongated shaft assembly **40** may have an outer diameter that is substantially the same as the outer diameter of the end effector **12** when in a closed position. For example, a 5 mm end effector may be coupled to an elongated shaft assembly **40** that has 5 mm cross-sectional diameter. However, as the present Detailed Description proceeds, it will become apparent that various embodiments of the present may be effectively used in connection with different sizes of end effectors. For example, a 10 mm end effector may be attached to an elongated shaft that has a 5 mm cross-sectional diameter. Conversely, for those applications wherein a 10 mm or larger access opening or passage is provided, the elongated shaft assembly **40** may have a 10 mm (or larger) cross-sectional diameter, but may also be able to actuate a 5 mm or 10 mm end effector. Accordingly, the outer shaft **40** may have an outer diameter that is the same as or is different from the outer diameter of a closed end effector **12** attached thereto.

As depicted, the elongated shaft assembly **40** extends distally from the handle assembly **100** in a generally straight line to define a longitudinal axis A-A. In various embodiments, for example, the elongated shaft assembly **40** may be approximately 9-16 inches (229-406 mm) long. However, the elongated shaft assembly **40** may be provided in other lengths and, in other embodiments, may have joints therein or be other-

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wise configured to facilitate articulation of the end effector **12** relative to other portions of the shaft or handle assembly as will be discussed in further detail below. In various embodiments, the elongated shaft assembly **40** includes a spine member **50** that extends from the handle assembly **100** to the end effector **12**. The proximal end of the elongated channel **14** of the end effector **12** has a pair of retention trunnions **17** protruding therefrom that are sized to be received within corresponding trunnion openings or cradles **52** that are provided in a distal end of the spine member **50** to enable the end effector **12** to be removably coupled the elongated shaft assembly **40**. The spine member **50** may be fabricated from, for example, 6061 or 7075 aluminum, stainless steel, titanium, etc.

In various embodiments, the handle assembly **100** comprises a pistol grip-type housing that may be fabricated in two or more pieces for assembly purposes. For example, the handle assembly **100** as shown comprises a right hand case member **102** and a left hand case member (not illustrated) that are molded or otherwise fabricated from a polymer or plastic material and are designed to mate together. Such case members may be attached together by snap features, pegs and sockets molded or otherwise formed therein and/or by adhesive, screws, etc. The spine member **50** has a proximal end **54** that has a flange **56** formed thereon. The flange **56** is configured to be rotatably supported within a groove **106** formed by mating ribs **108** that protrude inwardly from each of the case members **102**, **104**. Such arrangement facilitates the attachment of the spine member **50** to the handle assembly **100** while enabling the spine member **50** to be rotated relative to the handle assembly **100** about the longitudinal axis A-A in a 360° path.

As can be further seen in FIG. 1, the spine member **50** passes through and is supported by a mounting bushing **60** that is rotatably affixed to the handle assembly **100**. The mounting bushing **60** has a proximal flange **62** and a distal flange **64** that define a rotational groove **65** that is configured to rotatably receive a nose portion **101** of the handle assembly **100** therebetween. Such arrangement enables the mounting bushing **60** to rotate about longitudinal axis A-A relative to the handle assembly **100**. The spine member **50** is non-rotatably pinned to the mounting bushing **60** by a spine pin **66**. In addition, a rotation knob **70** is attached to the mounting bushing **60**. In one embodiment, for example, the rotation knob **70** has a hollow mounting flange portion **72** that is sized to receive a portion of the mounting bushing **60** therein. In various embodiments, the rotation knob **70** may be fabricated from, for example, glass or carbon filled Nylon, polycarbonate, Ultem®, etc. and is affixed to the mounting bushing **60** by the spine pin **66** as well. In addition, an inwardly protruding retention flange **74** is formed on the mounting flange portion **72** and is configured to extend into a radial groove **68** formed in the mounting bushing **60**. Thus, the surgeon may rotate the spine member **50** (and the end effector **12** attached thereto) about longitudinal axis A-A in a 360° path by grasping the rotation knob **70** and rotating it relative to the handle assembly **100**.

In various embodiments, the anvil **20** is retained in an open position by an anvil spring **21** and/or another biasing arrangement. The anvil **20** is selectively movable from the open position to various closed or clamping and firing positions by a firing system, generally designated as **109**. The firing system **109** includes a “firing member” **110** which, in various embodiments, comprises a hollow firing tube **110**. The hollow firing tube **110** is axially movable on the spine member **50** and thus forms the outer portion of the elongated shaft assembly **40**. The firing tube **110** may be fabricated from a polymer or other suitable material and have a proximal end that is

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attached to a firing yoke 114 of the firing system 109. In various embodiments for example, the firing yoke 114 may be over-molded to the proximal end of the firing tube 110. However, other fastener arrangements may be employed.

As can be seen in FIG. 1, the firing yoke 114 may be rotatably supported within a support collar 120 that is configured to move axially within the handle assembly 100. In various embodiments, the support collar 120 has a pair of laterally extending fins that are sized to be slidably received within fin slots formed in the right and left hand case members. Thus, the support collar 120 may slide axially within the handle housing 100 while enabling the firing yoke 114 and firing tube 110 to rotate relative thereto about the longitudinal axis A-A. In various embodiments, a longitudinal slot is provided through the firing tube 110 to enable the spine pin 66 to extend therethrough into the spine member 50 while facilitating the axial travel of the firing tube 110 on the spine member 50.

The firing system 109 further comprises a firing trigger 130 which serves to control the axial travel of the firing tube 110 on the spine member 50. See FIG. 1. Such axial movement in the distal direction of the firing tube 110 into firing interaction with the anvil 20 is referred to herein as “firing motion”. As can be seen in FIG. 1, the firing trigger 130 is movably or pivotally coupled to the handle assembly 100 by a pivot pin 132. A torsion spring 135 is employed to bias the firing trigger 130 away from the pistol grip portion 107 of the handle assembly 100 to an un-actuated “open” or starting position. As can be seen in FIG. 1, the firing trigger 130 has an upper portion 134 that is movably attached to (pinned) firing links 136 that are movably attached to (pinned) the support collar 120. Thus, movement of the firing trigger 130 from the starting position (FIG. 1) toward an ending position adjacent the pistol grip portion 107 of the handle assembly 100 will cause the firing yoke 114 and the firing tube 110 to move in the distal direction “DD”. Movement of the firing trigger 130 away from the pistol grip portion 107 of the handle assembly 100 (under the bias of the torsion spring 135) will cause the firing yoke 114 and firing tube 110 to move in the proximal direction “PD” on the spine member 50.

Various embodiments of the present invention may be employed with different sizes and configurations of implantable staple cartridges. For example, the surgical instrument 10, when used in connection with a first firing adapter 140, may be used with a 5 mm end effector 12 that is approximately 20 mm long (or in other lengths) which supports an implantable staple cartridge 30. Such end effector size may be particularly well-suited, for example, to complete relatively fine dissection and vascular transactions. However, as will be discussed in further detail below, the surgical instrument 10 may also be employed, for example, in connection with other sizes of end effectors and staple cartridges by replacing the first firing adapter 140 with a second firing adapter. In still other embodiments, the elongated shaft assembly 40 may be configured to be attached to only one form or size of end effector.

One method of removably coupling the end effector 12 to the spine member 50 will now be explained. The coupling process is commenced by inserting the retention trunnions 17 on the elongated channel 14 into the trunnion cradles 52 in the spine member 50. Thereafter, the surgeon advances the firing trigger 130 toward the pistol grip 107 of the housing assembly 100 to distally advance the firing tube 110 and the first firing adapter 140 over a proximal end portion 47 of the elongated channel 14 to thereby retain the trunnions 17 in their respective cradles 52. Such position of the first firing adapter 140 over the trunnions 17 is referred to herein as the “coupled

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position”. Various embodiments of the present invention may also have an end effector locking assembly for locking the firing trigger 130 in position after an end effector 12 has been attached to the spine member 50.

More specifically, one embodiment of the end effector locking assembly 160 includes a retention pin 162 that is movably supported in the upper portion 134 of the firing trigger 130. As discussed above, the firing tube 110 must initially be advanced distally to the coupled position wherein the first firing adapter 140 retains the retention trunnions 17 of the end effector 12 in the trunnion cradles 52 in the spine member 50. The surgeon advances the firing adapter 140 distally to the coupled position by pulling the firing trigger 130 from the starting position toward the pistol grip 107. As the firing trigger 130 is initially actuated, the retention pin 162 is moved distally until the firing tube 110 has advanced the first firing adapter 140 to the coupled position at which point the retention pin 162 is biased into a locking cavity 164 formed in the case member. In various embodiments, when the retention pin 162 enters into the locking cavity 164, the pin 162 may make an audible “click” or other sound, as well as provide a tactile indication to the surgeon that the end effector 12 has been “locked” onto the spine member 50. In addition, the surgeon cannot inadvertently continue to actuate the firing trigger 130 to start to form staples 32 in the end effector 12 without intentionally biasing the retention pin 162 out of the locking cavity 164. Similarly, if the surgeon releases the firing trigger 130 when in the coupled position, it is retained in that position by the retention pin 162 to prevent the firing trigger 130 from returning to the starting position and thereby releasing the end effector 12 from the spine member 50.

Various embodiments of the present invention may further include a firing system lock button 137 that is pivotally attached to the handle assembly 100. In one form, the firing system lock button 137 has a latch 138 formed on a distal end thereof that is oriented to engage the firing yoke 114 when the firing release button is in a first latching position. As can be seen in FIG. 1, a latch spring 139 serves to bias the firing system lock button 137 to the first latching position. In various circumstances, the latch 138 serves to engage the firing yoke 114 at a point where the position of the firing yoke 114 on the spine member 50 corresponds to a point wherein the first firing adapter 140 is about to distally advance up the clamping ramp 28 on the anvil 20. It will be understood that, as the first firing adapter 140 advances axially up the clamping ramp 28, the anvil 20 will move in a path such that its staple forming surface portion 22 is substantially parallel to the upper face 36 of the staple cartridge 30.

After the end effector 12 has been coupled to the spine member 50, the staple forming process is commenced by first depressing the firing system lock button 137 to enable the firing yoke 114 to be further moved distally on the spine member 50 and ultimately compress the anvil 20 into the staple cartridge 30. After depressing the firing system lock button 137, the surgeon continues to actuate the firing trigger 130 towards the pistol grip 107 thereby driving the first staple collar 140 up the corresponding staple forming ramp 29 to force the anvil 20 into forming contact with the staples 32 in the staple cartridge 30. The firing system lock button 137 prevents the inadvertent forming of the staples 32 until the surgeon is ready to start that process. In this embodiment, the surgeon must depress the firing system lock button 137 before the firing trigger 130 may be further actuated to begin the staple forming process.

The surgical instrument 10 may be solely used as a tissue stapling device if so desired. However, various embodiments

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of the present invention may also include a tissue cutting system, generally designated as **170**. In at least one form, the tissue cutting system **170** comprises a knife member **172** that may be selectively advanced from an un-actuated position adjacent the proximal end of the end effector **12** to an actuated position by actuating a knife advancement trigger **200**. The knife member **172** is movably supported within the spine member **50** and is attached or otherwise protrudes from a knife rod **180**. The knife member **172** may be fabricated from, for example, 420 or 440 stainless steel with a hardness of greater than 38HRC (Rockwell Hardness C-scale) and have a tissue cutting edge **176** formed on the distal end **174** thereof and be configured to slidably extend through a slot in the anvil **20** and a centrally disposed slot **33** in the staple cartridge **30** to cut through tissue that is clamped in the end effector **12**. In various embodiments, the knife rod **180** extends through the spine member **50** and has a proximal end portion which drivingly interfaces with a knife transmission that is operably attached to the knife advance trigger **200**. In various embodiments, the knife advance trigger **200** is attached to pivot pin **132** such that it may be pivoted or otherwise actuated without actuating the firing trigger **130**. In various embodiments, a first knife gear **192** is also attached to the pivot pin **132** such that actuation of the knife advance trigger **200** also pivots the first knife gear **192**. A firing return spring **202** is attached between the first knife gear **192** and the handle housing **100** to bias the knife advancement trigger **200** to a starting or un-actuated position.

Various embodiments of the knife transmission also include a second knife gear **194** that is rotatably supported on a second gear spindle and in meshing engagement with the first knife gear **192**. The second knife gear **194** is in meshing engagement with a third knife gear **196** that is supported on a third gear spindle. Also supported on the third gear spindle **195** is a fourth knife gear **198**. The fourth knife gear **198** is adapted to drivingly engage a series of annular gear teeth or rings on a proximal end of the knife rod **180**. Thus, such arrangement enables the fourth knife gear **198** to axially drive the knife rod **180** in the distal direction "DD" or proximal direction "PD" while enabling the firing rod **180** to rotate about longitudinal axis A-A with respect to the fourth knife gear **198**. Accordingly, the surgeon may axially advance the firing rod **180** and ultimately the knife member **172** distally by pulling the knife advancement trigger **200** towards the pistol grip **107** of the handle assembly **100**.

Various embodiments of the present invention further include a knife lockout system **210** that prevents the advancement of the knife member **172** unless the firing trigger **130** has been pulled to the fully fired position. Such feature will therefore prevent the activation of the knife advancement system **170** unless the staples have first been fired or formed into the tissue. As can be seen in FIG. 1, various implementations of the knife lockout system **210** comprise a knife lockout bar **211** that is pivotally supported within the pistol grip portion **107** of the handle assembly **100**. The knife lockout bar **211** has an activation end **212** that is adapted to be engaged by the firing trigger **130** when the firing trigger **130** is in the fully fired position. In addition, the knife lockout bar **211** has a retaining hook **214** on its other end that is adapted to hookingly engage a latch rod **216** on the first cut gear **192**. A knife lock spring **218** is employed to bias the knife lockout bar **211** to a "locked" position wherein the retaining hook **214** is retained in engagement with the latch rod **216** to thereby prevent actuation of the knife advancement trigger **200** unless the firing trigger **130** is in the fully fired position.

After the staples have been "fired" (formed) into the target tissue, the surgeon may depress the firing trigger release

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button **167** to enable the firing trigger **130** to return to the starting position under the bias of the torsion spring **135** which enables the anvil **20** to be biased to an open position under the bias of spring **21**. When in the open position, the surgeon may withdraw the end effector **12** leaving the implantable staple cartridge **30** and staples **32** behind. In applications wherein the end effector was inserted through a passage, working channel, etc. the surgeon will return the anvil **20** to the closed position by activating the firing trigger **130** to enable the end effector **12** to be withdrawn out through the passage or working channel. If, however, the surgeon desires to cut the target tissue after firing the staples, the surgeon activates the knife advancement trigger **200** in the above-described manner to drive the knife bar **172** through the target tissue to the end of the end effector. Thereafter, the surgeon may release the knife advancement trigger **200** to enable the firing return spring **202** to cause the firing transmission to return the knife bar **172** to the starting (un-actuated) position. Once the knife bar **172** has been returned to the starting position, the surgeon may open the end effector jaws **13**, **15** to release the implantable cartridge **30** within the patient and then withdraw the end effector **12** from the patient. Thus, such surgical instruments facilitate the use of small implantable staple cartridges that may be inserted through relatively smaller working channels and passages, while providing the surgeon with the option to fire the staples without cutting tissue or if desired to also cut tissue after the staples have been fired.

Various unique and novel embodiments of the present invention employ a compressible staple cartridge that supports staples in a substantially stationary position for forming contact by the anvil. In various embodiments, the anvil is driven into the unformed staples wherein, in at least one such embodiment, the degree of staple formation attained is dependent upon how far the anvil is driven into the staples. Such an arrangement provides the surgeon with the ability to adjust the amount of forming or firing pressure applied to the staples and thereby alter the final formed height of the staples. In other various embodiments of the present invention, surgical stapling arrangements can employ staple driving elements which can lift the staples toward the anvil. Such embodiments are described in greater detail further below.

In various embodiments, with regard to the embodiments described in detail above, the amount of firing motion that is applied to the movable anvil is dependent upon the degree of actuation of the firing trigger. For example, if the surgeon desires to attain only partially formed staples, then the firing trigger is only partially depressed inward towards the pistol grip **107**. To attain more staple formation, the surgeon simply compresses the firing trigger further which results in the anvil being further driven into forming contact with the staples. As used herein, the term "forming contact" means that the staple forming surface or staple forming pockets have contacted the ends of the staple legs and have started to form or bend the legs over into a formed position. The degree of staple formation refers to how far the staple legs have been folded over and ultimately relates to the forming height of the staple as referenced above. Those of ordinary skill in the art will further understand that, because the anvil **20** moves in a substantially parallel relationship with respect to the staple cartridge as the firing motions are applied thereto, the staples are formed substantially simultaneously with substantially the same formed heights.

FIGS. 2 and 3 illustrate an alternative end effector **12'** that is similar to the end effector **12** described above, except with the following differences that are configured to accommodate a knife bar **172'**. The knife bar **172'** is coupled to or protrudes

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from a knife rod **180** and is otherwise operated in the above described manner with respect to the knife bar **172**. However, in this embodiment, the knife bar **172'** is long enough to traverse the entire length of the end effector **12"** and therefore, a separate distal knife member is not employed in the end effector **12"**. The knife bar **172'** has an upper transverse member **173'** and a lower transverse member **175'** formed thereon. The upper transverse member **173'** is oriented to slidably transverse a corresponding elongated slot **250** in anvil **20"** and the lower transverse member **175'** is oriented to traverse an elongated slot **252** in the elongated channel **14"** of the end effector **12"**. A disengagement slot (not shown) is also provided in the anvil **20"** such that when the knife bar **172'** has been driven to an ending position within end effector **12"**, the upper transverse member **173'** drops through the corresponding slot to enable the anvil **20"** to move to the open position to disengage the stapled and cut tissue. The anvil **20"** may be otherwise identical to anvil **20** described above and the elongated channel **14"** may be otherwise identical to elongated channel **14** described above.

In these embodiments, the anvil **20"** is biased to a fully open position (FIG. **2**) by a spring or other opening arrangement (not shown). The anvil **20"** is moved between the open and fully clamped positions by the axial travel of the firing adapter **150** in the manner described above. Once the firing adapter **150** has been advanced to the fully clamped position (FIG. **3**), the surgeon may then advance the knife bar **172"** distally in the manner described above. If the surgeon desires to use the end effector as a grasping device to manipulate tissue, the firing adapter may be moved proximally to allow the anvil **20"** to move away from the elongated channel **14"** as represented in FIG. **4** in broken lines. In this embodiment, as the knife bar **172"** moves distally, the upper transverse member **173'** and the lower transverse member **175'** draw the anvil **20"** and elongated channel **14"** together to achieve the desired staple formation as the knife bar **172"** is advanced distally through the end effector **12"**. See FIG. **5**. Thus, in this embodiment, staple formation occurs simultaneously with tissue cutting, but the staples themselves may be sequentially formed as the knife bar **172"** is driven distally.

The unique and novel features of the various surgical staple cartridges and the surgical instruments of the present invention enable the staples in those cartridges to be arranged in one or more linear or non-linear lines. A plurality of such staple lines may be provided on each side of an elongated slot that is centrally disposed within the staple cartridge for receiving the tissue cutting member therethrough. In one arrangement, for example, the staples in one line may be substantially parallel with the staples in adjacent line(s) of staples, but offset therefrom. In still other embodiments, one or more lines of staples may be non-linear in nature. That is, the base of at least one staple in a line of staples may extend along an axis that is substantially transverse to the bases of other staples in the same staple line. For example, the lines of staples on each side of the elongated slot may have a zigzag appearance.

In various embodiments, a staple cartridge can comprise a cartridge body and a plurality of staples stored within the cartridge body. In use, the staple cartridge can be introduced into a surgical site and positioned on a side of the tissue being treated. In addition, a staple-forming anvil can be positioned on the opposite side of the tissue. In various embodiments, the anvil can be carried by a first jaw and the staple cartridge can be carried by a second jaw, wherein the first jaw and/or the second jaw can be moved toward the other. Once the staple cartridge and the anvil have been positioned relative to the tissue, the staples can be ejected from the staple cartridge

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body such that the staples can pierce the tissue and contact the staple-forming anvil. Once the staples have been deployed from the staple cartridge body, the staple cartridge body can then be removed from the surgical site. In various embodiments disclosed herein, a staple cartridge, or at least a portion of a staple cartridge, can be implanted with the staples. In at least one such embodiment, as described in greater detail further below, a staple cartridge can comprise a cartridge body which can be compressed, crushed, and/or collapsed by the anvil when the anvil is moved from an open position into a closed position. When the cartridge body is compressed, crushed, and/or collapsed, the staples positioned within the cartridge body can be deformed by the anvil. Alternatively, the jaw supporting the staple cartridge can be moved toward the anvil into a closed position. In either event, in various embodiments, the staples can be deformed while they are at least partially positioned within the cartridge body. In certain embodiments, the staples may not be ejected from the staple cartridge while, in some embodiments, the staples can be ejected from the staple cartridge along with a portion of the cartridge body.

Referring now to FIGS. **6A-6D**, a compressible staple cartridge, such as staple cartridge **1000**, for example, can comprise a compressible, implantable cartridge body **1010** and, in addition, a plurality of staples **1020** positioned in the compressible cartridge body **1010**, although only one staple **1020** is depicted in FIGS. **6A-6D**. FIG. **6A** illustrates the staple cartridge **1000** supported by a staple cartridge support, or staple cartridge channel, **1030**, wherein the staple cartridge **1000** is illustrated in an uncompressed condition. In such an uncompressed condition, the anvil **1040** may or may not be in contact with the tissue **T**. In use, the anvil **1040** can be moved from an open position into contact with the tissue **T** as illustrated in FIG. **6B** and position the tissue **T** against the cartridge body **1010**. Even though the anvil **1040** can position the tissue **T** against a tissue-contacting surface **1019** of staple cartridge body **1010**, referring again to FIG. **6B**, the staple cartridge body **1010** may be subjected to little, if any, compressive force or pressure at such point and the staples **1020** may remain in an unformed, or unfired, condition. As illustrated in FIGS. **6A** and **6B**, the staple cartridge body **1010** can comprise one or more layers and the staple legs **1021** of staples **1020** can extend upwardly through these layers. In various embodiments, the cartridge body **1010** can comprise a first layer **1011**, a second layer **1012**, a third layer **1013**, wherein the second layer **1012** can be positioned intermediate the first layer **1011** and the third layer **1013**, and a fourth layer **1014**, wherein the third layer **1013** can be positioned intermediate the second layer **1012** and the fourth layer **1014**. In at least one embodiment, the bases **1022** of the staples **1020** can be positioned within cavities **1015** in the fourth layer **1014** and the staple legs **1021** can extend upwardly from the bases **1022** and through the fourth layer **1014**, the third layer **1013**, and the second layer **1012**, for example. In various embodiments, each deformable leg **1021** can comprise a tip, such as sharp tip **1023**, for example, which can be positioned in the second layer **1012**, for example, when the staple cartridge **1000** is in an uncompressed condition. In at least one such embodiment, the tips **1023** may not extend into and/or through the first layer **1011**, wherein, in at least one embodiment, the tips **1023** may not protrude through the tissue-contacting surface **1019** when the staple cartridge **1000** is in an uncompressed condition. In certain other embodiments, the sharp tips **1023** may be positioned in the third layer **1013**, and/or any other suitable layer, when the staple cartridge is in an uncompressed condition. In various alternative embodi-

ments, a cartridge body of a staple cartridge may have any suitable number of layers such as less than four layers or more than four layers, for example.

In various embodiments, as described in greater detail below, the first layer **1011** can be comprised of a buttress material and/or plastic material, such as polydioxanone (PDS) and/or polyglycolic acid (PGA), for example, and the second layer **1012** can be comprised of a bioabsorbable foam material and/or a compressible haemostatic material, such as oxidized regenerated cellulose (ORC), for example. In various embodiments, one or more of the first layer **1011**, the second layer **1012**, the third layer **1013**, and the fourth layer **1014** may hold the staples **1020** within the staple cartridge body **1010** and, in addition, maintain the staples **1020** in alignment with one another. In various embodiments, the third layer **1013** can be comprised of a buttress material, or a fairly incompressible or inelastic material, which can be configured to hold the staple legs **1021** of the staples **1020** in position relative to one another. Furthermore, the second layer **1012** and the fourth layer **1014**, which are positioned on opposite sides of the third layer **1013**, can stabilize, or reduce the movement of, the staples **1020** even though the second layer **1012** and the fourth layer **1014** can be comprised of a compressible foam or elastic material. In certain embodiments, the staple tips **1023** of the staple legs **1021** can be at least partially embedded in the first layer **1011**. In at least one such embodiment, the first layer **1011** and the third layer **1013** can be configured to co-operatively and firmly hold the staple legs **1021** in position. In at least one embodiment, the first layer **1011** and the third layer **1013** can each be comprised of a sheet of bioabsorbable plastic, such as polyglycolic acid (PGA) which is marketed under the trade name Vicryl, polylactic acid (PLA or PLLA), polydioxanone (PDS), polyhydroxyalkanoate (PHA), poliglecaprone **25** (PGCL) which is marketed under the trade name Monocryl, polycaprolactone (PCL), and/or a composite of PGA, PLA, PDS, PHA, PGCL and/or PCL, for example, and the second layer **1012** and the fourth layer **1014** can each be comprised of at least one haemostatic material or agent.

Although the first layer **1011** can be compressible, the second layer **1012** can be substantially more compressible than the first layer **1011**. For example, the second layer **1012** can be about twice as compressible, about three times as compressible, about four times as compressible, about five times as compressible, and/or about ten times as compressible, for example, as the first layer **1011**. Stated another way, the second layer **1012** may compress about two times, about three times, about four times, about five times, and/or about ten times as much as first layer **1011**, for a given force. In certain embodiments, the second layer **1012** can be between about twice as compressible and about ten times as compressible, for example, as the first layer **1011**. In at least one embodiment, the second layer **1012** can comprise a plurality of air voids defined therein, wherein the amount and/or size of the air voids in the second layer **1012** can be controlled in order to provide a desired compressibility of the second layer **1012**. Similar to the above, although the third layer **1013** can be compressible, the fourth layer **1014** can be substantially more compressible than the third layer **1013**. For example, the fourth layer **1014** can be about twice as compressible, about three times as compressible, about four times as compressible, about five times as compressible, and/or about ten times as compressible, for example, as the third layer **1013**. Stated another way, the fourth layer **1014** may compress about two times, about three times, about four times, about five times, and/or about ten times as much as third layer **1013**, for a given force. In certain embodiments, the fourth layer **1014** can be

between about twice as compressible and about ten times as compressible, for example, as the third layer **1013**. In at least one embodiment, the fourth layer **1014** can comprise a plurality of air voids defined therein, wherein the amount and/or size of the air voids in the fourth layer **1014** can be controlled in order to provide a desired compressibility of the fourth layer **1014**. In various circumstances, the compressibility of a cartridge body, or cartridge body layer, can be expressed in terms of a compression rate, i.e., a distance in which a layer is compressed for a given amount of force. For example, a layer having a high compression rate will compress a larger distance for a given amount of compressive force applied to the layer as compared to a layer having a lower compression rate. This being said, the second layer **1012** can have a higher compression rate than the first layer **1011** and, similarly, the fourth layer **1014** can have a higher compression rate than the third layer **1013**. In various embodiments, the second layer **1012** and the fourth layer **1014** can be comprised of the same material and can comprise the same compression rate. In various embodiments, the second layer **1012** and the fourth layer **1014** can be comprised of materials having different compression rates. Similarly, the first layer **1011** and the third layer **1013** can be comprised of the same material and can comprise the same compression rate. In certain embodiments, the first layer **1011** and the third layer **1013** can be comprised of materials having different compression rates.

As the anvil **1040** is moved toward its closed position, the anvil **1040** can contact tissue **T** and apply a compressive force to the tissue **T** and the staple cartridge **1000**, as illustrated in FIG. **6C**. In such circumstances, the anvil **1040** can push the top surface, or tissue-contacting surface **1019**, of the cartridge body **1010** downwardly toward the staple cartridge support **1030**. In various embodiments, the staple cartridge support **1030** can comprise a cartridge support surface **1031** which can be configured to support the staple cartridge **1000** as the staple cartridge **1000** is compressed between the cartridge support surface **1031** and the tissue-contacting surface **1041** of anvil **1040**. Owing to the pressure applied by the anvil **1040**, the cartridge body **1010** can be compressed and the anvil **1040** can come into contact with the staples **1020**. More particularly, in various embodiments, the compression of the cartridge body **1010** and the downward movement of the tissue-contacting surface **1019** can cause the tips **1023** of the staple legs **1021** to pierce the first layer **1011** of cartridge body **1010**, pierce the tissue **T**, and enter into forming pockets **1042** in the anvil **1040**. As the cartridge body **1010** is further compressed by the anvil **1040**, the tips **1023** can contact the walls defining the forming pockets **1042** and, as a result, the legs **1021** can be deformed or curled inwardly, for example, as illustrated in FIG. **6C**. As the staple legs **1021** are being deformed, as also illustrated in FIG. **6C**, the bases **1022** of the staples **1020** can be in contact with or supported by the staple cartridge support **1030**. In various embodiments, as described in greater detail below, the staple cartridge support **1030** can comprise a plurality of support features, such as staple support grooves, slots, or troughs **1032**, for example, which can be configured to support the staples **1020**, or at least the bases **1022** of the staples **1020**, as the staples **1020** are being deformed. As also illustrated in FIG. **6C**, the cavities **1015** in the fourth layer **1014** can collapse as a result of the compressive force applied to the staple cartridge body **1010**. In addition to the cavities **1015**, the staple cartridge body **1010** can further comprise one or more voids, such as voids **1016**, for example, which may or may not comprise a portion of a staple positioned therein, that can be configured to allow the cartridge body **1010** to collapse. In various embodiments, the cavities **1015** and/or the voids **1016** can be configured to

collapse such that the walls defining the cavities and/or walls deflect downwardly and contact the cartridge support surface **1031** and/or contact a layer of the cartridge body **1010** positioned underneath the cavities and/or voids.

Upon comparing FIG. 6B and FIG. 6C, it is evident that the second layer **1012** and the fourth layer **1014** have been substantially compressed by the compressive pressure applied by the anvil **1040**. It may also be noted that the first layer **1011** and the third layer **1013** have been compressed as well. As the anvil **1040** is moved into its closed position, the anvil **1040** may continue to further compress the cartridge body **1010** by pushing the tissue-contacting surface **1019** downwardly toward the staple cartridge support **1030**. As the cartridge body **1010** is further compressed, the anvil **1040** can deform the staples **1020** into their completely-formed shape as illustrated in FIG. 6D. Referring to FIG. 6D, the legs **1021** of each staple **1020** can be deformed downwardly toward the base **1022** of each staple **1020** in order to capture at least a portion of the tissue T, the first layer **1011**, the second layer **1012**, the third layer **1013**, and the fourth layer **1014** between the deformable legs **1021** and the base **1022**. Upon comparing FIGS. 6C and 6D, it is further evident that the second layer **1012** and the fourth layer **1014** have been further substantially compressed by the compressive pressure applied by the anvil **1040**. It may also be noted upon comparing FIGS. 6C and 6D that the first layer **1011** and the third layer **1013** have been further compressed as well. After the staples **1020** have been completely, or at least sufficiently, formed, the anvil **1040** can be lifted away from the tissue T and the staple cartridge support **1030** can be moved away, and/or detached from, the staple cartridge **1000**. As depicted in FIG. 6D, and as a result of the above, the cartridge body **1010** can be implanted with the staples **1020**. In various circumstances, the implanted cartridge body **1010** can support the tissue along the staple line. In some circumstances, a haemostatic agent, and/or any other suitable therapeutic medicament, contained within the implanted cartridge body **1010** can treat the tissue over time. A haemostatic agent, as mentioned above, can reduce the bleeding of the stapled and/or incised tissue while a bonding agent or tissue adhesive can provide strength to the tissue over time. The implanted cartridge body **1010** can be comprised of materials such as ORC (oxidized regenerated cellulose), extracellular proteins such as collagen, polyglycolic acid (PGA) which is marketed under the trade name Vicryl, polylactic acid (PLA or PLLA), polydioxanone (PDS), polyhydroxyalkanoate (PHA), poliglecaprone **25** (PGCL) which is marketed under the trade name Monocryl, polycaprolactone (PCL), and/or a composite of PGA, PLA, PDS, PHA, PGCL and/or PCL, for example. In certain circumstances, the cartridge body **1010** can comprise an antibiotic and/or antimicrobial material, such as colloidal silver and/or triclosan, for example, which can reduce the possibility of infection in the surgical site.

In various embodiments, the layers of the cartridge body **1010** can be connected to one another. In at least one embodiment, the second layer **1012** can be adhered to the first layer **1011**, the third layer **1013** can be adhered to the second layer **1012**, and the fourth layer **1014** can be adhered to the third layer **1013** utilizing at least one adhesive, such as fibrin and/or protein hydrogel, for example. In certain embodiments, although not illustrated, the layers of the cartridge body **1010** can be connected together by interlocking mechanical features. In at least one such embodiment, the first layer **1011** and the second layer **1012** can each comprise corresponding interlocking features, such as a tongue and groove arrangement and/or a dovetail joint arrangement, for example. Similarly, the second layer **1012** and the third layer **1013** can each

comprise corresponding interlocking features while the third layer **1013** and the fourth layer **1014** can each comprise corresponding interlocking features. In certain embodiments, although not illustrated, the staple cartridge **1000** can comprise one or more rivets, for example, which can extend through one or more layers of the cartridge body **1010**. In at least one such embodiment, each rivet can comprise a first end, or head, positioned adjacent to the first layer **1011** and a second head positioned adjacent to the fourth layer **1014** which can be either assembled to or formed by a second end of the rivet. Owing to the compressible nature of the cartridge body **1010**, in at least one embodiment, the rivets can compress the cartridge body **1010** such that the heads of the rivets can be recessed relative to the tissue-contacting surface **1019** and/or the bottom surface **1018** of the cartridge body **1010**, for example. In at least one such embodiment, the rivets can be comprised of a bioabsorbable material, such as polyglycolic acid (PGA) which is marketed under the trade name Vicryl, polylactic acid (PLA or PLLA), polydioxanone (PDS), polyhydroxyalkanoate (PHA), poliglecaprone **25** (PGCL) which is marketed under the trade name Monocryl, polycaprolactone (PCL), and/or a composite of PGA, PLA, PDS, PHA, PGCL and/or PCL, for example. In certain embodiments, the layers of the cartridge body **1010** may not be connected to one another other than by the staples **1020** contained therein. In at least one such embodiment, the frictional engagement between the staple legs **1021** and the cartridge body **1010**, for example, can hold the layers of the cartridge body **1010** together and, once the staples have been formed, the layers can be captured within the staples **1020**. In certain embodiments, at least a portion of the staple legs **1021** can comprise a roughened surface or rough coating which can increase the friction forces between the staples **1020** and the cartridge body **1010**.

As described above, a surgical instrument can comprise a first jaw including the staple cartridge support **1030** and a second jaw including the anvil **1040**. In various embodiments, as described in greater detail further below, the staple cartridge **1000** can comprise one or more retention features which can be configured to engage the staple cartridge support **1030** and, as a result, releasably retain the staple cartridge **1000** to the staple cartridge support **1030**. In certain embodiments, the staple cartridge **1000** can be adhered to the staple cartridge support **1030** by at least one adhesive, such as fibrin and/or protein hydrogel, for example. In use, in at least one circumstance, especially in laparoscopic and/or endoscopic surgery, the second jaw can be moved into a closed position opposite the first jaw, for example, such that the first and second jaws can be inserted through a trocar into a surgical site. In at least one such embodiment, the trocar can define an approximately 5 mm aperture, or cannula, through which the first and second jaws can be inserted. In certain embodiments, the second jaw can be moved into a partially-closed position intermediate the open position and the closed position which can allow the first and second jaws to be inserted through the trocar without deforming the staples **1020** contained in the staple cartridge body **1010**. In at least one such embodiment, the anvil **1040** may not apply a compressive force to the staple cartridge body **1010** when the second jaw is in its partially-closed intermediate position while, in certain other embodiments, the anvil **1040** can compress the staple cartridge body **1010** when the second jaw is in its partially-closed intermediate position. Even though the anvil **1040** can compress the staple cartridge body **1010** when it is in such an intermediate position, the anvil **1040** may not sufficiently compress the staple cartridge body **1010** such that the anvil **1040** comes into contact with the staples **1020** and/or such that the staples

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1020 are deformed by the anvil 1040. Once the first and second jaws have been inserted through the trocar into the surgical site, the second jaw can be opened once again and the anvil 1040 and the staple cartridge 1000 can be positioned relative to the targeted tissue as described above.

In various embodiments, referring now to FIGS. 7A-7D, an end effector of a surgical stapler can comprise an implantable staple cartridge 1100 positioned intermediate an anvil 1140 and a staple cartridge support 1130. Similar to the above, the anvil 1140 can comprise a tissue-contacting surface 1141, the staple cartridge 1100 can comprise a tissue-contacting surface 1119, and the staple cartridge support 1130 can comprise a support surface 1131 which can be configured to support the staple cartridge 1100. Referring to FIG. 7A, the anvil 1140 can be utilized to position the tissue T against the tissue contacting surface 1119 of staple cartridge 1100 without deforming the staple cartridge 1100 and, when the anvil 1140 is in such a position, the tissue-contacting surface 1141 can be positioned a distance 1101a away from the staple cartridge support surface 1131 and the tissue-contacting surface 1119 can be positioned a distance 1102a away from the staple cartridge support surface 1131. Thereafter, as the anvil 1140 is moved toward the staple cartridge support 1130, referring now to FIG. 7B, the anvil 1140 can push the top surface, or tissue-contacting surface 1119, of staple cartridge 1100 downwardly and compress the first layer 1111 and the second layer 1112 of cartridge body 1110. As the layers 1111 and 1112 are compressed, referring again to FIG. 7B, the second layer 1112 can be crushed and the legs 1121 of staples 1120 can pierce the first layer 1111 and enter into the tissue T. In at least one such embodiment, the staples 1120 can be at least partially positioned within staple cavities, or voids, 1115 in the second layer 1112 and, when the second layer 1112 is compressed, the staple cavities 1115 can collapse and, as a result, allow the second layer 1112 to collapse around the staples 1120. In various embodiments, the second layer 1112 can comprise cover portions 1116 which can extend over the staple cavities 1115 and enclose, or at least partially enclose, the staple cavities 1115. FIG. 7B illustrates the cover portions 1116 being crushed downwardly into the staple cavities 1115. In certain embodiments, the second layer 1112 can comprise one or more weakened portions which can facilitate the collapse of the second layer 1112. In various embodiments, such weakened portions can comprise score marks, perforations, and/or thin cross-sections, for example, which can facilitate a controlled collapse of the cartridge body 1110. In at least one embodiment, the first layer 1111 can comprise one or more weakened portions which can facilitate the penetration of the staple legs 1121 through the first layer 1111. In various embodiments, such weakened portions can comprise score marks, perforations, and/or thin cross-sections, for example, which can be aligned, or at least substantially aligned, with the staple legs 1121.

When the anvil 1140 is in a partially closed, unfired position, referring again to FIG. 7A, the anvil 1140 can be positioned a distance 1101a away from the cartridge support surface 1131 such that a gap is defined therebetween. This gap can be filled by the staple cartridge 1100, having a staple cartridge height 1102a, and the tissue T. As the anvil 1140 is moved downwardly to compress the staple cartridge 1100, referring again to FIG. 7B, the distance between the tissue contacting surface 1141 and the cartridge support surface 1131 can be defined by a distance 1101b which is shorter than the distance 1101a. In various circumstances, the gap between the tissue-contacting surface 1141 of anvil 1140 and the cartridge support surface 1131, defined by distance 1101b, may be larger than the original, undeformed staple

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cartridge height 1102a. As the anvil 1140 is moved closer to the cartridge support surface 1131, referring now to FIG. 7C, the second layer 1112 can continue to collapse and the distance between the staple legs 1121 and the forming pockets 1142 can decrease. Similarly, the distance between the tissue-contacting surface 1141 and the cartridge support surface 1131 can decrease to a distance 1101c which, in various embodiments, may be greater than, equal to, or less than the original, undeformed cartridge height 1102a. Referring now to FIG. 7D, the anvil 1140 can be moved into a final, fired position in which the staples 1120 have been fully formed, or at least formed to a desired height. In such a position, the tissue-contacting surface 1141 of anvil 1140 can be a distance 1101d away from the cartridge support surface 1131, wherein the distance 1101d can be shorter than the original, undeformed cartridge height 1102a. As also illustrated in FIG. 7D, the staple cavities 1115 may be fully, or at least substantially, collapsed and the staples 1120 may be completely, or at least substantially, surrounded by the collapsed second layer 1112. In various circumstances, the anvil 1140 can be thereafter moved away from the staple cartridge 1100. Once the anvil 1140 has been disengaged from the staple cartridge 1100, the cartridge body 1110 can at least partially re-expand in various locations, i.e., locations intermediate adjacent staples 1120, for example. In at least one embodiment, the crushed cartridge body 1110 may not resiliently re-expand. In various embodiments, the formed staples 1120 and, in addition, the cartridge body 1110 positioned intermediate adjacent staples 1120 may apply pressure, or compressive forces, to the tissue T which may provide various therapeutic benefits.

As discussed above, referring again to the embodiment illustrated in FIG. 7A, each staple 1120 can comprise staple legs 1121 extending therefrom. Although staples 1120 are depicted as comprising two staple legs 1121, various staples can be utilized which can comprise one staple leg or, alternatively, more than two staple legs, such as three staple legs or four staple legs, for example. As illustrated in FIG. 7A, each staple leg 1121 can be embedded in the second layer 1112 of the cartridge body 1110 such that the staples 1120 are secured within the second layer 1112. In various embodiments, the staples 1120 can be inserted into the staple cavities 1115 in cartridge body 1110 such that the tips 1123 of the staple legs 1121 enter into the cavities 1115 before the bases 1122. After the tips 1123 have been inserted into the cavities 1115, in various embodiments, the tips 1123 can be pressed into the cover portions 1116 and incise the second layer 1112. In various embodiments, the staples 1120 can be seated to a sufficient depth within the second layer 1112 such that the staples 1120 do not move, or at least substantially move, relative to the second layer 1112. In certain embodiments, the staples 1120 can be seated to a sufficient depth within the second layer 1112 such that the bases 1122 are positioned or embedded within the staple cavities 1115. In various other embodiments, the bases 1122 may not be positioned or embedded within the second layer 1112. In certain embodiments, referring again to FIG. 7A, the bases 1122 may extend below the bottom surface 1118 of the cartridge body 1110. In certain embodiments, the bases 1122 can rest on, or can be directly positioned against, the cartridge support surface 1130. In various embodiments, the cartridge support surface 1130 can comprise support features extending therefrom and/or defined therein wherein, in at least one such embodiment, the bases 1122 of the staples 1120 may be positioned within and supported by one or more support grooves, slots, or troughs, 1132, for example, in the staple cartridge support 1130, as described in greater detail further below.

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In various embodiments, referring now to FIGS. 8 and 9, a staple cartridge, such as staple cartridge 1200, for example, can comprise a compressible, implantable cartridge body 1210 comprising an outer layer 1211 and an inner layer 1212. Similar to the above, the staple cartridge 1200 can comprise a plurality of staples 1220 positioned within the cartridge body 1210. In various embodiments, each staple 1220 can comprise a base 1222 and one or more staple legs 1221 extending therefrom. In at least one such embodiment, the staple legs 1221 can be inserted into the inner layer 1212 and seated to a depth in which the bases 1222 of the staples 1220 abut and/or are positioned adjacent to the bottom surface 1218 of the inner layer 1212, for example. In the embodiment depicted in FIGS. 8 and 9, the inner layer 1212 does not comprise staple cavities configured to receive a portion of the staples 1220 while, in other embodiments, the inner layer 1212 can comprise such staple cavities. In various embodiments, further to the above, the inner layer 1212 can be comprised of a compressible material, such as bioabsorbable foam and/or oxidized regenerated cellulose (ORC), for example, which can be configured to allow the cartridge body 1210 to collapse when a compressive load is applied thereto. In various embodiments, the inner layer 1212 can be comprised of a lyophilized foam comprising polylactic acid (PLA) and/or polyglycolic acid (PGA), for example. The ORC may be commercially available under the trade name Surgical and can comprise a loose woven fabric (like a surgical sponge), loose fibers (like a cotton ball), and/or a foam. In at least one embodiment, the inner layer 1212 can be comprised of a material including medicaments, such as freeze-dried thrombin and/or fibrin, for example, contained therein and/or coated thereon which can be water-activated and/or activated by fluids within the patient's body, for example. In at least one such embodiment, the freeze-dried thrombin and/or fibrin can be held on a Vicryl (PGA) matrix, for example. In certain circumstances, however, the activatable medicaments can be unintentionally activated when the staple cartridge 1200 is inserted into a surgical site within the patient, for example. In various embodiments, referring again to FIGS. 8 and 9, the outer layer 1211 can be comprised of a water impermeable, or at least substantially water impermeable, material such that liquids do not come into contact with, or at least substantially contact, the inner layer 1212 until after the cartridge body 1210 has been compressed and the staple legs have penetrated the outer layer 1211 and/or after the outer layer 1211 has been incised in some fashion. In various embodiments, the outer layer 1211 can be comprised of a buttress material and/or plastic material, such as polydioxanone (PDS) and/or polyglycolic acid (PGA), for example. In certain embodiments, the outer layer 1211 can comprise a wrap which surrounds the inner layer 1212 and the staples 1220. More particularly, in at least one embodiment, the staples 1220 can be inserted into the inner layer 1212 and the outer layer 1211 can be wrapped around the sub-assembly comprising the inner layer 1212 and the staples 1220 and then sealed.

In various embodiments described herein, the staples of a staple cartridge can be fully formed by an anvil when the anvil is moved into a closed position. In various other embodiments, referring now to FIGS. 10-13, the staples of a staple cartridge, such as staple cartridge 4100, for example, can be deformed by an anvil when the anvil is moved into a closed position and, in addition, by a staple driver system which moves the staples toward the closed anvil. The staple cartridge 4100 can comprise a compressible cartridge body 4110 which can be comprised of a foam material, for example, and a plurality of staples 4120 at least partially positioned within the compressible cartridge body 4110. In various embodi-

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ments, the staple driver system can comprise a driver holder 4160, a plurality of staple drivers 4162 positioned within the driver holder 4160, and a staple cartridge pan 4180 which can be configured to retain the staple drivers 4162 in the driver holder 4160. In at least one such embodiment, the staple drivers 4162 can be positioned within one or more slots 4163 in the driver holder 4160 wherein the sidewalls of the slots 4163 can assist in guiding the staple drivers 4162 upwardly toward the anvil. In various embodiments, the staples 4120 can be supported within the slots 4163 by the staple drivers 4162 wherein, in at least one embodiment, the staples 4120 can be entirely positioned in the slots 4163 when the staples 4120 and the staple drivers 4162 are in their unfired positions. In certain other embodiments, at least a portion of the staples 4120 can extend upwardly through the open ends 4161 of slots 4163 when the staples 4120 and staple drivers 4162 are in their unfired positions. In at least one such embodiment, referring primarily now to FIG. 11, the bases of the staples 4120 can be positioned within the driver holder 4160 and the tips of the staples 4120 can be embedded within the compressible cartridge body 4110. In certain embodiments, approximately one-third of the height of the staples 4120 can be positioned within the driver holder 4160 and approximately two-thirds of the height of the staples 4120 can be positioned within the cartridge body 4110. In at least one embodiment, referring to FIG. 10A, the staple cartridge 4100 can further comprise a water impermeable wrap or membrane 4111 surrounding the cartridge body 4110 and the driver holder 4160, for example.

In use, the staple cartridge 4100 can be positioned within a staple cartridge channel, for example, and the anvil can be moved toward the staple cartridge 4100 into a closed position. In various embodiments, the anvil can contact and compress the compressible cartridge body 4110 when the anvil is moved into its closed position. In certain embodiments, the anvil may not contact the staples 4120 when the anvil is in its closed position. In certain other embodiments, the anvil may contact the legs of the staples 4120 and at least partially deform the staples 4120 when the anvil is moved into its closed position. In either event, the staple cartridge 4100 can further comprise one or more sleds 4170 which can be advanced longitudinally within the staple cartridge 4100 such that the sleds 4170 can sequentially engage the staple drivers 4162 and move the staple drivers 4162 and the staples 4120 toward the anvil. In various embodiments, the sleds 4170 can slide between the staple cartridge pan 4180 and the staple drivers 4162. In embodiments where the closure of the anvil has started the forming process of the staples 4120, the upward movement of the staples 4120 toward the anvil can complete the forming process and deform the staples 4120 to their fully formed, or at least desired, height. In embodiments where the closure of the anvil has not deformed the staples 4120, the upward movement of the staples 4120 toward the anvil can initiate and complete the forming process and deform the staples 4120 to their fully formed, or at least desired, height. In various embodiments, the sleds 4170 can be advanced from a proximal end of the staple cartridge 4100 to a distal end of the staple cartridge 4100 such that the staples 4120 positioned in the proximal end of the staple cartridge 4100 are fully formed before the staples 4120 positioned in the distal end of the staple cartridge 4100 are fully formed. In at least one embodiment, referring to FIG. 12, the sleds 4170 can each comprise at least one angled or inclined surface 4711 which can be configured to slide underneath the staple drivers 4162 and lift the staple drivers 4162 as illustrated in FIG. 13.

In various embodiments, further to the above, the staples 4120 can be formed in order to capture at least a portion of the

tissue T and at least a portion of the compressible cartridge body **4110** of the staple cartridge **4100** therein. After the staples **4120** have been formed, the anvil and the staple cartridge channel **4130** of the surgical stapler can be moved away from the implanted staple cartridge **4100**. In various circumstances, the cartridge pan **4180** can be fixedly engaged with the staple cartridge channel **4130** wherein, as a result, the cartridge pan **4180** can become detached from the compressible cartridge body **4110** as the staple cartridge channel **4130** is pulled away from the implanted cartridge body **4110**. In various embodiments, referring again to FIG. 10, the cartridge pan **4180** can comprise opposing side walls **4181** between which the cartridge body **4110** can be removably positioned. In at least one such embodiment, the compressible cartridge body **4110** can be compressed between the side walls **4181** such that the cartridge body **4110** can be removably retained therebetween during use and releasably disengaged from the cartridge pan **4180** as the cartridge pan **4180** is pulled away. In at least one such embodiment, the driver holder **4160** can be connected to the cartridge pan **4180** such that the driver holder **4160**, the drivers **4162**, and/or the sleds **4170** can remain in the cartridge pan **4180** when the cartridge pan **4180** is removed from the surgical site. In certain other embodiments, the drivers **4162** can be ejected from the driver holder **4160** and left within the surgical site. In at least one such embodiment, the drivers **4162** can be comprised of a bioabsorbable material, such as polyglycolic acid (PGA) which is marketed under the trade name Vicryl, polylactic acid (PLA or PLLA), polydioxanone (PDS), polyhydroxyalkanoate (PHA), poliglecaprone **25** (PGCL) which is marketed under the trade name Monocryl, polycaprolactone (PCL), and/or a composite of PGA, PLA, PDS, PHA, PGCL and/or PCL, for example. In various embodiments, the drivers **4162** can be attached to the staples **4120** such that the drivers **4162** are deployed with the staples **4120**. In at least one such embodiment, each driver **4162** can comprise a trough configured to receive the bases of the staples **4120**, for example, wherein, in at least one embodiment, the troughs can be configured to receive the staple bases in a press-fit and/or snap-fit manner.

In certain embodiments, further to the above, the driver holder **4160** and/or the sleds **4170** can be ejected from the cartridge pan **4180**. In at least one such embodiment, the sleds **4170** can slide between the cartridge pan **4180** and the driver holder **4160** such that, as the sleds **4170** are advanced in order to drive the staple drivers **4162** and staples **4120** upwardly, the sleds **4170** can move the driver holder **4160** upwardly out of the cartridge pan **4180** as well. In at least one such embodiment, the driver holder **4160** and/or the sleds **4170** can be comprised of a bioabsorbable material, such as polyglycolic acid (PGA) which is marketed under the trade name Vicryl, polylactic acid (PLA or PLLA), polydioxanone (PDS), polyhydroxyalkanoate (PHA), poliglecaprone **25** (PGCL) which is marketed under the trade name Monocryl, polycaprolactone (PCL), and/or a composite of PGA, PLA, PDS, PHA, PGCL and/or PCL, for example. In various embodiments, the sleds **4170** can be integrally formed and/or attached to a drive bar, or cutting member, which pushes the sleds **4170** through the staple cartridge **4100**. In such embodiments, the sleds **4170** may not be ejected from the cartridge pan **4180** and may remain with the surgical stapler while, in other embodiments in which the sleds **4170** are not attached to the drive bar, the sleds **4170** may be left in the surgical site. In any event, further to the above, the compressibility of the cartridge body **4110** can allow thicker staple cartridges to be used within an end effector of a surgical stapler as the cartridge body **4110** can compress, or shrink, when the anvil of the stapler is closed. In

certain embodiments, as a result of the staples being at least partially deformed upon the closure of the anvil, taller staples, such as staples having an approximately 0.18" staple height, for example, could be used, wherein approximately 0.12" of the staple height can be positioned within the compressible layer **4110** and wherein the compressible layer **4110** can have an uncompressed height of approximately 0.14", for example.

In many embodiments described herein, a staple cartridge can comprise a plurality of staples therein. In various embodiments, such staples can be comprised of a metal wire deformed into a substantially U-shaped configuration having two staple legs. Other embodiments are envisioned in which staples can comprise different configurations such as two or more wires that have been joined together having three or more staple legs. In various embodiments, the wire, or wires, used to form the staples can comprise a round, or at least substantially round, cross-section. In at least one embodiment, the staple wires can comprise any other suitable cross-section, such as square and/or rectangular cross-sections, for example. In certain embodiments, the staples can be comprised of plastic wires. In at least one embodiment, the staples can be comprised of plastic-coated metal wires. In various embodiments, a cartridge can comprise any suitable type of fastener in addition to or in lieu of staples. In at least one such embodiment, such a fastener can comprise pivotable arms which are folded when engaged by an anvil. In certain embodiments, two-part fasteners could be utilized. In at least one such embodiment, a staple cartridge can comprise a plurality of first fastener portions and an anvil can comprise a plurality of second fastener portions which are connected to the first fastener portions when the anvil is compressed against the staple cartridge. In certain embodiments, as described above, a sled or driver can be advanced within a staple cartridge in order to complete the forming process of the staples. In certain embodiments, a sled or driver can be advanced within an anvil in order to move one or more forming members downwardly into engagement with the opposing staple cartridge and the staples, or fasteners, positioned therein.

In various embodiments described herein, a staple cartridge can comprise four rows of staples stored therein. In at least one embodiment, the four staple rows can be arranged in two inner staple rows and two outer staple rows. In at least one such embodiment, an inner staple row and an outer staple row can be positioned on a first side of a cutting member, or knife, slot within the staple cartridge and, similarly, an inner staple row and an outer staple row can be positioned on a second side of the cutting member, or knife, slot. In certain embodiments, a staple cartridge may not comprise a cutting member slot; however, such a staple cartridge may comprise a designated portion configured to be incised by a cutting member in lieu of a staple cartridge slot. In various embodiments, the inner staple rows can be arranged within the staple cartridge such that they are equally, or at least substantially equally, spaced from the cutting member slot. Similarly, the outer staple rows can be arranged within the staple cartridge such that they are equally, or at least substantially equally, spaced from the cutting member slot. In various embodiments, a staple cartridge can comprise more than or less than four rows of staples stored within a staple cartridge. In at least one embodiment, a staple cartridge can comprise six rows of staples. In at least one such embodiment, the staple cartridge can comprise three rows of staples on a first side of a cutting member slot and three rows of staples on a second side of the cutting member slot. In certain embodiments, a staple cartridge may comprise an odd number of staple rows. For example, a staple

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cartridge may comprise two rows of staples on a first side of a cutting member slot and three rows of staples on a second side of the cutting member slot. In various embodiments, the staple rows can comprise staples having the same, or at least substantially the same, unformed staple height. In certain other embodiments, one or more of the staple rows can comprise staples having a different unformed staple height than the other staples. In at least one such embodiment, the staples on a first side of a cutting member slot may have a first unformed height and the staples on a second side of a cutting member slot may have a second unformed height which is different than the first height, for example.

In various embodiments, as described above, a staple cartridge can comprise a cartridge body including a plurality of staple cavities defined therein. The cartridge body can comprise a deck and a top deck surface wherein each staple cavity can define an opening in the deck surface. As also described above, a staple can be positioned within each staple cavity such that the staples are stored within the cartridge body until they are ejected therefrom. Prior to being ejected from the cartridge body, in various embodiments, the staples can be contained within the cartridge body such that the staples do not protrude above the deck surface. As the staples are positioned below the deck surface, in such embodiments, the possibility of the staples becoming damaged and/or prematurely contacting the targeted tissue can be reduced. In various circumstances, the staples can be moved between an unfired position in which they do not protrude from the cartridge body and a fired position in which they have emerged from the cartridge body and can contact an anvil positioned opposite the staple cartridge. In various embodiments, the anvil, and/or the forming pockets defined within the anvil, can be positioned a predetermined distance above the deck surface such that, as the staples are being deployed from the cartridge body, the staples are deformed to a predetermined formed height. In some circumstances, the thickness of the tissue captured between the anvil and the staple cartridge may vary and, as a result, thicker tissue may be captured within certain staples while thinner tissue may be captured within certain other staples. In either event, the clamping pressure, or force, applied to the tissue by the staples may vary from staple to staple or vary between a staple on one end of a staple row and a staple on the other end of the staple row, for example. In certain circumstances, the gap between the anvil and the staple cartridge deck can be controlled such that the staples apply a certain minimum clamping pressure within each staple. In some such circumstances, however, significant variation of the clamping pressure within different staples may still exist. Surgical stapling instruments are disclosed in U.S. Pat. No. 7,380,696, which issued on Jun. 3, 2008, the entire disclosure of which is incorporated by reference herein. An illustrative multi-stroke handle for the surgical stapling and severing instrument is described in greater detail in the co-pending and co-owned U.S. patent application entitled SURGICAL STAPLING INSTRUMENT INCORPORATING A MULTISTROKE FIRING POSITION INDICATOR AND RETRACTION MECHANISM, Ser. No. 10/674,026, now U.S. Pat. No. 7,364,061, the disclosure of which is hereby incorporated by reference in its entirety. Other applications consistent with the present invention may incorporate a single firing stroke, such as described in co-pending and commonly owned U.S. patent application SURGICAL STAPLING INSTRUMENT HAVING SEPARATE DISTINCT CLOSING AND FIRING SYSTEMS, Ser. No. 10/441,632, now U.S. Pat. No. 7,000,818, the disclosure of which is hereby incorporated by reference in its entirety.

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In various embodiments described herein, a staple cartridge can comprise means for compensating for the thickness of the tissue captured within the staples deployed from the staple cartridge. In various embodiments, referring to FIG. 14, a staple cartridge, such as staple cartridge 10000, for example, can include a rigid first portion, such as support portion 10010, for example, and a compressible second portion, such as tissue thickness compensator 10020, for example. In at least one embodiment, referring primarily to FIG. 16, the support portion 10010 can comprise a cartridge body, a top deck surface 10011, and a plurality of staple cavities 10012 wherein, similar to the above, each staple cavity 10012 can define an opening in the deck surface 10011. A staple 10030, for example, can be removably positioned in each staple cavity 10012. In at least one such embodiment, each staple 10030 can comprise a base 10031 and one or more legs 10032 extending from the base 10031. Prior to the staples 10030 being deployed, as also described in greater detail below, the bases 10031 of the staples 10030 can be supported by staple drivers positioned within the support portion 10010 and, concurrently, the legs 10032 of the staples 10030 can be at least partially contained within the staple cavities 10012. In various embodiments, the staples 10030 can be deployed between an unfired position and a fired position such that the legs 10032 move through the tissue thickness compensator 10020, penetrate through a top surface of the tissue thickness compensator 10020, penetrate the tissue T, and contact an anvil positioned opposite the staple cartridge 10000. As the legs 10032 are deformed against the anvil, the legs 10032 of each staple 10030 can capture a portion of the tissue thickness compensator 10020 and a portion of the tissue T within each staple 10030 and apply a compressive force to the tissue. Further to the above, the legs 10032 of each staple 10030 can be deformed downwardly toward the base 10031 of the staple to form a staple entrapment area 10039 in which the tissue T and the tissue thickness compensator 10020 can be captured. In various circumstances, the staple entrapment area 10039 can be defined between the inner surfaces of the deformed legs 10032 and the inner surface of the base 10031. The size of the entrapment area for a staple can depend on several factors such as the length of the legs, the diameter of the legs, the width of the base, and/or the extent in which the legs are deformed, for example.

In previous embodiments, a surgeon was often required to select the appropriate staples having the appropriate staple height for the tissue being stapled. For example, a surgeon could select tall staples for use with thick tissue and short staples for use with thin tissue. In some circumstances, however, the tissue being stapled did not have a consistent thickness and, thus, some staples were unable to achieve the desired fired configuration. For example, FIG. 48 illustrates a tall staple used in thin tissue. Referring now to FIG. 49, when a tissue thickness compensator, such as tissue thickness compensator 10020, for example, is used with thin tissue, for example, the larger staple may be formed to a desired fired configuration.

Owing to the compressibility of the tissue thickness compensator, the tissue thickness compensator can compensate for the thickness of the tissue captured within each staple. More particularly, referring now to FIGS. 43 and 44, a tissue thickness compensator, such as tissue thickness compensator 10020, for example, can consume larger and/or smaller portions of the staple entrapment area 10039 of each staple 10030 depending on the thickness and/or type of tissue contained within the staple entrapment area 10039. For example, if thinner tissue T is captured within a staple 10030, the tissue thickness compensator 10020 can consume a larger portion of

the staple entrapment area **10039** as compared to circumstances where thicker tissue T is captured within the staple **10030**. Correspondingly, if thicker tissue T is captured within a staple **10030**, the tissue thickness compensator **10020** can consume a smaller portion of the staple entrapment area **10039** as compared to the circumstances where thinner tissue T is captured within the staple **10030**. In this way, the tissue thickness compensator can compensate for thinner tissue and/or thicker tissue and assure that a compressive pressure is applied to the tissue irrespective, or at least substantially irrespective, of the tissue thickness captured within the staples. In addition to the above, the tissue thickness compensator **10020** can compensate for different types, or compressibilities, of tissues captured within different staples **10030**. Referring now to FIG. 44, the tissue thickness compensator **10020** can apply a compressive force to vascular tissue T which can include vessels V and, as a result, restrict the flow of blood through the less compressible vessels V while still applying a desired compressive pressure to the surrounding tissue T. In various circumstances, further to the above, the tissue thickness compensator **10020** can also compensate for malformed staples. Referring to FIG. 45, the malformation of various staples **10030** can result in larger staple entrapment areas **10039** being defined within such staples. Owing to the resiliency of the tissue thickness compensator **10020**, referring now to FIG. 46, the tissue thickness compensator **10020** positioned within malformed staples **10030** may still apply a sufficient compressive pressure to the tissue T even though the staple entrapment areas **10039** defined within such malformed staples **10030** may be enlarged. In various circumstances, the tissue thickness compensator **10020** located intermediate adjacent staples **10030** can be biased against the tissue T by properly-formed staples **10030** surrounding a malformed staple **10030** and, as a result, apply a compressive pressure to the tissue surrounding and/or captured within the malformed staple **10030**, for example. In various circumstances, a tissue thickness compensator can compensate for different tissue densities which can arise due to calcifications, fibrous areas, and/or tissue that has been previously stapled or treated, for example.

In various embodiments, a fixed, or unchangeable, tissue gap can be defined between the support portion and the anvil and, as a result, the staples may be deformed to a predetermined height regardless of the thickness of the tissue captured within the staples. When a tissue thickness compensator is used with these embodiments, the tissue thickness compensator can adapt to the tissue captured between the anvil and the support portion staple cartridge and, owing to the resiliency of the tissue thickness compensator, the tissue thickness compensator can apply an additional compressive pressure to the tissue. Referring now to FIGS. 50-55, a staple **10030** has been formed to a predefined height H. With regard to FIG. 50, a tissue thickness compensator has not been utilized and the tissue T consumes the entirety of the staple entrapment area **10039**. With regard to FIG. 57, a portion of a tissue thickness compensator **10020** has been captured within the staple **10030**, compressed the tissue T, and consumed at least a portion of the staple entrapment area **10039**. Referring now to FIG. 52, thin tissue T has been captured within the staple **10030**. In this embodiment, the compressed tissue T has a height of approximately $\frac{2}{3}H$ and the compressed tissue thickness compensator **10020** has a height of approximately $\frac{1}{3}H$, for example. Referring now to FIG. 53, tissue T having an intermediate thickness has been captured within the staple **10030**. In this embodiment, the compressed tissue T has a height of approximately $\frac{1}{2}H$ and the compressed tissue thickness compensator **10020** has a height of approximately $\frac{1}{2}H$,

for example. Referring now to FIG. 54, tissue T having an intermediate thickness has been captured within the staple **10030**. In this embodiment, the compressed tissue T has a height of approximately $\frac{2}{3}H$ and the compressed tissue thickness compensator **10020** has a height of approximately $\frac{1}{3}H$, for example. Referring now to FIG. 53, thick tissue T has been captured within the staple **10030**. In this embodiment, the compressed tissue T has a height of approximately $\frac{1}{2}H$ and the compressed tissue thickness compensator **10020** has a height of approximately $\frac{1}{2}H$, for example. In various circumstances, the tissue thickness compensator can comprise a compressed height which comprises approximately 10% of the staple entrapment height, approximately 20% of the staple entrapment height, approximately 30% of the staple entrapment height, approximately 40% of the staple entrapment height, approximately 50% of the staple entrapment height, approximately 60% of the staple entrapment height, approximately 70% of the staple entrapment height, approximately 80% of the staple entrapment height, and/or approximately 90% of the staple entrapment height, for example.

In various embodiments, the staples **10030** can comprise any suitable unformed height. In certain embodiments, the staples **10030** can comprise an unformed height between approximately 2 mm and approximately 4.8 mm, for example. The staples **10030** can comprise an unformed height of approximately 2.0 mm, approximately 2.5 mm, approximately 3.0 mm, approximately 3.4 mm, approximately 3.5 mm, approximately 3.8 mm, approximately 4.0 mm, approximately 4.1 mm, and/or approximately 4.8 mm, for example. In various embodiments, the height H to which the staples can be deformed can be dictated by the distance between the deck surface **10011** of the support portion **10010** and the opposing anvil. In at least one embodiment, the distance between the deck surface **10011** and the tissue-contacting surface of the anvil can be approximately 0.097", for example. The height H can also be dictated by the depth of the forming pockets defined within the anvil. In at least one embodiment, the forming pockets can have a depth measured from the tissue-contacting surface, for example. In various embodiments, as described in greater detail below, the staple cartridge **10000** can further comprise staple drivers which can lift the staples **10030** toward the anvil and, in at least one embodiment, lift, or "overdrive", the staples above the deck surface **10011**. In such embodiments, the height H to which the staples **10030** are formed can also be dictated by the distance in which the staples **10030** are overdriven. In at least one such embodiment, the staples **10030** can be overdriven by approximately 0.028", for example, and can result in the staples **10030** being formed to a height of approximately 0.189", for example. In various embodiments, the staples **10030** can be formed to a height of approximately 0.8 mm, approximately 1.0 mm, approximately 1.5 mm, approximately 1.8 mm, approximately 2.0 mm, and/or approximately 2.25 mm, for example. In certain embodiments, the staples can be formed to a height between approximately 2.25 mm and approximately 3.0 mm, for example. Further to the above, the height of the staple entrapment area of a staple can be determined by the formed height of the staple and the width, or diameter, of the wire comprising the staple. In various embodiments, the height of the staple entrapment area **10039** of a staple **10030** can comprise the formed height H of the staple less two diameter widths of the wire. In certain embodiments, the staple wire can comprise a diameter of approximately 0.0089", for example. In various embodiments, the staple wire can comprise a diameter between approximately 0.0069" and approximately 0.0119", for example. In at least one exemplary embodiment, the formed height H of a staple **10030** can

be approximately 0.189" and the staple wire diameter can be approximately 0.0089" resulting in a staple entrapment height of approximately 0.171", for example.

In various embodiments, further to the above, the tissue thickness compensator can comprise an uncompressed, or pre-deployed, height and can be configured to deform to one of a plurality of compressed heights. In certain embodiments, the tissue thickness compensator can comprise an uncompressed height of approximately 0.125", for example. In various embodiments, the tissue thickness compensator can comprise an uncompressed height of greater than or equal to approximately 0.080", for example. In at least one embodiment, the tissue thickness compensator can comprise an uncompressed, or pre-deployed, height which is greater than the unfired height of the staples. In at least one embodiment, the uncompressed, or pre-deployed, height of the tissue thickness compensator can be approximately 10% taller, approximately 20% taller, approximately 30% taller, approximately 40% taller, approximately 50% taller, approximately 60% taller, approximately 70% taller, approximately 80% taller, approximately 90% taller, and/or approximately 100% taller than the unfired height of the staples, for example. In at least one embodiment, the uncompressed, or pre-deployed, height of the tissue thickness compensator can be up to approximately 100% taller than the unfired height of the staples, for example. In certain embodiments, the uncompressed, or pre-deployed, height of the tissue thickness compensator can be over 100% taller than the unfired height of the staples, for example. In at least one embodiment, the tissue thickness compensator can comprise an uncompressed height which is equal to the unfired height of the staples. In at least one embodiment, the tissue thickness compensator can comprise an uncompressed height which is less than the unfired height of the staples. In at least one embodiment, the uncompressed, or pre-deployed, height of the thickness compensator can be approximately 10% shorter, approximately 20% shorter, approximately 30% shorter, approximately 40% shorter, approximately 50% shorter, approximately 60% shorter, approximately 70% shorter, approximately 80% shorter, and/or approximately 90% shorter than the unfired height of the staples, for example. In various embodiments, the compressible second portion can comprise an uncompressed height which is taller than an uncompressed height of the tissue T being stapled. In certain embodiments, the tissue thickness compensator can comprise an uncompressed height which is equal to an uncompressed height of the tissue T being stapled. In various embodiments, the tissue thickness compensator can comprise an uncompressed height which is shorter than an uncompressed height of the tissue T being stapled.

As described above, a tissue thickness compensator can be compressed within a plurality of formed staples regardless of whether thick tissue or thin tissue is captured within the staples. In at least one exemplary embodiment, the staples within a staple line, or row, can be deformed such that the staple entrapment area of each staple comprises a height of approximately 2.0 mm, for example, wherein the tissue T and the tissue thickness compensator can be compressed within this height. In certain circumstances, the tissue T can comprise a compressed height of approximately 1.75 mm within the staple entrapment area while the tissue thickness compensator can comprise a compressed height of approximately 0.25 mm within the staple entrapment area, thereby totaling the approximately 2.0 mm staple entrapment area height, for example. In certain circumstances, the tissue T can comprise a compressed height of approximately 1.50 mm within the staple entrapment area while the tissue thickness compensator can comprise a compressed height of approximately 0.50

mm within the staple entrapment area, thereby totaling the approximately 2.0 mm staple entrapment area height, for example. In certain circumstances, the tissue T can comprise a compressed height of approximately 1.25 mm within the staple entrapment area while the tissue thickness compensator can comprise a compressed height of approximately 0.75 mm within the staple entrapment area, thereby totaling the approximately 2.0 mm staple entrapment area height, for example. In certain circumstances, the tissue T can comprise a compressed height of approximately 1.0 mm within the staple entrapment area while the tissue thickness compensator can comprise a compressed height of approximately 1.0 mm within the staple entrapment area, thereby totaling the approximately 2.0 mm staple entrapment area height, for example. In certain circumstances, the tissue T can comprise a compressed height of approximately 0.75 mm within the staple entrapment area while the tissue thickness compensator can comprise a compressed height of approximately 1.25 mm within the staple entrapment area, thereby totaling the approximately 2.0 mm staple entrapment area height, for example. In certain circumstances, the tissue T can comprise a compressed height of approximately 1.50 mm within the staple entrapment area while the tissue thickness compensator can comprise a compressed height of approximately 0.50 mm within the staple entrapment area, thereby totaling the approximately 2.0 mm staple entrapment area height, for example. In certain circumstances, the tissue T can comprise a compressed height of approximately 0.25 mm within the staple entrapment area while the tissue thickness compensator can comprise a compressed height of approximately 1.75 mm within the staple entrapment area, thereby totaling the approximately 2.0 mm staple entrapment area height, for example.

In various embodiments, further to the above, the tissue thickness compensator can comprise an uncompressed height which is less than the fired height of the staples. In certain embodiments, the tissue thickness compensator can comprise an uncompressed height which is equal to the fired height of the staples. In certain other embodiments, the tissue thickness compensator can comprise an uncompressed height which is taller than the fired height of the staples. In at least one such embodiment, the uncompressed height of a tissue thickness compensator can comprise a thickness which is approximately 110% of the formed staple height, approximately 120% of the formed staple height, approximately 130% of the formed staple height, approximately 140% of the formed staple height, approximately 150% of the formed staple height, approximately 160% of the formed staple height, approximately 170% of the formed staple height, approximately 180% of the formed staple height, approximately 190% of the formed staple height, and/or approximately 200% of the formed staple height, for example. In certain embodiments, the tissue thickness compensator can comprise an uncompressed height which is more than twice the fired height of the staples. In various embodiments, the tissue thickness compensator can comprise a compressed height which is from approximately 85% to approximately 150% of the formed staple height, for example. In various embodiments, as described above, the tissue thickness compensator can be compressed between an uncompressed thickness and a compressed thickness. In certain embodiments, the compressed thickness of a tissue thickness compensator can be approximately 10% of its uncompressed thickness, approximately 20% of its uncompressed thickness, approximately 30% of its uncompressed thickness, approximately 40% of its uncompressed thickness, approximately 50% of its uncompressed thickness, approximately 60% of its uncompressed

thickness, approximately 70% of its uncompressed thickness, approximately 80% of its uncompressed thickness, and/or approximately 90% of its uncompressed thickness, for example. In various embodiments, the uncompressed thickness of the tissue thickness compensator can be approximately two times, approximately ten times, approximately fifty times, and/or approximately one hundred times thicker than its compressed thickness, for example. In at least one embodiment, the compressed thickness of the tissue thickness compensator can be between approximately 60% and approximately 99% of its uncompressed thickness. In at least one embodiment, the uncompressed thickness of the tissue thickness compensator can be at least 50% thicker than its compressed thickness. In at least one embodiment, the uncompressed thickness of the tissue thickness compensator can be up to one hundred times thicker than its compressed thickness. In various embodiments, the compressible second portion can be elastic, or at least partially elastic, and can bias the tissue T against the deformed legs of the staples. In at least one such embodiment, the compressible second portion can resiliently expand between the tissue T and the base of the staple in order to push the tissue T against the legs of the staple. In certain embodiments, discussed in further detail below, the tissue thickness compensator can be positioned intermediate the tissue T and the deformed staple legs. In various circumstances, as a result of the above, the tissue thickness compensator can be configured to consume any gaps within the staple entrapment area.

In various embodiments, the tissue thickness compensator may comprise materials characterized by one or more of the following properties: biocompatible, bioabsorbable, bioresorbable, biodurable, biodegradable, compressible, fluid absorbable, swellable, self-expandable, bioactive, medicinal, pharmaceutically active, anti-adhesion, haemostatic, antibiotic, anti-microbial, anti-viral, nutritional, adhesive, permeable, hydrophilic and/or hydrophobic, for example. In various embodiments, a surgical instrument comprising an anvil and a staple cartridge may comprise a tissue thickness compensator associated with the anvil and/or staple cartridge comprising at least one of a haemostatic agent, such as fibrin and thrombin, an antibiotic, such as doxycycline, and medication, such as matrix metalloproteinases (MMPs).

In various embodiments, the tissue thickness compensator may comprise synthetic and/or non-synthetic materials. The tissue thickness compensator may comprise a polymeric composition comprising one or more synthetic polymers and/or one or more non-synthetic polymers. The synthetic polymer may comprise a synthetic absorbable polymer and/or a synthetic non-absorbable polymer. In various embodiments, the polymeric composition may comprise a biocompatible foam, for example. The biocompatible foam may comprise a porous, open cell foam and/or a porous, closed cell foam, for example. The biocompatible foam may have a uniform pore morphology or may have a gradient pore morphology (i.e. small pores gradually increasing in size to large pores across the thickness of the foam in one direction). In various embodiments, the polymeric composition may comprise one or more of a porous scaffold, a porous matrix, a gel matrix, a hydrogel matrix, a solution matrix, a filamentous matrix, a tubular matrix, a composite matrix, a membranous matrix, a biostable polymer, and a biodegradable polymer, and combinations thereof. For example, the tissue thickness compensator may comprise a foam reinforced by a filamentous matrix or may comprise a foam having an additional hydrogel layer that expands in the presence of bodily fluids to further provide the compression on the tissue. In various embodiments, a tissue thickness compensator could also be comprised of a coating

on a material and/or a second or third layer that expands in the presence of bodily fluids to further provide the compression on the tissue. Such a layer could be a hydrogel that could be either biodurable and/or biodegradable, for example. In various embodiments, the tissue thickness compensator may comprise a microgel or a nanogel. The hydrogel may comprise carbohydrate-derived microgels and/or nanogels. In certain embodiments, a tissue thickness compensator may be reinforced with fibrous non-woven materials or fibrous mesh type elements, for example, that can provide additional flexibility, stiffness, and/or strength. In various embodiments, a tissue thickness compensator that has a porous morphology which exhibits a gradient structure such as, for example, small pores on one surface and larger pores on the other surface. Such morphology could be more optimal for tissue in-growth or haemostatic behavior. Further, the gradient could be also compositional with a varying bio-absorption profile. A short term absorption profile may be preferred to address hemostasis while a long term absorption profile may address better tissue healing without leakages.

Examples of non-synthetic materials include, but are not limited to, lyophilized polysaccharide, glycoprotein, bovine pericardium, collagen, gelatin, fibrin, fibrinogen, elastin, proteoglycan, keratin, albumin, hydroxyethyl cellulose, cellulose, oxidized cellulose, oxidized regenerated cellulose (ORC), hydroxypropyl cellulose, carboxyethyl cellulose, carboxymethylcellulose, chitan, chitosan, casein, alginate, and combinations thereof.

Examples of synthetic absorbable materials include, but are not limited to, poly(lactic acid) (PLA), poly(L-lactic acid) (PLLA), polycaprolactone (PCL), polyglycolic acid (PGA), poly(trimethylene carbonate) (TMC), polyethylene terephthalate (PET), polyhydroxyalkanoate (PHA), a copolymer of glycolide and ϵ -caprolactone (PGCL), a copolymer of glycolide and -trimethylene carbonate, poly(glycerol sebacate) (PGS), poly(dioxanone) (PDS), polyesters, poly(orthoesters), polyoxaesters, polyetheresters, polycarbonates, polyamide esters, polyanhydrides, polysaccharides, poly(esteramides), tyrosine-based polyarylates, polyamines, tyrosine-based polyiminocarbonates, tyrosine-based polycarbonates, poly(D,L-lactide-urethane), poly(hydroxybutyrate), poly(B-hydroxybutyrate), poly(ϵ -caprolactone), polyethyleneglycol (PEG), poly[bis(carboxylatophenoxy)phosphazene]poly(amino acids), pseudo-poly(amino acids), absorbable polyurethanes, poly(phosphazene), polyphosphazenes, polyalkyleneoxides, polyacrylamides, polyhydroxyethylmethacrylate, polyvinylpyrrolidone, polyvinyl alcohols, poly(caprolactone), polyacrylic acid, polyacetate, polypropylene, aliphatic polyesters, glycerols, copoly(ether-esters), polyalkylene oxalates, polyamides, poly(iminocarbonates), polyalkylene oxalates, and combinations thereof. In various embodiments, the polyester is may be selected from the group consisting of polylactides, polyglycolides, trimethylene carbonates, polydioxanones, polycaprolactones, polybutesters, and combinations thereof.

In various embodiments, the synthetic absorbable polymer may comprise one or more of 90/10 poly(glycolide-L-lactide) copolymer, commercially available from Ethicon, Inc. under the trade designation VICRYL (polyglactin 910), polyglycolide, commercially available from American Cyanamid Co. under the trade designation DEXON, polydioxanone, commercially available from Ethicon, Inc. under the trade designation PDS, poly(glycolide-trimethylene carbonate) random block copolymer, commercially available from American Cyanamid Co. under the trade designation MAXON, 75/25 poly(glycolide- ϵ -caprolactone-poligleca-

prolactone 25) copolymer, commercially available from Ethicon under the trade designation MONOCRYL, for example.

Examples of synthetic non-absorbable materials include, but are not limited to, polyurethane, polypropylene (PP), polyethylene (PE), polycarbonate, polyamides, such as nylon, polyvinylchloride (PVC), polymethylmethacrylate (PMMA), polystyrene (PS), polyester, polyetheretherketone (PEEK), polytetrafluoroethylene (PTFE), polytrifluorochloroethylene (PTFCE), polyvinylfluoride (PVF), fluorinated ethylene propylene (FEP), polyacetal, polysulfone, silicones, and combinations thereof. The synthetic non-absorbable polymers may include, but are not limited to, foamed elastomers and porous elastomers, such as, for example, silicone, polyisoprene, and rubber. In various embodiments, the synthetic polymers may comprise expanded polytetrafluoroethylene (ePTFE), commercially available from W. L. Gore & Associates, Inc. under the trade designation GORE-TEX Soft Tissue Patch and co-polyetherester urethane foam commercially available from Polyganics under the trade designation NASOPORE.

In various embodiments, the polymeric composition may comprise from approximately 50% to approximately 90% by weight of the polymeric composition of PLLA and approximately 50% to approximately 10% by weight of the polymeric composition of PCL, for example. In at least one embodiment, the polymeric composition may comprise approximately 70% by weight of PLLA and approximately 30% by weight of PCL, for example. In various embodiments, the polymeric composition may comprise from approximately 55% to approximately 85% by weight of the polymeric composition of PGA and 15% to 45% by weight of the polymeric composition of PCL, for example. In at least one embodiment, the polymeric composition may comprise approximately 65% by weight of PGA and approximately 35% by weight of PCL, for example. In various embodiments, the polymeric composition may comprise from approximately 90% to approximately 95% by weight of the polymeric composition of PGA and approximately 5% to approximately 10% by weight of the polymeric composition of PLA, for example.

In various embodiments, the synthetic absorbable polymer may comprise a bioabsorbable, biocompatible elastomeric copolymer. Suitable bioabsorbable, biocompatible elastomeric copolymers include but are not limited to copolymers of ϵ -caprolactone and glycolide (preferably having a mole ratio of ϵ -caprolactone to glycolide of from about 30:70 to about 70:30, preferably 35:65 to about 65:35, and more preferably 45:55 to 35:65); elastomeric copolymers of ϵ -caprolactone and lactide, including L-lactide, D-lactide blends thereof or lactic acid copolymers (preferably having a mole ratio of ϵ -caprolactone to lactide of from about 35:65 to about 65:35 and more preferably 45:55 to 30:70); elastomeric copolymers of p-dioxanone (1,4-dioxan-2-one) and lactide including L-lactide, D-lactide and lactic acid (preferably having a mole ratio of p-dioxanone to lactide of from about 40:60 to about 60:40); elastomeric copolymers of ϵ -caprolactone and p-dioxanone (preferably having a mole ratio of ϵ -caprolactone to p-dioxanone of from about 30:70 to about 70:30); elastomeric copolymers of p-dioxanone and trimethylene carbonate (preferably having a mole ratio of p-dioxanone to trimethylene carbonate of from about 30:70 to about 70:30); elastomeric copolymers of trimethylene carbonate and glycolide (preferably having a mole ratio of trimethylene carbonate to glycolide of from about 30:70 to about 70:30); elastomeric copolymer of trimethylene carbonate and lactide including L-lactide, D-lactide, blends thereof or lactic acid copolymers (preferably having a mole ratio of trimethylene

carbonate to lactide of from about 30:70 to about 70:30) and blends thereof. In one embodiment, the elastomeric copolymer is a copolymer of glycolide and ϵ -caprolactone. In another embodiment, the elastomeric copolymer is a copolymer of lactide and ϵ -caprolactone.

The disclosures of U.S. Pat. No. 5,468,253, entitled ELASTOMERIC MEDICAL DEVICE, which issued on Nov. 21, 1995, and U.S. Pat. No. 6,325,810, entitled FOAM BUTTRESS FOR STAPLING APPARATUS, which issued on Dec. 4, 2001, are hereby incorporated by reference in their respective entireties.

In various embodiments, the tissue thickness compensator may comprise an emulsifier. Examples of emulsifiers may include, but are not limited to, water-soluble polymers, such as, polyvinyl alcohol (PVA), polyvinyl pyrrolidone (PVP), polyethylene glycol (PEG), polypropylene glycol (PPG), PLURONICS, TWEENS, polysaccharides and combinations thereof.

In various embodiments, the tissue thickness compensator may comprise a surfactant. Examples of surfactants may include, but are not limited to, polyacrylic acid, methalose, methyl cellulose, ethyl cellulose, propyl cellulose, hydroxy ethyl cellulose, carboxy methyl cellulose, polyoxyethylene cetyl ether, polyoxyethylene lauryl ether, polyoxyethylene octyl ether, polyoxyethylene octylphenyl ether, polyoxyethylene oleyl ether, polyoxyethylene sorbitan monolaurate, polyoxyethylene stearyl ether, polyoxyethylene nonylphenyl ether, dialkylphenoxy poly(ethyleneoxy)ethanol, and polyoxamers.

In various embodiments, the polymeric composition may comprise a pharmaceutically active agent. The polymeric composition may release a therapeutically effective amount of the pharmaceutically active agent. In various embodiments, the pharmaceutically active agent may be released as the polymeric composition is desorbed/absorbed. In various embodiments, the pharmaceutically active agent may be released into fluid, such as, for example, blood, passing over or through the polymeric composition. Examples of pharmaceutically active agents may include, but are not limited to, haemostatic agents and drugs, such as, for example, fibrin, thrombin, and oxidized regenerated cellulose (ORC); anti-inflammatory drugs, such as, for example, diclofenac, aspirin, naproxen, sulindac, and hydrocortisone; antibiotic and antimicrobial drug or agents, such as, for example, triclosan, ionic silver, ampicillin, gentamicin, polymyxin B, chloramphenicol; and anticancer agents, such as, for example, cisplatin, mitomycin, adriamycin.

In various embodiments, the polymeric composition may comprise a haemostatic material. The tissue thickness compensator may comprise haemostatic materials comprising poly(lactic acid), poly(glycolic acid), poly(hydroxybutyrate), poly(caprolactone), poly(dioxanone), polyalkyleneoxides, copoly(ether-esters), collagen, gelatin, thrombin, fibrin, fibrinogen, fibronectin, elastin, albumin, hemoglobin, ovalbumin, polysaccharides, hyaluronic acid, chondroitin sulfate, hydroxyethyl starch, hydroxyethyl cellulose, cellulose, oxidized cellulose, hydroxypropyl cellulose, carboxyethyl cellulose, carboxymethyl cellulose, chitan, chitosan, agarose, maltose, maltodextrin, alginate, clotting factors, methacrylate, polyurethanes, cyanoacrylates, platelet agonists, vasoconstrictors, alum, calcium, RGD peptides, proteins, protamine sulfate, ϵ -amino caproic acid, ferric sulfate, ferric subsulfates, ferric chloride, zinc, zinc chloride, aluminum chloride, aluminum sulfates, aluminum acetates, permanganates, tannins, bone wax, polyethylene glycols, fucans and combinations thereof. The tissue thickness compensator may be characterized by haemostatic properties.

The polymeric composition of a tissue thickness compensator may be characterized by percent porosity, pore size, and/or hardness, for example. In various embodiments, the polymeric composition may have a percent porosity from approximately 30% by volume to approximately 99% by volume, for example. In certain embodiments, the polymeric composition may have a percent porosity from approximately 60% by volume to approximately 98% by volume, for example. In various embodiments, the polymeric composition may have a percent porosity from approximately 85% by volume to approximately 97% by volume, for example. In at least one embodiment, the polymeric composition may comprise approximately 70% by weight of PLLA and approximately 30% by weight of PCL, for example, and can comprise approximately 90% porosity by volume, for example. In at least one such embodiment, as a result, the polymeric composition would comprise approximately 10% copolymer by volume. In at least one embodiment, the polymeric composition may comprise approximately 65% by weight of PGA and approximately 35% by weight of PCL, for example, and can have a percent porosity from approximately 93% by volume to approximately 95% by volume, for example. In various embodiments, the polymeric composition may comprise greater than 85% porosity by volume. The polymeric composition may have a pore size from approximately 5 micrometers to approximately 2000 micrometers, for example. In various embodiments, the polymeric composition may have a pore size between approximately 10 micrometers to approximately 100 micrometers, for example. In at least one such embodiment, the polymeric composition can comprise a copolymer of PGA and PCL, for example. In certain embodiments, the polymeric composition may have a pore size between approximately 100 micrometers to approximately 1000 micrometers, for example. In at least one such embodiment, the polymeric composition can comprise a copolymer of PLLA and PCL, for example.

According to certain aspects, the hardness of a polymeric composition may be expressed in terms of the Shore Hardness, which can be defined as the resistance to permanent indentation of a material as determined with a durometer, such as a Shore Durometer. In order to assess the durometer value for a given material, a pressure is applied to the material with a durometer indenter foot in accordance with ASTM procedure D2240-00, entitled, "Standard Test Method for Rubber Property-Durometer Hardness", the entirety of which is incorporated herein by reference. The durometer indenter foot may be applied to the material for a sufficient period of time, such as 15 seconds, for example, wherein a reading is then taken from the appropriate scale. Depending on the type of scale being used, a reading of 0 can be obtained when the indenter foot completely penetrates the material, and a reading of 100 can be obtained when no penetration into the material occurs. This reading is dimensionless. In various embodiments, the durometer may be determined in accordance with any suitable scale, such as Type A and/or Type OO scales, for example, in accordance with ASTM D2240-00. In various embodiments, the polymeric composition of a tissue thickness compensator may have a Shore A hardness value from approximately 4A to approximately 16A, for example, which is approximately 45 OO to approximately 65 OO on the Shore OO range. In at least one such embodiment, the polymeric composition can comprise a PLLA/PCL copolymer or a PGA/PCL copolymer, for example. In various embodiments, the polymeric composition of a tissue thickness compensator may have a Shore A Hardness value of less than 15 A. In various embodiments, the polymeric composition of a tissue thickness compensator may have a Shore A Hardness value of

less than 10 A. In various embodiments, the polymeric composition of a tissue thickness compensator may have a Shore A Hardness value of less than 5 A. In certain embodiments, the polymeric material may have a Shore OO composition value from approximately 35 OO to approximately 75 OO, for example.

In various embodiments, the polymeric composition may have at least two of the above-identified properties. In various embodiments, the polymeric composition may have at least three of the above-identified properties. The polymeric composition may have a porosity from 85% to 97% by volume, a pore size from 5 micrometers to 2000 micrometers, and a Shore A hardness value from 4 A to 16 A and Shore OO hardness value from 45 OO to 65 OO, for example. In at least one embodiment, the polymeric composition may comprise 70% by weight of the polymeric composition of PLLA and 30% by weight of the polymeric composition of PCL having a porosity of 90% by volume, a pore size from 100 micrometers to 1000 micrometers, and a Shore A hardness value from 4 A to 16 A and Shore OO hardness value from 45 OO to 65 OO, for example. In at least one embodiment, the polymeric composition may comprise 65% by weight of the polymeric composition of PGA and 35% by weight of the polymeric composition of PCL having a porosity from 93% to 95% by volume, a pore size from 10 micrometers to 100 micrometers, and a Shore A hardness value from 4 A to 16 A and Shore OO hardness value from 45 OO to 65 OO, for example.

In various embodiments, the tissue thickness compensator may comprise a material that expands. As discussed above, the tissue thickness compensator may comprise a compressed material that expands when uncompressed or deployed, for example. In various embodiments, the tissue thickness compensator may comprise a self-expanding material formed in situ. In various embodiments, the tissue thickness compensator may comprise at least one precursor selected to spontaneously crosslink when contacted with at least one of other precursor(s), water, and/or bodily fluids. Referring to FIG. 205, in various embodiments, a first precursor may contact one or more other precursors to form an expandable and/or swellable tissue thickness compensator. In various embodiments, the tissue thickness compensator may comprise a fluid-swellable composition, such as a water-swellable composition, for example. In various embodiments, the tissue thickness compensator may comprise a gel comprising water.

Referring to FIGS. 189A and B, for example, a tissue thickness compensator 70000 may comprise at least one hydrogel precursor 70010 selected to form a hydrogel in situ and/or in vivo to expand the tissue thickness compensator 70000. FIG. 189A illustrates a tissue thickness compensator 70000 comprising an encapsulation comprising a first hydrogel precursor 70010A and a second hydrogel precursor 70010B prior to expansion. In certain embodiments, as shown in FIG. 189A, the first hydrogel precursor 70010A and second hydrogel precursor 70010B may be physically separated from other in the same encapsulation. In certain embodiments, a first encapsulation may comprise the first hydrogel precursor 70010A and a second encapsulation may comprise the second hydrogel precursor 70010B. FIG. 189B illustrates the expansion of the thickness tissue compensator 70000 when the hydrogel is formed in situ and/or in vivo. As shown in FIG. 189B, the encapsulation may be ruptured, and the first hydrogel precursor 70010A may contact the second hydrogel precursor 70010B to form the hydrogel 70020. In certain embodiments, the hydrogel may comprise an expandable material. In certain embodiments, the hydrogel may expand up to 72 hours, for example.

In various embodiments, the tissue thickness compensator may comprise a biodegradable foam having an encapsulation comprising dry hydrogel particles or granules embedded therein. Without wishing to be bound to any particular theory, the encapsulations in the foam may be formed by contacting an aqueous solution of a hydrogel precursor and an organic solution of biocompatible materials to form the foam. As shown in FIG. 206, the aqueous solution and organic solution may form micelles. The aqueous solution and organic solution may be dried to encapsulate dry hydrogel particles or granules within the foam. For example, a hydrogel precursor, such as a hydrophilic polymer, may be dissolved in water to form a dispersion of micelles. The aqueous solution may contact an organic solution of dioxane comprising poly(glycolic acid) and polycaprolactone. The aqueous and organic solutions may be lyophilized to form a biodegradable foam having dry hydrogel particles or granules dispersed therein. Without wishing to be bound to any particular theory, it is believed that the micelles form the encapsulation having the dry hydrogel particles or granules dispersed within the foam structure. In certain embodiments, the encapsulation may be ruptured, and the dry hydrogel particles or granules may contact a fluid, such as a bodily fluid, and expand.

In various embodiments, the tissue thickness compensator may expand when contacted with an activator, such as a fluid, for example. Referring to FIG. 190, for example, a tissue thickness compensator 70050 may comprise a swellable material, such as a hydrogel, that expands when contacted with a fluid 70055, such as bodily fluids, saline, water and/or an activator, for example. Examples of bodily fluids may include, but are not limited to, blood, plasma, peritoneal fluid, cerebral spinal fluid, urine, lymph fluid, synovial fluid, vitreous fluid, saliva, gastrointestinal luminal contents, bile, and/or gas (e.g., CO₂). In certain embodiments, the tissue thickness compensator 70050 may expand when the tissue thickness compensator 70050 absorbs the fluid. In another example, the tissue thickness compensator 70050 may comprise a non-crosslinked hydrogel that expands when contacted with an activator 70055 comprising a cross-linking agent to form a crosslinked hydrogel. In various embodiments, the tissue thickness compensator may expand when contacted with an activator. In various embodiments, the tissue thickness compensator may expand or swell from contact up to 72 hours, such as from 24-72 hours, up to 24 hours, up to 48 hours, and up to 72 hours, for example, to provide continuously increasing pressure and/or compression to the tissue. As shown in FIG. 190, the initial thickness of the tissue thickness compensator 70050 may be less than an expanded thickness after the fluid 70055 contacts the tissue thickness compensator 70050.

Referring to FIGS. 187 and 188, in various embodiments, a staple cartridge 70100 may comprise a tissue thickness compensator 70105 and a plurality of staples 70110 each comprising staple legs 70112. As shown in FIG. 187, tissue thickness compensator 70105 may have an initial thickness or compressed height that is less than the fired height of the staples 70110. The tissue thickness compensator 70100 may be configured to expand in situ and/or in vivo when contacted with a fluid 70102, such as bodily fluids, saline, and/or an activator for example, to push the tissue T against the legs 70112 of the staple 70110. As shown in FIG. 188, the tissue thickness compensator 70100 may expand and/or swell when contacted with a fluid 70102. The tissue thickness compensator 70105 can compensate for the thickness of the tissue T captured within each staple 70110. As shown in FIG. 188,

tissue thickness compensator 70105 may have an expanded thickness or an uncompressed height that is less than the fired height of the staples 70110.

In various embodiments, as described above, the tissue thickness compensator may comprise an initial thickness and an expanded thickness. In certain embodiments, the initial thickness of a tissue thickness compensator can be approximately 0.001% of its expanded thickness, approximately 0.01% of its expanded thickness, approximately 0.1% of its expanded thickness, approximately 1% of its expanded thickness, approximately 10% of its expanded thickness, approximately 20% of its expanded thickness, approximately 30% of its expanded thickness, approximately 40% of its expanded thickness, approximately 50% of its expanded thickness, approximately 60% of its expanded thickness, approximately 70% of its expanded thickness, approximately 80% of its expanded thickness, and/or approximately 90% of its expanded thickness, for example. In various embodiments, the expanded thickness of the tissue thickness compensator can be approximately two times, approximately five times, approximately ten times, approximately fifty times, approximately one hundred times, approximately two hundred times, approximately three hundred times, approximately four hundred times, approximately five hundred times, approximately six hundred times, approximately seven hundred times, approximately eight hundred times, approximately nine hundred times, and/or approximately one thousand times thicker than its initial thickness, for example. In various embodiments, the initial thickness of the tissue thickness compensator can be up to 1% its expanded thickness, up to 5% its expanded thickness, up to 10% its expanded thickness, and up to 50% its expanded thickness. In various embodiments, the expanded thickness of the tissue thickness compensator can be at least 50% thicker than its initial thickness, at least 100% thicker than its initial thickness, at least 300% thicker than its initial thickness, and at least 500% thicker than its initial thickness. As described above, in various circumstances, as a result of the above, the tissue thickness compensator can be configured to consume any gaps within the staple entrapment area.

As discussed above, in various embodiments, the tissue thickness compensator may comprise a hydrogel. In various embodiments, the hydrogel may comprise homopolymer hydrogels, copolymer hydrogels, multipolymer hydrogels, interpenetrating polymer hydrogels, and combinations thereof. In various embodiments, the hydrogel may comprise microgels, nanogels, and combinations thereof. The hydrogel may generally comprise a hydrophilic polymer network capable of absorbing and/or retaining fluids. In various embodiments, the hydrogel may comprise a non-crosslinked hydrogel, a crosslinked hydrogel, and combinations thereof. The hydrogel may comprise chemical crosslinks, physical crosslinks, hydrophobic segments and/or water insoluble segments. The hydrogel may be chemically crosslinked by polymerization, small-molecule crosslinking, and/or polymer-polymer crosslinking. The hydrogel may be physically crosslinked by ionic interactions, hydrophobic interactions, hydrogen bonding interactions, stereocomplexation, and/or supramolecular chemistry. The hydrogel may be substantially insoluble due to the crosslinks, hydrophobic segments and/or water insoluble segments, but be expandable and/or swellable due to absorbing and/or retaining fluids. In certain embodiments, the precursor may crosslink with endogenous materials and/or tissues.

In various embodiments, the hydrogel may comprise an environmentally sensitive hydrogel (ESH). The ESH may comprise materials having fluid-swelling properties that

relate to environmental conditions. The environmental conditions may include, but are not limited to, the physical conditions, biological conditions, and/or chemical conditions at the surgical site. In various embodiments, the hydrogel may swell or shrink in response to temperature, pH, electric fields, ionic strength, enzymatic and/or chemical reactions, electrical and/or magnetic stimuli, and other physiological and environmental variables, for example. In various embodiments, the ESH may comprise multifunctional acrylates, hydroxyethylmethacrylate (HEMA), elastomeric acrylates, and related monomers.

In various embodiments, the tissue thickness compensator comprising a hydrogel may comprise at least one of the non-synthetic materials and synthetic materials described above. The hydrogel may comprise a synthetic hydrogel and/or a non-synthetic hydrogel. In various embodiments, the tissue thickness compensator may comprise a plurality of layers. The plurality of the layers may comprise porous layers and/or non-porous layers. For example, the tissue thickness compensator may comprise a non-porous layer and a porous layer. In another example, the tissue thickness compensator may comprise a porous layer intermediate a first non-porous layer and a second non-porous layer. In another example, the tissue thickness compensator may comprise a non-porous layer intermediate a first porous layer and a second porous layer. The non-porous layers and porous layers may be positioned in any order relative to the surfaces of the staple cartridge and/or anvil.

Examples of the non-synthetic material may include, but are not limited to, albumin, alginate, carbohydrate, casein, cellulose, chitin, chitosan, collagen, blood, dextran, elastin, fibrin, fibrinogen, gelatin, heparin, hyaluronic acid, keratin, protein, serum, and starch. The cellulose may comprise hydroxyethyl cellulose, oxidized cellulose, oxidized regenerated cellulose (ORC), hydroxypropyl cellulose, carboxyethyl cellulose, carboxymethylcellulose, and combinations thereof. The collagen may comprise bovine pericardium. The carbohydrate may comprise a polysaccharide, such as lyophilized polysaccharide. The protein may comprise glycoprotein, proteoglycan, and combinations thereof.

Examples of the synthetic material may include, but are not limited to, poly(lactic acid), poly(glycolic acid), poly(hydroxybutyrate), poly(phosphazene), polyesters, polyethylene glycols, polyethylene oxide, polyethylene oxide-co-polypropylene oxide, co-polyethylene oxide, polyalkyleneoxides, polyacrylamides, polyhydroxyethylmethacrylate, poly(vinylpyrrolidone), polyvinyl alcohols, poly(caprolactone), poly(dioxanone), polyacrylic acid, polyacetate, polypropylene, aliphatic polyesters, glycerols, poly(amino acids), copoly(ether-esters), polyalkylene oxalates, polyamides, poly(iminocarbonates), polyoxaesters, polyorthoesters, polyphosphazenes and combinations thereof. In certain embodiments, the above non-synthetic materials may be synthetically prepared, e.g., synthetic hyaluronic acid, utilizing conventional methods.

In various embodiments, the hydrogel may be made from one or more hydrogel precursors. The precursor may comprise a monomer and/or a macromer. The hydrogel precursor may comprise an electrophile functional group and/or a nucleophile electrophile functional group. In general, electrophiles may react with nucleophiles to form a bond. The term "functional group" as used herein refers to electrophilic or nucleophilic groups capable of reacting with each other to form a bond. Examples of electrophilic functional groups may include, but are not limited to, N-hydroxysuccinimides ("NHS"), sulfosuccinimides, carbonyldiimidazole, sulfonyl chloride, aryl halides, sulfosuccinimidyl esters, N-hydrox-

ysuccinimidyl esters, succinimidyl esters such as succinimidyl succinates and/or succinimidyl propionates, isocyanates, thiocyanates, carbodiimides, benzotriazole carbonates, epoxides, aldehydes, maleimides, imidoesters, combinations thereof, and the like. In at least one embodiment, the electrophilic functional group may comprise a succinimidyl ester. Examples of nucleophile functional groups may include, but are not limited to, —NH_2 , —SH , —OH , —PH_2 , and —CO—NH—NH_2 .

In various embodiments, the hydrogel may be formed from a single precursor or multiple precursors. In certain embodiments, the hydrogel may be formed from a first precursor and a second precursor. The first hydrogel precursor and second hydrogel precursor may form a hydrogel in situ and/or in vivo upon contact. The hydrogel precursor may generally refer to a polymer, functional group, macromolecule, small molecule, and/or crosslinker that can take part in a reaction to form a hydrogel. The precursor may comprise a homogeneous solution, heterogeneous, or phase separated solution in a suitable solvent, such as water or a buffer, for example. The buffer may have a pH from about 8 to about 12, such as, about 8.2 to about 9, for example. Examples of buffers may include, but are not limited to borate buffers. In certain embodiments, the precursor(s) may be in an emulsion. In various embodiments, a first precursor may react with a second precursor to form a hydrogel. In various embodiments, the first precursor may spontaneously crosslink when contacted with the second precursor. In various embodiments, a first set of electrophilic functional groups on a first precursor may react with a second set of nucleophilic functional groups on a second precursor. When the precursors are mixed in an environment that permits reaction (e.g., as relating to pH, temperature, and/or solvent), the functional groups may react with each other to form covalent bonds. The precursors may become crosslinked when at least some of the precursors react with more than one other precursor.

In various embodiments, the tissue thickness compensator may comprise at least one monomer selected from the group consisting of 3-sulfopropyl acrylate potassium salt ("KSPA"), sodium acrylate ("NaA"), N-(tris(hydroxymethyl)methyl)acrylamide ("tris acryl"), and 2-acrylamido-2-methyl-1-propane sulfonic acid (AMPS). The tissue thickness compensator may comprise a copolymer comprising two or more monomers selected from the group consisting of KSPA, NaA, tris acryl, AMPS. The tissue thickness compensator may comprise homopolymers derived from KSPA, NaA, trisacryl and AMPS. The tissue thickness compensator may comprise hydrophilicity modifying monomers copolymerizable therewith. The hydrophilicity modifying monomers may comprise methylmethacrylate, butylacrylate, cyclohexylacrylate, styrene, styrene sulphonic acid.

In various embodiments, the tissue thickness compensator may comprise a crosslinker. The crosslinker may comprise a low molecular weight di- or polyvinyl crosslinking agent, such as ethyleneglycol diacrylate or dimethacrylate, di-, tri- or tetraethyleneglycol diacrylate or dimethacrylate, allyl (meth)acrylate, a $\text{C}_2\text{—C}_8$ -alkylene diacrylate or dimethacrylate, divinyl ether, divinyl sulfone, di- and trivinylbenzene, trimethylolpropane triacrylate or trimethacrylate, pentaerythritol tetraacrylate or tetramethacrylate, bisphenol A diacrylate or dimethacrylate, methylene bisacrylamide or bis-methacrylamide, ethylene bisacrylamide or ethylene bismethacrylamide, triallyl phthalate or diallyl phthalate. In at least one embodiment, the crosslinker may comprise N,N'-methylenebisacrylamide ("MBAA").

In various embodiments, the tissue thickness compensator may comprise at least one of acrylate and/or methacrylate

functional hydrogels, biocompatible photoinitiator, alkyl-cyanoacrylates, isocyanate functional macromers, optionally comprising amine functional macromers, succinimidyl ester functional macromers, optionally comprising amine and/or sulfhydryl functional macromers, epoxy functional macromers, optionally comprising amine functional macromers, mixtures of proteins and/or polypeptides and aldehyde crosslinkers, Genipin, and water-soluble carbodiimides, anionic polysaccharides and polyvalent cations.

In various embodiments, the tissue thickness compensator may comprise unsaturated organic acid monomers, acrylic substituted alcohols, and/or acrylamides. In various embodiments, the tissue thickness compensator may comprise methacrylic acids, acrylic acids, glycerolacrylate, glycerolmethacrylate, 2-hydroxyethylmethacrylate, 2-hydroxyethylacrylate, 2-(dimethylaminoethyl) methacrylate, N-vinyl pyrrolidone, methacrylamide, and/or N,N-dimethylacrylamide poly(methacrylic acid).

In various embodiments, the tissue thickness compensator may comprise a reinforcement material. In various embodiments, the reinforcement material may comprise at least one of the non-synthetic materials and synthetic materials described above. In various embodiments, the reinforcement material may comprise collagen, gelatin, fibrin, fibrinogen, elastin, keratin, albumin, hydroxyethyl cellulose, cellulose, oxidized cellulose, hydroxypropyl cellulose, carboxyethyl cellulose, carboxymethylcellulose, chitan, chitosan, alginate, poly(lactic acid), poly(glycolic acid), poly(hydroxybutyrate), poly(phosphazene), polyesters, polyethylene glycols, polyalkyleneoxides, polyacrylamides, polyhydroxyethylmethacrylate, polyvinylpyrrolidone, polyvinyl alcohols, poly(ε-caprolactone), poly(dioxanone), polyacrylic acid, polyacetate, polycaprolactone, polypropylene, aliphatic polyesters, glycerols, poly(amino acids), copoly(ether-esters), polyalkylene oxalates, polyamides, poly(iminocarbonates), polyalkylene oxalates, polyoxaesters, polyorthoesters, polyphosphazenes and combinations thereof.

In various embodiments, the tissue thickness compensator may comprise a layer comprising the reinforcement material. In certain embodiments, a porous layer and/or a non-porous layer of a tissue thickness compensator may comprise the reinforcement material. For example, the porous layer may comprise the reinforcement material and the non-porous layer may not comprise the reinforcement material. In various embodiments, the reinforcement layer may comprise an inner layer intermediate a first non-porous layer and a second non-porous layer. In certain embodiments, the reinforcement layer may comprise an outer layer of the tissue thickness compensator. In certain embodiments, the reinforcement layer may comprise an exterior surface of the tissue thickness compensator.

In various embodiments, the reinforcement material may comprise meshes, monofilaments, multifilament braids, fibers, mats, felts, particles, and/or powders. In certain embodiments, the reinforcement material may be incorporated into a layer of the tissue thickness compensator. The reinforcement material may be incorporated into at least one of a non-porous layer and a porous layer. A mesh comprising the reinforcement material may be formed using conventional techniques, such as, for example, knitting, weaving, tatting, and/or knipling. In various embodiments, a plurality of reinforcement materials may be oriented in a random direction and/or a common direction. In certain embodiments, the common direction may be one of parallel to the staple line and perpendicular to the staple line, for example. For example, the monofilaments and/or multifilament braids may be oriented in a random direction and/or a common direction. The

monofilaments and multifilament braids may be associated with the non-porous layer and/or the porous layer. In various embodiments, the tissue thickness compensator may comprise a plurality of reinforcement fibers oriented in a random direction within a non-porous layer. In various embodiments, the tissue thickness compensator may comprise a plurality of reinforcement fibers oriented in a common direction within a non-porous layer.

In various embodiments, referring to FIG. 199, an anvil 70300 may comprise a tissue thickness compensator 70305 comprising a first non-porous layer 70307 and a second non-porous layer 70309 sealingly enclosing a reinforcement layer 70310. In various embodiments, the reinforcement layer 70310 may comprise a hydrogel comprising ORC particles or fibers embedded therein, and the non-porous layers may comprise ORC. As shown in FIG. 199, the tissue thickness compensator 70305 may be configured to conform to the contour of the anvil 70300. The inner layer of the tissue thickness compensator 70305 may conform to the inner surface of the anvil 70300, which includes the forming pockets 70301.

The fibers may form a non-woven material, such as, for example, a mat and a felt. The fibers may have any suitable length, such as, for example from 0.1 mm to 100 mm and 0.4 mm to 50 mm. The reinforcement material may be ground to a powder. The powder may have a particle size from 10 micrometers to 1 cm, for example. The powder may be incorporated into the tissue thickness compensator.

In various embodiments, the tissue thickness compensator may be formed in situ. In various embodiments, the hydrogel may be formed in situ. The tissue thickness compensator may be formed in situ by covalent, ionic, and/or hydrophobic bonds. Physical (non-covalent) crosslinks may result from complexation, hydrogen bonding, desolvation, Van der Waals interactions, ionic bonding, and combinations thereof. Chemical (covalent) crosslinking may be accomplished by any of a number of mechanisms, including: free radical polymerization, condensation polymerization, anionic or cationic polymerization, step growth polymerization, electrophile-nucleophile reactions, and combinations thereof.

In various embodiments, in situ formation of the tissue thickness compensator may comprise reacting two or more precursors that are physically separated until contacted in situ and/or react to an environmental condition to react with each other to form the hydrogel. In situ polymerizable polymers may be prepared from precursor(s) that can be reacted to form a polymer at the surgical site. The tissue thickness compensator may be formed by crosslinking reactions of the precursor(s) in situ. In certain embodiments, the precursor may comprise an initiator capable of initiating a polymerization reaction for the formation of the in situ tissue thickness compensator. The tissue thickness compensator may comprise a precursor that can be activated at the time of application to create, in various embodiments, a crosslinked hydrogel. In situ formation of the tissue thickness compensator may comprise activating at least one precursor to form bonds to form the tissue thickness compensator. In various embodiments, activation may be achieved by changes in the physical conditions, biological conditions, and/or chemical conditions at the surgical site, including, but not limited to temperature, pH, electric fields, ionic strength, enzymatic and/or chemical reactions, electrical and/or magnetic stimuli, and other physiological and environmental variables. In various embodiments, the precursors may be contacted outside the body and introduced to the surgical site.

In various embodiments, the tissue thickness compensator may comprise one or more encapsulations, or cells, which can be configured to store at least one component therein. In

certain embodiments, the encapsulation may be configured to store a hydrogel precursor therein. In certain embodiments, the encapsulation may be configured to store two components therein, for example. In certain embodiments, the encapsulation may be configured to store a first hydrogel precursor and a second hydrogel precursor therein. In certain embodiments, a first encapsulation may be configured to store a first hydrogel precursor therein and a second encapsulation may be configured to store a second hydrogel precursor therein. As described above, the encapsulations can be aligned, or at least substantially aligned, with the staple legs to puncture and/or otherwise rupture the encapsulations when the staple legs contact the encapsulation. In certain embodiments, the encapsulations may be compressed, crushed, collapsed, and/or otherwise ruptured when the staples are deployed. After the encapsulations have been ruptured, the component(s) stored therein can flow out of the encapsulation. The component stored therein may contact other components, layers of the tissue thickness compensator, and/or the tissue. In various embodiments, the other components may be flowing from the same or different encapsulations, provided in the layers of the tissue thickness compensator, and/or provided to the surgical site by the clinician. As a result of the above, the component(s) stored within the encapsulations can provide expansion and/or swelling of the tissue thickness compensator.

In various embodiments, the tissue thickness compensator may comprise a layer comprising the encapsulations. In various embodiments, the encapsulation may comprise a void, a pocket, a dome, a tube, and combinations thereof associated with the layer. In certain embodiments, the encapsulations may comprise voids in the layer. In at least one embodiment, the layer can comprise two layers that can be attached to one another wherein the encapsulations can be defined between the two layers. In certain embodiments, the encapsulations may comprise domes on the surface of the layer. For example, at least a portion of the encapsulations can be positioned within domes extending upwardly from the layer. In certain embodiments, the encapsulations may comprise pockets formed within the layer. In certain embodiments, a first portion of the encapsulations may comprise a dome and a second portion of the encapsulations may comprise a pocket. In certain embodiments, the encapsulations may comprise a tube embedded within the layer. In certain embodiments, the tube may comprise the non-synthetic materials and/or synthetic materials described herein, such as PLA. In at least one embodiment, the tissue thickness compensator may comprise a bioabsorbable foam, such as ORC, comprising PLA tubes embedded therein, and the tube may encapsulate a hydrogel, for example. In certain embodiments, the encapsulations may comprise discrete cells that are unconnected to each other. In certain embodiments, one or more of the encapsulations can be in fluid communication with each other via one or more passageways, conduits, and/or channels, for example, extending through the layer.

The rate of release of a component from the encapsulation may be controlled by the thickness of the tissue thickness compensator, the composition of tissue thickness compensator, the size of the component, the hydrophilicity of the component, and/or the physical and/or chemical interactions among the component, the composition of the tissue thickness compensator, and/or the surgical instrument, for example. In various embodiments, the layer can comprise one or more thin sections or weakened portions, such as partial perforations, for example, which can facilitate the incision of the layer and the rupture of the encapsulations. In various embodiments, the partial perforations may not completely

extend through a layer while, in certain embodiments, perforations may completely extend through the layer.

Referring to FIGS. 194 and 195, in various embodiments, a tissue thickness compensator 70150 may comprise an outer layer 70152A and an inner layer 70152B comprising encapsulations 70154. In certain embodiments, the encapsulation may comprise a first encapsulated component and a second encapsulated component. In certain embodiments, the encapsulations may independently comprise one of a first encapsulated component and a second encapsulated component. The first encapsulated component may be separated from the second encapsulated component. The outer layer 70152A may comprise a tissue-contacting surface. The inner layer 70152B may comprise an instrument-contacting surface. The instrument-contacting surface 70152B may be releasably attached to the anvil 70156. The outer layer 70152A may be attached to the inner layer 70152B to define a void between the outer layer 70152A and inner layer 70152B. As shown in FIG. 194, each encapsulation 70154 may comprise a dome on the instrument-contacting surface of the inner layer 70152B. The dome may comprise partial perforations to facilitate the incision of the layer by the staple legs and the rupture of the encapsulation. As shown in the FIG. 195, the anvil 70156 can comprise a plurality of forming pocket rows 70158 wherein the domes of the encapsulations 70154 may be aligned with the forming pocket 70158. The tissue-contacting surface may comprise a flat surface lacking domes. In certain embodiments, the tissue-contacting surface may comprise one or more encapsulations, such as encapsulations 70154, for example, extending therefrom.

In various embodiments, an anvil may comprise a tissue thickness compensator comprising an encapsulated component comprising at least one microsphere particle. In certain embodiments, the tissue thickness compensator may comprise an encapsulation comprising a first encapsulated component and a second encapsulated component. In certain embodiments, the tissue thickness compensator may comprise an encapsulation comprising a first microsphere particle and a second microsphere particle.

In various embodiments, referring to FIG. 196, a stapling apparatus may comprise an anvil 70180 and a staple cartridge (illustrated in other figures). The staples 70190 of a staple cartridge can be deformed by an anvil 70180 when the anvil 70180 is moved into a closed position and/or by a staple driver system 70192 which moves the staples 70190 toward the closed anvil 70180. The legs 70194 of the staples may contact the anvil 70180 such that the staples 70190 are at least partially deformed. The anvil 70180 may comprise a tissue thickness compensator 70182 comprising an outer layer 70183A, an inner layer 70183B. The tissue thickness compensator 70182 may comprise a first encapsulated component and a second encapsulated component. In certain embodiments, the encapsulations 210185 can be aligned, or at least substantially aligned, such that, when the staple legs 70194 are pushed through the tissue T and the outer layer 70183A, the staple legs 70194 can puncture and/or otherwise rupture the encapsulations 70185. As shown in FIG. 196, the staple 70190C is in its fully fired position, the staple 70190B is in the process of being fired, and the staple 70190A is in its unfired position. The legs of staples 70190C and 70190B have moved through the tissue T, the outer layer 70183A, and the inner layer 70183B of the tissue thickness compensator 70182, and have contacted an anvil 70180 positioned opposite the staple cartridge. After the encapsulations 70185 have been ruptured, the encapsulated components can flow out and contact each other, bodily fluids, and/or the tissue T, for example. The encapsulated components may react to form a reaction prod-

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uct such as a hydrogel, for example, to expand between the tissue T and the base of the staple and to push the tissue T against the legs of the staple. In various circumstances, as a result of the above, the tissue thickness compensator can be configured to consume any gaps within the staple entrapment area.

In various embodiments, the tissue thickness compensator may be suitable for use with a surgical instrument. As described above the tissue thickness compensator may be associated with the staple cartridge and/or the anvil. The tissue thickness compensator may be configured into any shape, size and/or dimension suitable to fit the staple cartridge and/or anvil. As described herein, the tissue thickness compensator may be releasably attached to the staple cartridge and/or anvil. The tissue thickness compensator may be attached to the staple cartridge and/or anvil in any mechanical and/or chemical manner capable of retaining the tissue thickness compensator in contact with the staple cartridge and/or anvil prior to and during the stapling process. The tissue thickness compensator may be removed or released from the staple cartridge and/or anvil after the staple penetrates the tissue thickness compensator. The tissue thickness compensator may be removed or released from the staple cartridge and/or anvil as the staple cartridge and/or anvil is moved away from the tissue thickness compensator.

Referring to FIGS. 191-193, stapling apparatus 70118 may comprise an anvil 70120 and a staple cartridge 70122 comprising a firing member 70124, a plurality of staples 70128, a knife edge 70129, and a tissue thickness compensator 70130. The tissue thickness compensator 70130 may comprise at least one encapsulated component. The encapsulated component may be ruptured when the tissue thickness compensator is compressed, stapled, and/or cut. Referring to FIG. 192, for example, the staples 70128 can be deployed between an unfired position and a fired position such that the staple legs move through the tissue thickness compensator 70130, penetrate through a bottom surface and a top surface of the tissue thickness compensator 70130, penetrate the tissue T, and contact an anvil 70120 positioned opposite the staple cartridge 70118. The encapsulated components may react with each other, a hydrophilic powder embedded or dispersed in the tissue thickness compensator, and/or bodily fluids to expand or swell the tissue thickness compensator 70130. As the legs are deformed against the anvil, the legs of each staple can capture a portion of the tissue thickness compensator 70130 and a portion of the tissue T within each staple 70128 and apply a compressive force to the tissue T. As shown in FIGS. 192 and 193, the tissue thickness compensator 70130 can compensate for the thickness of the tissue T captured within each staple 70128.

Referring to FIG. 197, a surgical instrument 70200 may comprise an anvil 70205 comprising an upper tissue thickness compensator 70210 and a staple cartridge 70215 comprising a lower tissue thickness compensator comprising an outer layer 70220 and an inner layer 70225. The upper tissue thickness compensator 70210 can be positioned on a first side of the targeted tissue and the lower tissue thickness compensator can be positioned on a second side of the tissue. In certain embodiments, the upper tissue thickness compensator 70210 may comprise ORC, the outer layer of the lower tissue thickness compensator may comprise a hydrogel having ORC particles embedded therein, and the inner layer of the lower tissue thickness compensator may comprise ORC, for example.

Referring to FIGS. 200-202, in various embodiments, a surgical instrument 70400 may comprise a staple cartridge 70405 and an anvil 70410. The staple cartridge 70405 may

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comprise a tissue thickness compensator 70415 including bioabsorbable foam. In various embodiments, the bioabsorbable foam can comprise an encapsulation which comprises an encapsulated component 70420. The bioabsorbable foam may comprise ORC and the encapsulated component may comprise a medicament, for example. The tissue thickness compensator 70415 of the anvil 70410 may comprise an inner layer 70425 and an outer layer 70430. The inner layer 70425 may comprise a bioabsorbable foam, and the outer layer 70430 may comprise a hydrogel, optionally comprising reinforcement materials, for example. During an exemplary firing sequence, referring primarily to FIG. 201, a sled 70435 can first contact staple 70440A and begin to lift the staple upwardly. As the sled 70435 is advanced further distally, the sled 70435 can begin to lift staples 70440B-D, and any other subsequent staples, in a sequential order. The sled 70435 can drive the staples 70440 upwardly such that the legs of the staples contact the opposing anvil 70410 and are deformed to a desired shape. With regard to the firing sequence illustrated in FIG. 201, the staples 70440A-C have been moved into their fully fired positions, the staple 70440D is in the process of being fired, and the staple 70420E is still in its unfired position. The encapsulated component 70470 may be ruptured by the staple legs during the exemplary firing sequence. The encapsulated component 70420 may flow from the encapsulation around the staple legs to contact the tissue T. In various circumstances, additional compression of the tissue thickness compensator can squeeze additional medicament out of the encapsulation. In various embodiments, the medicament can immediately treat the tissue and can reduce bleeding from the tissue.

In various circumstances, a surgeon, or other clinician, may deliver a fluid to the tissue thickness compensator to manufacture a tissue thickness compensator comprising at least one medicament stored and/or absorbed therein. In various embodiments, a staple cartridge and/or anvil may comprise a port configured to provide access to the tissue thickness compensator. Referring to FIG. 203B, a staple cartridge 70500 may comprise a port 70505 at a distal end thereof, for example. The port 70505 may be configured to receive a needle 70510, such as a fenestrated needle shown in FIG. 203A. In at least one embodiment, the clinician may insert a needle 70510 through the port 70505 into the tissue thickness compensator 70515 to deliver the fluid to the tissue thickness compensator 70515. In various embodiments, the fluid may comprise a medicament and hydrogel precursor, for example. As described above, the fluid may be released from tissue thickness compensator to the tissue when the tissue thickness compensator is ruptured and/or compressed. For example, the medicament may be released from the tissue thickness compensator 70515 as the tissue thickness compensator 70515 biodegrades.

In various embodiments, referring now to FIG. 14, a staple cartridge, such as staple cartridge 10000, for example, can comprise a support portion 10010 and a compressible tissue thickness compensator 10020. Referring now to FIGS. 16-18, the support portion 10010 can comprise a deck surface 10011 and a plurality of staple cavities 10012 defined within the support portion 10010. Each staple cavity 10012 can be sized and configured to removably store a staple, such as a staple 10030, for example, therein. The staple cartridge 10000 can further comprise a plurality of staple drivers 10040 which can each be configured to support one or more staples 10030 within the staple cavities 10012 when the staples 10030 and the staple drivers 10040 are in their unfired positions. In at least one such embodiment, referring primarily to FIGS. 22 and 23, each staple driver 10040 can comprise one or more

cradles, or troughs, **10041**, for example, which can be configured to support the staples and limit relative movement between the staples **10030** and the staple drivers **10040**. In various embodiments, referring again to FIG. 16, the staple cartridge **10000** can further comprise a staple-firing sled **10050** which can be moved from a proximal end **10001** to a distal end **10002** of the staple cartridge in order to sequentially lift the staple drivers **10040** and the staples **10030** from their unfired positions toward an anvil positioned opposite the staple cartridge **10000**. In certain embodiments, referring primarily to FIGS. 16 and 18, each staple **10030** can comprise a base **10031** and one or more legs **10032** extending from the base **10031** wherein each staple can be at least one of substantially U-shaped and substantially V-shaped, for example. In at least one embodiment, the staples **10030** can be configured such that the tips of the staple legs **10032** are recessed with respect to the deck surface **10011** of the support portion **10010** when the staples **10030** are in their unfired positions. In at least one embodiment, the staples **10030** can be configured such that the tips of the staple legs **10032** are flush with respect to the deck surface **10011** of the support portion **10010** when the staples **10030** are in their unfired positions. In at least one embodiment, the staples **10030** can be configured such that the tips of the staple legs **10032**, or at least some portion of the staple legs **10032**, extend above the deck surface **10011** of the support portion **10010** when the staples **10030** are in their unfired positions. In such embodiments, the staple legs **10032** can extend into and can be embedded within the tissue thickness compensator **10020** when the staples **10030** are in their unfired positions. In at least one such embodiment, the staple legs **10032** can extend above the deck surface **10011** by approximately 0.075", for example. In various embodiments, the staple legs **10032** can extend above the deck surface **10011** by a distance between approximately 0.025" and approximately 0.125", for example. In certain embodiments, further to the above, the tissue thickness compensator **10020** can comprise an uncompressed thickness between approximately 0.08" and approximately 0.125", for example.

In use, further to the above and referring primarily to FIG. 31, an anvil, such as anvil, **10060**, for example, can be moved into a closed position opposite the staple cartridge **10000**. As described in greater detail below, the anvil **10060** can position tissue against the tissue thickness compensator **10020** and, in various embodiments, compress the tissue thickness compensator **10020** against the deck surface **10011** of the support portion **10010**, for example. Once the anvil **10060** has been suitably positioned, the staples **10030** can be deployed, as also illustrated in FIG. 31. In various embodiments, as mentioned above, the staple-firing sled **10050** can be moved from the proximal end **10001** of the staple cartridge **10000** toward the distal end **10002**, as illustrated in FIG. 32. As the sled **10050** is advanced, the sled **10050** can contact the staple drivers **10040** and lift the staple drivers **10040** upwardly within the staple cavities **10012**. In at least one embodiment, the sled **10050** and the staple drivers **10040** can each comprise one or more ramps, or inclined surfaces, which can co-operate to move the staple drivers **10040** upwardly from their unfired positions. In at least one such embodiment, referring to FIGS. 19-23, each staple driver **10040** can comprise at least one inclined surface **10042** and the sled **10050** can comprise one or more inclined surfaces **10052** which can be configured such that the inclined surfaces **10052** can slide under the inclined surface **10042** as the sled **10050** is advanced distally within the staple cartridge. As the staple drivers **10040** are lifted upwardly within their respective staple cavities **10012**, the staple drivers **10040** can lift the staples **10030** upwardly

such that the staples **10030** can emerge from their staple cavities **10012** through openings in the staple deck **10011**. During an exemplary firing sequence, referring primarily to FIGS. 25-27, the sled **10050** can first contact staple **10030a** and begin to lift the staple **10030a** upwardly. As the sled **10050** is advanced further distally, the sled **10050** can begin to lift staples **10030b**, **10030c**, **10030d**, **10030e**, and **10030f**, and any other subsequent staples, in a sequential order. As illustrated in FIG. 27, the sled **10050** can drive the staples **10030** upwardly such that the legs **10032** of the staples contact the opposing anvil, are deformed to a desired shape, and ejected therefrom the support portion **10010**. In various circumstances, the sled **10030** can move several staples upwardly at the same time as part of a firing sequence. With regard to the firing sequence illustrated in FIG. 27, the staples **10030a** and **10030b** have been moved into their fully fired positions and ejected from the support portion **10010**, the staples **10030c** and **10030d** are in the process of being fired and are at least partially contained within the support portion **10010**, and the staples **10030e** and **10030f** are still in their unfired positions.

As discussed above, and referring to FIG. 33, the staple legs **10032** of the staples **10030** can extend above the deck surface **10011** of the support portion **10010** when the staples **10030** are in their unfired positions. With further regard to this firing sequence illustrated in FIG. 27, the staples **10030e** and **10030f** are illustrated in their unfired position and their staple legs **10032** extend above the deck surface **10011** and into the tissue thickness compensator **10020**. In various embodiments, the tips of the staple legs **10032**, or any other portion of the staple legs **10032**, may not protrude through a top tissue-contacting surface **10021** of the tissue thickness compensator **10020** when the staples **10030** are in their unfired positions. As the staples **10030** are moved from their unfired positions to their fired positions, as illustrated in FIG. 27, the tips of the staple legs can protrude through the tissue-contacting surface **10032**. In various embodiments, the tips of the staple legs **10032** can comprise sharp tips which can incise and penetrate the tissue thickness compensator **10020**. In certain embodiments, the tissue thickness compensator **10020** can comprise a plurality of apertures which can be configured to receive the staple legs **10032** and allow the staple legs **10032** to slide relative to the tissue thickness compensator **10020**. In certain embodiments, the support portion **10010** can further comprise a plurality of guides **10013** extending from the deck surface **10011**. The guides **10013** can be positioned adjacent to the staple cavity openings in the deck surface **10011** such that the staple legs **10032** can be at least partially supported by the guides **10013**. In certain embodiments, a guide **10013** can be positioned at a proximal end and/or a distal end of a staple cavity opening. In various embodiments, a first guide **10013** can be positioned at a first end of each staple cavity opening and a second guide **10013** can be positioned at a second end of each staple cavity opening such that each first guide **10013** can support a first staple leg **10032** of a staple **10030** and each second guide **10013** can support a second staple leg **10032** of the staple. In at least one embodiment, referring to FIG. 33, each guide **10013** can comprise a groove or slot, such as groove **10016**, for example, within which a staple leg **10032** can be slidably received. In various embodiments, each guide **10013** can comprise a cleat, protrusion, and/or spike that can extend from the deck surface **10011** and can extend into the tissue thickness compensator **10020**. In at least one embodiment, as discussed in greater detail below, the cleats, protrusions, and/or spikes can reduce relative movement between the tissue thickness compensator **10020** and the support portion **10010**. In certain embodiments, the tips of the staple legs **10032** may be positioned within the guides **10013** and may

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not extend above the top surfaces of the guides **10013** when the staples **10030** are in their unfired position. In at least such embodiment, the guides **10013** can define a guide height and the staples **10030** may not extend above this guide height when they are in their unfired position.

In various embodiments, a tissue thickness compensator, such as tissue thickness compensator **10020**, for example, can be comprised of a single sheet of material. In at least one embodiment, a tissue thickness compensator can comprise a continuous sheet of material which can cover the entire top deck surface **10011** of the support portion **10010** or, alternatively, cover less than the entire deck surface **10011**. In certain embodiments, the sheet of material can cover the staple cavity openings in the support portion **10010** while, in other embodiments, the sheet of material can comprise openings which can be aligned, or at least partially aligned, with the staple cavity openings. In various embodiments, a tissue thickness compensator can be comprised of multiple layers of material. In some embodiments, referring now to FIG. 15, a tissue thickness compensator can comprise a compressible core and a wrap surrounding the compressible core. In certain embodiments, a wrap **10022** can be configured to releasably hold the compressible core to the support portion **10010**. In at least one such embodiment, the support portion **10010** can comprise one or more projections, such as projections **10014** (FIG. 18), for example, extending therefrom which can be received within one or more apertures and/or slots, such as apertures **10024**, for example, defined in the wrap **10022**. The projections **10014** and the apertures **10024** can be configured such that the projections **10014** can retain the wrap **10022** to the support portion **10010**. In at least one embodiment, the ends of the projections **10014** can be deformed, such as by a heat-stake process, for example, in order to enlarge the ends of the projections **10014** and, as a result, limit the relative movement between the wrap **10022** and the support portion **10010**. In at least one embodiment, the wrap **10022** can comprise one or more perforations **10025** which can facilitate the release of the wrap **10022** from the support portion **10010**, as illustrated in FIG. 15. Referring now to FIG. 24, a tissue thickness compensator can comprise a wrap **10022** including a plurality of apertures **10023**, wherein the apertures **10023** can be aligned, or at least partially aligned, with the staple cavity openings in the support portion **10010**. In certain embodiments, the core of the tissue thickness compensator can also comprise apertures which are aligned, or at least partially aligned, with the apertures **10023** in the wrap **10022**. In other embodiments, the core of the tissue thickness compensator can comprise a continuous body and can extend underneath the apertures **10023** such that the continuous body covers the staple cavity openings in the deck surface **10011**.

In various embodiments, as described above, a tissue thickness compensator can comprise a wrap for releasably holding a compressible core to the support portion **10010**. In at least one such embodiment, referring to FIG. 16, a staple cartridge can further comprise retainer clips **10026** which can be configured to inhibit the wrap, and the compressible core, from prematurely detaching from the support portion **10010**. In various embodiments, each retainer clip **10026** can comprise apertures **10028** which can be configured to receive the projections **10014** extending from the support portion **10010** such that the retainer clips **10026** can be retained to the support portion **10010**. In certain embodiments, the retainer clips **10026** can each comprise at least one pan portion **10027** which can extend underneath the support portion **10010** and can support and retain the staple drivers **10040** within the support portion **10010**. In certain embodiments, as described above, a tissue thickness compensator can be removably

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attached to the support portion **10010** by the staples **10030**. More particularly, as also described above, the legs of the staples **10030** can extend into the tissue thickness compensator **10020** when the staples **10030** are in their unfired position and, as a result, releasably hold the tissue thickness compensator **10020** to the support portion **10010**. In at least one embodiment, the legs of the staples **10030** can be in contact with the sidewalls of their respective staple cavities **10012** wherein, owing to friction between the staple legs **10032** and the sidewalls, the staples **10030** and the tissue thickness compensator **10020** can be retained in position until the staples **10030** are deployed from the staple cartridge **10000**. When the staples **10030** are deployed, the tissue thickness compensator **10020** can be captured within the staples **10030** and held against the stapled tissue T. When the anvil is thereafter moved into an open position to release the tissue T, the support portion **10010** can be moved away from the tissue thickness compensator **10020** which has been fastened to the tissue. In certain embodiments, an adhesive can be utilized to removably hold the tissue thickness compensator **10020** to the support portion **10010**. In at least one embodiment, a two-part adhesive can be utilized wherein, in at least one embodiment, a first part of the adhesive can be placed on the deck surface **10011** and a second part of the adhesive can be placed on the tissue thickness compensator **10020** such that, when the tissue thickness compensator **10020** is placed against the deck surface **10011**, the first part can contact the second part to activate the adhesive and detachably bond the tissue thickness compensator **10020** to the support portion **10010**. In various embodiments, any other suitable means could be used to detachably retain the tissue thickness compensator to the support portion of a staple cartridge.

In various embodiments, further to the above, the sled **10050** can be advanced from the proximal end **10001** to the distal end **10002** to fully deploy all of the staples **10030** contained within the staple cartridge **10000**. In at least one embodiment, referring now to FIGS. 56-60, the sled **10050** can be advanced distally within a longitudinal cavity **10016** within the support portion **10010** by a firing member, or knife bar, **10052** of a surgical stapler. In use, the staple cartridge **10000** can be inserted into a staple cartridge channel in a jaw of the surgical stapler, such as staple cartridge channel **10070**, for example, and the firing member **10052** can be advanced into contact with the sled **10050**, as illustrated in FIG. 56. As the sled **10050** is advanced distally by the firing member **10052**, the sled **10050** can contact the proximal-most staple driver, or drivers, **10040** and fire, or eject, the staples **10030** from the cartridge body **10010**, as described above. As illustrated in FIG. 56, the firing member **10052** can further comprise a cutting edge **10053** which can be advanced distally through a knife slot in the support portion **10010** as the staples **10030** are being fired. In various embodiments, a corresponding knife slot can extend through the anvil positioned opposite the staple cartridge **10000** such that, in at least one embodiment, the cutting edge **10053** can extend between the anvil and the support portion **10010** and incise the tissue and the tissue thickness compensator positioned therebetween. In various circumstances, the sled **10050** can be advanced distally by the firing member **10052** until the sled **10050** reaches the distal end **10002** of the staple cartridge **10000**, as illustrated in FIG. 58. At such point, the firing member **10052** can be retracted proximally. In some embodiments, the sled **10050** can be retracted proximally with the firing member **10052** but, in various embodiments, referring now to FIG. 59, the sled **10050** can be left behind in the distal end **10002** of the staple cartridge **10000** when the firing member **10052** is retracted. Once the firing member **10052** has been sufficiently

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retracted, the anvil can be re-opened, the tissue thickness compensator **10020** can be detached from the support portion **10010**, and the remaining non-implanted portion of the expended staple cartridge **10000**, including the support portion **10010**, can be removed from the staple cartridge channel **10070**.

After the expended staple cartridge **10000** has been removed from the staple cartridge channel, further to the above, a new staple cartridge **10000**, or any other suitable staple cartridge, can be inserted into the staple cartridge channel **10070**. In various embodiments, further to the above, the staple cartridge channel **10070**, the firing member **10052**, and/or the staple cartridge **10000** can comprise co-operating features which can prevent the firing member **10052** from being advanced distally a second, or subsequent, time without a new, or unfired, staple cartridge **10000** positioned in the staple cartridge channel **10070**. More particularly, referring again to FIG. **56**, as the firing member **10052** is advanced into contact with the sled **10050** and, when the sled **10050** is in its proximal unfired position, a support nose **10055** of the firing member **10052** can be positioned on and/or over a support ledge **10056** on the sled **10050** such that the firing member **10052** is held in a sufficient upward position to prevent a lock, or beam, **10054** extending from the firing member **10052** from dropping into a lock recess defined within the staple cartridge channel. As the lock **10054** will not drop into the lock recess, in such circumstances, the lock **10054** may not abut a distal sidewall **10057** of the lock recess as the firing member **10052** is advanced. As the firing member **10052** pushes the sled **10050** distally, the firing member **10052** can be supported in its upward firing position owing to the support nose **10055** resting on the support ledge **10056**. When the firing member **10052** is retracted relative to the sled **10050**, as discussed above and illustrated in FIG. **59**, the firing member **10052** can drop downwardly from its upward position as the support nose **10055** is no longer resting on the support ledge **10056** of the sled **10050**. In at least one such embodiment, the surgical staple can comprise a spring **10058**, and/or any other suitable biasing element, which can be configured to bias the firing member **10052** into its downward position. Once the firing member **10052** has been completely retracted, as illustrated in FIG. **60**, the firing member **10052** cannot be advanced distally through the spent staple cartridge **10000** once again. More particularly, the firing member **10052** can't be held in its upper position by the sled **10050** as the sled **10050**, at this point in the operating sequence, has been left behind at the distal end **10002** of the staple cartridge **10000**. Thus, as mentioned above, in the event that the firing member **10052** is advanced once again without replacing the staple cartridge, the lock beam **10054** will contact the sidewall **10057** of the lock recess which will prevent the firing member **10052** from being advanced distally into the staple cartridge **10000** once again. Stated another way, once the spent staple cartridge **10000** has been replaced with a new staple cartridge, the new staple cartridge will have a proximally-positioned sled **10050** which can hold the firing member **10052** in its upper position and allow the firing member **10052** to be advanced distally once again.

As described above, the sled **10050** can be configured to move the staple drivers **10040** between a first, unfired position and a second, fired position in order to eject staples **10030** from the support portion **10010**. In various embodiments, the staple drivers **10040** can be contained within the staple cavities **10012** after the staples **10030** have been ejected from the support portion **10010**. In certain embodiments, the support portion **10010** can comprise one or more retention features which can be configured to block the staple drivers **10040**

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from being ejected from, or falling out of, the staple cavities **10012**. In various other embodiments, the sled **10050** can be configured to eject the staple drivers **10040** from the support portion **10010** with the staples **10030**. In at least one such embodiment, the staple drivers **10040** can be comprised of a bioabsorbable and/or biocompatible material, such as Ultem, for example. In certain embodiments, the staple drivers can be attached to the staples **10030**. In at least one such embodiment, a staple driver can be molded over and/or around the base of each staple **10030** such that the driver is integrally formed with the staple. U.S. patent application Ser. No. 11/541,123, entitled SURGICAL STAPLES HAVING COMPRESSIBLE OR CRUSHABLE MEMBERS FOR SECURING TISSUE THEREIN AND STAPLING INSTRUMENTS FOR DEPLOYING THE SAME, filed on Sep. 29, 2006, is hereby incorporated by reference in its entirety.

As described above, a surgical stapling instrument can comprise a staple cartridge channel configured to receive a staple cartridge, an anvil rotatably coupled to the staple cartridge channel, and a firing member comprising a knife edge which is movable relative to the anvil and the staple cartridge channel. In use, a staple cartridge can be positioned within the staple cartridge channel and, after the staple cartridge has been at least partially expended, the staple cartridge can be removed from the staple cartridge channel and replaced with a new staple cartridge. In some such embodiments, the staple cartridge channel, the anvil, and/or the firing member of the surgical stapling instrument may be re-used with the replacement staple cartridge. In certain other embodiments, a staple cartridge may comprise a part of a disposable loading unit assembly which can include a staple cartridge channel, an anvil, and/or a firing member, for example, which can be replaced along with the staple cartridge as part of replacing the disposable loading unit assembly. Certain disposable loading unit assemblies are disclosed in U.S. patent application Ser. No. 12/031,817, entitled END EFFECTOR COUPLING ARRANGEMENTS FOR A SURGICAL CUTTING AND STAPLING INSTRUMENT, which was filed on Feb. 15, 2008, now U.S. Patent Application Publication No. 2009/0206131, the entire disclosure of which is incorporated by reference herein.

In various embodiments, the tissue thickness compensator may comprise an extrudable, a castable, and/or moldable composition comprising at least one of the synthetic and/or non-synthetic materials described herein. In various embodiments, the tissue thickness compensator may comprise a film or sheet comprising two or more layers. The tissue thickness compensator may be obtained using conventional methods, such as, for example, mixing, blending, compounding, spraying, wicking, solvent evaporating, dipping, brushing, vapor deposition, extruding, calendaring, casting, molding and the like. In extrusion, an opening may be in the form of a die comprising at least one opening to impart a shape to the emerging extrudate. In calendaring, an opening may comprise a nip between two rolls. Conventional molding methods may include, but are not limited to, blow molding, injection molding, foam injection, compression molding, thermoforming, extrusion, foam extrusion, film blowing, calendaring, spinning, solvent welding, coating methods, such as dip coating and spin coating, solution casting and film casting, plastisol processing (including knife coating, roller coating and casting), and combinations thereof. In injection molding, an opening may comprise a nozzle and/or channels/runners and/or mold cavities and features. In compression molding, the composition may be positioned in a mold cavity, heated to a suitable temperature, and shaped by exposure to compression

under relatively high pressure. In casting, the composition may comprise a liquid or slurry that may be poured or otherwise provided into, onto and/or around a mold or object to replicate features of the mold or object. After casting, the composition may be dried, cooled, and/or cured to form a solid.

In various embodiments, a method of manufacturing a tissue thickness compensator may generally comprise providing a tissue thickness compensator composition, liquifying the composition to make it flowable, and forming the composition in the molten, semi-molten, or plastic state into a layer and/or film having the desired thickness. Referring to FIG. 198A, a tissue thickness compensator may be manufactured by dissolving a hydrogel precursor in an aqueous solution, dispersing biocompatible particles and/or fibers therein, providing a mold having biocompatible particles therein, providing the solution into the mold, contacting an activator and the solution, and curing the solution to form the tissue thickness compensator comprising an outer layer comprising biocompatible particles and an inner layer comprising biocompatible particles embedded therein. A shown in FIG. 198A, a biocompatible layer 70250 may be provided in the bottom of a mold 70260, and an aqueous solution of a hydrogel precursor 70255 having biocompatible particles 70257 disposed therein may be provided to the mold 70260, and the aqueous solution may be cured to form a tissue thickness compensator having a first layer comprising a biocompatible material, such as ORC, for example, and a second layer comprising a hydrogel having biocompatible fibers, such as ORC fibers, disposed therein. The tissue thickness compensator may comprise a foam comprising an outer layer comprising biocompatible particles and an inner layer comprising biocompatible particles embedded therein. In at least one embodiment, a tissue thickness compensator may be manufactured by dissolving a sodium alginate in water, dispersing ORC particles therein, providing a mold having ORC particles therein, pouring the solution into the mold, spraying or infusing calcium chloride to contact the solution to initiate crosslinking of the sodium alginate, freeze drying the hydrogel to form the tissue thickness compensator comprising an outer layer comprising ORC and an inner layer comprising a hydrogel and ORC particles embedded therein.

Referring to FIG. 198B, in various embodiments, a method of manufacturing a trilayer tissue thickness compensator may generally comprise by dissolving a first hydrogel precursor in a first aqueous solution, dispersing biocompatible particles and/or fibers in the first aqueous solution, providing a mold 70260 having a first layer 70250 of biocompatible particles therein, providing the first aqueous solution into the mold, contacting an activator and the first aqueous solution, curing the first aqueous solution to form a second layer 70255, dissolving a second hydrogel precursor in a second aqueous solution, providing the second aqueous solution into the mold, curing the second aqueous solution to form a third layer 70265. In at least one embodiment, a trilayer tissue thickness compensator may be manufactured by dissolving a sodium alginate in water to form a first aqueous solution, dispersing ORC particles in the first aqueous solution, providing a mold having a first layer of ORC particles therein, pouring the first aqueous solution into the mold, spraying or infusing calcium chloride to contact the first aqueous solution to initiate crosslinking of the sodium alginate, freeze drying the first aqueous solution to form a second layer comprising a hydrogel having ORC particles embedded therein, dissolving a sodium alginate in water to form a second aqueous solution, pouring the second aqueous solution into the mold, spraying or infusing calcium chloride to contact the second aqueous

solution to initiate crosslinking of the sodium alginate, freeze drying the second aqueous solution to form a third layer comprising a hydrogel.

In various embodiments, a method of manufacturing a tissue thickness compensator comprising at least one medicament stored and/or absorbed therein may generally comprise providing a tissue thickness compensator and contacting the tissue thickness compensator and the medicament to retain the medicament in the tissue thickness compensator. In at least one embodiment, a method of manufacturing a tissue thickness compensator comprising an antibacterial material may comprise providing a hydrogel, drying the hydrogel, swelling the hydrogel in an aqueous solution of silver nitrate, contacting the hydrogel and a solution of sodium chloride to form the tissue thickness compensator having antibacterial properties. The tissue thickness compensator may comprise silver dispersed therein.

Referring to FIG. 204, in various embodiments, a method for manufacturing a tissue thickness compensator may comprise co-extrusion and/or bonding. In various embodiments, the tissue thickness compensator 70550 may comprise a laminate comprising a first layer 70555 and a second layer 70560 sealingly enclosing an inner layer 70565 comprising a hydrogel, for example. The hydrogel may comprise a dry film, a dry foam, a powder, and/or granules, for example. The hydrogel may comprise super absorbent materials, such as, for example, polyvinylpyrrolidone, carboxy methylcellulose, poly sulfur propyl acrylate. The first and/or second layers may be made in-line by feeding raw materials of the first and second layers, respectively, into an extruder from a hopper, and thereafter supplying the first and second layers. The raw materials of the inner layer 70565 may be added to a hopper of an extruder. The raw materials can be dispersively mixed and compounded at an elevated temperature within the extruder. As the raw materials exit the die 70570 at an opening, the inner layer 70565 may be deposited onto a surface of the first layer 70555. In various embodiments, the tissue thickness compensator may comprise a foam, film, powder, and/or granule. The first and second layers 70555 and 70560 may be positioned in the face-to-face relationship. The second layer 70560 may be aligned with the first layer 70555 in a face-to-face relationship by a roller 70575. The first layer 70555 may adhere to the second layer 70560 wherein the first and second layers 70555, 70560 may physically entrap the inner layer 70565. The layers may be joined together under light pressure, under conventional calendar bonding processes, and/or through the use of adhesives, for example, to form the tissue thickness compensator 70550. In at least one embodiment, as shown in FIG. 78, the first and second layers 70555 and 70560 may be joined together through a rolling process utilizing a grooved roller 70580, for example. In various embodiments, as a result of the above, the inner layer 70565 may be contained and/or sealed by the first and second layers 70555 and 70560 which can collectively form an outer layer, or barrier. The outer layer may prevent or reduce moisture from contacting the inner layer 70565 until the outer layer is ruptured.

Referring to FIG. 61, an end effector 12 for a surgical instrument 10 (FIG. 1) can be configured to receive a fastener cartridge assembly, such as staple cartridge 20000, for example. As illustrated in FIG. 61, the staple cartridge 20000 can be configured to fit in a cartridge channel 20072 of a jaw 20070 of the end effector 12. In other embodiments, the staple cartridge 20000 can be integral to the end effector 12 such that the staple cartridge 20000 and the end effector 12 are formed as a single unit construction. The staple cartridge 20000 can comprise a first body portion, such as rigid support portion

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20010, for example. The staple cartridge 20000 can also comprise a second body portion, such as a compressible portion or a tissue thickness compensator 20020, for example. In other embodiments, the tissue thickness compensator 20020 may not comprise an integral part of the staple cartridge 20000 but may be otherwise positioned relative to the end effector 12. For example, the tissue thickness compensator 20020 can be secured to an anvil 20060 of the end effector 12 or can be otherwise retained in the end effector 12. In at least one embodiment, referring to FIG. 78, the staple cartridge can further comprise retainer clips 20126 which can be configured to inhibit the tissue thickness compensator 20020 from prematurely detaching from the support portion 20010. The reader will appreciate that the tissue thickness compensators described herein can be installed in or otherwise engaged with a variety of end effectors and that such embodiments are within the scope of the present disclosure.

Similar to the tissue thickness compensators described herein, referring now to FIG. 78, the tissue thickness compensator 20020 can be released from or disengaged with the surgical end effector 12. For example, in some embodiments, the rigid support portion 20010 of the staple cartridge 20000 can remain engaged with the fastener cartridge channel 20072 of the end effector jaw 20070 while the tissue thickness compensator 20020 disengages from the rigid support portion 20010. In various embodiments, the tissue thickness compensator 20020 can release from the end effector 12 after staples 20030 (FIGS. 78-83) are deployed from staple cavities 20012 in the rigid support portion 20010, similar to various embodiments described herein. Staples 20030 can be fired from staple cavities 20012 such that the staples 20030 engage the tissue thickness compensator 20020. Also similar to various embodiments described herein, referring generally to FIGS. 63, 82 and 83, a staple 20030 can capture a portion of the tissue thickness compensator 20020 along with stapled tissue T. In some embodiments, the tissue thickness compensator 20020 can be deformable and the portion of the tissue thickness compensator 20020 that is captured within a fired staple 20030 can be compressed. Similar to the tissue thickness compensators described herein, the tissue thickness compensator 20020 can compensate for different thicknesses, compressibilities, and/or densities of tissue T captured within each staple 20030. Further, as also described herein, the tissue thickness compensator 20020 can compensate for gaps created by malformed staples 20030.

The tissue thickness compensator 20020 can be compressible between non-compressed height(s) and compressed height(s). Referring to FIG. 78, the tissue thickness compensator 20020 can have a top surface 20021 and a bottom surface 20022. The height of the tissue thickness compensator can be the distance between the top surface 20021 and the bottom surface 20022. In various embodiments, the non-compressed height of the tissue thickness compensator 20020 can be the distance between the top surface 20021 and the bottom surface 20022 when minimal or no force is applied to the tissue thickness compensator 20020, i.e., when the tissue thickness compensator 20020 is not compressed. The compressed height of the tissue thickness compensator 20020 can be the distance between the top surface 20021 and the bottom surface 20022 when a force is applied to the tissue thickness compensator 20020, such as when a fired staple 20030 captures a portion of the tissue thickness compensator 20020, for example. The tissue thickness compensator 20020 can have a distal end 20025 and a proximal end 20026. As illustrated in FIG. 78, the non-compressed height of the tissue thickness compensator 20020 can be uniform between the distal end 20025 and the proximal end 20026 of the tissue thickness

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compensator 20020. In other embodiments, the non-compressed height can vary between the distal end 20025 and the proximal end 20026. For example, the top surface 20021 and/or bottom surface 20022 of the tissue thickness compensator 20020 can be angled and/or stepped relative to the other such that the non-compressed height varies between the proximal end 20026 and the distal end 20025. In some embodiments, the non-compressed height of the tissue thickness compensator 20020 can be approximately 0.08 inches, for example. In other embodiments, the non-compressed height of the tissue thickness compensator 20020 can vary between approximately 0.025 inches and approximately 0.10 inches, for example.

As described in greater detail herein, the tissue thickness compensator 20020 can be compressed to different compressed heights between the proximal end 20026 and the distal end 20025 thereof. In other embodiments, the tissue thickness compensator 20020 can be uniformly compressed throughout the length thereof. The compressed height(s) of the tissue thickness compensator 20020 can depend on the geometry of the end effector 12, characteristics of the tissue thickness compensator 20020, the engaged tissue T and/or the staples 20030, for example. In various embodiments, the compressed height of the tissue thickness compensator 20020 can relate to the tissue gap in the end effector 12. In various embodiments, when the anvil 20060 is clamped towards the staple cartridge 20000, the tissue gap can be defined between a top deck surface 20011 (FIG. 78) of the staple cartridge 20000 and a tissue contacting surface 20061 (FIG. 61) of the anvil 20060, for example. The tissue gap can be approximately 0.025 inches or approximately 0.100 inches, for example. In some embodiments, the tissue gap can be approximately 0.750 millimeters or approximately 3.500 millimeters, for example. In various embodiments, the compressed height of the tissue thickness compensator 20020 can equal or substantially equal the tissue gap, for example. When tissue T is positioned within the tissue gap of the end effector 12, the compressed height of the tissue thickness compensator can be less in order to accommodate the tissue T. For example, where the tissue gap is approximately 0.750 millimeters, the compressed height of the tissue thickness compensator can be approximately 0.500 millimeters. In embodiments where the tissue gap is approximately 3.500 millimeters, the compressed height of the tissue thickness compensator 20020 can be approximately 2.5 mm, for example. Furthermore, the tissue thickness compensator 20020 can comprise a minimum compressed height. For example, the minimum compressed height of the tissue thickness compensator 20020 can be approximately 0.250 millimeters. In various embodiments, the tissue gap defined between the deck surface of the staple cartridge and the tissue contacting surface of the anvil can equal, or at least substantially equal, the uncompressed height of the tissue thickness compensator, for example.

Referring primarily to FIG. 62, the tissue thickness compensator 20020 can comprise a fibrous, nonwoven material 20080 including fibers 20082. In some embodiments, the tissue thickness compensator 20020 can comprise felt or a felt-like material. Fibers 20082 in the nonwoven material 20080 can be fastened together by any means known in the art, including, but not limited to, needle-punching, thermal bonding, hydro-entanglement, ultrasonic pattern bonding, chemical bonding, and meltblown bonding. Further, in various embodiments, layers of nonwoven material 20080 can be mechanically, thermally, or chemically fastened together to form the tissue thickness compensator 20020. As described in greater detail herein, the fibrous, nonwoven material 20080

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can be compressible, which can enable compression of the tissue thickness compensator **20020**. In various embodiments, the tissue thickness compensator **20020** can comprise a non-compressible portion as well. For example, the tissue thickness compensator **20020** can comprise a compressible nonwoven material **20080** and a non-compressible portion.

Still referring primarily to FIG. **62**, the nonwoven material **20080** can comprise a plurality of fibers **20082**. At least some of the fibers **20082** in the nonwoven material **20080** can be crimped fibers **20086**. The crimped fibers **20086** can be, for example, crimped, twisted, coiled, bent, crippled, spiraled, curled, and/or bowed within the nonwoven material **20080**. As described in greater detail herein, the crimped fibers **20086** can be formed in any suitable shape such that deformation of the crimped fibers **20086** generates a spring load or restoring force. In some embodiments, the crimped fibers **20086** can be heat-shaped to form a coiled or substantially coil-like shape. The crimped fibers **20086** can be formed from non-crimped fibers **20084**. For example, non-crimped fibers **20084** can be wound around a heated mandrel to form a substantially coil-like shape.

In various embodiments, the tissue thickness compensator **20020** can comprise a homogeneous absorbable polymer matrix. The homogenous absorbable polymer matrix can comprise a foam, gel, and/or film, for example. Further, the plurality of fibers **20082** can be dispersed throughout the homogenous absorbable polymer matrix. At least some of the fibers **20082** in the homogenous absorbable polymer matrix can be crimped fibers **20086**, for example. As described in greater detail herein, the homogeneous absorbable polymer matrix of the tissue thickness compensator **2002** can be compressible.

In various embodiments, referring to FIGS. **65** and **66**, crimped fibers **20086** can be randomly dispersed throughout at least a portion of the nonwoven material **20080**. For example, crimped fibers **20086** can be randomly dispersed throughout the nonwoven material **20080** such that a portion of the nonwoven material **20080** comprises more crimped fibers **20086** than other portions of the nonwoven material **20080**. Further, the crimped fibers **20086** can congregate in fiber clusters **20085a**, **20085b**, **20085c**, **20085d** and **20085e**, for example, in the nonwoven material **20080**. The shape of the crimped fibers **20086** can cause entanglement of the fibers **20086** during manufacturing of the nonwoven material **20080**; entanglement of the crimped fibers **20086** can, in turn, result in the formation of the fiber clusters **20085a**, **20085b**, **20085c**, **20085d** and **20085e**. Additionally or alternatively, crimped fibers **20086** can be randomly oriented throughout the nonwoven material **20080**. For example, referring to FIG. **62**, a first crimped fiber **20086a** can be oriented in a first direction, a second crimped fiber **20086b** can be oriented in a second direction, and a third crimped fiber **20086c** can be oriented in a third direction.

In some embodiments, the crimped fibers **20086** can be systematically distributed and/or arranged throughout at least a portion of the nonwoven material **20080**. For example, referring now to FIG. **67**, crimped fibers **20186** can be positioned in an arrangement **20185**, in which a plurality of crimped fibers **20186a** are arranged in a first direction and another plurality of crimped fibers **20186b** are arranged in a second direction. The crimped fibers **20186** can overlap such that they become entangled or interconnected with each other. In various embodiments, the crimped fibers **20186** can be systematically arranged such that a crimped fiber **20186a** is substantially parallel to another crimped fiber **20186a**. Still another crimped fiber **20186b** can be substantially transverse to some crimped fibers **20186a**. In various embodiments,

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crimped fibers **20186a** can be substantially aligned with a first axis Y and crimped fibers **20186b** can be substantially aligned with a second axis X. In some embodiments the first axis Y can be perpendicular or substantially perpendicular to the second axis X, for example.

Referring primarily to FIG. **68**, in various embodiments, crimped fibers **20286** can be arranged in an arrangement **20285**. In some embodiments, each crimped fibers **20286** can comprise a longitudinal axis defined between a first end **20287** and a second end **20289** of the crimped fiber **20286**. In some embodiments, the crimped fibers **20286** can be systematically distributed in the nonwoven material **20080** such that a first end **20287** of one crimped fiber **20286** is positioned adjacent to a second end **20289** of another crimped fiber **20286**. In another embodiment, referring now to FIG. **69**, a fiber arrangement **20385** can comprise a first crimped fiber **20386a** oriented in a first direction, a second crimped fiber **20386b** oriented in a second direction, and a third crimped fiber **20386c** oriented in a third direction, for example. In various embodiments, a single pattern or arrangement of crimped fibers **20286** can be repeated throughout the nonwoven material **20080**. In at least one embodiment, crimped fibers can be arranged in different patterns throughout the nonwoven material **20080**. In still other embodiments, the nonwoven material **20080** can comprise at least one pattern of crimped fibers, as well as a plurality of randomly oriented and/or randomly distributed crimped fibers.

Referring again to FIG. **62**, the plurality of fibers **20082** in the nonwoven material **20080** can comprise at least some non-crimped fibers **20084**. The non-crimped fibers **20084** and crimped fibers **20086** in the nonwoven material **20080** can be entangled or interconnected. In one embodiment, the ratio of crimped fibers **20086** to non-crimped fibers **20084** can be approximately 25:1, for example. In another embodiment, the ratio of crimped fibers **20086** to non-crimped fibers **20084** can be approximately 1:25, for example. In other embodiments, the ratio of crimped fibers **20086** to non-crimped fibers **20084** can be approximately 1:1, for example. As described in greater detail herein, the number of crimped fibers **20086** per unit volume of nonwoven material **20080** can affect the restoring force generated by the nonwoven material **20080** when the nonwoven material **20080** has been deformed. As also described in greater detail herein, the restoring force generated by the nonwoven material **20080** can also depend on, for example, the material, shape, size, position and/or orientation of crimped and non-crimped fibers **20086**, **20084** in the nonwoven material **20080**.

In various embodiments, the fibers **20082** of the nonwoven material **20080** can comprise a polymeric composition. The polymeric composition of the fibers **20082** can comprise non-absorbable polymers, absorbable polymers, or combinations thereof. In some embodiments, the absorbable polymers can include bioabsorbable, biocompatible elastomeric polymers. Furthermore, the polymeric composition of the fibers **20082** can comprise synthetic polymers, non-synthetic polymers, or combinations thereof. Examples of synthetic polymers include, but are not limited to, polyglycolic acid (PGA), poly(lactic acid) (PLA), polycaprolactone (PCL), polydioxanone (PDO), and copolymers thereof. For example, the fibers **20082** can comprise a 90/10 poly(glycolide-L-lactide) copolymer, such as, for example, the copolymer commercially available from Ethicon, Inc. under the trade designation "VICRYL (polyglactin 910)." Examples of non-synthetic polymers include, but are not limited to, lyophilized polysaccharide, glycoprotein, elastin, proteoglycan, gelatin, collagen, and oxidized regenerated cellulose (ORC). In various embodiments, similar to the polymeric compositions in tissue

thickness compensators described herein, the polymeric composition of the fibers **20082** can include varied amounts of absorbable polymers, non-absorbable polymers, synthetic polymers, and/or non-synthetic polymers, for example, by weight percentage.

In some embodiments, the crimped fibers **20086** of the nonwoven material **20080** can comprise a first polymeric composition and the non-crimped fibers **20084** of the nonwoven material **20080** can comprise a different polymeric composition. For example, the crimped fibers **20086** can comprise synthetic polymer(s), such as, for example, 90/10 poly(glycolide-L-lactide), while the non-crimped fibers **20084** can comprise non-synthetic polymer(s), such as, for example, oxidized regenerated cellulose. In other embodiments, the crimped fibers **20086** and the non-crimped fibers **20084** can comprise the same polymeric composition.

As described herein, crimped fibers **20086** and non-crimped fibers **20084** can be fastened together, for example, by needle-punching, thermal bonding, hydro-entanglement, ultrasonic pattern bonding, chemical bonding, and meltblown bonding. In some embodiments, crimped fibers **20086** comprising synthetic polymers such as, for example, "VICRYL (polyglactic 910)", and non-crimped fibers **20084** comprising oxidized regenerated cellulose can be needle-punched together to form the nonwoven material **20080**. In various embodiments, the nonwoven material **20080** can comprise approximately 5% to 50% crimped "VICRYL (polyglactic 910)" fibers **20086** by weight and approximately 5% to 50% non-crimped oxidized regenerated cellulose (ORC) fibers **20084** by weight, for example. When the nonwoven material **20080** contacts tissue T, the non-crimped ORC fibers **20084** can rapidly react with plasma in the tissue to form a gelatinous mass, for example. In various embodiments, the formation of the gelatinous ORC mass can be instantaneous or nearly instantaneous with the tissue contact. Further, after the formation of the gelatinous ORC mass, the crimped "VICRYL (polyglactic 910)" fibers **20086** can remain dispersed throughout the nonwoven material **20080**. For example, the crimped fibers **20086** can be suspended in the gelatinous ORC mass. As the gelatinous ORC mass is bioabsorbed, the crimped "VICRYL (polyglactic 910)" fibers **20086** can exert a springback force on adjacent tissue, as described in greater detail herein. Further, the tissue can begin to heal around the "VICRYL (polyglactic 910)" fibers and/or the formed staples **30030**, as also described in greater detail herein.

In at least one embodiment, referring primarily to FIGS. **78-81**, the support portion **20010** of the staple cartridge **20000** can comprise a cartridge body **20017**, a top deck surface **20011**, and a plurality of staple cavities **20012**. Similar to the embodiments described herein, each staple cavity **20012** can define an opening in the deck surface **20011**. A staple **20030** can be removably positioned in a staple cavity **20012**. In various embodiments, a single staple **20030** is disposed in each staple cavity **20012**. In at least one embodiment, referring primarily to FIGS. **82** and **83** and similar to the staples described herein, each staple **20030** can comprise a base **20031** having a first end **20035** and a second end **20036**. A staple leg **20032** can extend from the first end **20035** of the base **20031** and another staple leg **20032** can extend from the second end **20036** of the base **20031**. Referring again to FIGS. **78-81**, prior to the deployment of the staples **20030**, the base **20031** of each staple **20030** can be supported by a staple driver **20040** positioned within the rigid support portion **20010** of the staple cartridge **20000**. Also prior to deployment of the staples **20030**, the legs **20032** of each staple **20030** can be at least partially contained within a staple cavity **20012**.

In various embodiments, the staples **20030** can be deployed between an initial position and a fired position. For example, referring primarily to FIG. **81**, staples **20030** can be in an initial position (staples **20030e**, **20030f**), a partially fired or intermediate position (staples **20030c**, **20030d**), or a fired position (staples **20030a**, **20030b**). A driver **20040** can motivate the staples between the initial position and the fired position. For example, the base **20031** of each staple **20030** can be supported by a driver **20040**. The legs **20032** of a staple (staples **20030e**, **20030f** in FIG. **80**, for example) can be positioned within a staple cavity **20012**. As the firing member or staple-firing sled **20050** translates from the proximal end **20001** to the distal end **20002** of the staple cartridge **20000**, an inclined surface **20051** on the sled **20050** can contact an inclined surface **20042** on a driver **20040** to deploy the staple **20030** positioned above the contacted driver **20040**. In various embodiments, the staples **20030** can be deployed between an initial position and a fired position such that the legs **20032** move through the nonwoven material **20080** of the tissue thickness compensator **20020**, penetrate the top surface **20021** of the tissue thickness compensator **20020**, penetrate tissue T, and contact an anvil **20060** (FIG. **61**) positioned opposite the staple cartridge **20000** in the end effector **12**. The staple legs **20032** can be deformed against the anvil **20060** and the legs **20032** of each staple **20030** can capture a portion of the nonwoven material **20080** and a portion of the tissue T.

In the fired configuration (FIGS. **82** and **83**), each staple **20030** can apply a compressive force to the tissue T and to the tissue thickness compensator **20020** captured within the staple **20030**. Referring primarily to FIGS. **80** and **81**, the legs **20032** of each staple **20030** can be deformed downwardly toward the base **20031** of the staple **20030** to form a staple entrapment area **20039**. The staple entrapment area **20039** can be the area in which the tissue T and the tissue thickness compensator **20020** can be captured by a fired staple **20030**. In various circumstances, the staple entrapment area **20039** can be defined between the inner surfaces of the deformed legs **20032** and the inner surface of the base **20031** of a staple **20030**. The size of the entrapment area **20039** for a staple **20030** can depend on several factors such as the length of the legs, the diameter of the legs, the width of the base, and/or the extent in which the legs are deformed, for example.

In various embodiments, when a nonwoven material **20080** is captured in a staple entrapment area **20039**, the captured portion of the nonwoven material **20080** can be compressed. The compressed height of the nonwoven material **20080** captured in a staple entrapment area **20039** can vary within the staple cartridge **20000** depending on the tissue T in that same staple entrapment area **20039**. For example, where the tissue T is thinner, the staple entrapment area **20039** may have more room for the nonwoven material **20080** and, as a result, the nonwoven material **20080** may not be as compressed as it would be if the tissue T were thicker. Where the tissue T is thicker, the nonwoven material **20080** can be compressed more to accommodate the thicker tissue T, for example. For example, referring to FIG. **82**, the nonwoven material **20080** can be compressed to a first height in a first staple entrapment area **20039a**, a second height in a second staple entrapment area **20039b**, a third height in a third staple entrapment area **20039c**, a fourth height in a fourth staple entrapment area **20039d**, and a fifth height in a fifth staple entrapment area **20039e**, for example. Similarly, as illustrated in FIG. **83**, the nonwoven material **20080** can be compressed to a first height in the first staple entrapment area **20039a**, a second height in the second staple entrapment area **20039b**, a third height in the third staple entrapment area **20039c**, and a fourth height in the fourth staple entrapment area **20039d**. In other embodi-

ments, the compressed height of the nonwoven material **20080** can be uniform throughout the staple cartridge **20010**.

In various embodiments, an applied force can move the nonwoven material **20080** from an initial uncompressed configuration to a compressed configuration. Further, the nonwoven material **20080** can be resilient, such that, when compressed, the nonwoven material **20080** can generate a springback or restoring force. When deformed, the nonwoven material **20080** can seek to rebound from the compressed or deformed configuration. As the nonwoven material **20080** seeks to rebound, it can exert a springback or restoring force on the tissue also captured in the staple entrapment area **30039**, as described in greater detail herein. When the applied force is subsequently removed, the restoring force can cause the nonwoven material to rebound from the compressed configuration. In various embodiments, the nonwoven material **20080** can rebound to the initial, uncompressed configuration or may rebound to a configuration substantially similar to the initial, uncompressed configuration. In various embodiments, the deformation of the nonwoven material **20080** can be elastic. In some embodiments, the deformation of the nonwoven material can be partially elastic and partially plastic.

When a portion of the nonwoven material **20080** is compressed in a staple entrapment area **20039**, the crimped fibers **20086** in that portion of the nonwoven compensator **20039** can also be compressed or otherwise deformed. The amount a crimped fiber **20086** is deformed can correspond to the amount that the captured portion of the nonwoven material **20080** is compressed. For example, referring to FIG. 63, the nonwoven material **20080** can be captured by deployed staples **20030**. Where the nonwoven material **20080** is more compressed by a deployed staple **20030**, the average deformation of crimped fibers **20086** can be greater. Further, where the nonwoven material **20080** is less compressed by a deployed staple, the average deformation of crimped fibers **20086** can be smaller. Similarly, referring to FIGS. 82 and 83, in a staple entrapment area **20039d** where the nonwoven material **20080** is more compressed, the crimped fibers **20086** in that staple entrapment area **20039d** can be, on average, more deformed. Further, in a staple entrapment area **20039a** where the nonwoven material **20080** is less compressed, the crimped fibers **20086** in that staple entrapment area **20039a** can be, on average, less deformed.

The ability of the nonwoven material **20080** to rebound from the deformed configuration, i.e., the resiliency of the nonwoven material **20080**, can be a function of the resiliency of the crimped fibers **20086** in the nonwoven material **20080**. In various embodiments, the crimped fibers **20086** can deform elastically. In some embodiments, deformation of the crimped fibers **20086** can be partially elastic and partially plastic. In various embodiments, compression of each crimped fiber **20086** can cause the compressed crimped fibers **20086** to generate a springback or restoring force. For example, the compressed crimped fibers **20086** can generate a restoring force as the fibers **20086** seek to rebound from their compressed configuration. In various embodiments, the fibers **20086** can seek to return to their initial, uncompressed configuration or to a configuration substantially similar thereto. In some embodiments, the crimped fibers **20086** can seek to partially return to their initial configuration. In various embodiments, only a portion of the crimped fibers **20086** in the nonwoven material **20080** can be resilient. When a crimped fiber **20086** is comprised of a linear-elastic material, the restoring force of the compressed crimped fiber **20086** can be a function of the amount the crimped fiber **20086** is compressed and the spring rate of the crimped fiber **20086**, for

example. The spring rate of the crimped fiber **20086** can at least depend on the orientation, material, shape and/or size of the crimped fiber **20086**, for example.

In various embodiments, the crimped fibers **20086** in the nonwoven material **20080** can comprise a uniform spring rate. In other embodiments, the spring rate of the crimped fibers **20086** in the nonwoven material **20080** can vary. When a crimped fiber **20086** having a large spring rate is greatly compressed, the crimped fiber **20086** can generate a large restoring force. When a crimped fiber **20086** having the same large spring rate is less compressed, the crimped fiber **20086** can generate a smaller restoring force. The aggregate of restoring forces generated by compressed crimped fibers **20086** in the nonwoven material **20080** can generate a combined restoring force throughout the nonwoven material **20080** of the tissue thickness compensator **20020**. In various embodiments, the nonwoven material **20080** can exert the combined restoring force on tissue T captured within a fired staple **20030** with the compressed nonwoven material **20080**.

Furthermore, the number of crimped fibers **20086** per unit volume of nonwoven material **20080** can affect the spring rate of the nonwoven material **20080**. For example, the resiliency in a nonwoven material **20080** can be low when the number of crimped fibers **20086** per unit volume of nonwoven material **20080** is low, for example; the resiliency of the nonwoven material **20080** can be higher when the number of crimped fibers **20086** per unit volume of nonwoven material **20080** is higher, for example; and the resiliency of the nonwoven material **20080** can be higher still when the number of crimped fibers **20086** per unit volume of nonwoven material **20080** is even higher, for example. When the resiliency of the nonwoven material **20080** is low, such as when the number of crimped fibers **20086** per unit volume of nonwoven material **20080** is low, the combined restoring force exerted by the tissue thickness compensator **20020** on captured tissue T can also be low. When the resiliency of the nonwoven material **20080** is higher, such as when the number of crimped fibers **20086** per unit volume of nonwoven material **20080** is higher, the aggregate restoring force exerted by the tissue thickness compensator **20020** on captured tissue T can also be higher.

In various embodiments, referring primarily to FIG. 64, a nonwoven material **20080'** of a tissue thickness compensator **20020'** can comprise a therapeutic agent **20088**, such as a medicament and/or pharmaceutically active agent, for example. In various embodiments, the nonwoven material **20080'** can release a therapeutically effective amount of the therapeutic agent **20088**. For example, the therapeutic agent **20088** can be released as the nonwoven material **20080'** is absorbed. In various embodiments, the therapeutic agent **20088** can be released into fluid, such as blood, for example, passing over or through the nonwoven material **20080'**. Examples of therapeutic agents **20088** can include, but are not limited to, haemostatic agents and drugs such as, for example, fibrin, thrombin, and/or oxidized regenerated cellulose (ORC); anti-inflammatory drugs such as, for example, diclofenac, aspirin, naproxen, sulindac, and/or hydrocortisone; antibiotic and antimicrobial drugs or agents such as, for example, triclosan, ionic silver, ampicillin, gentamicin, polymyxin B, and/or chloramphenicol; and anticancer agents such as, for example, cisplatin, mitomycin, and/or adriamycin. In various embodiments, the therapeutic agent **20088** can comprise a biologic, such as a stem cell, for example. In some embodiments, the fibers **20082** of the nonwoven material **20080'** can comprise the therapeutic agent **20088**. In other embodiments, the therapeutic agent **20088** can be added to the nonwoven material **20080'** or otherwise integrated into the tissue thickness compensator **20020'**.

In some embodiments, primarily referring to FIGS. 70-70B, a tissue thickness compensator 20520 for an end effector 12 (FIG. 61) can comprise a plurality of springs or coiled fibers 20586. Similar to the crimped fibers 20086 described herein, the coiled fibers 20586 can be, for example, crimped, twisted, coiled, bent, crippled, spiraled, curled, and/or bowed within the tissue thickness compensator 20520. In some embodiments, the coiled fibers 20586 can be wound around a mandrel to form a coiled or substantially coil-like shape. Similar to the embodiments described herein, the coiled fibers 20586 can be randomly oriented and/or randomly distributed throughout the tissue thickness compensator 20520. In other embodiments, the coiled fibers 20586 can be systematically arranged and/or uniformly distributed throughout the tissue thickness compensator 20520. For example, referring to FIG. 70, the coiled fibers 20586 can comprise a longitudinal axis between a first end 20587 and a second end 20589 of the coiled fiber 20586. The longitudinal axes of the coiled fibers 20520 in the tissue thickness compensator 20520 can be parallel or substantially parallel. In some embodiments, the first end 20587 of each coiled fiber 20520 can be positioned along a first longitudinal side 20523 of the tissue thickness compensator 20520 and the second end 20589 of each coiled fiber 20586 can be positioned along a second longitudinal side 20524 of the tissue thickness compensator 20520. In such an arrangement, the coiled fibers 20586 can laterally traverse the tissue thickness compensator. In other embodiments, the coiled fibers 20586 can longitudinally or diagonally traverse the tissue thickness compensator 20520.

In various embodiments, similar to the crimped fibers 20086 described herein, the coiled fibers 20586 can comprise a polymeric composition. The crimped fibers 20586 can be at least partially elastic such that deformation of the crimped fibers 20586 generates a restoring force. In some embodiments, the polymeric composition of the coiled fibers 20586 can comprise polycaprolactone (PCL), for example, such that the coiled fibers 20586 are not soluble in a chlorophyll solvent. Referring to FIG. 70A, the springs or coiled fibers 20520 can be retained in a compensation material 20580. In various embodiments, the compensation material 20580 can hold the coiled fibers 20586 in a loaded position such that the coiled fibers 20586 exert a spring load on, or within, the compensation material 20580. In certain embodiments, the compensation material 20580 can hold the coiled fibers 20586 in a neutral position where the coiled fibers 20586 are not exerting a spring load on, or within, the compensation material 20580. The compensation material 20580 can be bioabsorbable and, in some embodiments, can comprise a foam, such as, for example, polyglycolic acid (PGA) foam. Furthermore, the compensation material 20580 can be soluble in a chlorophyll solvent, for example. In some embodiments the tissue thickness compensator can comprise coiled fibers 20586 that comprise polycaprolactone (PCL) and compensation material 20580 that comprises polyglycolic acid (PGA) foam, for example, such that the coiled fibers 20520 are not soluble in a chlorophyll solvent while the compensation material 20580 is soluble in the chlorophyll solvent. In various embodiments, the compensation material 20580 can be at least partially elastic, such that compression of the compensation material 20580 generates a restoring force. Further, similar to the embodiments described herein, referring to FIG. 70B, the compensation material 20580 of the tissue thickness compensator 20520 can comprise a therapeutic agent 20588, such as stem cells, for example. The compensation material 20580 can release a therapeutically

effective amount of the therapeutic agent 20588 as the compensation material 20580 is absorbed.

Similar to the tissue thickness compensator 20020 described herein, the tissue thickness compensator 20520 can be compressible. For example, as staples 20030 (FIGS. 78-81) are deployed from an initial position to a fired position, the staples 20030 can engage a portion of tissue thickness compensator 20520. In various embodiments, a staple 20030 can capture a portion of the tissue thickness compensator 20520 and adjacent tissue T. The staple 20030 can apply a compressive force to the captured portion of the tissue thickness compensator 20520 and tissue T such that the tissue thickness compensator 20520 is compressed from a non-compressed height to a compressed height. Similar to the embodiments described herein, compression of the tissue thickness compensator 20520 can result in a corresponding deformation of the coiled fibers 20586 therein. As described in greater detail herein, deformation of each coiled fiber 20586 can generate a restoring force that can depend on the resiliency of the coiled fiber, for example, the amount the coiled fiber 20586 is deformed and/or the spring rate of the coiled fiber 20586. The spring rate of the coiled fiber 20586 can at least depend on the orientation, material, shape and/or size of the coiled fiber 20586, for example. Deformation of the coiled fibers 20586 in the tissue thickness compensator 20520 can generate restoring forces throughout the tissue thickness compensator 20520. Similar to the embodiments described herein, the tissue thickness compensator 20520 can exert the aggregate restoring force generated by the deformed coiled fibers 20586 and/or the resilient compensation material 20586 on the captured tissue T in the fired staples 20030.

In some embodiments, primarily referring to FIGS. 71 and 72, a tissue thickness compensator 20620 for an end effector 12 can comprise a plurality of spring coils 20686. Similar to the crimped fibers 20086 and coiled fibers 20586 described herein, spring coils 20686 can be, for example, crimped, twisted, coiled, bent, crippled, spiraled, curled, and/or bowed within the tissue thickness compensator 20620. In various embodiments, similar to the fibers and coils described herein, the spring coils 20686 can comprise a polymeric composition. Further, the spring coils 20686 can be at least partially elastic such that deformation of the spring coils 20686 generates a restoring force. The spring coils 20686 can comprise a first end 20687, a second end 20689, and a longitudinal axis therebetween. Referring to FIG. 71, the first end 20686 of a spring coil 20686 can be positioned at or near a proximal end 20626 of the tissue thickness compensator and the second end 20689 of the same spring coil 20686 can be positioned at or near a distal end 20625 of the tissue thickness compensator 20620 such that the spring coil 20686 longitudinally traverses the tissue thickness compensator 20620, for example. In other embodiments, the coiled fibers 20686 can laterally or diagonally traverse the tissue thickness compensator 20620.

The tissue thickness compensator 20620 can comprise an outer film 20680 that at least partially surrounds at least one spring coil 20686. In various embodiments, referring to FIG. 71, the outer film 20680 can extend around the perimeter of multiple spring coils 20686 in the tissue thickness compensator 20620. In other embodiments, the outer film 20680 can completely encapsulate the spring coils 20686 or at least one spring coil 20686 in the tissue thickness compensator 20620. The outer film 20680 can retain the spring coils 20686 in the end effector 12. In various embodiments, the outer film 20680 can hold the spring coils 20686 in a loaded position such that the spring coils 20686 generate a spring load and exert a springback force on the outer film 20680. In other embodiments, the outer film 20680 can hold the spring coils 20686 in

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a neutral position. The tissue thickness compensator **20620** can also comprise a filling material **20624**. In some embodiments, the filling material **20624** can be retained within and/or around the spring coils **20686** by the outer film **20680**. In some embodiments, the filling material **20624** can comprise a therapeutic agent **20688**, similar to the therapeutic agents described herein. Further, the filling material **20624** can support the spring coils **20686** within the tissue thickness compensator **20620**. The filling material **20624** can be compressible and at least partially resilient, such that the filling material **20624** contributes to the springback or restoring force generated by the tissue thickness compensator **20620**, as described in greater detail herein.

Similar to the tissue thickness compensators described herein, the tissue thickness compensator **20620** can be compressible. As staples **20030** (FIGS. **78-81**) are deployed from an initial position to a fired position, in various embodiments, the staples **20030** can engage a portion of the tissue thickness compensator **20620**. In various embodiments, each staple **20030** can capture a portion of the tissue thickness compensator **20620** along with adjacent tissue T. The staple **20030** can apply a compressive force to the captured portion of the tissue thickness compensator **20620** and the captured tissue T such that the tissue thickness compensator **20620** is compressed between a non-compressed height and a compressed height. Similar to the embodiments described herein, compression of the tissue thickness compensator **20620** can result in a corresponding deformation of the spring coils **20686** retained therein (FIG. **72**). As described in greater detail herein, deformation of each spring coils **20686** can generate a restoring force that depends on the resiliency of the spring coil **20686**, for example, the amount the spring coil **20686** is deformed and/or the spring rate of the spring coil **20686**. The spring rate of a spring coil **20686** can at least depend on the material, shape and/or dimensions of the spring coil **20686**, for example. Furthermore, depending on the resiliency of the filling material **20624** and the outer film **20680**, compression of the filling material **20624** and/or the outer film **20680** can also generate restoring forces. The aggregate of restoring forces generated at least by the deformed spring coils **20686**, the filling material **20624** and/or the outer film **20680** in the tissue thickness compensator **20620** can generate restoring forces throughout the tissue thickness compensator **20620**. Similar to the embodiments described herein, the tissue thickness compensator **20620** can exert the aggregate restoring force generated by the deformed spring coils **20686** on the captured tissue T in a fired staple **20030**.

In various embodiments, primarily referring to FIGS. **73-75**, a tissue thickness compensator **20720** for an end effector **12** can comprise a plurality of spring coils **20786**. Similar to the coiled fibers and springs described herein, spring coils **20786** can be, for example, crimped, twisted, coiled, bent, crippled, spiraled, curled, and/or bowed within the tissue thickness compensator **20720**. The spring coils **20786** can be at least partially elastic such that deformation of the spring coils **20786** generates a restoring force. Further, the spring coils **20786** can comprise a first end **20787**, a second end **20789**, and a longitudinal axis therebetween. Referring primarily to FIG. **75**, the first end **20787** of the spring coil **20786** can be positioned at or near a proximal end **20726** of the tissue thickness compensator **20720** and the second end **20789** of the spring coil **20786** can be positioned at or near a distal end **20725** of the tissue thickness compensator **20720** such that the spring coil **20786** longitudinally traverses the tissue thickness compensator **20720**. In some embodiments, the spring coil **20786** can longitudinally extend in two parallel rows in the tissue thickness compensator **20720**. The tissue thickness

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compensator **20720** can be positioned in an end effector **12** such that a sled **20050** (FIG. **61**) or cutting element **20052** can translate along a slot **20015** between the parallel rows of spring coils **20786**. In other embodiments, similar to various embodiments described herein, the spring coils **20786** can laterally or diagonally traverse the tissue thickness compensator **20720**.

Referring again to FIG. **75**, the spring coils **20786** can be retained or embedded in a compensation material **20780**. The compensation material **20780** can be bioabsorbable and, in some embodiments, can comprise foam, such as, for example, polyglycolic acid (PGA) foam. In various embodiments, the compensation material **20780** can be resilient such that deformation of the compensation material **20780** generates a springback force. The compensation material **20780** can be soluble in a chlorophyll solvent, for example. In some embodiments, for example, the tissue thickness compensator can comprise spring coils **20786** that comprise polycaprolactone (PCL) and compensation material **20780** that comprises polyglycolic acid (PGA) foam such that the spring coils **20786** are not soluble in a chlorophyll solvent while the compensation material **20780** is soluble in a chlorophyll solvent, for example. The compensation material **20780** can be at least partially resilient such that deformation of the compensation material **20780** generates a spring load or restoring force.

In various embodiments, the tissue thickness compensator **20720** can comprise interwoven threads **20790**, which can extend between parallel rows of spring coils **20786**. For example, referring to FIG. **75**, a first interwoven thread **20790** can diagonally traverse the two parallel rows of spring coils **20786** and a second interwoven thread **20790** can also diagonally traverse the two parallel rows of spring coils **20786**. In some embodiments, the first and second interwoven threads **20790** can crisscross. In various embodiments, the interwoven threads **20790** can crisscross multiple times along the length of the tissue thickness compensator **20720**. The interwoven threads **20790** can hold the spring coils **20786** in a loaded configuration such that the spring coils **20786** are held in a substantially flat position in the tissue thickness compensator **20720**. In some embodiments, the interwoven threads **20790** that traverse the tissue thickness compensator **20720** can be directly attached to the spring coils **20786**. In other embodiments, the interwoven threads **20790** can be coupled to the spring coils **20786** via a support **20792** that extends through each spring coil **20786** along the longitudinal axis thereof.

As described in greater detail herein, in various embodiments, a staple cartridge **20000** can comprise a slot **20015** configured to receive a translating sled **20050** comprising a cutting element **20052** (FIG. **61**). As the sled **20050** translates along the slot **20015**, the sled **20050** can eject staples **20030** from fastener cavities **20012** in the staple cartridge **20000** and the cutting element **20052** can simultaneously or nearly simultaneously sever tissue T. In various embodiments, referring again to FIG. **75**, as the cutting element **20052** translates, it can also sever the interwoven threads **20790** that crisscross between the parallel rows of spring coils **20786** in the tissue thickness compensator **20720**. As the interwoven threads **20790** are severed, each spring coil **20786** can be released from its loaded configuration such that each spring coil **20786** reverts from the loaded, substantially flat position to an expanded position in the tissue thickness compensator **20720**. In various embodiments, when a spring coil **20786** is expanded, the compensation material **20780** surrounding the spring coil **20786** can also expand.

In various embodiments, as staples **20030** (FIGS. **78-81**) are deployed from an initial position to a fired position, the staples **20030** can engage a portion of the tissue thickness compensator **20720** and the tissue thickness compensator **20720** can expand, or attempt to expand, within the staples **20030** and can apply a compressive force to the tissue T. In various embodiments, at least one staple **20030** can capture a portion of the tissue thickness compensator **20720**, along with adjacent tissue T. The staple **20030** can apply a compressive force to the captured portion of the tissue thickness compensator **20720** and the captured tissue T, such that the tissue thickness compensator **20720** is compressed between a non-compressed height and a compressed height. Similar to the embodiments described herein, compression of the tissue thickness compensator **20720** can result in a corresponding deformation of the spring coils **20786** and compensation material **20780** retained therein. As described in greater detail herein, deformation of each spring coils **20786** can generate a restoring force that can depend on the resiliency of the spring coil, for example, the amount the spring coil **20786** is deformed and/or the spring rate of the spring coil **20786**. The spring rate of a spring coil **20786** can at least depend on the orientation, material, shape and/or size of the spring coil **20786**, for example. The aggregate of restoring forces generated by at least the deformed spring coils **20786** and/or the compensation material **30380** in the tissue thickness compensator **20720** can generate restoring forces throughout the tissue thickness compensator **20720**. Similar to the embodiments described herein, the tissue thickness compensator **20720** can exert the aggregate restoring force generated by the deformed spring coils **20786** in the tissue thickness compensator **20720** on the captured tissue T and fired staples **20030**.

In various embodiments, primarily referring to FIGS. **76** and **77**, a tissue thickness compensator **20820** for a surgical end effector **12** can comprise a spring coil **20886**. Similar to the fibers and coils described herein, spring coil **20886** can be, for example, crimped, twisted, coiled, bent, crippled, spiraled, curled, and/or bowed within the tissue thickness compensator **20820**. The spring coil **20886** can comprise a polymeric composition and can be at least partially elastic, such that deformation of the spring coil **20886** generates a spring-back force. Further, the spring coil **20886** can comprise a first end **20887** and a second end **20889**. Referring to FIG. **76**, the first end **20887** can be positioned at or near a proximal end **20826** of the tissue thickness compensator **20820** and the second end **20889** can be positioned at or near a distal end **20825** of the tissue thickness compensator **20820**. The spring coil **20886** can wind or meander from the proximal end **20825** to the distal end **20826** of the tissue thickness compensator **20820**.

Referring again to FIG. **76**, the spring coil **20886** can be retained or embedded in a compensation material **20880**. The compensation material **20880** can be bioabsorbable and, in some embodiments, can comprise a foam, such as, for example, polyglycolic acid (PGA) foam. The compensation material **20880** can be soluble in a chlorophyll solvent, for example. In some embodiments, the tissue thickness compensator can comprise spring coils **20886** comprising polycaprolactone (PCL) and compensation material **20880** comprising polyglycolic acid (PGA) foam, for example, such that the spring coil **20886** is not soluble in a chlorophyll solvent while the compensation material **20880** is soluble in a chlorophyll solvent. The compensation material **20880** can be at least partially resilient such that deformation of the compensation material **20880** generates a spring load or restoring force.

Similar to tissue thickness compensators described herein, for example, the tissue thickness compensator **20820** can be compressible. Compression of the tissue thickness compensator **20820** can result in a deformation of at least a portion of the spring coil **20886** retained or embedded in the compensation material **20880** of the tissue thickness compensator **20820**. As described in greater detail herein, deformation of the spring coil **20886** can generate restoring forces that can depend on the resiliency of the spring coil **20886**, the amount the spring coil **20886** is deformed, and/or the spring rate of the spring coil **20886**, for example. The aggregate of restoring forces generated by the deformed spring coil **20886** and/or deformed compensation material **20880** can generate restoring forces throughout the tissue thickness compensator **20820**. The tissue thickness compensator **20820** can exert the aggregate restoring force on the captured tissue T in the fired staples **20030**.

Referring now to FIG. **84**, a surgical end effector **12** can comprise a tissue thickness compensator **30020** having at least one tubular element **30080**. The tissue thickness compensator **30020** can be retained in the surgical end effector **12**. As described in greater detail herein, a fastener in the end effector **12** can be deployed such that the fastener moves to a fired position and deforms at least a portion of the tubular element **30080** in the tissue thickness compensator **30020**. The reader will appreciate that tissue thickness compensators comprising at least one tubular element as described herein can be installed in or otherwise engaged with a variety of surgical end effectors and that such embodiments are within the scope of the present disclosure.

In various embodiments, still referring to FIG. **84**, the tissue thickness compensator **30020** can be positioned relative to the anvil **30060** of the end effector **12**. In other embodiments, the tissue thickness compensator **30020** can be positioned relative to a fastener cartridge assembly, such as staple cartridge **30000**, of the end effector **12**. In various embodiments, the staple cartridge **30000** can be configured to fit in a cartridge channel **30072** of a jaw **30070** of the end effector **12**. For example, the tissue thickness compensator **30020** can be releasably secured to the staple cartridge **30000**. In at least one embodiment, the tubular element **30080** of the tissue thickness compensator **30020** can be positioned adjacent to a top deck surface **30011** of a rigid support portion **30010** of the staple cartridge **30000**. In various embodiments, the tubular element **30080** can be secured to the top deck surface **30011** by an adhesive or by a wrap, similar to at least one of the wraps described herein (e.g., FIG. **16**). In various embodiments, the tissue thickness compensator **30020** can be integral to an assembly comprises the staple cartridge **30000** such that the staple cartridge **30000** and the tissue thickness compensator **30020** are formed as a single unit construction. For example, the staple cartridge **30000** can comprise a first body portion, such as the rigid support portion **30010**, and a second body portion, such as the tissue thickness compensator **30020**, for example.

Referring to FIGS. **84-86**, the tubular element **30080** in the tissue thickness compensator **30020** can comprise an elongate portion **30082** having at least one lumen **30084** that extends at least partially therethrough. Referring primarily to FIG. **86**, the elongate portion **30082** of the tubular element **30080** can comprise woven or braided strands **30090**, as described in greater detail herein. In other embodiments, the elongate portion **30082** can comprise a solid structure, such as a polymer extrusion, rather than woven strands **30090**. The elongate portion **30082** of the tubular element **30080** can comprise a thickness. In various embodiments, the thickness of the elongate portion **30082** can be substantially uniform

throughout the length and around the diameter thereof; in other embodiments, the thickness can vary. The elongate portion **30082** can be elongated such that the length of the elongate portion **30082** is greater than the diameter of the elongate portion **30082**, for example. In various embodiments, the elongate portion can comprise a length of approximately 1.20 inches to approximately 2.60 inches and a diameter of approximately 0.10 inches to approximately 0.15 inches, for example. In some embodiments, the length of the tubular element **30080** can be approximately 1.40 inches, for example, and the diameter of the tubular element **30080** can be approximately 0.125 inches, for example. Furthermore, the elongate portion **30082** can define a substantially circular or elliptical cross-sectional shape, for example. In other embodiments, the cross-sectional shape can comprise a polygonal shape, such as, for example, a triangle, a hexagon and/or an octagon. Referring again to FIG. **84**, the tubular element **30080** can comprise a first distal end **30083** and a second proximal end **30085**. In various embodiments, the cross-sectional shape of the elongate portion **30082** can narrow at the first and/or second end **30083**, **30085** wherein at least one end **30083**, **30085** of the tubular element **30080** can be closed and/or sealed. In other embodiments, a lumen **30084** can continue through the distal ends **30083**, **30085** of the tubular element **30080** such that the ends **30083**, **30085** are open.

In various embodiments, the tubular element **30080** can comprise a single central lumen **30084** that extends at least partially through the elongate portion **30084**. In some embodiments, the lumen **30084** can extend through the entire length of the elongate portion **30084**. In still other embodiments, the tubular element **30080** can comprise multiple lumens **30084** extending therethrough. Lumens **30084** extending through the tubular element **30080** can be circular, semi-circular, wedge-shaped, and/or combinations thereof. In various embodiments, a tubular element **30080** can also comprise support webs that can form a modified "T" or "X" shape, for example, within the lumen **30084**. In various embodiments, the dimensions, lumen(s), and/or support web(s) within the tubular element **30080** can define the cross-sectional shape of the tubular element **30080**. The cross-sectional shape of the tubular element **30080** can be consistent throughout the length thereof or, in other embodiments, the cross-sectional shape of the tubular element **30080** can vary along the length thereof. As described in greater detail herein, the cross-sectional shape of the tubular element **30080** can affect the compressibility and resiliency of the tubular element **30080**.

In various embodiments, the tubular element **30080** can comprise a vertical diameter and a horizontal diameter; the dimensions thereof can be selected depending on the arrangement of the tubular element **30080** in the end effector **12**, the dimensions of the end effector **12**, including the tissue gap of the end effector **12**, and the expected geometry of the staple entrapment areas **30039**. For example, the vertical diameter of the tubular element **30080** can relate to the expected height of a formed staple. In such embodiments, the vertical diameter of the tubular element **30080** can be selected such that the vertical diameter can be reduced approximately 5% to approximately 20% when the tubular element **30080** is captured within a formed staple **30030**. For example, a tubular element **30080** having a vertical diameter of approximately 0.100 inches may be used for staples having an expected formed height of approximately 0.080 inches to approximately 0.095 inches. As a result, the vertical diameter of the tubular element **30080** can be reduced approximately 5% to approximately 20% when captured within the formed staple

30030 even when no tissue **T** is captured therein. When tissue **T** is captured within the formed staple **30030**, the compression of the tubular element **30080** may be even greater. In some embodiments, the vertical diameter can be uniform throughout the length of the tubular element **30080** or, in other embodiments, the vertical diameter can vary along the length thereof.

In some embodiments, the horizontal diameter of the tubular element **30080** can be greater than, equal to, or less than the vertical diameter of the tubular element **30080** when the tubular element **30080** is in an undeformed or rebounded configuration. For example, referring to FIG. **85**, the horizontal diameter can be approximately three times larger than the vertical diameter, for example. In some embodiments the horizontal diameter can be approximately 0.400 inches and the vertical diameter can be approximately 0.125 inches, for example. In other embodiments, referring now to FIG. **87**, the horizontal diameter of a tubular element **31080** can be equal to or substantially equal to the vertical diameter of the tubular element **31080** when the tubular element **31080** is in an undeformed or rebounded configuration. In some embodiments the horizontal diameter can be approximately 0.125 inches and the vertical diameter can also be approximately 0.125 inches, for example. In various embodiments, the tubular element **30080** can comprise a vertical diameter of approximately 0.125 inches, a horizontal diameter of approximately 0.400 inches, and a length of approximately 1.400 inches. As described in greater detail herein, when a force **A** is applied to the tubular element **30080** and/or **31080**, the tubular element can deform such that the cross-sectional geometry, including the horizontal and vertical diameters, can change.

Referring again to FIGS. **84-86**, the tubular element **30080** in the tissue thickness compensator **30020** can be deformable. In various embodiments, the entire tubular element **30080** can be deformable. For example, the tubular element **30080** can be deformable from the proximal end **30083** to the distal end **30085** of the elongate portion **30082** and around the entire circumference thereof. In other embodiments, only a portion of the tubular element **30080** can be deformable. For example, in various embodiments, only an intermediate length of the elongate portion **30082** and/or only a portion of the circumference of the tubular element **30080** can be deformable.

When a compressive force is applied to a contact point on the elongate portion **30082** of the tubular element **30080**, the contact point can shift, which can alter the cross-sectional dimensions of the tubular element **30080**. For example, referring again to FIG. **85**, the tubular element **30080** can comprise a top apex **30086** and a bottom apex **30088** on the elongate portion **30082**. In the initial, undeformed configuration, the tubular element **30080** can comprise undeformed cross-sectional dimensions, including an undeformed vertical diameter between the top apex **30086** and the bottom apex **30088**. When a compressive force **A** is applied to the top apex **30086**, the tubular element **30080** can move to a deformed configuration. In the deformed configuration, the cross-sectional dimensions of the tube **30080** can be altered. For example, the tube **30086** can comprise a deformed vertical diameter between the top apex **30086** and the bottom apex **30088**, which can be less than the undeformed vertical diameter. In some embodiments, referring to FIG. **87**, the horizontal diameter of the deformed tube **30080** can be lengthened, for example, when the tubular element **30080** moves from an undeformed configuration to a deformed configuration. The deformed cross-sectional dimensions of the deformed tube **30080** can at least depend on the position, angular orientation, and/or magnitude of the applied force **A**. As described in

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greater detail herein, deformation of a tubular element **30080** can generate a springback or restoring force that can depend on the resiliency of the tubular element **30080**.

Referring still to FIG. **85**, the tubular element **30080** can generate a springback or restoring force when compressed. In such embodiments, as described herein, the tubular element **30080** can move from an initial undeformed configuration to a deformed configuration when a force A is applied to a contact point on the elongate portion **30082** of the tubular element **30080**. When the applied force A is removed, the deformed tube **30080** can rebound from the deformed configuration. The deformed tube **30080** may rebound to the initial, undeformed configuration or may rebound to a configuration substantially similar to the initial, undeformed configuration. The ability of the tubular element **30080** to rebound from a deformed configuration relates to the resiliency of the tubular element **30080**.

Referring again to FIG. **85**, a tubular element **30080** can exert a springback or restoring force. The restoring force can be generated by the tubular element **30080** when an applied force A is exerted on the tubular element **30080**, for example, by a staple **30030** (FIGS. **88** and **89**), as described in greater detail herein. An applied force A can alter the cross-sectional dimensions of the tubular element **30080**. Furthermore, in linear-elastic materials, the restoring force of each deformed portion of the tubular element **30080** can be a function of the deformed dimensions of the tubular element **30080** and the spring rate of that portion of the tubular element **30080**. The spring rate of a tubular element **30080** can at least depend on the orientation, material, cross-sectional geometry and/or dimensions of the tubular element **30080**, for example. In various embodiments, the tubular element **30080** in a tissue thickness compensator **30020** can comprise a uniform spring rate. In other embodiments, the spring rate can vary along the length and/or around the diameter of the tubular element **30080**. When a portion of a tubular element **30080** having a first spring rate is greatly compressed, the tubular element **30080** can generate a large restoring force. When a portion of the tubular element **30080** having the same first spring rate is less compressed, the tubular element **30080** can generate a smaller restoring force.

Referring again to FIG. **84**, the tubular element **30080** in the tissue thickness compensator **30020** can comprise a polymeric composition. In some embodiments, the elongate portion **30082** of the tubular element **30080** can comprise the polymeric composition. Further, in various embodiments, the polymeric composition can comprise an at least partially elastic material such that deformation of the tubular element **30080** generates a restoring force. The polymeric composition can comprise non-absorbable polymers, absorbable polymers, or combinations thereof, for example. Examples of synthetic polymers include, but are not limited to, polyglycolic acid (PGA), poly(lactic acid) (PLA), polycaprolactone (PCL), polydioxanone (PDO), and copolymers thereof. In some embodiments, the absorbable polymers can include bioabsorbable, biocompatible elastomeric polymers, for example. Furthermore, the polymeric composition of the tubular element **30080** can comprise synthetic polymers, non-synthetic polymers, or combinations thereof, for example. In various embodiments, similar to the polymeric compositions in embodiments described herein, the polymeric composition of the tubular element **30080** can include varied amounts of absorbable polymers, non-absorbable polymers, synthetic polymers, and/or non-synthetic polymers, for example, by weight percentage.

Referring to FIGS. **84** and **85**, the tubular element **30080** can comprise a therapeutic agent **30098** such as a pharmaceu-

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tically active agent or medicament, for example. In various embodiments, the therapeutic agent **30098** can be retained in the lumen **30084** of the tubular element **30080**. The elongate portion **30082** can encapsulate or partially encapsulate the therapeutic agent **30098**. Additionally or alternatively, the polymeric composition of the elongate portion **30082** can comprise the therapeutic agent **30098**. The tubular element **30080** can release a therapeutically effective amount of the therapeutic agent **30098**. In various embodiments, the therapeutic agent **30098** can be released as the tubular element **30080** is absorbed. For example, the therapeutic agent **30098** can be released into fluid (such as blood) passing over or through the tubular element **30080**. In still other embodiments, the therapeutic agent **30098** can be released when a staple **30030** (FIGS. **88** and **89**) pierces the tubular element **30080** and/or when the cutting element **30052** on the staple-firing sled **30050** (FIG. **84**) cuts a portion of the tubular element **30080**, for example. Examples of therapeutic agents **30098** can include, but are not limited to, haemostatic agents and drugs such as, for example, fibrin, thrombin, and/or oxidized regenerated cellulose (ORC), anti-inflammatory drugs such as, for example, diclofenac, aspirin, naproxen, sulindac, and/or hydrocortisone, antibiotic and antimicrobial drugs or agents such as, for example, triclosan, ionic silver, ampicillin, gentamicin, polymyxin B, and/or chloramphenicol, anticancer agents such as, for example, cisplatin, mitomycin, and/or adriamycin, and/or biologics such as, for example, stem cells.

In various embodiments, referring again to FIGS. **84**, **88** and **89**, fasteners such as staples **30030**, for example, can be deployed from a staple cartridge **30000** such that the staples **30030** engage a tissue thickness compensator **30020** and apply a force A to a tubular element **32080** therein. As described herein, application of a force A to the tubular element **30080** can cause deformation of the tubular element **30080**. Similar to the end effectors **12** described herein, the rigid support portion **30010** of the staple cartridge **30000** can comprise a cartridge body **30017**, a deck surface **30011**, and a plurality of staple cavities **30012** therein. Each staple cavity **30012** can define an opening in the deck surface **30011** and a staple **30030** can be removably positioned in a staple cavity **30012** (FIG. **104**). In at least one embodiment, referring primarily to FIGS. **88** and **89**, each staple **30030** can comprise a base **30031** and two staple legs **30032** extending from the base **30031**. Prior to the deployment of the staples **30030**, the base **30031** of each staple **30030** can be supported by a staple driver **30040** (FIG. **104**) positioned within the rigid support portion **30010** of the staple cartridge **30000**. Also prior to the deployment of the staples **30030**, the legs **30032** of each staple **30030** can be at least partially contained within the staple cavity **30012** (FIG. **104**).

In various embodiments, as described in greater detail herein, the staples **30030** can be deployed between an initial position and a fired position. For example, a staple-firing sled **30050** can engage a driver **30040** (FIG. **104**) to move at least one staple **30030** between the initial position and the fired position. In various embodiments, referring primarily to FIG. **88**, the staple **30030** can be moved to a fired position, wherein the legs **30032** of the staple **30030** engage a tubular element **32080** of a tissue thickness compensator **32020**, penetrate tissue T, and contact an anvil **30060** (FIG. **104**) positioned opposite the staple cartridge **30000** in the surgical end effector **12**. Staple forming pockets **30062** in the anvil **30060** can bend the staple legs **30032** such that the fired staple **30030** captures a portion of the tubular element **32080** and a portion of the tissue T in a staple entrapment area **30039**. As described in greater detail herein, at least one staple leg **30032** can pierce the tubular element **32080** of the tissue thickness com-

compensator **32020** when the staple **30030** moves between the initial position and the fired position. In other embodiments, the staple legs **30032** can move around the perimeter of the tubular element **32080** such that the staple legs **30032** avoid piercing the tubular element **32080**. Similar to the fasteners described herein, the legs **30032** of each staple **30030** can be deformed downwardly toward the base **30031** of the staple **30030** to form a staple entrapment area **30039** therebetween. The staple entrapment area **30039** can be the area in which tissue **T** and a portion of the tissue thickness compensator **32020** can be captured by a fired staple **30030**. In the fired position, each staple **30030** can apply a compressive force to the tissue **T** and to the tissue thickness compensator **32020** captured within the staple entrapment area **30039** of the staple **30030**.

In various embodiments, referring still to FIG. **88**, when the tubular element **32080** is captured in a staple entrapment area **30039**, the captured portion of the tubular element **32080** can be deformed, as described herein. Furthermore, the tubular element **32080** can be deformed to different deformed configurations in different staple entrapment areas **30039** depending on, for example, the thickness, compressibility, and/or density of the tissue **T** captured in that same staple entrapment area **30039**. In various embodiments, the tubular element **32080** in the tissue thickness compensator **32080** can extend longitudinally through successive staple entrapment areas **30039**. In such an arrangement, the tubular element **32080** can be deformed to different deformed configurations in each staple entrapment area **30039** along a row of fired staples **30030**. Referring now to FIG. **89**, tubular elements **33080** in a tissue thickness compensator **33020** can be laterally arranged in the staple entrapment areas **30039** along a row of fired staples **30030**. In various embodiments, the tubular elements **33080** can be retained by a flexible shell **33210**. In such arrangements, the tubular elements **33080** and flexible shell **33210** can be deformed to different deformed configurations in each staple entrapment area **30039**. For example, where the tissue **T** is thinner, the tubular elements **33080** can be compressed less and where the tissue **T** is thicker, the tubular elements **33080** can be compressed more to accommodate the thicker tissue **T**. In other embodiments, the deformed dimensions of the tubular elements **33080** can be uniform throughout the entire length and/or width of the tissue thickness compensator **33020**.

Referring to FIGS. **90-92**, in various embodiments, a tubular element **34080** in a tissue thickness compensator **34020** can comprise a plurality of strands **34090**. Referring primarily to FIG. **90**, in some embodiments, the strands **34090** can be woven or braided into a tubular lattice **34092** forming the tubular element **34080**. The tubular lattice **34092** formed by the strands **34090** can be substantially hollow. The strands **34090** of the tubular element **34080** can be solid strands, tubular strands, and/or another other suitable shape. For example, referring to FIG. **91**, a single strand **34090** of the tubular lattice **34092** can be a tube. In various embodiments, referring to FIG. **93**, a strand **34090** can comprise at least one lumen **34094** extending therethrough. The number, geometry and/or dimensions(s) of the lumens **34094** can determine the cross-sectional shape of the strand **34090**. For example, a strand **34090** can comprise circular lumen(s), semi-circular lumen(s), wedge-shaped lumen(s), and/or combinations thereof. In various embodiments, a strand **34090** can also comprise support webs **34096** that can form a modified “T” or “X” shape, for example. At least the diameter of the strand **34090**, the lumen(s) extending therethrough, and the support web(s) can characterize the cross-sectional shape of a strand **34090**. The cross-sectional shape of each strand **34090**, as

discussed in greater detail herein, can affect the springback or restoring force generated by the strand **34090** and the corresponding springback or restoring force generated by the tubular element **34080**.

Referring to FIG. **94**, a tubular lattice **34092** of strands **34090** can be deformable. In various embodiments, the tubular lattice **34092** can produce or contribute to the deformability and/or the resiliency of the tubular element **34080**. For example, the strands **34090** of the tubular lattice **34092** can be woven together such that the strands **34090** are configured to slide and/or bend relative to each other. When a force is applied to the elongate portion **34082** of the tubular element **34080**, the strands **34090** therein may slide and/or bend such that the tubular lattice **34092** moves to a deformed configuration. For example, referring still to FIG. **94**, a staple **30030** can compress the tubular lattice **34092** and the tissue **T** captured in a staple entrapment area **34039** which can cause the strands **34090** of the tubular lattice **34092** to slide and/or bend relative to each other. A top apex **34086** of the tubular lattice **34092** can move towards a bottom apex **34088** of the tubular lattice **34092** when the tubular lattice **34092** is compressed to the deformed configuration in order to accommodate the captured tissue **T** in a staple entrapment area **30039**. In various circumstances, the tubular lattice **34092** captured in a fired stapled **30030** will seek to regain its undeformed configuration and can apply a restoring force to the captured tissue **T**. Further, the portions of the tubular lattice **34092** positioned between staple entrapment areas **30039**, i.e., not captured within a fired staple **30030**, can also be deformed due to the deformation of adjacent portions of the tubular lattice **34092** that are within the staple entrapment areas **30039**. Where the tubular lattice **34092** is deformed, the tubular lattice **34092** can seek to rebound or partially rebound from the deformed configuration. In various embodiments, portions of the tubular lattice **34092** can rebound to their initial configurations and other portions of the tubular lattice **34092** can only partially rebound and/or remain fully compressed.

Similar to the description of the tubular elements herein, each strand **34090** can also be deformable. Further, deformation of a strand **34090** can generate a restoring force that depends on the resiliency of each strand **34090**. In some embodiments, referring primarily to FIGS. **91** and **92**, each strand **34090** of a tubular lattice **34092** can be tubular. In other embodiments, each strand **34090** of a tubular lattice **34092** can be solid. In still other embodiments, the tubular lattice **30092** can comprise at least one tubular strand **34090**, at least one solid strand **34090**, at least one “X”- or “T”-shaped strand **34090**, and/or a combination thereof.

In various embodiments, the strands **34090** in the tubular element **34080** can comprise a polymeric composition. The polymeric composition of a strand **34090** can comprise non-absorbable polymers, absorbable polymers, or combinations thereof. Examples of synthetic polymers include, but are not limited to, polyglycolic acid (PGA), poly(lactic acid) (PLA), polycaprolactone (PCL), polydioxanone (PDO), and copolymers thereof. In some embodiments, the absorbable polymers can include bioabsorbable, biocompatible elastomeric polymers, for example. Furthermore, the polymeric composition of the strand **34090** can comprise synthetic polymers, non-synthetic polymers, and/or combinations thereof. In various embodiments, similar to the polymeric compositions in embodiments described herein, the polymeric composition of the strand **34090** can include varied amounts of absorbable polymers, non-absorbable polymers, synthetic polymers, and/or non-synthetic polymers, for example, by weight percentage.

The strands **34090** in the tubular element **34080** can further comprise a therapeutic agent **34098** (FIG. **91**) such as a pharmaceutically active agent or medicament, for example. In some embodiments, the strand **34090** can release a therapeutically effective amount of the therapeutic agent **34098**. In various embodiments, the therapeutic agent **34098** can be released as the tubular strand **34090** is absorbed. For example, the therapeutic agent **34098** can be released into fluid, such as blood for example, passing over or through the strand **34090**. In still other embodiments, the therapeutic agent **34098** can be released when a staple **30030** pierces the strand **34090** and/or when the cutting element **30052** on the staple-firing sled **30050** (FIG. **84**) cuts a portion of the tubular lattice **34092**, for example. Examples of therapeutic agents **34098** can include, but are not limited to, haemostatic agents and drugs such as, for example, fibrin, thrombin, and/or oxidized regenerated cellulose (ORC), anti-inflammatory drugs such as, for example, diclofenac, aspirin, naproxen, sulindac, and/or hydrocortisone, antibiotic and antimicrobial drugs or agents such as, for example, triclosan, ionic silver, ampicillin, gentamicin, polymyxin B, and/or chloramphenicol, anticancer agents such as, for example, cisplatin, mitomycin, and/or adriamycin; and/or biologics such as, for example, stem cells.

Referring to FIGS. **95** and **96**, a tubular element **35080** can comprise multiple layers **35100** of strands **35090**. In some embodiments, the tubular element **35080** can comprise multiple layers **35100** of tubular lattices **35092**. Referring to FIG. **95**, the tubular element **35080** can comprise a first layer **35100a** and a second layer **35100b** of strands **35090**, for example. Referring now to FIG. **96**, a tubular element **35180** of a tissue thickness compensator **35120** can comprise a third layer **35100c** of strands **35090**, for example. Furthermore, different layers **35100** in the tubular element **35180** can comprise different materials. In some embodiments, each layer **35100a**, **35100b**, **35100c** can be bioabsorbable, wherein, in at least one embodiment, each layer **35100a**, **35100b**, **35100c** can comprise a different polymeric composition. For example, the first layer **35100a** can comprise a first polymeric composition; the second layer **35100b** can comprise a second polymeric composition; and the third layer **35100c** can comprise a third polymeric composition. In such embodiments, layers **35100a**, **35100b**, **35100c** of the tubular element **35180** can be bioabsorbed at different rates. For example, the first layer **35100a** can absorb quickly, the second layer **35100b** can absorb slower than the first layer **35100a**, and the third layer **35100c** can absorb slower than the first layer **35100a** and/or the second layer **35100b**. In other embodiments, the first layer **35100a** can absorb slowly, the second layer **35100b** can absorb faster than the first layer **35100a**, and the third layer **35100c** can absorb faster than the first layer **35100a** and/or the second layer **35100b**.

Similar to strands **34090** described herein, the strands **35090** in the tubular element **35180** can comprise a medicament **35098**. In various embodiments, referring again to FIG. **95**, to control elution or release of the medicament(s) **35098**, the first layer **35100a** of strands **35090** comprising a medicament **35098a** can be bioabsorbed at a first rate and the second layer **35100b** of strands **35090** comprising a medicament **35098b** can be bioabsorbed at a second rate. For example, the first layer **35100a** can absorb quickly to allow for a rapid initial release of the medicament **35098a** and the second layer **35100b** can absorb slower to allow controlled release of the medicament **35098b**. The medicament **35098a** in the strands **35090** of the first layer **35100a** can be different than the medicament **35098b** in the strands **35090** of the second layer **35100b**. For example, the strands **35090** in the first layer **35100a** can comprise oxidized regenerated cellulose (ORC)

and the strands **35090** in the second layer **35100b** can comprise a solution comprising hyaluronic acid. In such embodiments, initial absorption of the first layer **35100a** can release oxidized regenerated cellulose to help control bleeding while subsequent absorption of the second layer **35100b** can release a solution comprising hyaluronic acid to help prevent the adhesion of tissue. In other embodiments, the layers **35100a**, **35100b** can comprise the same medicament **35098a**, **35098b**. For example, referring again to FIG. **96**, strands **35090** in layers **35100a**, **35100b** and **35100c** can comprise an anticancer agent, such as, for example, cisplatin. Furthermore, the first layer **35100a** can absorb quickly to allow for a rapid initial release of cisplatin, the second layer **35100b** can absorb slower to allow for a controlled release of cisplatin, and the third layer **35100c** can absorb slowest to allow for a more extended, controlled release of cisplatin.

In various embodiments, referring to FIGS. **97** and **98**, a tissue thickness compensator **36020** can comprise an overmold material **36024**. The overmold material **36024** can be formed outside a tubular element **36080**, inside a tubular element **36080**, or both inside and outside a tubular element **36080**. In some embodiments, referring to FIG. **97**, the overmold material **36024** can be coextruded both inside and outside the tubular element **36080** and, in at least one embodiment, the tubular element **36080** can comprise a tubular lattice **36092** of strands **36090**. Similar to the polymeric composition described herein, the overmold material **36024** can comprise polyglycolic acid (PGA), poly(lactic acid) (PLA), and/or any other suitable, bioabsorbable and biocompatible elastomeric polymers, for example. Further, the overmold material **36024** can be non-porous such that the overmold material **36024** forms a fluid-impervious layer in the tubular element **36080**. In various embodiments, the overmold material **36024** can define a lumen **36084** therethrough.

Further to the discussion above, the tubular element **36080** and/or the strands **36090** in a tubular lattice **36092** can comprise a therapeutic agent **36098**. In some embodiments, referring still to FIGS. **97** and **98**, a non-porous overmold material **36024** can contain the medicament **36098** within an inner lumen **36084a**. Alternatively or additionally, the non-porous, overmold material **36024** can contain the medicament **36098** within an intermediate lumen **36084b**, such as, for example, the intermediate lumen **36084b** that contains the tubular lattice **36092** of medicament-comprising strands **36090**. Similar to the above, the tubular element **36080** can be positioned relative to staple cavities **30012** and a cutting element **30052** in staple cartridge **30000** (FIG. **84**). In several such embodiments, the deployment of the staples **30030** and/or the translation of the cutting element **30052** can be configured to pierce or rupture the non-porous, overmold material **36024** such that the medicament **36098** contained in at least one lumen **36084** of the tubular element **36080** can be released from the lumen **36084**. In various embodiments, referring to FIG. **99**, a tubular element **37080** can comprise a non-porous film **37110**. The non-porous film **37110** can at least partially surround a tubular lattice **37092** or a first layer **37100a** and a second layer **37100b** of tubular lattices **30092** to provide a fluid-impervious cover similar to the overmold material **36024** described herein.

As described herein, a tubular element can comprise at least one of a bioabsorbable material, a therapeutic agent, a plurality of strands, a tubular lattice, layers of tubular lattices, an overmold material, a non-porous film, or combinations thereof. For example, referring to FIG. **100**, a tubular element **38080** can comprise an overmold material **38024** and a plurality of strands **38090** positioned through a central lumen **38084** of the tubular element **38080**. In some embodi-

ments, the strands **38090** can comprise a therapeutic agent **38098**. In other embodiments, for example, referring to FIG. **101**, a tubular element **39080** can comprise an overmold material **39024** and a therapeutic agent **39098** positioned in a central lumen **39084** of the tubular element **39080**, for example. In various embodiments, at least one of the tubular element **39080** and overmold material **39024** can comprise a fluidic therapeutic agent **39098**.

In various embodiments, referring again primarily FIG. **84**, the tubular element **30080** can be positioned relative to the rigid support portion **30010** of the staple cartridge **30000**. The tubular element **30080** can be longitudinally positioned adjacent to the rigid support portion **30010**. In some embodiments, the tubular element **30080** can be substantially parallel to or aligned with a longitudinal slot or cavity **30015** in the rigid support portion **30010**. The tubular element **30080** can be aligned with the longitudinal slot **30015** such that a portion of the tubular element **30080** overlaps a portion of the longitudinal slot **30015**. In such embodiments, a cutting element **30052** on the staple-firing sled **30050** can sever a portion of the tubular element **30080** as the cutting edge **30052** translates along the longitudinal slot **30015**. In other embodiments, the tubular element **30080** can be longitudinally positioned on a first or second side of the longitudinal slot **30015**. In still other embodiments, the tubular element **30080** can be positioned relative to the rigid support portion **30010** of the staple cartridge **30000** such that the tubular element **30080** laterally or diagonally traverses at least a portion of the rigid support portion **30010**.

In various embodiments, referring to FIG. **102** for example, a tissue thickness compensator **40020** can comprise multiple tubular elements **40080**. In some embodiments, the tubular elements **40080** can comprise different lengths, cross-sectional shapes, and/or materials, for example. Further, the tubular elements **40080** can be positioned relative to the rigid support portion **40010** of the staple cartridge **30000** such that the tubular axes of the tubular elements **40080** are parallel to each other. In some embodiments, the tubular axes of tubular elements **40080** can be longitudinally aligned such that a first tubular element **40080** is positioned within another tubular element **40080**. In other embodiments, parallel tubular elements **40080** can longitudinally traverse the staple cartridge **30000**, for example. In still other embodiments, parallel tubular elements **40080** can laterally or diagonally traverse the staple cartridge **30000**. In various other embodiments, non-parallel tubular elements **40080** can be angularly-oriented relative to each other such that their tubular axes intersect and/or are not parallel to each other.

Referring to FIGS. **102-105**, a tissue thickness compensator **40020** can have two tubular elements **40080**; a first tubular element **40080a** can be longitudinally positioned on a first side of the longitudinal slot **30015** in the rigid support portion **30010** and a second tubular element **40080b** can be longitudinally positioned on a second side of the longitudinal slot **30015**. Each tubular element **40080** can comprise a tubular lattice **40092** of strands **40090**. In various embodiments, the staple cartridge **30000** can comprise a total of six rows of staple cavities **30012**, wherein three rows of staple cavities **30012** are positioned on each side of the longitudinal slot **30015**, for example. In such embodiments, the cutting edge **30052** on the translating staple-firing sled **30050** may not be required to sever a portion of the tubular element **40080**.

Similarly, referring now to FIGS. **106-107**, a tissue thickness compensator **41020** can comprise two tubular elements **41080a**, **41080b** longitudinally arranged in the staple cartridge **30000**. Similar to the above, staples **30030** from three rows of staple cavities **30012** can engage one tubular element

41080a and staples **30030** from three different rows of staple cavities **30012** can engage another tubular element **41080b**. In various embodiments, referring still to FIGS. **106-107**, deployed staples **30030** can engage the tubular element **40080** at different locations across the cross-section of the tubular element **40080**. As discussed herein, the springback resiliency and corresponding restoring force exerted by the tubular element **41080** can depend on the cross-sectional shape of the tubular element **41080**, among other things. In some embodiments, a staple **30030** positioned in a staple entrapment area **30039** located at or near an arced portion of the tubular element **41080** can experience a greater restoring force than a staple **30030** in a staple entrapment area **30039** positioned near a non-arced portion. Similarly, a staple **30030** positioned in staple entrapment area **30039** in the non-arced portion of the tubular element **41080** can experience a lesser restoring force than the restoring force experienced by a staple **30030** positioned at or nearer to the arced portion of the tubular element **30080**. In other words, the arced portions of a tubular element **41080** can have a greater spring rate than the non-arced portion of the tubular element **41080** owing to the possibility that a larger quantity of elastic material may be captured by the staples **30030** along such portions. In various embodiments, as a result, referring primarily to FIG. **107**, the restoring force generated by the tissue thickness compensator **41020** can be greater near staples **30030a** and **30030c** and less near staple **30030b** in tubular element **30080a**. Correspondingly, the restoring force generated by the tissue thickness compensator **41020** can be greater near staples **30030d** and **30030f** than near staple **30030e** in tubular element **30080b**.

Referring again to FIGS. **102-105**, in various embodiments, the cross-sectional geometries of strands **40090** comprising the tubular lattice **40092** can be selected in order to provide a desired springback resiliency and corresponding restoring force exerted by the tubular lattice **40092**. For example, referring again to FIG. **103**, strands **40090a** positioned in arced portions of the tubular element **40080** can comprise X-shaped cross-sections, whereas strands **40090b** positioned in non-arced portions of the tubular element **40080** can comprise tubular cross-sections. In some embodiments, strands **40090a** and **40090b** comprising different cross-sectional geometries can be woven together to form the tubular lattice **40092**. In other embodiments, the strands **40090a** and **40090b** can be attached to one another with an adhesive, for example. Referring to FIGS. **104** and **105**, the different cross-sectional geometries of strands **40090** in the tubular element **40080** can optimize the restoring force experienced in staple entrapment areas **30039** across the staple cartridge **30000**. In some embodiments, specific cross-sectional geometries can be selected such that the springback constant in staple entrapment areas **30039** across the staple cartridge is substantially balanced or equal.

In some embodiments, referring to FIG. **108**, the tubular elements **41080a**, **41080b** of a tissue thickness compensator **41120** can be fastened together by an adjoining portion **41126**. Though the translating cutting element **30052** can be configured to pass between tubular elements **41080a** and **41080b**, the cutting element **30052** can be required to sever at least a portion of the adjoining portion **41126**. In some embodiments, the adjoining portion **41126** can comprise a soft material, such as, for example, a foam or gel, which is easily severed by the translating cutting element **30052**. In various embodiments, the adjoining portion **41026** can releasably secure the tissue thickness compensator **41120** to the surgical end effector **12**. In at least one embodiment, the adjoining portion **41126** can be fixed to the top deck surface **30011** of the rigid support portion **30010** such that the adjoining

ing portion **41126** remains retained in the surgical end effector **12** after the tubular elements **41080a**, **41080b** are released therefrom.

In various embodiments, referring to FIGS. **109-110**, a tissue thickness compensator **42020** can comprise multiple tubular elements **42080** such that the number of tubular elements **42080** is the same as the number of rows of staple cavities **30012** in the staple cartridge **30000**, for example. In at least one embodiment, the staple cartridge **30000** can comprise six rows of staple cavities **30012** and the tissue thickness compensator **42020** can comprise six tubular elements **42080**. Each tubular element **42080** can be substantially aligned with a row of staple cavities **30012**. When staples **30030** are ejected from a row of staple cavities **30012**, each staple **30030** from that row can pierce the same tubular element **42080** (FIG. **110**). In various embodiments, the deformation of one tube **42080** can have little or no impact on the deformation of an adjacent tube **42080**. Accordingly, the tubular elements **42080** can exert a substantially discrete and customized springback force in staple entrapment areas **30039** across the width of the staple cartridge **30030**. In some embodiments, where staples **30030** fired from multiple rows of staple cavities **30012** engage the same tubular element **35080** (FIG. **107**), the deformation of the tubular element **35080** can be less customized. For example, the deformation of a tubular element **35080** in a staple entrapment area **30039** in a first row can impact the deformation of that tubular element **35080** in staple entrapment area **30039** in another row. In at least one embodiment, the translating cutting edge **30052** can avoid severing the tubular elements **42080**. In other embodiments, referring to FIG. **111**, a tissue thickness compensator **43020** can comprise more than six tubular elements **43080**, such as, for example, seven tubular elements **44080**. Further, the tubular elements **43080** can be symmetrically or non-symmetrically arranged in the end effector **12**. When an odd number of tubular elements **43080** are longitudinally and symmetrically arranged in the end effector **12**, the translating cutting element **30052** can be configured to sever the middle tubular element that overlies the longitudinal channel **30015**.

In various embodiments, referring to FIG. **112**, a tissue thickness compensator **44020** can comprise a central tubular element **44080b** that is at least partially aligned with the longitudinal slot **30015** in the rigid support portion **33010** of the staple cartridge **30000**. The tissue thickness compensator **44020** can further comprise at least one peripheral tubular element **44080a**, **44080c** located on a side of the longitudinal slot **30015**. For example, the tissue thickness compensator **44020** can comprise three tubular elements **44080**: a first peripheral tubular element **44080a** can be longitudinally positioned on a first side of the longitudinal slot **30015** of the staple cartridge **30000**, a central tubular element **44080b** can be substantially positioned over and/or aligned with the longitudinal slot **30015**, and a second peripheral tubular element **44080c** can be longitudinally positioned on a second side of the longitudinal slot **30015**. In some embodiments, the central tubular element **44080b** can comprise a horizontal diameter that is substantially elongated relative to the vertical diameter. In various embodiments, the central tubular element **44080b**, and/or any other tubular element, can overlap multiples rows of staple cavities **30012**. Referring still to FIG. **112**, the central tubular element **44080b** can overlap four staple rows of staple cavities **30012** and each peripheral tubular element **44080a**, **44080c** can overlap a single row of staple cavities **30012**, for example. In other embodiments, the central tubular element **44080b** can overlap less than four rows of staple cavities **30012**, such as, for example, two rows of staple cavities **30012**, for example. Further, peripheral tubular ele-

ments **44080a**, **44080c** can overlap more than one row of staple cavities **30012**, such as, for example, two rows of staple cavities **30012**. Referring now to FIG. **113**, a central tubular element **44180b** of a tissue thickness compensator **44120** can comprise a therapeutic agent **44198** in a lumen **44184** of the central tubular element **44180b**. In various embodiments, central tubular element **44180b** and/or at least one peripheral tubular element **44080a**, **44080c** can comprise the therapeutic agent **44198** and/or any other suitable therapeutic agent.

In various embodiments, referring to FIG. **114**, the tissue thickness compensator **44220** can comprise a shell **44224**, which can be similar to overmold material **32024** described herein. In various embodiments, the shell **44224** retains multiple tubular elements **44080** in position in the end effector **12**. The shell **44224** can be coextruded with the tubular elements **44080**. In some embodiments, the tubular elements **44080** can comprise a tubular lattice **44092** of strands **44090**. Similar to the polymeric compositions described in embodiments herein, the shell **44224** can comprise polyglycolic acid (PGA), poly(lactic acid) (PLA), and/or any other suitable bioabsorbable, biocompatible elastomeric polymers, for example. Further, the shell **44224** can be non-porous such that the shell **44224** forms a fluid-impervious layer in the tissue thickness compensator **44220**, for example. Further to the discussion herein, the tubular element **44080** and/or the strands **44090** in the tubular lattice **44092** can comprise a therapeutic agent **44098**. In some embodiments, the non-porous shell **44224** can contain the therapeutic agent **44098** within the tissue thickness compensator. As described herein, the tubular element **44080** can be positioned relative to staple cavities **30012** and a cutting element **30052** in staple cartridge **30000**. In several such embodiments, deployment of the staples **30030** and/or translation of the cutting element **30052** can be configured to pierce or rupture the non-porous, shell **44224** such that the therapeutic agent **44198** contained therein can be released from the tissue thickness compensator **44020**.

Referring to FIG. **115**, a tissue thickness compensator **44320** can comprise a central tubular element **44380b** comprising a tubular lattice **44392**. The tubular lattice **44392** can have a non-woven portion or a gap **44381** that is substantially aligned with the longitudinal slot **30015** of the rigid support portion **30010**. In such embodiments, a woven portion of the tubular lattice **44092** of the tubular element **44380b** does not overlap the longitudinal slot **30015**. Accordingly, the cutting element **30052** on the translating staple-fire sled **30052** can translate along the longitudinal slot **30015** without severing an overlapping a woven portion of the tubular lattice **44392**. Though staples **30030c** and **30030d** positioned adjacent to the gap **44381** in tubular element **44380b** may receive less support from the tubular lattice **44392** structure, in some embodiments, additional features can provide support for those staples **30030** and/or additional restoring force in the staple entrapment areas **30039** thereof. For example, as described in greater detail herein, additional tubular elements, support webbing, springs and/or buttressing material can be positioned at least one of inside and outside tubular element **44380b** near gap **44381**, for example.

Referring now to FIGS. **116-119**, in various embodiments, a tissue thickness compensator **45020** can comprise multiple tubular elements **45080** that laterally traverse the staple cartridge **30000**. The tubular elements **45080** can be positioned perpendicular to the rows of staple cavities **30012** and/or the longitudinal axis of the rigid support portion **30010** of the staple cartridge **30000**. In some embodiments, referring to FIG. **116**, the tubular elements **45080** can traverse the longitudinal slot **30015** in the staple cartridge **30000** such that the

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cutting element **30052** on the staple-firing sled **30050** is configured to sever the tubular elements **45080** as the staple-firing sled **30050** translates along the longitudinal slot **30015**. In other embodiments, referring now to FIG. **117**, the tissue thickness compensator **46020** can comprise two sets of laterally traversing tubular elements **46080**. The first set of laterally traversing tubular elements **46080a** can be positioned on a first side of the longitudinal slot **30015** and the second set of laterally traversing tubular elements **46080b** can be positioned on a second side of the longitudinal slot **30015**. In such an arrangement, the cutting element **30052** can be configured to pass between the two sets of tubular elements **46080** without severing a portion of the tubular elements **46080**. In other embodiments, the cutting element **30052** can sever at least one tubular element **46080** that traverses the longitudinal slot **30015** while at least one other tubular element **46080** does not traverse the longitudinal slot **30015** and is not severed by the cutting element **30052**.

As the tubular elements **45080** laterally traverse the staple cartridge **30000**, referring to FIGS. **118** and **119**, a staple **30030** can engage at least one tubular element **45080** in each staple entrapment area **30039**. In such an arrangement, each tubular element **45080** can provide a discrete restoring force along the length of the staple cartridge **30000**. For example, referring primarily to FIG. **119**, the tubular elements **45080** positioned near the proximal end of the tissue thickness compensator **45020** where the tissue is thicker can be greatly compressed compared to the tubular elements **45080** positioned near to the distal end of the tissue thickness compensator **45020** where the tissue is thinner. As a result, the tubular elements **45080** positioned closer to the proximal end of the tissue thickness compensator **45020** can provide a greater restoring force than the restoring force that could be generated by the tubular elements **46080** positioned closer to the distal end of the tissue thickness compensator **45020**. Further, referring still to FIG. **119**, the deformation of one tube **45080** can have little or no impact on the deformation of an adjacent tube **45080**. Accordingly, the tubular elements **45080** can exert a substantially discrete and customized springback force in staple entrapment areas **30039** along the length of the staple cartridge **30030**. In some embodiments, where multiple staples **30030** fired from a single row of staple cavities **30012** engage the same tubular element **35080**, the deformation of the tubular element **35080** can be less customized. For example, the deformation of a tubular element **35080** in one staple entrapment area **30039** can impact the deformation of that tubular element **35080** in another staple entrapment area **30039**.

In still other embodiments, referring to FIGS. **120-125**, tubular elements **47080** of the tissue thickness compensator **47020** can diagonally traverse the staple cartridge **30000**. The tubular elements **47080** can traverse the longitudinal slot **30015** of the staple cartridge **30000** such that the cutting element **30052** on the staple-firing sled **30050** is configured to sever the diagonally traversing tubular elements **47080** as the staple-firing sled **30052** translates along the longitudinal slot **30015**. In other embodiments, the tissue thickness compensator **47020** can comprise two sets of diagonally traversing tubular elements **47080**. A first set of diagonally traversing tubular elements **47080** can be positioned on a first side of the longitudinal slot **30015** and a second set of diagonally traversing tubular elements **47080** can be positioned on a second side of the longitudinal slot **30015**. In such an arrangement, the cutting element **30052** can pass between the two sets of tubular elements **47080** and may not sever any tubular element **47080**.

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Referring still to FIGS. **120-123**, the diagonally traversing tubular elements **47080** can be positioned in the staple cartridge **30000** such that a gap is defined between the tubular elements **47080**. A gap between adjacent tubular elements **47080** can provide space for horizontal expansion of the tubular elements **47080** when a compressive force is applied thereto, such as, for example, by tissue **T** captured within the staple entrapment area **30039** of the formed staple **30030**. The tubular elements **47080** can be connected across a gap by a film or sheet of material **47024**. The sheet of material can be positioned on at least one of the deck surface **30011** of the rigid support portion **30010** and/or the tissue contacting side of the tubular elements **47080**.

In various embodiments, referring to FIGS. **124** and **125**, at least one diagonally traversing tubular element **47080** can be positioned relative to the staple cavities **30012** in the staple cartridge **30000** such that the tubular element **47080** is positioned between the legs **30032** of the staples **30030** deployed from multiple rows of staple cavities **30012**. As the staples **30030** are moved from the initial position to the fired position, as described in greater detail herein, the staple legs **30032** can remain positioned around the tubular element **47080**. Further, the staples can be deformed such that the staple legs **30032** wrap around the perimeter of the tubular element **47080**, for example. In such an arrangement, the staples **30030** can be configured to move to the fired or formed position without piercing the tubular element **47080**. Movement of the staple legs **30032** around the tubular element **47080** could in some embodiments, prevent the inadvertent release of a therapeutic agent **47098** retained therein. The selected angular orientation of each tubular element **47080** relative to the longitudinal slot **30015** of the staple cartridge **30000** can depend on the position of the staple cavities **30012** in the staple cartridge **30000**. For example, in some embodiments, the tubular elements **47080** can be positioned at an approximately forty-five (45) degree angle relative to the longitudinal slot **30015** of the staple cartridge **30000**. In other embodiments, the tubular elements **47080** can be positioned at a fifteen (15) to seventy-five (75) degree angle relative to the longitudinal slot **30015** of the staple cartridge **30000**, for example.

Similar to descriptions throughout the present disclosure, multiple tubular elements in a tissue thickness compensator can be connected by a binding agent, wrap, webbing, overmold, compensation material, and/or any other suitable connecting adhesive or structure, for example. In various embodiments, referring to FIGS. **126-128**, a flexible shell **48024** may surround or encapsulate tubular elements **48080** in a tissue thickness compensator **48020**. In various embodiments, the flexible shell **48024** can restrain the tubular elements **48080** in the end effector **12** and can hold each tubular element **48080** in position, such as, for example, in longitudinal alignment with a row of staple cavities **30012**. In at least one embodiment, the tissue thickness compensator **48020** can comprise six tubular elements **48080**, for example. In various embodiments, the flexible shell **48024** can be sufficiently deformable and resilient to restrain the tubular elements **48020** encased therein while permitting deformation and rebound of the tubular elements **48080**. Further, in some embodiments, the flexible shell **48024** can tautly surround the tubular elements **48080** and can remain tautly engaged with the tubular elements **48080** as they deform and/or rebound.

Referring to FIG. **127**, prior to the deployment of staples **30030**, the anvil **30060** can be pivoted or rotated downwardly to compress the tissue thickness compensator **48020** and tissue **T** between the anvil **30060** and the staple cartridge **30000**. Compression of the tissue thickness compensator **48020** can include a corresponding compression of the flexible shell

48024 and the tubular elements **48020** therein. As the tubular elements **48020** deform, the flexible shell **48024** can similarly deform. In various embodiments, the tubular elements **48020** can be uniformly compressed across the width of the staple cartridge **30000** and the flexible shell **48024** can experience a similarly uniform compression across the tubular elements **48080**. Referring to FIG. 128, when the anvil **30060** is opened after the staples **30030** have been deployed from the staple cartridge **30000**, the tubular elements **48080** can rebound or partially rebound from the compressed configurations (FIG. 127). In various embodiments, a tubular element **48080** can rebound such that the tubular element **48080** returns to its initial, undeformed configuration. In some embodiments, a tubular element **48080** can partially rebound such that the tubular element **48080** partially returns to its initial undeformed configuration. For example, the deformation of the tubular element **48080** can be partially elastic and partially plastic. As the tubular elements **48080** rebound, the flexible shell **48024** can remain tautly engaged with each tubular element **48080**. The tubular elements **48080** and flexible shell **48024** can rebound to such a degree that the tubular elements **48080** and tissue T fill the staple entrapment areas **30039** while the tubular elements **48080** exert an appropriate restoring force on the tissue T therein. Referring to FIG. 129, in other embodiments, a tissue thickness compensator **48120** comprising six tubular elements **48180** retained in a flexible shell **48124** can be positioned on the anvil **30060** of the end effector **12**, for example.

Referring to FIGS. 130-133, a tissue thickness compensator **49020** can comprise a tubular element **49080** longitudinally positioned along the longitudinal axis of the anvil **30060**. In various embodiments, the tissue thickness compensator **49020** can be secured to the anvil **30060** of the end effector **12** by a compressible compensation material **49024**. Further, the compressible compensation material **49024** can surround or encapsulate the tubular element **49080**. Similar to the descriptions herein, the tubular element **49080** can comprise at least one therapeutic agent **49098** which may be released by the absorption of various components of the tissue thickness compensator **49020**, the piercing of the tubular element **49080** by staples **30030** fired from the staple cartridge **30000**, and/or by the cutting element **30052**.

Referring to FIG. 131, a staple cartridge **30000** can comprise staples **30030** positioned in staple cavities **30012**, wherein, prior to deployment of the staples **30030**, the anvil **30060** and the tissue thickness compensator **49020** attached thereto can pivot toward the staple cartridge **30000** and compress tissue T captured therebetween. In some embodiments, the tubular element **49080** of the tissue thickness compensator **49020** can be uniformly deformed along the length of the staple cartridge **30000** by the pivoting anvil **30060** (FIG. 131). Referring to FIGS. 132 and 133, the staple-firing sled **30050** can translate along the longitudinal slot **30015** in the staple cartridge **30000** and engage each driver **30040** positioned beneath a staple **30030** in a staple cavity **30010**, wherein each engaged driver **30040** can fire or eject the staple **30030** from the staple cavity **30012**. When the anvil **30060** releases pressure on the tissue T and the tissue thickness compensator **49020**, the tissue thickness compensator **49020**, including the tubular element **49080** and the compressible compensation material **49024**, can rebound or partially rebound from the compressed configurations (FIG. 131) to a rebounded configuration (FIGS. 132 and 133). The tubular element **49080** and compressible compensation material **49024** can rebound to such a degree that the tissue thickness compensator **49020**

and tissue T fill the staple entrapment areas **30039** while the tissue thickness compensator **49020** exert an a restoring force on the captured tissue T.

In various embodiments, referring to FIGS. 124-126, two tissue thickness compensators **50020a**, **50020b** can be positioned in the end effector **12** of a surgical instrument. For example, a first tissue thickness compensator **50020a** can be attached to the staple cartridge **30000** in the lower jaw **30070** and a second tissue thickness compensator **50020b** can be attached to the anvil **30060**. In at least one embodiment, the first tissue thickness compensator **50020a** can comprise a plurality of tubular elements **50080** longitudinally arranged and retained in a first compensation material **50024a**. At least one tubular element **50080** can comprise a therapeutic agent **50098**, similar to the therapeutic agents described herein. The first compensation material **50024a** can be deformable or substantially rigid. Further, in some embodiments, the first compensation material **50024a** can hold the tubular elements **50080** in position relative to the staple channel **30000**. For example, the first compensation material **50024a** can hold each tubular element **50080** in longitudinal alignment with a row of staple cavities **30012**. In at least one embodiment, the second tissue thickness compensator **50020b** can comprise the first compensation material **50024a**, a second compensation material **50024b** and/or a third compensation material **50024c**. The second and third compensation material **50024b**, **50024c** can be deformable or substantially rigid.

Similar to at least one embodiment described herein, the anvil **30060** can pivot and apply a compressive force to the tissue thickness compensators **50020a**, **50020b** and the tissue T between the anvil **30060** and the staple cartridge **30000**. In some embodiments, neither the first tissue thickness compensators **50020a** nor the second tissue thickness compensators **50020b** can be compressible. In other embodiments, at least one component of the first tissue thickness compensators **50020a** and/or the second tissue thickness compensators **50020b** can be compressible. When the staples **30030** are fired from the staple cartridge **30000**, referring now to FIGS. 135 and 136, each staple **30030** can pierce a tubular element **50080** retained in the first tissue thickness compensator **50020a**. As shown in FIG. 135, the therapeutic agent **50098** retained in the tubular element **50080** can be released when a staple **30030** pierces the tubular element **50080**. When released, the therapeutic agent **50098** can coat the staple legs **30032** and tissue T surrounding the fired staple **30030**. In various embodiments, the staples **30030** can also pierce the second tissue thickness compensator **50020b** when the staples **30030** are fired from the staple cartridge **30000**.

Referring to FIGS. 137-140, a tissue thickness compensator **51020** can comprise at least one tubular element **51080** that laterally traverses the tissue thickness compensator **51020**. For example, referring to FIG. 137, the tissue thickness compensator **51020** can be positioned relative to the staple cartridge **30000** such that a first end **51083** of the laterally traversing tubular element **51080** can be positioned near a first longitudinal side of the staple cartridge **30000** and a second end **51085** of the laterally traversing tubular element **51080** can be positioned near a second longitudinal side of the staple cartridge **30000**. In various embodiments, the tubular element **51080** can comprise a capsule-like shape, for example. As illustrated in FIG. 138, the tubular element **51080** can be perforated between the first end **51083** and the second end **51085** and, in some embodiments, the tubular element **51080** can be perforated at or near the center **51087** of the tubular element **51080**. The tubular element **51080** can comprise a polymeric composition, such as a bioabsorbable, biocompatible elastomeric polymer, for example. Further,

referring again to FIG. 137, the tissue thickness compensator 51020 can comprise a plurality of laterally traversing tubular elements 51080. In at least one embodiment, thirteen tubular elements 51080 can be laterally arranged in the tissue thickness compensator 51020, for example.

Referring again to FIG. 137, the tissue thickness compensator 51020 can further comprise a compensation material 51024 that at least partially surrounds the tubular elements 51080. In various embodiments, the compensation material 51024 can comprise a bioabsorbable polymer, such as, for example, lyophilized polysaccharide, glycoprotein, elastin, proteoglycan, gelatin, collagen, and/or oxidized regenerated cellulose (ORC). The compensation material 51024 can hold the tubular elements 51080 in position in the tissue thickness compensator 51020. Further, the compensation material 51024 can be secured to the top deck surface 30011 of the rigid support portion 30010 of the staple cartridge 30000 such that the compensation material 51020 is securely positioned in the end effector 12. In some embodiments, the compensation material 51024 can comprise at least one medicament 51098.

Still referring to FIG. 137, laterally positioned tubular elements 51080 can be positioned relative to the translating cutting element 30052 such that the cutting element 30052 is configured to sever the tubular elements 51080. In various embodiments, the cutting element 30052 can sever the tubular elements 51080 at or near the perforation therein. When the tubular elements 51080 are severed in two halves, the severed portions of the tubular elements 51080 can be configured to swell or expand, as illustrated in FIG. 139. For example, in various embodiments, the tubular element 51080 can comprise a hydrophilic substance 51099 that can be released and/or exposed when the tubular element 51080 is severed. Furthermore, when the hydrophilic substance 51099 contacts bodily fluids in tissue T, the hydrophilic substance 51099 can attract the fluid, which can cause the tubular element 51080 to swell or expand. As the tubular element 51080 expands, the compensation material 51024 surrounding the tubular element 51080 can shift or adjust to accommodate the swollen tubular element 51080. For example, when the compensation material 51024 comprises gelatin, the gelatin can shift to accommodate the swollen tubular elements 51080. Referring now to FIG. 140, expansion of the tubular elements 51080 and shifting of the compensation material 51024 can cause a corresponding expansion of the tissue thickness compensator 51020.

Similar to other tissue thickness compensators discussed throughout the present disclosure, the tissue thickness compensator 51020 can be deformed or compressed by an applied force. Further, the tissue thickness compensator 51020 can be sufficiently resilient such that it produces a springback force when deformed by the applied force and can subsequently rebound or partially rebound when the applied force is removed. In various embodiments, when the tissue thickness compensator 51020 is captured in a staple entrapment area 30039, the staple 30030 can deform the tissue thickness compensator 51020. For example, the staple 30030 can deform the tubular elements 51080 and/or the compensation material 51024 of the tissue thickness compensator 51020 that are captured within the fired staple 30030. In various embodiments, non-captured portions of the tissue thickness compensator 51020 can also be deformed due to the deformation in the staple entrapment areas 30039. When deformed, the tissue thickness compensator 51020 can seek to rebound from the deformed configuration. In various embodiments, such a rebound may occur prior to the hydrophilic expansion of the tubular element 51080, simultaneously with the hydrophilic

expansion of the tubular element 51080, and/or after the hydrophilic expansion of the tubular element 51080. As the tissue thickness compensator 51020 seeks to rebound, it can exert a restoring force on the tissue also captured in the staple entrapment area 30039, as described in greater detail herein.

In various embodiments, at least one of the tubular elements 51080 and/or the compensation material 51024 in the tissue thickness compensator 51020 can comprise a therapeutic agent 51098. When the tubular element 51080 that contains a therapeutic agent 51098 is severed, the therapeutic agent 51098 contained within the tubular elements 51080 can be released. Furthermore, when the compensation material 51024 comprises the therapeutic agent 51098, the therapeutic agent 51098 can be released as the bioabsorbable compensation material 51024 is absorbed. In various embodiments, the tissue thickness compensator 51020 can provide for a rapid initial release of the therapeutic agent 51098 followed by a controlled release of the therapeutic agent 51098. For example, the tissue thickness compensator 51020 can provide a rapid initial release of the therapeutic agent 51098 from the tubular elements 51080 to the tissue T along the cut line when the tubular elements 51080 comprising the therapeutic agent 51098 are severed. Further, as the bioabsorbable compensation material 51024 comprising the therapeutic agent 51098 is absorbed, the tissue thickness compensator 51020 can provide an extended, controlled release of the therapeutic agent 51098. In some embodiments, at least some of the therapeutic agent 51098 can remain in the tubular element 51080 for a short period of time before the therapeutic agent 51098 flows into the compensation material 51024. In other embodiments, at least some of the therapeutic agent 51098 can remain in the tubular element 51080 until the tubular element 51080 is absorbed. In various embodiments, the therapeutic agent 51098 released from the tubular element 51080 and the compensation material 51024 can be the same. In other embodiments, the tubular element 51080 and the compensation material 51024 can comprise different therapeutic agents or different combinations of therapeutic agents, for example.

Referring still to FIG. 140, in various embodiments, the end effector 12 can cut tissue T and fire staples 30030 into the severed tissue T nearly simultaneously or in quick succession. In such embodiments, a staple 30030 can be deployed into the tissue T immediately after the cutting element 30052 has severed the tubular element 51080 adjacent to the tissue T. In other words, the staples 30030 can engage the tissue thickness compensator 51020 immediately following or simultaneously with the swelling of the tubular element 51080 and the expansion of the tissue thickness compensator 51020. In various embodiments, the tissue thickness compensator 51020 can continue to grow or expand after the staples 30030 have been fired into the tissue T. In various embodiments, the staples 30030 can be configured to puncture the tubular elements 51080 when the staples 30030 are deployed. In such embodiments, therapeutic agents 51098 still retained in the severed tubular elements 51080 can be released from the tubular elements 51080 and, in some embodiments, can cover the legs 30031 of the fired staples 30030.

Referring to FIG. 141, the tissue thickness compensator 51020 can be manufactured by a molding technique, for example. In various embodiments, a frame, or a mold, 51120 can comprise a first longitudinal side 51122 and a second longitudinal side 51124. Each longitudinal side 51124 can comprise one or more notches 51130, which can each be configured to receive the first or second end 50183, 50185 of a tubular element 51080. In some embodiments, the first end 50183 of the tubular element 51080 can be positioned in a first notch 51130a on the first longitudinal side 51122 and the

second end **50183** of the tubular element **51080** can be positioned in a second notch **51130b** on the second longitudinal side **51124** such that the tubular element **51080** laterally traverses the frame **51120**. In various embodiments, the notch **51180** can comprise a semi-circular groove, which can securely fit the first or second end **50183**, **50185** of the tubular element **51080** therein. In various embodiments, the first notch **51130a** can be positioned directly across from the second notch **51130b** and the tubular element **51080** can be positioned perpendicular, or at least substantially perpendicular, to the longitudinal axis of the frame **51120**. In other embodiments, the first notch **51130a** can be offset from the second notch **51130b** such that the tubular element **51080** is angularly positioned relative to the longitudinal axis of the frame **51120**. In still other embodiments, at least one tubular element **51080** can be longitudinally positioned within the frame **51120** such that the tubular element extends between the lateral sides **51126**, **51128** of the frame **51120**. Further, at least one tubular element can be angularly positioned in the frame between two notches on the lateral sides **51126**, **51128** of the frame and/or between a notch on a lateral side **51126** and a notch on a longitudinal side **51124**, for example. In various embodiments, the frame **51120** can comprise a support ledge **51136**, which can support the tubular elements **51080** positioned within the frame **51120**.

In various embodiments, the frame **51120** can comprise notches **51130** to accommodate twelve tubular elements **51080**, for example. In some embodiments, the frame notches **51130** can be filled with tubular elements **51080** while, in other embodiments, less than all of the notches **51130** may be filled. In various embodiments, at least one tubular element **51080** can be positioned in the frame **51120**. In some embodiments, at least half the notches **51130** can receive tubular elements **51080**. In at least one embodiment, once the tubular elements **51080** are positioned in the frame **51120**, compensation material **51024** can be added to the frame **51120**. The compensation material **51024** can be fluidic when added to the frame **51120**. For example, in various embodiments, the compensation material **51024** can be poured into the frame **51120** and can flow around the tubular elements **51080** positioned therein. Referring to FIG. 142, the fluidic compensation material **51024** can flow around the tubular element **51080** supported by notches **51130** in the frame **51120**. After the compensation material **51024** cures, or at least sufficiently cures, referring now to FIG. 143, the tissue thickness compensator **51020** comprising the compensation material **51024** and tubular elements **51080** can be removed from the frame **51120**. In at least one embodiment, the tissue thickness compensator **51020** can be trimmed. For example, excess compensation material **51024** can be removed from the tissue thickness compensator **51020** such that the longitudinal sides of the compensation material are substantially planar. Furthermore, in some embodiments, referring to FIG. 144, the first and second ends **50183**, **50185** of the tubular elements **51080** can be pressed together, or closed, to seal the tubular element **51080**. In some embodiments, the ends can be closed before the tubular elements **51080** are placed in the frame **51120**. In other embodiments, the trimming process may transect the ends **51083**, **51085** and a heat stacking process can be used to seal and/or close the ends **51083**, **51085** of the tubular elements **51080**.

In various embodiments, referring again to FIG. 141, a stiffening pin **51127** can be positioned within each tubular element **51080**. For example, the stiffening pin **51127** can extend through a longitudinal lumen of the tubular element **51080**. In some embodiments, the stiffening pin **51127** can extend beyond each tubular element **51080** such that the

stiffening pin **51127** can be positioned in notches **51130** in the frame **51120**. In embodiments having stiffening pins **51127**, the stiffening pins **51127** can support the tubular elements **51080** when the compensation material **51024** is poured into the frame **51120** and as the fluidic compensation material **51024** flows around the tubular elements **51080**, for example. Once the compensation material **51024** cures, solidifies, and/or lyophilizes or sufficiently cures, solidifies, and/or lyophilizes the tissue thickness compensator **51020** can be removed from the frame **51120** and the stiffening pins **51127** can be removed from the longitudinal lumens of the tubular elements **51080**. In some embodiments, the tubular elements **51080** can then be filled with medicaments, for example. Similar to at least one embodiment described herein, after the tubular elements **51080** are filled with medicaments, the tissue thickness compensator **51020**, including the ends **51083**, **51085** of the tubular elements **51080**, for example, can be trimmed. In various embodiments, the tissue thickness compensator **51020** can be die cut, for example, and/or sealed by heat and/or pressure, for example.

As discussed herein, the tissue thickness compensator **52020** can comprise multiple tubular elements **51080**. Referring now to FIG. 145, the tubular elements **51080** can comprise different material properties, dimensions and geometries. For example, a first tubular element **51080a** can comprise a first thickness and a first material and a second tubular element **51080b** can comprise a second thickness and a second material. In various embodiments, at least two tubular elements **51080** in the tissue thickness compensator **52020** can comprise the same material. In other embodiments, each tubular element **51080** in the tissue thickness compensator **52020** can comprise different materials. Similarly, in various embodiments, at least two tubular elements **51080** in the tissue thickness compensator **52020** can comprise the same geometry. In other embodiments, each tubular element **51080** in the tissue thickness compensator **52020** can comprise different geometries.

Referring now to FIGS. 208-211, a tissue thickness compensator **51220** can comprise at least one tubular element **51280** that laterally traverses the tissue thickness compensator **51220**. In various embodiments, referring to FIG. 208, the tissue thickness compensator **51220** can be positioned relative to the anvil **30060** of the end effector **12**. The tissue thickness compensator **51220** can be secured to a securing surface **30061** of the anvil **30060** of the end effector **12**, for example. In various embodiments, referring primarily to FIG. 209, the tubular element **51280** can comprise a capsule-like shape, for example. The tubular element **51280** can comprise a polymeric composition, such as a bioabsorbable, biocompatible elastomeric polymer, for example.

Referring again to FIG. 208, the tissue thickness compensator **51220** can further comprise a compensation material **51224** that at least partially surrounds the tubular elements **51280**. In various embodiments, the compensation material **51224** can comprise a bioabsorbable polymer, such as, for example, lyophilized polysaccharide, glycoprotein, elastin, proteoglycan, gelatin, collagen, and/or oxidized regenerated cellulose (ORC), for example. Similar to the above, the compensation material **51024** can hold the tubular elements **51280** in position in the tissue thickness compensator **51220**. Further, the compensation material **51224** can be secured to the securing surface **30061** of the anvil **30060** such that the compensation material **51220** is securely positioned in the end effector **12**. In some embodiments, the compensation material **51224** can comprise at least one medicate.

Still referring to FIG. 208, the laterally positioned tubular elements **51280** can be positioned relative to the cutting ele-

ment **30252** on a translating sled **30250** such that the translatable cutting element **30252** is configured to sever the tubular elements **51280**. In various embodiments, the cutting element **30252** can sever the tubular elements **51280** at or near the center of each tubular element **51280**, for example. When the tubular elements **51280** are severed in two halves, the severed portions of the tubular elements **51280** can be configured to swell or expand, as illustrated in FIG. **208**. Referring primarily to FIG. **210**, in various embodiments, a tubular element **51280** can comprise a hydrophilic substance **51099** that can be released and/or exposed when the tubular element **51280** is severed. Furthermore, referring now to FIG. **211**, when the hydrophilic substance **51099** contacts bodily fluids in the tissue **T**, the hydrophilic substance **51099** can attract the fluid, which can cause the tubular element **51280** to swell or expand. As the tubular element **51280** expands, the compensation material **51224** surrounding the tubular element **51280** can shift or adjust to accommodate the swollen tubular element **51280**. For example, when the compensation material **51224** comprises gelatin, the gelatin can shift to accommodate the swollen tubular element **51280**. Referring again to FIG. **208**, expansion of the tubular elements **51280** and shifting of the compensation material **51224** can cause a corresponding expansion of the tissue thickness compensator **51220**.

Similar to other tissue thickness compensators discussed throughout the present disclosure, the tissue thickness compensator **51220** can be deformed or compressed by an applied force. Further, the tissue thickness compensator **51220** can be sufficiently resilient such that it produces a springback force when deformed by the applied force and can subsequently rebound or partially rebound when the applied force is removed. In various embodiments, when the tissue thickness compensator **51220** is captured in a staple entrapment area **30039** (FIG. **88**), the staple **30030** can deform the tissue thickness compensator **51220**. For example, the staple **30030** can deform the tubular elements **51280** and/or the compensation material **51224** of the tissue thickness compensator **51220** captured within the fired staple **30030**. In various embodiments, non-captured portions of the tissue thickness compensator **51220** can also be deformed due to the deformation in the staple entrapment areas **30039**. When deformed, the tissue thickness compensator **51220** can seek to rebound from the deformed configuration. In various embodiments, such a rebound may occur prior to the hydrophilic expansion of the tubular element **51280**, simultaneously with the hydrophilic expansion of the tubular element **51280**, and/or after the hydrophilic expansion of the tubular element **51280**. As the tissue thickness compensator **51220** seeks to rebound, it can exert a restoring force on the tissue also captured in the staple entrapment area **30039**, as described in greater detail herein.

Referring to FIGS. **146-149**, a tissue thickness compensator **52020** can comprise one or more tubular elements **52080** that laterally traverse the tissue thickness compensator **52020**, similar to at least one tissue thickness compensator described herein. In various embodiments, the tissue thickness compensator **52020** can comprise multiple laterally traversing tubular elements **52080**. The tissue thickness compensator **52020** can further comprise one or more sheets of material **52024** that hold or retain at least one tubular element **52080** in the tissue thickness compensator **52020**. In various embodiments, the one or more sheets of material **52024** can be positioned above and/or below the tubular elements **52080** and can securely retain each tubular element **52080** in the tissue thickness compensator **52020**. Referring primarily to FIG. **146**, the tissue thickness compensator can comprise a

first sheet of material **52024a** and a second sheet of material **52024b**. In various embodiments, the tubular elements **52080** can be positioned between the first and second sheets of material **52024a**, **52024b**. Further, referring still to FIG. **146**, the sheet of material **52024b** can be secured to the top deck surface **30011** of the rigid support portion of the staple cartridge **30000** such that the tissue thickness compensator **52020** is securely positioned in the end effector **12**. In other embodiments, one or more of the sheets of material **52024** can be secured to the anvil **30060** or otherwise retained in the end effector **12**.

In various embodiments, referring primarily to FIG. **147**, the tissue thickness compensator **52020** can be porous and/or permeable. For example, the sheet of material **52024** can comprise a plurality of apertures **52026**. In various embodiments, the apertures **52026** can be substantially circular. In at least one embodiment, the apertures **52036** can be visible in the sheet of material **52024**. In other embodiments, the apertures **52036** can be microscopic. Referring still to FIG. **147**, the tubular elements **52080** can comprise a plurality of apertures **52026**, as well. In various embodiments, referring to FIG. **148**, a tissue thickness compensator **52120** can comprise a sheet of material **52124** that comprises a plurality of non-circular apertures **52126**. For example, the apertures **52126** can comprise a diamond and/or slotted shape. In various other embodiments, referring to FIG. **149**, a tissue thickness compensator **52220** can comprise a tubular element **52280** that comprises a permeable tubular lattice **52292**. In various embodiments, the sheet of material **52224** can comprise a bioabsorbable, biocompatible elastomeric polymer and can comprise a medicament, for example.

Similar to at least one embodiment described herein, at least one tubular element **52080** can be configured to swell or expand, as illustrated in FIGS. **150A-150D**. For example, referring to FIG. **150A**, the tubular elements **52080** can be positioned intermediate the first and second sheet of material **52024a**, **52024b** in the tissue thickness compensator **52020**. When the tissue thickness compensator **52020** contacts tissue **T**, as illustrated in FIG. **150B**, the tissue thickness compensator **52020** can expand. In various embodiments, for example, the tubular elements **52080** can comprise a hydrophilic substance **52099** that expands when exposed to fluid in and/or on the tissue **T**. Further, the sheet of material **52024** and tubular elements **52080** can be permeable, as described herein, such that fluid from the tissue **T** can permeate the tissue thickness compensator **52020** thereby allowing the fluid to contact the hydrophilic substance **52099** within the tubular elements **52080**. As the tubular elements **52080** expand, the sheet of material **52024** surrounding the tubular elements **52080** can shift or adjust to accommodate the swollen tubular elements **52080**. Similar to various tissue thickness compensators discussed throughout the present disclosure, the expanded tissue thickness compensator **52020** can be deformed or compressed by an applied force, such as, for example, a compressive force applied by fired staples, as illustrated in FIG. **150C**. Further, the tissue thickness compensator **52020** can be sufficiently resilient such that it produces a springback force when deformed by the applied force and can subsequently rebound when the applied force is removed. Referring now to FIGS. **150D** and **150E**, the tissue thickness compensator **52020** can rebound to different configurations in different staple entrapment areas **30039** to appropriately accommodate the captured tissue **T**.

Referring to FIGS. **151-156**, a tissue thickness compensator **53020** can comprise a plurality of vertically positioned tubular elements **53080**. In various embodiments, each tubular element **53080** can comprise a tubular axis that is substan-

tially perpendicular to the top deck surface **30011** of the rigid support portion **30010** of the staple cartridge **30000**. Further, the first end of each tubular element **53080** can be positioned adjacent to the top deck surface **30011**, for example. Similar to at least one embodiment described herein, the tubular elements **53080** can be deformable and may comprise an elastomeric polymer, for example. In various embodiments, as illustrated in FIG. **152**, the tubular elements **53080** can be compressed when captured in a staple entrapment area **30039** with stapled tissue **T**. A tubular element **53080** can comprise an elastic material such that deformation of the tubular element **53080** generates a restoring force as the tubular element **53080** seeks to rebound from the deformed configuration. In some embodiments, deformation of the tubular element **53080** can be at least partially elastic and at least partially plastic. The tubular element **53080** can be configured to act as a spring under an applied force and, in various embodiments, can be configured not to buckle. In various embodiments, referring to FIG. **153**, the tubular elements **53080** can be substantially cylindrical. In some embodiments, referring to FIG. **154**, a tubular element **53180** can comprise a buckling region **53112**. The tubular element **53180** can be configured to buckle or deform at the buckling region **53112** when a compressive force is applied thereto. The tubular element **53180** can deform elastically and/or plastically and then be designed to buckle suddenly at the buckling region **53112** under a preselected buckling force.

Referring primarily to FIG. **155**, a first tubular element **53080** can be positioned at a first end of a staple cavity **30012** and another tubular element **53080** can be positioned at a second end of the staple cavity **30012**. As illustrated in FIG. **153**, the tubular element **53080** can comprise a lumen **53084** extending therethrough. Referring again to FIG. **152**, when the staple **30030** is moved from the initial position to the fired position, each staple leg **30032** can be configured to pass through a lumen **53084** of each tubular element **53080**. In various other embodiments, referring primarily to FIG. **156**, vertically positioned tubular elements **54080** can be arranged in a tissue thickness compensator **54020** such that the tubular elements **54080** abut or contact each other. In other words, the tubular elements **54080** can be clustered or gathered together. In some embodiments, the tubular elements **54080** can be systematically arranged in the tissue thickness compensator **54020**; however, in other embodiments, the tubular elements **54080** can be randomly arranged.

Referring again to FIGS. **151**, **155**, and **156**, the tissue thickness compensator **53020** can also comprise a sheet of material **53024** that holds or retains the tubular elements **53080** in the tissue thickness compensator **53020**. In various embodiments, the sheet of material **53024** can be positioned above and/or below the tubular elements **53080** and can securely retain each tubular element **53080** in the tissue thickness compensator **53020**. In various embodiments, the tissue thickness compensator **53020** can comprise a first and a second sheet of material **53024**. In various embodiments, the tubular elements **53080** can be positioned between the first and second sheets of material **53024**. Further, the sheet of material **53024** can be secured to the top deck surface **30011** of the rigid support portion of the staple cartridge **30000** such that the tissue thickness compensator **53020** is securely positioned in the end effector **12**. In other embodiments, a sheet of material **53024** can be secured to the anvil **30060** or otherwise retained in the end effector **12**. Similar to at least one embodiment described herein, the sheet of material **53024** can be sufficiently deformable such that the sheet of material **53024** deforms as springs **55080** within the tissue thickness compensator are deformed.

Referring to FIGS. **157** and **158**, a tissue thickness compensator **55020** can comprise at least one spring **55080** that is sufficiently resilient such that it is capable of producing a springback force when deformed. Referring primarily to FIG. **157**, the tissue thickness compensator **55020** can comprise a plurality of springs **55080**, such as, for example, three rows of springs **55080**. The springs **55080** can be systematically and/or randomly arranged in the tissue thickness compensator **55020**. In various embodiments, the springs **55080** can comprise an elastomeric polymer, for example. In some embodiments, the shape of the springs **55080** can allow for deformation thereof. In various embodiments, the springs **55080** can be deformed from an initial configuration to a deformed configuration. For example, when a portion of the tissue thickness compensator **55020** is captured in a staple entrapment area **30039**, the springs **55080** in and/or around the staple entrapment area **30039** can be deformed. In various embodiments, the springs **55080** can buckle or collapse under a compressive force applied for a fired staple **30030** and the springs **55080** may generate a restoring force that is a function of the spring rate of the deformed spring **55080** and/or the amount the spring **55080** is deformed, for example. In some embodiments, the spring **55080** can act as a sponge under a compressive force applied by a fired staple **30030**. Further, the spring **55080** can comprise a compensation material, as described in greater detail throughout the present disclosure.

The tissue thickness compensator **55020** can further comprise one or more sheets of material **55024** that hold or retain at least one spring **55080** in the tissue thickness compensator **55020**. In various embodiments, the sheets of material **55024** can be positioned above and/or below the springs **55080** and can securely retain the springs **55080** in the tissue thickness compensator **55020**. In at least one embodiment, the tissue thickness compensator **55020** can comprise a first sheet of material **55024a** and a second sheet of material **55024b**. In various embodiments, the tubular elements **52080** can be positioned between the first and second sheets of material **55024a**, **55024b**. Referring primarily to FIG. **158**, in various embodiments, the tissue thickness compensator **55020** can further comprise a third sheet of material **55024c** positioned adjacent to either the first or second sheet of material **55024a**, **55024b**. In various embodiments, at least one sheet of material **55024** can be secured to the top deck surface **30011** of the rigid support portion of the staple cartridge **30000**, such that the tissue thickness compensator **55020** is securely positioned in the end effector **12**. In other embodiments, at least one sheet of material **55024** can be secured to the anvil **30060** or otherwise retained in the end effector **12**.

Referring now to FIG. **158**, when a staple **30030** is fired from the staple cartridge **30000** (FIG. **156**), the staple **30030** can engage the tissue thickness compensator **55020**. In various embodiments, the fired staple **30030** can capture tissue **T** and a portion of the tissue thickness compensator **55020** in the staple entrapment area **30039**. The springs **55080** can be deformable such that the tissue thickness compensator **55020** compresses when captured by a fired staple **30030**. In some embodiments, the springs **55080** can be positioned between fired staples **30030** in the tissue thickness compensator **55020**. In other embodiments, at least one spring **55080** can be captured within the staple entrapment area **30039**.

Referring to FIG. **159**, a tissue thickness compensator **60020** can comprise at least two compensation layers **60022**. In various embodiments, the tissue thickness compensator **60020** can comprise a plurality of compensation layers **60022** which can be stacked on top of each other, positioned side-by-side, or a combination thereof. As described in greater detail herein, the compensation layers **60022** of the tissue

thickness compensator **60020** can comprise different geometric and/or material properties, for example. Furthermore, as described in greater detail herein, pockets and/or channels can exist between adjacently stacked compensation layers **60022**. For example, a tissue thickness compensator **60020** can comprise six compensation layers **62022a**, **62022b**, **62022c**, **62022d**, **62022e**, **62022f**, which can be adjacently stacked on top of each other (FIG. 174).

Referring to FIGS. 160, 161, and 163-168, a tissue thickness compensator can comprise a first compensation layer **60122a** and a second compensation layer **60122b**. In various embodiments, the first compensation layer **60122a** can be adjacently stacked on top of the second compensation layer **60122b**. In at least one embodiment, adjacently stacked compensation layers **60122** can be separated by a separation gap or pocket **60132**. Referring primarily to FIG. 160, a tissue thickness compensator **60120** can also comprise at least one cantilever beam or support **60124** positioned between the first and second compensation layers **60122a**, **60122b**. In various embodiments, the support **60124** can be configured to position the first compensation layer **60122a** relative to the second compensation layer **60122b** such that compensation layers **60122** are separated by the separation gap **60132**. As described in greater detail herein, deformation of the support **60124** and/or the compensation layers **60122a**, **60122b**, for example, can reduce the separation gap **60132**.

The support beam of a tissue thickness compensator can comprise various geometries and dimensions. For example, the support beam can be a simple I-beam, a centered, single-bend support beam **60124** (FIG. 160), an off-centered, single-bend support beam **60224** (FIG. 161), an elliptical support beam **60324** (FIG. 163), a multi-bend support beam **60424** (FIG. 164), and/or a symmetrical, dual-cantilevered support beam **60524** (FIG. 165). Furthermore, referring now to FIGS. 160, 166, and 167, a support beam **60624** can be thinner than at least one compensation layer **60122** (FIG. 166), a support beam **60724** can be thicker than at least one compensation layer **60122** (FIG. 167), and/or a support beam **60124** can be substantially the same thickness as at least one compensation layer **60122** (FIG. 160), for example. The material, geometry and/or dimensions of the support beam **60124**, for example, can affect the deformability and springback resiliency of the tissue thickness compensator **60120**.

Referring still to FIG. 160, the compensation layers **60122** and support beam **60124** of the tissue thickness compensator **60120** can comprise different materials, such as, for example, structural material, biological material, and/or electrical material, for example. For example, in various embodiments, at least one compensation layer **60122** can comprise a polymeric composition. The polymeric composition can comprise an at least partially elastic material such that deformation of the compensation layer **60122** and/or the support beam **60124** can generate a springback force. The polymeric composition of the compensation layer **60122** can comprise non-absorbable polymers, absorbable polymers, or combinations thereof. In some embodiments, the absorbable polymers can include bioabsorbable, biocompatible elastomeric polymers, for example. Furthermore, the polymeric composition of the compensation layer **60122** can comprise synthetic polymers, non-synthetic polymers, or combinations thereof. Examples of synthetic polymers include, but are not limited to, polyglycolic acid (PGA), poly(lactic acid) (PLA), polycaprolactone (PCL), polydioxanone (PDO), and copolymers thereof. Examples of non-synthetic polymers include, but are not limited to, polysaccharides, glycoprotein, elastin, proteoglycan, gelatin, collagen, and oxidized regenerated cellulose (ORC). In various embodiments, similar to the polymeric

compositions in embodiments described herein, the polymeric composition of the compensation layers **60122** can include varied amounts of absorbable polymers, non-absorbable polymers, synthetic polymers, and non-synthetic polymers, for example, by weight percentage. In various embodiments, each compensation layer **60022** in the tissue thickness compensator **60120** can comprise a different polymeric composition or, in various other embodiments, at least two compensation layers **60122** can comprise the same polymeric composition.

Referring again to FIG. 159, in various embodiments, at least one compensation layer **60022** can comprise a therapeutic agent **60098** such as a medicament or pharmaceutically active agent, for example. The compensation layer **60022** can release a therapeutically effective amount of the therapeutic agent **60098**. In various embodiments, the therapeutic agent **60098** can be released as the compensation layer **60022** is absorbed. Examples of therapeutic agents **60098** can include, but are not limited to, haemostatic agents and drugs, such as, for example, fibrin, thrombin, and/or oxidized regenerated cellulose (ORC), anti-inflammatory drugs such as, for example, diclofenac, aspirin, naproxen, sulindac, and/or hydrocortisone antibiotic and antimicrobial drugs or agents such as, for example, triclosan, ionic silver, ampicillin, gentamicin, polymyxin B, and/or chloramphenicol, and/or anticancer agents such as, for example, cisplatin, mitomycin, and/or adriamycin. In some embodiments, the therapeutic agent **60098** can comprise a biologic, such as a stem cell, for example. In various embodiments, each compensation layer **60022** in a tissue thickness compensator **60020** can comprise a different therapeutic agent **60098** or, in various other embodiments, at least two compensation layers **60022** can comprise the same therapeutic agent **60098**. In at least one embodiment, a compensation layer **60022** comprising a therapeutic agent **60098**, such as a biologic, for example, can be encased between two structural compensation layers **60022** comprising a polymeric composition, such as, for example, polyglycolic acid (PGA) foam, for example. In various embodiments, a compensation layer **60022** can also comprise an electrically conductive material, such as, for example, copper.

In various embodiments, referring again to FIG. 174, the compensation layers **62022** in the tissue thickness compensator **62020** can have different geometries. When layers **62022** are adjacently positioned in the tissue thickness compensator **62020**, the compensation layers **62022** can form at least one three-dimensional conduit **62032** between the layers **62022**. For example, when a second compensation layer **62022b** comprising a channel is positioned above a substantially flat third compensation layer **62022c**, the channel and flat surface of the third compensation layer **62022c** can define a three-dimensional conduit **62032a** therebetween. Similarly, for example, when a fifth compensation layer **62022e** comprising a channel is positioned below a fourth compensation layer **62022d** comprising a corresponding channel, the channels can form a three-dimensional conduit **62032b** defined by the channels in the adjacently stacked compensation layers **62022d**, **62022e**. In various embodiments, the conduits **62032** can direct therapeutic agents and/or bodily fluids as the fluids flow through the tissue thickness compensator **62020**.

In various embodiments, referring to FIG. 170, a tissue thickness compensator **61020** can comprise compensation layers **61022**, such as layers **60122a** and **21022b**, configured to receive staples **30030** deployed from the staple cartridge **20000** (FIG. 169). As a staple **30030** is moved from an initial position to a fired position, the geometry of at least one compensation layer **61022** can guide the staple legs **30032** to

the fired position. In various embodiments, at least one compensation layer **61022** can comprise apertures **61030** extending therethrough, wherein the apertures **61030** can be arranged to receive the staple legs **30032** of deployed staples **30030** when the staples **30030** are fired from the staple cartridge **20000** (FIG. **169**), as described in greater detail herein. In various other embodiments, referring again to FIG. **174**, staple legs **30032** can pierce through at least one compensation layer, such as compensation layer **62022f**; for example, and can be received through apertures **62030** in at least one compensation layer, such as, for example, compensation layer **62022a**.

Referring primarily to FIG. **170**, the tissue thickness compensator **60120** can comprise at least one support tab **61026** on one of the compensation layers **61022a**, **61022b**. The support tab **61026** can protrude into the separation gap **61032** defined between adjacent compensation layers, such as the gap **61032** between the first compensation layer **61020a** and second compensation layer **61020b**. In various embodiments, the support tab **61026** can protrude from a longitudinal side of a first compensation layer **61022a**. Further, the support tab **61026** can extend along the length of the longitudinal side or only along a portion thereof. In various embodiments, at least one support tab **61026** can protrude from two longitudinal sides of the compensation layer **61022a**, **61022b**. Further, adjacently positioned compensation layers **61022a**, **61022b** can comprise corresponding support tabs **61026**, such that the support tab **61026** that extends from the first compensation layer **61022a** can at least partially align with the support tab **61026** that extends from the second compensation layer **61022b**. In at least one embodiment, referring again to FIG. **168**, a tissue thickness compensator **60820** can comprise a limiter plate **60828** between adjacent compensation layers **61022a**, **61022b**. The limiter plate **60828** can be positioned in the gap **61032** defined between the first compensation layer **61022a** and the second compensation layer **61022b**, for example. As described in greater detail herein, support tab(s) **61026** and/or limiter plate(s) **60828** can control the deformation and/or deflection of a support **60124** and/or the compensation layers **61022a**, **61022b**.

As described herein, in various embodiments, the compensation layers **60022** of the tissue thickness compensator **60020** can comprise different materials, geometries and/or dimensions. Such tissue thickness compensators **60020** can be assembled by a variety of manufacturing techniques. Referring primarily to FIG. **159**, the tissue thickness compensator **60022** can be manufactured by lithographic, stereolithographic (SLA), or silk screening processes. For example, a stereolithographic manufacturing process can create a tissue thickness compensator **60020** in which each compensation layer **60022** comprises different materials and/or geometric features. For example, an ultraviolet light in a stereolithography machine can draw the geometry of a first compensation layer **60022**, such that the first compensation layer **60022** comprising a first material, geometry and/or dimensions is cured by the ultraviolet light. The ultraviolet light can subsequently draw the geometry of a second compensation layer **60022**, such that the second compensation layer **60022** comprising a second material, geometry and/or dimensions is cured by the ultraviolet light. In various embodiments, a stereolithography machine can draw compensation layers **60022** on top of each other, side-by-side, or a combination thereof. Further, the compensation layers **60022** can be drawn such that pockets **60132** exist between adjacent compensation layers **60022**. Because a stereolithography machine can create very thin layers having unique geometries, a tissue

thickness compensator **60020** manufactured by a stereolithographic process can comprise a very complex three-dimensional geometry.

In various embodiments, referring to FIG. **169**, the tissue thickness compensator **60920** can be positioned in the end effector **12** of a surgical instrument **10** (FIG. **1**). The tissue thickness compensator **60920** can be positioned relative to the staple cartridge **20000** of the end effector **12**. For example, the tissue thickness compensator **60920** can be releasably secured to the staple cartridge **20000**. In at least one embodiment, at least one compensation layer **60922** of the tissue thickness compensator **60920** can be positioned adjacent to the top deck surface **20011** (FIG. **79**) of the staple cartridge **20000**. For example, a second compensation layer **60922b** can be secured to the top deck surface **20011** by an adhesive or by a wrap, similar to at least one of the wraps described herein (FIG. **16**). In various embodiments, the tissue thickness compensator **60920** can be integral to the staple cartridge **20000** such that the staple cartridge **20000** and the tissue thickness compensator **60920** are formed as a single unit construction. For example, the staple cartridge **20000** can comprise a first body portion, such as the rigid support portion **20010** (FIG. **79**), and a second body portion, such as the tissue thickness compensator **60920**.

Still referring to FIG. **169**, the tissue thickness compensator **60920** can comprise a first compensator portion **60920a** and a second compensator portion **60920b**. The first compensator portion **60920a** can be positioned on a first longitudinal side of the staple cartridge **20000** and the second compensator portion **60920b** can be positioned on a second longitudinal side of the staple cartridge **20000**. In various embodiments, when the tissue thickness compensator **60920** is positioned relative to the staple cartridge **20000**, the longitudinal slot **20015** (FIG. **78**) in the rigid support portion **20010** (FIG. **78**) can extend between the first compensator portion **60920a** and the second compensator portion **60920b**. When the cutting element **20052** on the staple-firing sled **20050** (FIG. **78**) translates through the end effector **12**, the cutting element **20052** can pass through the longitudinal slot **20015** between the first compensator portion **60920a** and the second compensator portion **60920b** without severing a portion of the tissue thickness compensator **60920**, for example. In other embodiments, the cutting element **20052** can be configured to sever a portion of the tissue thickness compensator **60920**.

In various embodiments, referring now to FIG. **162**, a tissue thickness compensator **63020** can be configured to fit in the end effector **12'** of a circular surgical instrument. In various embodiments, the tissue thickness compensator **62030** can comprise a circular first compensation layer **63022a** and a circular second compensation layer **63022b**. The second compensation layer **63022b** can be positioned on a circular top deck surface **20011'** of a circular staple cartridge **20000'**, wherein the second compensation layer **63022b** can comprise a geometry that corresponds to the geometry of the deck surface **20011'**. For example, the deck surface **20011'** can comprise a stepped portion and the second compensation layer **63022b** can comprise a corresponding stepped portion. Similar to various embodiments described herein, the tissue thickness compensator can further comprise at least one support **63024** and/or support tabs **63026**, for example, extending around the tissue thickness compensator **63020**.

Referring again to FIG. **170**, fired staples **30030** can be configured to engage the tissue thickness compensator **60920**. As described throughout the present disclosure, a fired staple **30030** can capture a portion of the tissue thickness compensator **60920** and tissue **T** and apply a compressive force to the tissue thickness compensator **60920**. Further,

referring primarily to FIGS. 171-173, the tissue thickness compensator 60920 can be deformable. In various embodiments, as described herein, a first compensation layer 60920a can be separated from a second compensation layer 60920b by a separation gap 60932. Referring to FIG. 171, prior to compression of the tissue thickness compensator 60920, the gap 60932 can comprise a first distance. When a compressive force A is applied to the tissue thickness compensator 60920 and tissue T, for example, by a fired staple 30030 (FIG. 170), the support 60924 can be configured to deform. Referring now to FIG. 172, the single-bend support beam 60924 can bend under the compressive force A such that the separation gap 60932 between the first compensation layer 60920a and the second compensation layer 60920b is reduced to a second distance. Referring primarily to FIG. 173, the first and second compensation layers 60922a, 60922b can also deform under the compressive force A. In various embodiments, the support tabs 60926 can control deformation of the compensation layers 60920. For example, the support tabs 60926 can prevent excessive bending of the compensation layers 60920 by supporting the longitudinal sides of the compensation layer 60920 when they come into contact with one another. The support tabs 60926 can also be configured to bend or bow under the compressive force A. Additionally or alternatively, the limiter plate 60128 (FIG. 168) described in greater detail herein, can limit the deformation of the compensation layers 60920 when the compensation layers 60920 and/or support tabs 60926 contact the limiter plate 60128.

Furthermore, similar to various tissue thickness compensators described herein, tissue thickness compensator 60920 can generate a springback or restoring force when deformed. The restoring force generated by the deformed tissue thickness compensator can at least depend on the orientation, dimensions, material, and/or geometry of the tissue thickness compensator 60920, as well as the amount of the tissue thickness compensator 60920 that is deformed by the applied force. Furthermore, in various embodiments, at least a portion of the tissue thickness compensator 60920 can be resilient such that the tissue thickness compensator 60920 generates a spring load or restoring force when deformed by a fired staple 30030. In at least one embodiment, the support 60924 can comprise an elastic material and/or at least one compensation layer 60922 can comprise an elastic material such that the tissue thickness compensator 60920 is resilient.

In various embodiments, referring now to FIG. 175, an end effector of a surgical stapling instrument can comprise a first jaw and a second jaw, wherein at least one of the first jaw and the second jaw can be configured to be moved relative to the other. In certain embodiments, the end effector can comprise a first jaw including a staple cartridge channel 19070 and a second jaw including an anvil 19060, wherein the anvil 19060 can be pivoted toward and/or away from the staple cartridge channel 19070, for example. The staple cartridge channel 19070 can be configured to receive a staple cartridge 19000, for example, which, in at least one embodiment, can be removably retained within the staple cartridge channel 19070. In various embodiments, the staple cartridge 19000 can comprise a cartridge body 19010 and a tissue thickness compensator 19020 wherein, in at least one embodiment, the tissue thickness compensator 19020 can be removably attached to the cartridge body 19010. Similar to other embodiments described herein, referring now to FIG. 176, the cartridge body 19010 can comprise a plurality of staple cavities 19012 and a staple 19030 positioned within each staple cavity 19012. Also similar to other embodiments described herein, the staples 19030 can be supported by staple drivers 19040 positioned within the cartridge body 19010 wherein a

sled and/or firing member, for example, can be advanced through the staple cartridge 19000 to lift the staple drivers 19040 upwardly within the staple cavities 19012, as illustrated in FIG. 177, and eject the staples 19030 from the staple cavities 19012.

In various embodiments, referring primarily to FIGS. 175 and 176, the tissue thickness compensator 19020 can comprise resilient members 19022 and a vessel 19024 encapsulating the resilient members 19022. In at least one embodiment, the vessel 19024 can be sealed and can define a cavity containing an inner atmosphere having a pressure which is different than the surrounding atmospheric pressure. In certain embodiments, the pressure of the inner atmosphere can be greater than the pressure of the surrounding atmosphere while, in other embodiments, the pressure of the inner atmosphere can be less than the pressure of the surrounding atmosphere. In the embodiments in which the vessel 19024 contains a pressure less than the pressure of the surrounding atmosphere, the sidewall of the vessel 19024 can enclose a vacuum. In such embodiments, the vacuum can cause the vessel 19024 to distort, collapse, and/or flatten wherein the resilient members 19022 positioned within the vessel 19024 can be resiliently compressed within the vessel 19024. When a vacuum is drawn on the vessel 19024, the resilient members 19022 can deflect or deform downwardly and can be held in position by the sidewalls of the vessel 19024 in a compressed, or vacuum-packed, state.

Resilient member 19022 and vessel 19024 are comprised of biocompatible materials. In various embodiments, resilient member 19022 and/or vessel 19024 can be comprised of bioabsorbable materials such as PLLA, PGA, and/or PCL, for example. In certain embodiments, resilient member 19022 can be comprised of a resilient material. Resilient member 19022 can also comprise structural resilience. For example, resilient member 19022 can be in the form of a hollow tube.

Further to the above, the tissue thickness compensator 19020 can be positioned against or adjacent to the deck surface 19011 of the cartridge body 19010. When the staples 19030 are at least partially fired, referring now to FIG. 177, the legs of the staples 19030 can puncture or rupture the vessel 19024. In certain embodiments, the vessel 19024 can comprise a central portion 19026 which can be positioned over a cutting slot 19016 of the cartridge body 19010 such that, when a cutting member 19080 is advanced to incise tissue T positioned between the staple cartridge 19000 and the anvil 19060, the cutting member 19080 can also incise the central portion 19026 of the vessel 19024 thereby puncturing or rupturing the vessel 19024. In either event, once the vessel 19024 has been ruptured, the inner atmosphere within the vessel 19024 can equalize with the atmosphere surrounding the tissue thickness compensator 19020 and allow the resilient members 19022 to resiliently expand to regain, or at least partially regain, their undistorted and/or unflattened configuration. In such circumstances, the resilient members 19022 can apply a biasing force to the tissue T captured within the deformed staples 19020. More specifically, after being deformed by the forming surfaces of pockets 19062 defined in the anvil 19060, the legs of the staples 19030 can capture tissue T and at least a portion of a resilient member 19022 within the staples 19030 such that, when the vessel 19024 ruptures, the tissue thickness compensator 19020 can compensate for the thickness of the tissue T captured within the staples 19030. For instance, when the tissue T captured within a staple 19030 is thinner, a resilient member 19022 captured within that staple 19030 can expand to fill gaps within the staple 19030 and apply a sufficient compression force to the tissue T. Correspondingly, when the tissue T captured within

a staple 19030 is thicker, a resilient member 19022 captured within that staple 19030 can remain compressed to make room for the thicker tissue within the staple 19030 and, likewise, apply a sufficient compression force to the tissue T.

When the vessel 19024 is punctured, as outlined above, the resilient members 19022 can expand in an attempt to resiliently return to their original configuration. In certain circumstances, the portion of resilient members 19022 that have been captured within the staples 19030 may not be able to return to their original undistorted shape. In such circumstances, the resilient members 19022 can comprise a spring which can apply a compression force to the tissue T captured within the staples 19030. In various embodiments, a resilient member 19022 can emulate a linear spring wherein the compression force applied by the resilient member 19022 is linearly proportional to the amount, or distance, in which the resilient member 19022 remains deflected within the staple 19030. In certain other embodiments, a resilient member 19022 can emulate a non-linear spring wherein the compression force applied by the resilient member 19022 is not linearly proportional to the amount, or distance, in which the resilient member 19022 remains deflected within the staple 19030.

In various embodiments, referring primarily to FIGS. 178 and 179, a staple cartridge 19200 can comprise a tissue thickness compensator 19220 which can comprise one or more sealed vessels 19222 therein. In at least one embodiment, each of the vessels 19222 can be sealed and can contain an inner atmosphere. In certain embodiments, the pressure of the inner atmosphere within a sealed vessel 19222 can exceed atmospheric pressure while, in certain other embodiments, the pressure of the inner atmosphere within a sealed vessel 19222 can be below atmospheric pressure. In embodiments where the pressure of the inner atmosphere within a vessel 19222 is below atmospheric pressure, the vessel 19222 can be described as containing a vacuum. In various embodiments, one or more of the vessels 19222 can be wrapped or contained in an outer shroud, container, wrap, and/or film 19224, for example, wherein the tissue thickness compensator 19220 can be positioned above a deck surface 19011 of the cartridge body 19010. In certain embodiments, each vessel 19222 can be manufactured from a tube having a circular, or an at least substantially circular, cross-section, for example, having a closed end and an open end. A vacuum can be drawn on the open end of the tube and, when a sufficient vacuum has been reached within the tube, the open end can be closed and sealed. In at least one such embodiment, the tube can be comprised of a polymeric material, for example, wherein the open end of the tube can be heat staked in order to close and seal the same. In any event, the vacuum within each vessel 19222 can pull the sidewalls of the tube inwardly and resiliently distort and/or flatten the tube. The vessels 19222 are illustrated in an at least partially flattened state in FIG. 179.

When the staples 19030 are in their unfired position, as illustrated in FIG. 179, the tips of the staples 19030 can be positioned below the tissue thickness compensator 19220. In at least one such embodiment, the staples 19030 can be positioned within their respective staple cavities 19012 such that the staples 19030 do not contact the vessels 19222 until the staples 19030 are moved from the unfired positions, illustrated in FIG. 179, to their fired positions, illustrated in FIG. 180. In certain embodiments, the wrap 19224 of the tissue thickness compensator 19220 can protect the vessels 19222 from being prematurely punctured by the staples 19030. When the staples 19030 are at least partially fired, referring now to FIG. 180, the legs of the staples 19030 can puncture or rupture the vessels 19222. In such circumstances, the inner

atmospheres within the vessels 19222 can equalize with the atmosphere surrounding the vessels 19222 and resiliently expand to regain, or at least partially regain, their undistorted and/or unflattened configuration. In such circumstances, the punctured vessels 19222 can apply a biasing force to the tissue captured within the deformed staples 19030. More specifically, after being deformed by the forming surfaces of pockets 19062 defined in the anvil 19060, the legs of the staples 19030 can capture tissue T and at least a portion of a vessel 19222 within the staples 19030 such that, when the vessels 19222 rupture, the vessels 19222 can compensate for the thickness of the tissue T captured within the staples 19030. For instance, when the tissue T captured within a staple 19030 is thinner, a vessel 19222 captured within that staple 19030 can expand to fill gaps within the staple 19030 and, concurrently, apply a sufficient compression force to the tissue T. Correspondingly, when the tissue T captured within a staple 19030 is thicker, a vessel 19222 captured within that staple 19030 can remain compressed to make room for the thicker tissue within the staple 19030 and, concurrently, apply a sufficient compression force to the tissue T.

When the vessels 19222 are punctured, as outlined above, the vessels 19222 can expand in an attempt to resiliently return to their original configuration. The portion of vessels 19222 that have captured within the staples 19030 may not be able to return to their original undistorted shape. In such circumstances, the vessel 19222 can comprise a spring which can apply a compression force to the tissue T captured within the staples 19030. In various embodiments, a vessel 19222 can emulate a linear spring wherein the compression force applied by the vessel 19222 is linearly proportional to the amount, or distance, in which the vessel 19222 remains deflected within the staple 19030. In certain other embodiments, a vessel 19222 can emulate a non-linear spring wherein the compression force applied by the vessel 19222 is not linearly proportional to the amount, or distance, in which the vessel 19222 remains deflected within the staple 19030. In various embodiments, the vessels 19222 can be hollow and, in at least one embodiment, empty when they are in their sealed configuration. In certain other embodiments, each of the vessels 19222 can define a cavity and can further include at least one medicament contained therein. In at least some embodiments, the vessels 19222 can be comprised of at least one medicament which can be released and/or bioabsorbed, for example.

In various embodiments, the vessels 19222 of the tissue thickness compensator 19220 can be arranged in any suitable manner. As illustrated in FIG. 178, the staple cavities 19012 defined in the cartridge body 19010, and the staples 19030 positioned in the staple cavities 19012, can be arranged in rows. In at least the illustrated embodiment, the staple cavities 19012 can be arranged in six longitudinal, linear rows, for example; however, any suitable arrangement of staple cavities 19012 could be utilized. As also illustrated in FIG. 178, the tissue thickness compensator 19220 can comprise six vessels 19222 wherein each of the vessels 19222 can be aligned with, or positioned over, a row of staple cavities 19012. In at least one embodiment, each of the staples 19030 within a row of staple cavities 19012 can be configured to puncture the same vessel 19222. In certain situations, some of the staple legs of the staples 19030 may not puncture the vessel 19222 positioned thereover; however, in embodiments where the vessel 19222 defines a continuous internal cavity, for example, the cavity can be sufficiently punctured by at least one of the staples 19030 in order to allow the pressure of the internal cavity atmosphere to equalize with the atmospheric pressure surrounding the vessel 19222. In various

embodiments, referring now to FIG. 185, a tissue thickness compensator can comprise a vessel, such as vessel 19222', for example, which can extend in a direction which is transverse to a line of staples 19030. In at least one such embodiment, a vessel 19222' can extend across multiple staple rows. In certain embodiments, referring now to FIG. 186, a tissue thickness compensator 19220" can comprise a plurality of vessels 19222" which extend in a direction which is perpendicular, or at least substantially perpendicular, to a line of staples 19030. In at least one such embodiment, some of the vessels 19222" may be punctured by the staples 19030 while others may not be punctured by the staples 19030. In at least one embodiment, the vessels 19222" can extend across or through a cutting path in which a cutting member could transect and rupture the vessels 19222", for example.

In various embodiments, as described above, a tissue thickness compensator, such as tissue thickness compensator 19220, for example, can comprise a plurality of sealed vessels, such as vessels 19222, for example. As also described above, each of the sealed vessels 19222 can comprise a separate internal atmosphere. In certain embodiments, the vessels 19222 can have different internal pressures. In at least one embodiment, for example, a first vessel 19222 can comprise an internal vacuum having a first pressure and a second vessel 19222 can comprise an internal vacuum having a second, different pressure, for example. In at least one such embodiment, the amount of distortion or flattening of a vessel 19222 can be a function of the vacuum pressure of the internal atmosphere contained therein. For instance, a vessel 19222 having a greater vacuum can be distorted or flattened a greater amount as compared to a vessel 19222 having a smaller vacuum. In certain embodiments, the cavity of a vessel can be segmented into two or more separate, sealed cavities wherein each separate, sealed cavity can comprise a separate internal atmosphere. In at least one such embodiment, some of the staples within a staple row can be configured and arranged to puncture a first cavity defined in the vessel while other staples within the staple row can be configured and arranged to puncture a second cavity defined in the vessel, for example. In such embodiments, especially in embodiments in which the staples in a staple row are sequentially fired from one end of the staple row to the other, as described above, one of the cavities can remain intact and can maintain its internal atmosphere when another cavity is ruptured. In certain embodiments, the first cavity can have an inner atmosphere having a first vacuum pressure and the second cavity can have an inner atmosphere having a second, different vacuum pressure, for example. In various embodiments, a cavity that remains intact can maintain its inner pressure until the vessel is bioabsorbed thereby creating a timed pressure release.

In various embodiments, referring now to FIGS. 181 and 182, a tissue thickness compensator, such as tissue thickness compensator 19120, for example, can be attached to an anvil 19160. Similar to the above, the tissue thickness compensator 19120 can comprise a vessel 19124 and a plurality of resilient members 19122 positioned therein. Also similar to the above, the vessel 19124 can define a cavity containing an inner atmosphere having a pressure which is less than or greater than the pressure of the atmosphere surrounding the tissue thickness compensator 19120. In embodiments where the inner atmosphere within the vessel 19124 comprises a vacuum, the vessel 19124 and the resilient members 19122 positioned therein can be distorted, collapsed, and/or flattened by the difference in pressure between the vacuum in the vessel 19124 and the atmospheric pressure outside of the vessel 19124. In use, the anvil 19160 can be moved into a closed position in which it is positioned opposite a staple

cartridge 19100 and in which a tissue engaging surface 19121 on the vessel 19124 can engage the tissue T positioned intermediate the tissue thickness compensator 19120 and a staple cartridge 19100. In use, the firing member 19080 can be advanced distally to fire the staples 19030, as described above, and, at the same time, incise the tissue T. In at least one embodiment, the tissue thickness compensator 19120 can further comprise an intermediate portion 19126 which can be aligned with a cutting slot defined in the anvil 19160 wherein, when the firing member 19080 is advanced distally through the tissue thickness compensator 19120, the firing member 19080 can puncture or rupture the vessel 19124. Also, similar to the above, the firing member 19080 can lift the staple drivers 19040 upwardly and fire the staples 19030 such that the staples 19030 can contact the anvil 19160 and be deformed into their deformed configuration, as illustrated in FIG. 183. When the staples 19030 are fired, the staples 19030 can pierce the tissue T and then pierce or rupture the vessel 19124 such that the resilient members 19122 positioned within the vessel 19124 can at least partially expand, as outlined above.

In various embodiments, further to the above, a tissue thickness compensator can be comprised of a biocompatible material. The biocompatible material, such as, a foam, may comprise tackifiers, surfactants, fillers, cross-linkers, pigments, dyes, antioxidants and other stabilizers and/or combinations thereof to provide desired properties to the material. In certain embodiments, a biocompatible foam may comprise a surfactant. The surfactant may be applied to the surface of the material and/or dispersed within the material. Without wishing to be bound to any particular theory, the surfactant applied to the biocompatible material may reduce the surface tension of the fluids contacting the material. For example, the surfactant may reduce the surface tension of water contacting the material to accelerate the penetration of water into the material. In various embodiments, the water may act as a catalyst. The surfactant may increase the hydrophilicity of the material.

In various embodiments, the surfactant may comprise an anionic surfactant, a cationic surfactant, and/or a non-ionic surfactant. Examples surfactants include, but are not limited to polyacrylic acid, methalose, methyl cellulose, ethyl cellulose, propyl cellulose, hydroxy ethyl cellulose, carboxy methyl cellulose, polyoxyethylene cetyl ether, polyoxyethylene lauryl ether, polyoxyethylene octyl ether, polyoxyethylene octylphenyl ether, polyoxyethylene oleyl ether, polyoxyethylene sorbitan monolaurate, polyoxyethylene stearyl ether, polyoxyethylene nonylphenyl ether, dialkylphenoxy poly(ethyleneoxy)ethanol, and polyoxamers, and combinations thereof. In at least one embodiment, the surfactant may comprise a copolymer of polyethylene glycol and polypropylene glycol. In at least one embodiment, the surfactant may comprise a phospholipid surfactant. The phospholipid surfactant may provide antibacterial stabilizing properties and/or disperse other materials in the biocompatible material. In various embodiments, the tissue thickness compensator may comprise at least one medicament. The tissue thickness compensator may comprise one or more of the natural materials, non-synthetic materials, and/or synthetic materials described herein. In certain embodiments, the tissue thickness compensator may comprise a biocompatible foam comprising gelatin, collagen, hyaluronic acid, oxidized regenerated cellulose, polyglycolic acid, polycaprolactone, polylactic acid, polydioxanone, polyhydroxyalkanoate, poliglecaprone, and combinations thereof. In certain embodiments, the tissue thickness compensator may comprise a film comprising the at least one medicament. In certain embodiments, the tissue thick-

ness compensator may comprise a biodegradable film comprising the at least one medicament. In certain embodiments, the medicament may comprise a liquid, gel, and/or powder. In various embodiments, the medicaments may comprise anti-cancer agents, such as, for example, cisplatin, mitomycin, and/or adriamycin.

In various embodiments, the tissue thickness compensator may comprise a biodegradable material to provide controlled elution of the at least one medicament as the biodegradable material degrades. In various embodiments, the biodegradable material may degrade may decompose, or loses structural integrity, when the biodegradable material contacts an activator, such as, for example an activator fluid. In various embodiments, the activator fluid may comprise saline or any other electrolyte solution, for example. The biodegradable material may contact the activator fluid by conventional techniques, including, but not limited to spraying, dipping, and/or brushing. In use, for example, a surgeon may dip an end effector and/or a staple cartridge comprising the tissue thickness compensator comprising the at least one medicament into an activator fluid comprising a salt solution, such as sodium chloride, calcium chloride, and/or potassium chloride. The tissue thickness compensator may release the medicament as the tissue thickness compensator degrades. In certain embodiments, the elution of the medicament from the tissue thickness compensator may be characterized by a rapid initial elution rate and a slower sustained elution rate.

In various embodiments, a tissue thickness compensator, for example, can be comprised of a biocompatible material which may comprise an oxidizing agent. In various embodiments, the oxidizing agent may be an organic peroxide and/or an inorganic peroxide. Examples of oxidizing agents may include, but are not limited to, hydrogen peroxide, urea peroxide, calcium peroxide, and magnesium peroxide, and sodium percarbonate. In various embodiments, the oxidizing agent may comprise peroxygen-based oxidizing agents and hypochlorite-based oxidizing agents, such as, for example, hydrogen peroxide, hypochlorous acid, hypochlorites, hypochlorites, and percarbonates. In various embodiments, the oxidizing agent may comprise alkali metal chlorites, hypochlorites and perborates, such as, for example, sodium chlorite, sodium hypochlorite and sodium perborate. In certain embodiments, the oxidizing agent may comprise vanadate. In certain embodiments, the oxidizing agent may comprise ascorbic acid. In certain embodiments, the oxidizing agent may comprise an active oxygen generator. In various embodiments, a tissue scaffold may comprise the biocompatible material comprising an oxidizing agent.

In various embodiments, the biocompatible material may comprise a liquid, gel, and/or powder. In certain embodiments, the oxidizing agent may comprise microparticles and/or nanoparticles, for example. For example, the oxidizing agent may be milled into microparticles and/or nanoparticles. In certain embodiments, the oxidizing agent may be incorporated into the biocompatible material by suspending the oxidizing agent in a polymer solution. In certain embodiments, the oxidizing agent may be incorporated into the biocompatible material during the lyophilization process. After lyophilization, the oxidizing agent may be attached to the cell walls of the biocompatible material to interact with the tissue upon contact. In various embodiments, the oxidizing agent may not be chemically bonded to the biocompatible material. In at least one embodiment, a percarbonate dry power may be embedded within a biocompatible foam to provide a prolonged biological effect by the slow release of oxygen. In at least one embodiment, a percarbonate dry power may be embedded within a polymeric fiber in a non-woven structure

to provide a prolonged biological effect by the slow release of oxygen. In various embodiments, the biocompatible material may comprise an oxidizing agent and a medicament, such as, for example, doxycycline and ascorbic acid.

In various embodiments, the biocompatible material may comprise a rapid release oxidizing agent and/or a slower sustained release oxidizing agent. In certain embodiments, the elution of the oxidizing agent from the biocompatible material may be characterized by a rapid initial elution rate and a slower sustained elution rate. In various embodiments, the oxidizing agent may generate oxygen when the oxidizing agent contacts bodily fluid, such as, for example, water. Examples of bodily fluids may include, but are not limited to, blood, plasma, peritoneal fluid, cerebral spinal fluid, urine, lymph fluid, synovial fluid, vitreous fluid, saliva, gastrointestinal luminal contents, and/or bile. Without wishing to be bound to any particular theory, the oxidizing agent may reduce cell death, enhance tissue viability and/or maintain the mechanical strength of the tissue to tissue that may be damaged during cutting and/or stapling. In various embodiments, the biocompatible material may comprise at least one microparticle and/or nanoparticle. The biocompatible material may comprise one or more of the natural materials, non-synthetic materials, and synthetic materials described herein. In various embodiments, the biocompatible material may comprise particles having a mean diameter of about 10 nm to about 100 nm and/or about 10 μ m to about 100 μ m, such as, for example, 45-50 nm and/or 45-50 μ m. In various embodiments, the biocompatible material may comprise biocompatible foam comprising at least one microparticle and/or nanoparticle embedded therein. The microparticle and/or nanoparticle may not be chemically bonded to the biocompatible material. The microparticle and/or nanoparticle may provide controlled release of the medicament. In certain embodiments, the microparticle and/or nanoparticle may comprise at least one medicament. In certain embodiments, the microparticle and/or nanoparticle may comprise a hemostatic agent, an anti-microbial agent, and/or an oxidizing agent, for example. In certain embodiments, the tissue thickness compensator may comprise a biocompatible foam comprising a hemostatic agent comprising oxidized regenerated cellulose, an anti-microbial agent comprising doxycycline and/or Gentamicin, and/or an oxidizing agent comprising a percarbant. In various embodiments, the microparticle and/or nanoparticle may provide controlled release of the medicament up to three days, for example.

In various embodiments, the microparticle and/or nanoparticle may be embedded in the biocompatible material during a manufacturing process. For example, a biocompatible polymer, such as, for example, a PGA/PCL, may contact a solvent, such as, for example, dioxane to form a mixture. The biocompatible polymer may be ground to form particles. Dry particles, with or without ORC particles, may be contacted with the mixture to form a suspension. The suspension may be lyophilized to form a biocompatible foam comprising PGA/PCL having dry particles and/or ORC particles embedded therein.

In various embodiments, the tissue thickness compensators or layers disclosed herein can be comprised of an absorbable polymer, for example. In certain embodiments, a tissue thickness compensator can be comprised of foam, film, fibrous woven, fibrous non-woven PGA, PGA/PCL (Poly (glycolic acid-co-caprolactone)), PLA/PCL (Poly(lactic acid-co-polycaprolactone)), PLLA/PCL, PGA/TMC (Poly (glycolic acid-co-trimethylene carbonate)), PDS, PEPBO or other absorbable polyurethane, polyester, polycarbonate, Polyorthoesters, Polyanhydrides, Polyesteramides, and/or

Polyoxaesters, for example. In various embodiments, a tissue thickness compensator can be comprised of PGA/PLA (Poly (glycolic acid-co-lactic acid)) and/or PDS/PLA (Poly(p-dioxanone-co-lactic acid)), for example. In various embodiments, a tissue thickness compensator can be comprised of an organic material, for example. In certain embodiments, a tissue thickness compensator can be comprised of Carboxymethyl Cellulose, Sodium Alginate, Cross-linked Hyaluronic Acid, and/or Oxidized regenerated cellulose, for example. In various embodiments, a tissue thickness compensator can comprise a durometer in the 3-7 Shore A (30-50 Shore OO) ranges with a maximum stiffness of 15 Shore A (65 Shore OO), for example. In certain embodiments, a tissue thickness compensator can undergo 40% compression under 3 lbf load, 60% compression under 6 lbf load, and/or 80% compression under 20 lbf load, for example. In certain embodiments, one or more gasses, such as air, nitrogen, carbon dioxide, and/or oxygen, for example, can be bubbled through and/or contained within the tissue thickness compensator. In at least one embodiment, a tissue thickness compensator can comprise beads therein which comprise between approximately 50% and approximately 75% of the material stiffness comprising the tissue thickness compensator.

In various embodiments, a tissue thickness compensator can comprise hyaluronic acid, nutrients, fibrin, thrombin, platelet rich plasma, Sulfasalazine (Azulfidine®-5ASA+Sulfapyridine diazo bond)-prodrug-colonic bacterial (Azoreductase), Mesalamine (5ASA with different prodrug configurations for delayed release), Asacol® (5ASA+Eudragit-S coated-pH>7 (coating dissolution)), Pentasa® (5ASA+ethylcellulose coated-time/pH dependent slow release), Mesasal® (5ASA+Eudragit-L coated-pH>6), Olsalazine (5ASA+5ASA-colonic bacterial (Azoreductase)), Balsalazide (5ASA+4-Aminobenzoyl-B-alanine)-colonic bacterial (Azoreductase)), Granulated mesalamine, Lialda (delay and SR formulation of mesalamine), HMPL-004 (herbal mixture that may inhibit TNF-alpha, interleukin-1 beta, and nuclear-kappa B activation), CCX282-B (oral chemokine receptor antagonist that interferes with trafficking of T lymphocytes into the intestinal mucosa), Rifaximin (nonabsorbable broad-spectrum antibiotic), Infliximab, murine chymieric (monoclonal antibody directed against TNF-alpha-approved for reducing signs/symptoms and maintaining clinical remission in adult/pediatric patients with moderate/severe luminal and fistulizing Crohn's disease who have had inadequate response to conventional therapy), Adalimumab, Total Human IgG1 (anti-TNF-alpha monoclonal antibody-approved for reducing signs/symptoms of Crohn's disease, and for the induction and maintenance of clinical remission in adult patients with moderate/severe active Crohn's disease with inadequate response to conventional therapies, or who become intolerant to Infliximab), Certolizumab pegoll, humanized anti-TNF FAB' (monoclonal antibody fragment linked to polyethylene glycol-approved for reducing signs/symptoms of Crohn's disease and for the induction and maintenance of response in adult patients w/moderate/severe disease with inadequate response to conventional therapies), Natalizumab, First non-TNF-alpha inhibitor (biologic compound approved for Crohn's disease), Humanized monoclonal IgG4 antibody (directed against alpha-4 integrin-FDA approved for inducing and maintaining clinical response and remission in patients with moderate/severe disease with evidence of inflammation and who have had inadequate response to or are unable to tolerate conventional Crohn's therapies and inhibitors of TNF-alpha), concomitant Immunomodulators potentially given with Infliximab, Azathioprine 6-Mercaptopurine (purine synthesis

inhibitor-prodrug), Methotrexate (binds dihydrofolate reductase (DHFR) enzyme that participates in tetrahydrofolate synthesis, inhibits all purine synthesis), Allopurinol and Thioprine therapy, PPI, H2 for acid suppression to protect the healing line, C-Diff-Flagyl, Vancomycin (fecal translocation treatment; probiotics; repopulation of normal endoluminal flora), and/or Rifaximin (treatment of bacterial overgrowth (notably hepatic encephalopathy); not absorbed in GI tract with action on intraluminal bacteria), for example.

As described herein, a tissue thickness compensator can compensate for variations in the thickness of tissue that is captured within the staples ejected from a staple cartridge and/or contained within a staple line, for example. Stated another way, certain staples within a staple line can capture thick portions of the tissue while other staples within the staple line can capture thin portions of the tissue. In such circumstances, the tissue thickness compensator can assume different heights or thicknesses within the staples and apply a compressive force to the tissue captured within the staples regardless of whether the captured tissue is thick or thin. In various embodiments, a tissue thickness compensator can compensate for variations in the hardness of the tissue. For instance, certain staples within a staple line can capture highly compressible portions of the tissue while other staples within the staple line can capture portions of the tissue which are less compressible. In such circumstances, the tissue thickness compensator can be configured to assume a smaller height within the staples that have captured tissue having a lower compressibility, or higher hardness, and, correspondingly, a larger height within the staples that have captured tissue having a higher compressibility, or lower hardness, for example. In any event, a tissue thickness compensator, regardless of whether it compensates for variations in tissue thickness and/or variations in tissue hardness, for example, can be referred to as a 'tissue compensator' and/or as a 'compensator', for example.

The devices disclosed herein can be designed to be disposed of after a single use, or they can be designed to be used multiple times. In either case, however, the device can be reconditioned for reuse after at least one use. Reconditioning can include any combination of the steps of disassembly of the device, followed by cleaning or replacement of particular pieces, and subsequent reassembly. In particular, the device can be disassembled, and any number of the particular pieces or parts of the device can be selectively replaced or removed in any combination. Upon cleaning and/or replacement of particular parts, the device can be reassembled for subsequent use either at a reconditioning facility, or by a surgical team immediately prior to a surgical procedure. Those skilled in the art will appreciate that reconditioning of a device can utilize a variety of techniques for disassembly, cleaning/replacement, and reassembly. Use of such techniques, and the resulting reconditioned device, are all within the scope of the present application.

Preferably, the invention described herein will be processed before surgery. First, a new or used instrument is obtained and if necessary cleaned. The instrument can then be sterilized. In one sterilization technique, the instrument is placed in a closed and sealed container, such as a plastic or TYVEK bag. The container and instrument are then placed in a field of radiation that can penetrate the container, such as gamma radiation, x-rays, or high-energy electrons. The radiation kills bacteria on the instrument and in the container. The sterilized instrument can then be stored in the sterile container. The sealed container keeps the instrument sterile until it is opened in the medical facility.

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Any patent, publication, or other disclosure material, in whole or in part, that is said to be incorporated by reference herein is incorporated herein only to the extent that the incorporated materials does not conflict with existing definitions, statements, or other disclosure material set forth in this disclosure. As such, and to the extent necessary, the disclosure as explicitly set forth herein supersedes any conflicting material incorporated herein by reference. Any material, or portion thereof, that is said to be incorporated by reference herein, but which conflicts with existing definitions, statements, or other disclosure material set forth herein will only be incorporated to the extent that no conflict arises between that incorporated material and the existing disclosure material.

While this invention has been described as having exemplary designs, the present invention may be further modified within the spirit and scope of the disclosure. This application is therefore intended to cover any variations, uses, or adaptations of the invention using its general principles. Further, this application is intended to cover such departures from the present disclosure as come within known or customary practice in the art to which this invention pertains.

What is claimed is:

1. A fastener cartridge assembly for a surgical instrument, the fastener cartridge assembly comprising:

- a cartridge body comprising a longitudinal row of fastener cavities;
- a deformable tube positioned relative to said cartridge body, wherein said deformable tube comprises a resilient material, and wherein said deformable tube comprises:
 - a top portion;
 - a bottom portion;
 - a first end;
 - a second end; and
 - a tubular channel intermediate said top portion and said bottom portion and extending between said first end and said second end, wherein said top portion and said bottom portion are positioned above said cartridge body; and
- a fastener moveable between an initial position and a fired position, wherein said fastener is positioned in a fastener cavity in said row of fastener cavities when said fastener is in said initial position, and wherein said fastener is configured to engage a portion of said deformable tube when said fastener is moved to said fired position.

2. The fastener cartridge assembly of claim 1, wherein said cartridge body further comprises a deck, wherein said deformable tube overlies at least a portion of said longitudinal row of fastener cavities.

3. The fastener cartridge assembly of claim 2, wherein said deformable tube is positioned adjacent to said deck of said cartridge body.

4. The fastener cartridge assembly of claim 2, wherein said cartridge body comprises a plurality of substantially parallel rows of fastener cavities, wherein said plurality of substantially parallel rows of fastener cavities comprises said longitudinal row of fastener cavities, and wherein said cartridge body further comprises:

- a slot extending between two said substantially parallel rows of fastener cavities; and
- a cutting element configured to translate within said slot, wherein at least a portion of said deformable tube overlies said slot such that said cutting element is configured to cut at least a portion of said deformable tube.

5. The fastener cartridge assembly of claim 2, wherein said deformable tube comprises a first deformable tube, wherein the fastener cartridge assembly further comprises a second

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deformable tube, wherein said second deformable tube is substantially parallel to said first deformable tube.

6. The fastener cartridge assembly of claim 5, wherein said second deformable tube is positioned within said first deformable tube.

7. The fastener cartridge assembly of claim 6, further comprising a third deformable tube, wherein said third deformable tube is positioned within said second deformable tube.

8. The fastener cartridge assembly of claim 5, further comprising a third deformable tube, wherein said first deformable tube is aligned with a longitudinal axis defined by said cartridge body, wherein said second deformable tube is positioned on a first side of said first deformable tube, and wherein said third deformable tube is positioned on a second side of said first deformable tube.

9. The fastener cartridge assembly of claim 5, wherein said first deformable tube and said second deformable tube are coextruded with an adjoining portion to form a single piece.

10. The fastener cartridge assembly of claim 1, wherein said deformable tube comprises a lattice of strands woven together to form a tube wall.

11. The fastener cartridge assembly of claim 10, wherein said lattice of strands comprises tubular strands.

12. The fastener cartridge assembly of claim 10, wherein said lattice of strands comprises bioabsorbable strands.

13. The fastener cartridge assembly of claim 10, wherein said deformable tube further comprises a non-porous tube positioned one of outside and inside said lattice of strands, and wherein said non-porous tube is coextruded with said lattice of strands.

14. The fastener cartridge assembly of claim 13, wherein said lattice of strands is at least partially filled with a therapeutic agent to treat tissue.

15. A fastener cartridge for a surgical instrument, the fastener cartridge comprising:

- a cartridge body defining a longitudinal axis;
- a first plurality of strands woven into a resilient lattice, wherein said resilient lattice is substantially parallel to said longitudinal axis, and wherein said resilient lattice comprises:
 - a top wall;
 - a bottom wall; and
 - a channel intermediate said top wall and said bottom wall, wherein said top wall and said bottom wall are positioned above said cartridge body; and
- fasteners moveable between an initial position and a fired position, wherein at least one said fastener is configured to compress a portion of said resilient lattice when said at least one fastener is moved to said fired position.

16. The fastener cartridge of claim 15, wherein said resilient lattice comprises a first resilient lattice, wherein said fastener cartridge further comprises a second plurality of strands woven into a second resilient lattice, wherein said second resilient lattice is substantially parallel to said longitudinal axis, and wherein at least one of said first plurality of strands and said second plurality of strands comprises tubular strands.

17. An end effector assembly for a surgical instrument, the end effector assembly comprising:

- an anvil;
- a fastener cartridge, comprising:
 - at least one row of fastener cavities; and
 - fasteners moveable between an initial position and a fired position, wherein each said fastener is positioned in a said fastener cavity when each said fastener is in said initial position; and

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a tube, wherein said tube comprises a resilient material, wherein said tube is substantially parallel to said at least one row of fastener cavities, and wherein said tube comprises:

a top portion;

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a bottom portion; and

a tubular passage intermediate said top portion and said bottom portion, wherein said top portion and said bottom portion are positioned between said anvil and said fastener cartridge;

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wherein at least one said fastener, when moved to said fired position, is configured to deform a portion of said tube.

18. The end effector assembly of claim **17**, wherein said tube comprises a therapeutic agent to treat tissue.

19. The end effector assembly of claim **18**, wherein said tube is bioabsorbable such that said tube releases said therapeutic agent as said tube is being bioabsorbed.

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20. The end effector assembly of claim **18**, further comprising a cutting element configured to translate along at least a portion of a slot in said fastener cartridge, wherein at least one of said cutting element and said fasteners is configured to penetrate said tube such that said therapeutic agent is released from said tube.

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